

Early integration of a bone plug in the femoral tunnel in rectangular tunnel ACL reconstruction with a bone-patellar tendon-bone graft: a prospective computed tomography analysis

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Abstract

Purpose The purpose of this prospective study was to evaluate how early the bone plug was integrated into the rectangular femoral tunnel after anatomical ACL reconstruction using a bone-patellar tendon-bone (BTB) graft via a rectangular tunnel (RT BTB ACL-R).

Methods Twenty consecutive patients who had undergone the reconstruction procedure were evaluated by CT scans at 4 and 8 weeks postoperatively. In each scan, 30 slices for multiplanar reconstruction were collected parallel to the long axis of the parallelepiped femoral tunnel and perpendicular to the tendinous plane of the bone plug. Each slice was classified as “complete,” indicating no visible gap between the plug and the tunnel wall or trabecular continuity or “incomplete,” showing a visible gap. Bone plug-tunnel integration was evaluated as “excellent,” “good,” “fair,” or “poor” for >20, 11–20, 5–10, and <4 “complete” slices, respectively.

Results In this evaluation, 55% of the patients were rated as “excellent” on the first scan, and 80% were “excellent”

on the second scan, showing healing over time. The CT values at the anterior interface between the bone plug and the tunnel wall were also measured on both scans. The mean changes in CT value at 8 weeks were significantly lower than those at 4 weeks.

Conclusion This study shows that bone plug-femoral tunnel integration was almost complete by 8 weeks after surgery using RT BTB ACL-R.

Keywords ACL reconstruction · Bone-patellar tendon-bone (BTB) graft · Rectangular tunnel · Bone plug-tunnel integration · CT value · Direct bone healing

Introduction

Secure graft fixation with a proper femoral tunnel is an important factor in ACL reconstruction, especially in the early postoperative period [3, 13, 16]. Shino et al recently developed an innovative operative procedure in which a BTB graft is placed to mimic the natural fiber arrangement of the normal ACL following the concept of double-bundle reconstruction, with the additional goal of maximizing the graft-tunnel contact area [25, 26]. Thus, a parallelepiped femoral tunnel with a rectangular aperture is created in accordance with the rectangular cross section of the graft. This method seems to be beneficial for graft-bone integration in the femoral tunnel.

In principle, a wider interface and closer contact is likely to lead to earlier bone plug integration, but it is difficult to determine the period required for the grafted bone to integrate into the tunnel postoperatively. The time period for graft-tunnel integration has been examined in conventional round tunnel ACL reconstruction [7, 9, 14] but has not been studied in detail in rectangular tunnel ACL

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reconstruction. Our hypothesis was that the bone plug could be integrated into the rectangular femoral tunnel in early postoperative stage after RT BTB ACL reconstruction. Thus, this prospective study was to evaluate minute changes in bone plug integration using macroscopic analysis of slices from CT-MPR images and to examine macroscopically undetectable changes using CT values.

Materials and methods

Twenty consecutive patients (19 men; 1 woman) of the average age of 21 years old (range, 16–36) were included in the study. The average time from injury to surgery was 124 days (range, 7–376). All subjects gave informed consent prior to participating in the study.

Surgical technique and postoperative regimen

The details of the RT BTB ACL-R procedure have been described previously [25, 26] (Fig. 1). All patients underwent arthroscopic primary RT BTB ACL-R performed by one orthopedic surgeon (K.S.). Briefly, a 10-mm-wide BTB graft was harvested from the central portion of the patellar tendon with 15-mm-long bone plugs on both ends. The tibial bone plug was shaped to a size of $5 \times 10 \times 15$ mm (thickness \times width \times length) and used for the femoral socket (Fig. 1).

