# Hemodynamic changes during neural deactivation in human brain: A positron emission tomography study of crossed cerebellar diaschisis

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The mechanism of crossed cerebellar diaschisis (CCD) is considered to be secondary hypoperfusion due to neural deactivation. To elucidate the hemodynamics during neural deactivation, the hemodynamics of CCD was investigated. The cerebral blood flow (CBF), cerebral blood volume (CBV), cerebral oxygen extraction fraction (OEF), cerebral metabolic rate of oxygen (CMRO<sub>2</sub>), and vascular responses to hypercapnia and acetazolamide stress for CCD were measured in 20 patients with cerebrovascular disease by positron emission tomography with H<sub>2</sub><sup>15</sup>O, C<sup>15</sup>O, and <sup>15</sup>O<sub>2</sub>. Vascular responses to hypercapnia and acetazolamide stress were almost the same between CCD side and unaffected side of the cerebellum, a finding that supports the idea that the mechanism of CCD is secondary hypoperfusion due to neural deactivation. The degree of decrease in CBF on the CCD side was almost the same as that in CBV, indicating that vascular blood velocity does not change during neural deactivation. The relation between CBF and CBV of the CCD and unaffected sides was CBV = 0.29 CBF<sup>0.56</sup>. On the CCD side, the degree of decrease in CMRO<sub>2</sub> was less than that in CBF, resulting in a significantly increased OEF. The increased OEF along with the decreased CBV on the CCD side might indicate that neural deactivation primarily causes vasoconstriction rather than a reduction of oxygen metabolism.

Key words: neural deactivation, hemodynamics, cerebellum, diaschisis, PET

### **INTRODUCTION**

POSITRON EMISSION TOMOGRAPHY (PET) studies of the hemodynamics of crossed cerebellar diaschisis (CCD), which is caused by contralateral supratentorial lesions, have shown a reduction in cerebral blood flow (CBF) and cerebral metabolic rate of oxygen (CMRO<sub>2</sub>).<sup>1-4</sup> No differences in vascular response to hypercapnia, hypocapnia, or acetazolamide stress were observed between the CCD side and the unaffected side of the cerebellum.<sup>5,6</sup> This finding implies that the mechanism of CCD is secondary hypoperfusion due to neural deactivation.

We recently used photic flicker visual stimulation to investigate changes in both regional CBF and regional

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cerebral blood volume (CBV) during neural activation.<sup>7</sup> In our observations, when the increase in CBF was large, it was caused primarily by an increase in vascular blood velocity rather than by an increase in CBV, but the relation between CBF and CBV during neural deactivation is not well understood. Since the mechanism of CCD is secondary hypoperfusion due to neural deactivation, CCD can be used to investigate the hemodynamics of neural deactivation. To the best of our knowledge, only one report showed almost the same reduction levels of CBF and CBV on the CCD side as on the unaffected side,<sup>4</sup> indicating no noticeable change in vascular blood velocity between the CCD and unaffected sides.

In the present study, CBF, CBV, cerebral oxygen extraction fraction (OEF), CMRO<sub>2</sub>, and vascular responses to hypercapnia and acetazolamide stress for CCD were measured in each patient on the same day by the same modality. Data on vascular responses to hypercapnia and acetazolamide stress were used to confirm that the mechanism of CCD is secondary hypoperfusion due to neural deactivation. Data on CBF, CBV, OEF and CMRO<sub>2</sub>

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were used to investigate the hemodynamics of neural deactivation.

### **METHODS**

### **Subjects**

We studied the case records of 20 patients (15 men and 5 women; age,  $60 \pm 12$  yr, mean  $\pm$  SD) with steno-occlusive lesions of the major cerebral artery who were affected by CCD that was sufficiently visualized on the CBF image at rest (affected/unaffected ratio < 0.93).<sup>6</sup> All patients were selected retrospectively from a large series of patients whose CBF, CBV, OEF, CMRO<sub>2</sub>, and CBF responses to hypercapnia and acetazolamide stress had been measured by PET. All patients gave written informed consent before the PET examination. Patient information is listed in Table 1. The interval between the onset of stroke and PET examination ranged from 1 to 19 weeks. Exclusion criteria were crossed cerebellar atrophy and other morphological lesions of the cerebellum or brain stem as detected on magnetic resonance imaging (MRI), and steno-occlusive lesions in the vertebrobasilar system detected by angiography.

# PET procedures

A Headtome-V PET camera (Shimadzu Corp., Kyoto, Japan) was used for all studies; it provides 47 sections with center-to-center distances of 3.125 mm.<sup>8</sup> The intrinsic spatial resolution was 4.0 mm in-plane and 4.3 mm full width at half maximum (FWHM) axially. Reconstruction with a Butterworth filter resulted in a final in-plane resolution of approximately 8 mm FWHM.