Viewing the ACL femoral attachment area with a 45°C oblique arthroscope through the AM portal, the fibrous tissue is delicately removed using radiofrequency device with the knee flexed at $75\text{--}80^\circ\text{C}$ by gravity. After cleaning, an almost linear “resident’s ridge” was consistently visualized on the wall (Fig. 1a). Since this ridge forms as the

anterior border of the attachment area, the crescent-shaped attachment area is clearly delineated [8, 11, 27]. A $5 \times 10 \times 20$ mm rectangular parallelepiped socket was created with an inside-out dilator posterior to the resident’s ridge [1] (Fig. 1b) (SNE#6901100 femoral dilator 5_10, Ref #6901100; Smith & Nephew Endoscopy).

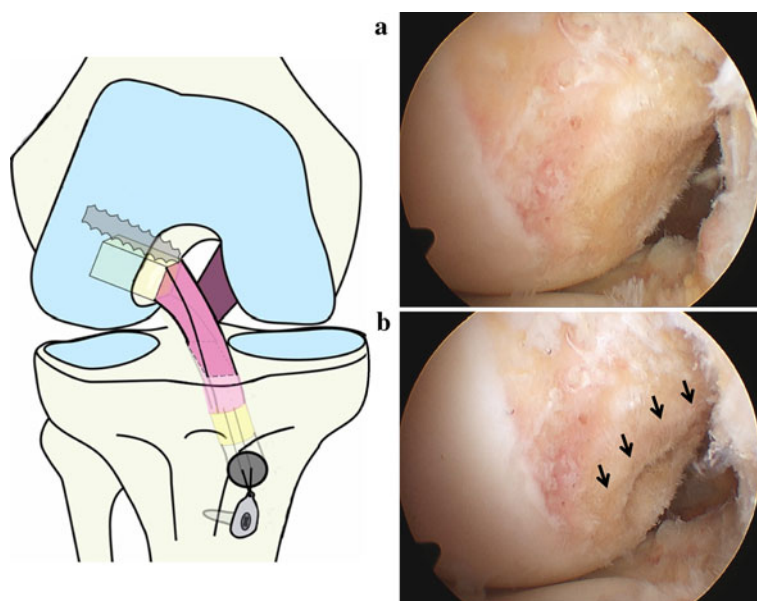
With two leading sutures, the graft was passed from the tibial tunnel to the femoral socket with the parallelepiped bone plug kept on top and the cancellous bone surface maintained anteriorly (Fig. 2). Femoral graft fixation with a $6 \text{ mm} \times 20\text{--}30$ mm interference screw was achieved in an outside-in fashion using a 7-mm skin protector (SNE#6901106) through an additional small lateral femoral incision. Tibial fixation was achieved with a modified pullout suture technique using the DSP (Double Spike Plate, made by Meira Co., Aichi, Japan, and distributed by SNE) system to fix the graft under a predetermined amount of tension [23].

Postoperatively, the knee was immobilized in $10\text{--}15^\circ\text{C}$ for a week with a brace. Partial weight bearing was allowed at 2 weeks, followed by full weight bearing at 4 weeks.

Radiographic analysis

The patients underwent multi-detector computed tomography (MDCT) with multiplanar reconstruction (MPR) using an Asteion 4 Multislice CT System (Toshiba Medical Systems, Tochigi, Japan) at 3–5 weeks and 7–8 weeks postoperatively. Each CT scan was performed with the following parameters: 512×512 matrix, 1.00 mm slice thickness, 120 kVp, and 150 mA. Volume data were saved with a DICOM pattern and imaging software (Virtual Place-M; AZE Ltd., Tokyo Japan) was used to create MPR

Fig. 1 The surgical procedure of rectangular BPTB-ACL reconstruction under a clear view with an oblique arthroscope through the anteromedial portal with the knee in 90°C of flexion, the bony surface undulation around the ACL attachment area is clearly observed (a). The created 5-mm-wide, 10-mm-long, 20-mm-deep parallelepiped socket inside the attachment area. Note the “resident’s ridge” (solid arrows) (b)



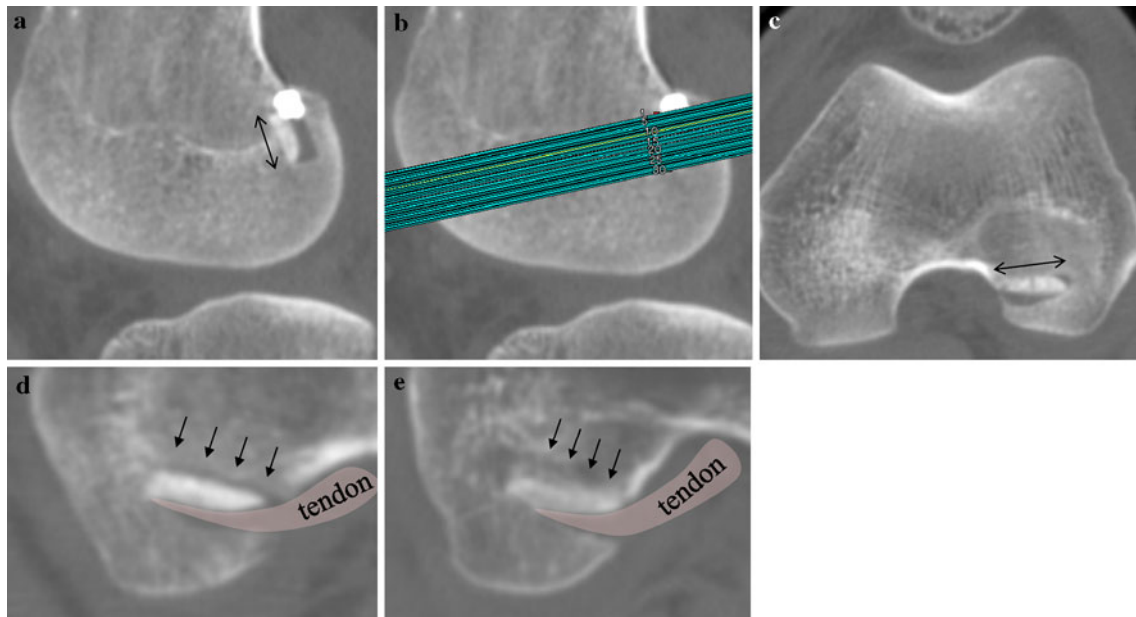


Fig. 2 The bone plug of the graft was introduced into the tunnel with its tendinous portion placed posteriorly and fixed with an 6-mm interference screw just posterior-superior to the bone plug (a). Oblique axial (b) multiplanar reconstruction computed tomography 30 images obtained parallel to the femoral rectangular tunnel and

bone plug. Bony integration at the just anterior interface (ACL force direction) between the bone plug and the tunnel wall was evaluated (c arrow). Examples of “incomplete” slice (d) with visible hair line or gap and “complete” one (e) showing absence of a border or presence of trabecular continuity

images. Since the bone plug and femoral tunnel are rectangular parallelepipeds of $5 \times 10 \times 15$ mm, 30 slices were created parallel to the long axis of the parallelepiped bone plug and perpendicular to its tendinous plane (Fig. 2). Similar CT images for 4 patients were also taken at a mean of 3 days (range, 2–4 days) after surgery to examine the conditions prior to healing.

Morphological CT evaluation

For morphological CT evaluation, the 30 reconstructed slices were evaluated as “complete,” indicating no border between the plug and the tunnel wall or showing trabecular continuity or “incomplete,” indicating a visible gap of >1 mm [7]. To evaluate bone integration, cases in which >20 of the 30 slices were categorized as “complete” without bone absorption were determined to be “excellent” and those with 11–20, 5–10, and <5 “complete” slices were classified as “good,” “fair,” and “poor,” respectively. Data from these evaluations were compared at the two time points after surgery (Fig. 2).