### $C^{15}O$ study

To measure CBV, a  $C^{15}O$  PET study was performed according to a previously described method.<sup>9</sup> Transmission scanning for attenuation correction was performed just before the C<sup>15</sup>O PET scanning. A head fixation system with individual molds for each subject was used to minimize head movement during the PET measurements. The static PET scan was started 3 minutes after 1 minute of continuous inhalation of C<sup>15</sup>O gas (approximately a total of 5 GBq supplied to the mouth). The scan time was 4 minutes. Three arterial blood samples were taken during the PET scanning.

## $^{15}O_2$ study

To measure OEF and CMRO<sub>2</sub>, a  ${}^{15}O_2$  PET study was performed as previously described.<sup>10,11</sup> The scanning protocol consisted of a 180-second static scan following 1.5 minutes of continuous inhalation of  ${}^{15}O_2$  gas (approximately a total of 5 GBq supplied to the mouth). The arterial input function was obtained with a beta probe for continuous measurement of arterial whole blood radioactivity. Two blood samples were taken, one at the beginning and one at the end of scanning to measure the arterial O<sub>2</sub> gas pressure and pH. The arterial plasma concentration of  ${}^{15}O$  labeled metabolic water was calculated according to a previously reported method.<sup>12</sup> Correction for remaining radioactivity in cerebral blood vessels was done.<sup>13</sup>

Patient	Age (y)/Sex	Lesion location	Angiography findings	Time since stroke
1	39/M	L parietal	L ICA occlusion	7 wk
2	67/F	L parietal	L MCA stenosis	6 wk
3	67/M	L basal ganglia	L MCA stenosis	10 wk
4	58/F	R frontal & parietal	R MCA stenosis	7 wk
5	29/M	R basal ganglia & insula	R MCA stenosis	5 wk
6	73/F	L parietal	L ICA stenosis	8 wk
7	61/M	R centrum semiovale	R ICA occlusion	19 wk
8	70/M	L frontal & temporal	L ICA occlusion	4 wk
9	62/M	L centrum semiovale	L ICA occlusion	3 wk
10	51/M	R basal ganglia	R MCA stenosis	4 wk
11	68/M	R basal ganglia & insula	R MCA stenosis	4 wk
12	64/M	L corona radiata	L ICA stenosis	2 wk
13	73/F	R centrum semiovale	R MCA stenosis	10 wk
14	41/M	L frontal	L ICA stenosis	1 wk
15	62/M	L centrum semiovale	L ICA stenosis	5 wk
16	72/M	L basal ganglia	L MCA stenosis	13 wk
17	56/M	L centrum semiovale	L ICA occlusion	1 wk
18	68/M	L frontal & parietal	L ICA stenosis	8 wk
19	59/M	R basal ganglia	R MCA occlusion	3 wk
20	57/F	L basal ganglia	L MCA stenosis	2 wk

 Table 1
 Clinical characteristics of the 20 patients with cerebral infarction

M, male; F, female

R, right; L, left; ICA, internal carotid artery; MCA, middle cerebral artery

Condition	P <sub>a</sub> CO <sub>2</sub> (mm Hg)	P <sub>a</sub> O <sub>2</sub> (mm Hg)	рН	BP (Systole/Diastole) (mm Hg)	HR (beats/min)	
Rest	$38.5 \pm 2.5$	85.7 ± 11.0	$7.431 \pm 0.017$	151 ± 24/76 ± 14	67 ± 13	
CO <sub>2</sub>	43.8 ± 2.9*	$104.2 \pm 12.6*$	7.391 ± 0.021*	$158 \pm 30^{\dagger}/79 \pm 16$	68 ± 15	
Acetazolamide	$35.9 \pm 2.3*$	99.5 ± 10.6*	$7.443 \pm 0.018*$	$154 \pm 29/77 \pm 13$	$67 \pm 13$	

Table 2 P<sub>a</sub>CO<sub>2</sub>, P<sub>a</sub>O<sub>2</sub>, pH, blood pressure (BP) and heart rate (HR) during each H<sub>2</sub><sup>15</sup>O PET scan

Values are shown as mean  $\pm$  SD.

Significant difference vs. values at rest: p < 0.001, p < 0.01 (by paired t-test)

Table 3CBF values at rest and during  $CO_2$  inhalation and<br/>acetazolamide stress, and percentage changes in CBF in re-<br/>sponse to  $CO_2$  inhalation and acetazolamide stress for contralat-<br/>eral and ipsilateral cerebellum

	Contralateral	Ipsilateral
CBF (ml/100 ml/min)		
Rest	41 ± 10*	$51 \pm 10$
CO <sub>2</sub>	56 ± 17*	$72 \pm 20$
Acetazolamide	65 ± 21*	83 ± 23
% Change in CBF from rest		
CO <sub>2</sub> (%/mm Hg)	$7.6 \pm 6.4$	$8.0 \pm 6.4$
Acetazolamide (%)	57 ± 19	61 ± 29

Values are shown as mean  $\pm$  SD.