CT value changes

For a more detailed quantitative analysis, the CT value was determined for a slice selected from the central portion (landmark of suture hall) of the 30 slices as a region of interest. In the selected slice, a straight line of

1.5 cm was drawn perpendicular to the long axis of the bone plug using image analysis software (virtual place M). This made it possible to visualize the CT value sequentially at each point on a graph (Fig. 3). Since the value changes from anterior to posterior according to the bone mineral density (BMD), the graph has a minimum at the point of the interface (point b in Fig. 3) at the anterior wall of the tunnel of dilated cancellous bone (point a in Fig. 3), reaches a peak at the cortex of the bone plug (point c in Fig. 3), and then decreases to the lowest value in the tendinous region. Since the BMD varies among patients, the change in the CT value at the interface and the depth of the minimum were normalized by dividing by the peak value for the cortex. In this manner, the relative drop in the CT value was calculated and expressed as a percentage.

Reliability measurement

Reliability calculations were based on positioning the planes for the MPR and determine the ingrowth on each slice by the same observer (three time repeat) and by three different observers (T.S., H.O., and T.I.). The intra- and inter-observer intraclass correlation coefficient (ICC) and kappa coefficient were calculated, respectively. After assessing reliability measurement, one author determined the positioning the plane for MPR and the ingrowth on each slice.

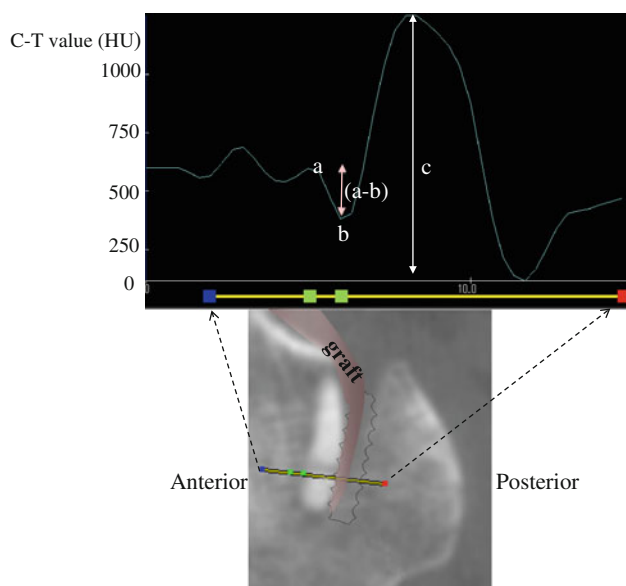


Fig. 3 The CT value was measured sequentially from anterior to posterior through the bone plug along the transverse cutting. The anterior wall of the tunnel of dilated cancellous bone was defined as “point *a*,” a minimum at the point of the interface as “point *b*,” and a peak at the cortex of the bone plug as “point *c*,” after which the CT value decreased to the lowest level in the tendinous region

Statistical analysis

The mean numbers of slices sorted into each category for the first and second CT scans were compared by paired *t* test. A *P* value of less than 0.05 was considered to indicate a significant difference.

Results

There were no intraoperative complications during fixation of the bone plug, including blow-out cortical fracture, bone plug fracture, bone plug dislocation, and graft failure.

Reliability measurement

The intra- and inter-observer intraclass correlation coefficient (ICC) concerning the measurements of radiographic assessment on positioning the planes for the MPR was 0.95 and 0.91. kappa coefficient was 0.83. The intra- and inter-observer reliabilities were substantial to excellent.

In the first postoperative week (days 2 and 4), all slices were macroscopically “incomplete” with a clear gap, leading to a classification of “poor” integration. The normalized change in the CT value at the border was 14.2 ± 4.3 , and points *a* and *b* showed especially sharp angles in the graph (Tables 1, 2; Fig. 3).

Table 1 Numbers of “complete” and “incomplete” slices after rectangular tunnel ACL reconstruction in 20 patients

Postoperative period	“Complete” slices	“Incomplete” slices
3 days	0	30
4 weeks	19.3 ± 6.7	10.8 ± 5.4
8 weeks	$25.1 \pm 5.4^*$	$4.9 \pm 4.8^*$

**P* < 0.05 for 4 versus 8 weeks

In the first scan after 4 weeks (range 3–5 weeks), 19.3 ± 6.7 of the 30 slices were evaluated as macroscopically “complete” and 10.7 ± 5.4 slices were “incomplete.” Of the 20 cases, 55% were categorized as showing “excellent” integration (Tables 1, 2).

In the second scan after 8 weeks (range 7–9 weeks), 25.1 ± 5.4 of the 30 slices were macroscopically “complete,” showing a significant increase compared to 4 weeks (*P* = 0.004) and 4.9 ± 4.8 were “incomplete,” indicating a significant decrease over time (*P* = 0.00004) (Table 1). Of the 20 cases, 80% showed “excellent” integration (Fig. 4). The normalized change in the CT value at the border was 10.9 ± 7.2 , which was significantly lower than this value at 4 weeks (*P* = 0.00305) (Tables 1, 2).

Discussion

The most important finding in this study was that the bone plug was integrated into femoral tunnel in early postoperative stage after RT BTB ACL reconstruction using macroscopic analysis of slices from CT-MPR images and to examine macroscopically undetectable changes using CT values.

One of the keys to success in ACL reconstruction is to restore the bone-tendon junction around the ACL femoral attachment [15, 29]. Since tremendous stress is exerted on the ACL femoral attachment in the functional position of the knee, and because the force direction in this area is dramatically changed by knee flexion and extension [10, 20], early re-establishment of the bone-tendon junction is desirable [3, 13, 16, 19, 21]. However, excessive gap space may be present around the interference screw used for fixing a parallelepiped or triangle pillar bone plug into a round tunnel in the traditional operation (Fig. 4) [13, 14, 22]. In contrast, the technique used in this study, in which the bone plug is first matched to the parallelepiped bone tunnel with subsequent screw fixation, may be better for earlier biological bone plug-tunnel integration and reestablishment of the bone-tendon junction by maximizing the interface of the graft and tunnel wall (Fig. 4) [4, 5, 17, 24].

This raises the question of the difference in time required for bone plug-tunnel integration between the

Table 2 CT values (shown in Hounsfield units (HU)) at each time point and normalized changes in CT values

Postoperative period	Point a (dilated cancellous)	Point b (Gap)	Point c (Cortex)	Normalized change in the CT value
3 days	514 ± 29 HU	363 ± 41 HU	966 ± 163 HU	14.2 ± 4.3
4 weeks	498 ± 99 HU	317 ± 62 HU	982 ± 123 HU	18.4 ± 10.9
8 weeks	360 ± 76 HU*	264 ± 72 HU*	966 ± 161 HU	10.9 ± 7.2*

* $P < 0.05$ for 4 versus 8 weeks

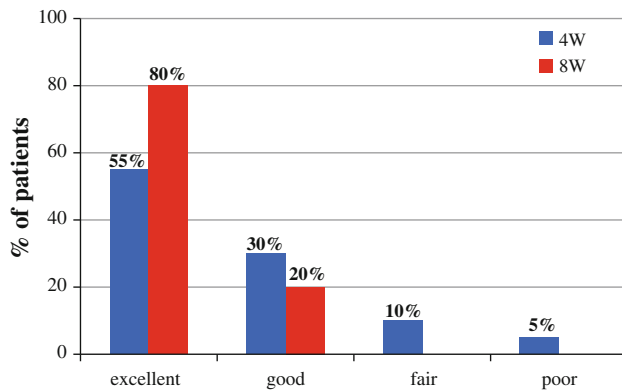


Fig. 4 Macroscopic evaluation of CT slices. Excellent integration was observed in 55% of the cases at 4 weeks and in 80% of the cases at 8 weeks

conventional technique and our approach. Clancy et al. [6] found that the bone plug and a round bone tunnel established histological fixation at 8 weeks postoperatively in rhesus monkey. Among clinical studies, Lomasney used CT images to show fixation in 28.6% of cases at 8 weeks postoperatively after conventional surgery with a bone-patellar tendon-bone graft and a round bone tunnel [14]. The value of MDCT and MPR images for evaluation of bone fracture and bone integration after bone graft has been reported [2, 12, 18, 30], and imaging analysis is useful for clinical evaluation of bone integration postoperatively [14]. However, evaluation of bone plug integration after ACL reconstruction is uncommon since (1) analysis of the integration of a small bone plug with the femoral cancellous bone is much more difficult than for diaphyseal fracture healing and (2) evaluation is difficult since the surplus space between the bone plug and the tunnel is large and it takes a long time to fill the gap [7]. In this study, we used 30 slices in a plane parallel to an arbitrary long axis of the bone graft and the tunnel (a plane vertical to the anterior plane) in MPR images collected by MDCT [2, 12] at two postoperative time points [14]. A region of interest was established in the anterior surface of the evaluated site to detect slight changes; patterns of changes in CT values for the bone graft, bone tunnel and the surrounding area were observed, and the data were evaluated based on the difference in CT values at the boundary. This approach allowed the first detailed analysis of bone plug-tunnel integration after ACL reconstruction.

There are two types of healing processes for a bone plug with the tunnel [4, 5, 17]. In indirect healing, granulation tissue is generated between bone segments, callus develops, the gap between the bone segments increases, and neonatal bone finally fills the gap [4, 5]. In contrast, direct healing proceeds without generation of callus at the boundary or bone absorption at the bone edge at the interface, with no gap forming in a stable mechanical environment [15]. Our morphological CT evaluation indicated that direct healing occurs after the surgical technique used in this study. The clear boundary present after a few postoperative days gradually became unclear over time with no bone absorption observed. The number of “complete” slices on CT at 8 weeks postoperatively was significantly higher than that after 4 weeks, and the number of “incomplete” slices significantly decreased after 8 weeks. This indicates that early biological fixation is likely with this technique. If a gap was made at the interface, a postoperative period of 8 weeks would be insufficient to fill the gap.

The changes in CT values appear to support the macroscopic evaluations [2]. Slight changes that cannot be detected macroscopically were detectable by quantification of changes in the CT value in the region of interest. In addition, these changes gave an intuitive understanding of the healing process of the bone plug [2, 28]. The surrounding area of the bone tunnel and the graft had a slightly higher CT value than the surrounding cancellous bone, which might be caused by dilation, and a peak CT value that was probably due to pressure applied anteriorly was observed in all cases. A dip was also observed just anterior to that point. The CT value of the cancellous bone showed a general decrease over time, probably due to osteoporotic changes caused by non-weight bearing postoperatively. This change in the CT value decreased over time based on the values at 0, 4, and 8 weeks. Thus, the normalized change in the CT value at the border may be a useful marker for monitoring direct healing of the plug [4, 5, 17].

There is some limitation in this study. We did not include a control group of subjects treated by conventional techniques, while earlier bone plug integration was shown by CT [12, 18]. Thus, we still have to be cautious to accelerate postoperative rehabilitation, as it is still unclear how earlier the graft itself is remodeled postoperatively by accelerated healing of the bone plug to the tunnel wall.

However, we believe earlier integration of the bone plug to the tunnel accelerates the graft healing itself. Surgeons should pay attention to minimize extra space between the graft and the tunnel or to maximize contact area between them by adjusting the cross-sectional shape of the femoral tunnel aperture to that of the bone plug.

Conclusion

Because a snug fit is achieved at the bone plug-femoral tunnel interface, this method is beneficial for graft-bone integration in early postoperative stage after RT BTB ACL reconstruction.

In this technique of RT BTB ACL reconstruction, the bone plug integrated with the femoral tunnel in 55% of cases as early as 4 weeks postoperatively and in 80% of cases by 8 weeks postoperatively.

Conflict of interest The authors declare that they have no conflict of interest.

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