\*Significant difference between contralateral and ipsilateral cerebellum, p < 0.001 (by paired t-test)

 Table 4
 CBF at rest, CBV, OEF, CMRO<sub>2</sub>, and MTT values for contralateral and ipsilateral cerebellum

	Contralateral	Ipsilateral
CBF (ml/100 ml/min)	41 ± 10*	51 ± 10
CBV (ml/100 ml)	$2.1 \pm 0.6^{\dagger}$	$2.8 \pm 0.5$
OEF	$0.42 \pm 0.07*$	$0.39 \pm 0.06$
CMRO <sub>2</sub> (ml/100 ml/min)	$3.0 \pm 0.7*$	$3.4 \pm 0.7$
MTT (sec)	$3.2 \pm 0.8$	$3.3 \pm 0.8$

Values are shown as mean  $\pm$  SD.

\*<sup>†</sup>Significant difference between contralateral and ipsilateral cerebellum, \*p < 0.001, <sup>†</sup>p < 0.005 (by paired t-test)

# $H_2^{15}O$ study

 $H_2^{15}O$  PET studies were performed with the subjects at rest and during hypercapnia and acetazolamide stress. The interval between  $H_2^{15}O$  PET studies was at least 15 minutes. The scanning protocol consisted of a 180-second static scan following continuous intravenous infusion of  $H_2^{15}O$  over 2 minutes. The dose of radioactivity was 0.9 to 1.7 GBq at the start of the scan. The arterial input function was obtained with a beta probe for continuous measurement of arterial whole blood radioactivity. Dispersion and delay occurring in the beta detector system and in the internal-arterial line were corrected according to previously reported methods.<sup>14,15</sup> Two blood samples were taken, one at the beginning and one at the end of scanning to measure the arterial CO<sub>2</sub> gas pressure. The CBF images were calculated by an autoradiographic method.<sup>16,17</sup> Forced hypercapnia was induced by inhalation of 7% CO<sub>2</sub> gas, starting 1 minute before the beginning of the scan and continuing until the end of scan.<sup>18</sup> Acetazolamide (1 g) was administered intravenously over 2 minutes starting 10 minutes before the beginning of the scan.

### Data analysis

Regions of interest (ROIs) were drawn on PET images. Elliptical ROIs were defined for the cerebellar cortex (16 mm  $\times$  32 mm) in three adjacent sections, and data were pooled to obtain the average concentration of radioactivity for the whole volume of interest.

For each whole volume of interest, vascular mean transit time (MTT) was calculated as follows<sup>19</sup>:

$$MTT = \frac{CBV}{CBF} \qquad \qquad Eq. 1$$

For each whole volume of interest, the vascular response to hypercapnia was calculated as the percentage change in CBF per absolute change in  $P_aCO_2$  (mmHg) as follows<sup>18</sup>:

Vascular response to hypercapnia (%/mmHg)

$$= 100 \times \frac{\text{CBF}_{a} - \text{CBF}_{r}}{\text{CBF}_{r}} \times \frac{1}{|P_{a}\text{CO}_{2a} - P_{a}\text{CO}_{2r}|} \text{ Eq. 2}$$

The vascular response to acetazolamide stress was calculated as the percentage change in CBF as follows:

Vascular response to acetazolamide stress (%)

$$= 100 \times \frac{\text{CBF}_{a} - \text{CBF}_{r}}{\text{CBF}_{r}} \qquad \text{Eq. 3}$$

where the subscripts "r" and "a" denote the rest and activation conditions (hypercapnia and acetazolamide), respectively.

#### RESULTS

PaCO<sub>2</sub>, PaO<sub>2</sub>, pH, blood pressure and heart rate during each H<sub>2</sub><sup>15</sup>O PET scan are summarized for each condition in Table 2. The hemoglobin concentration and hematocrit were 13.1  $\pm$  1.7 g/dl and 39.1%  $\pm$  4.2%, respectively (mean  $\pm$  SD).

The CBF values during rest, hypercapnia, and aceta-



**Fig. 1** A: The ratios of contralateral to ipsilateral cerebellum CBF values at rest and during hypercapnia (CO<sub>2</sub>) and acetazolamide (ACZ) stress, and the ratios of vascular responses (Change) to hypercapnia and acetazolamide stress (mean  $\pm$  SD). B: The ratios of contralateral to ipsilateral cerebellum CBF at rest, CBV, OEF, CMRO<sub>2</sub>, and MTT (mean  $\pm$  SD).

zolamide stress, and the vascular response to hypercapnia and acetazolamide stress are given in Table 3. CBF for the contralateral (affected) cerebellum was significantly lower than that for the ipsilateral (unaffected) side during all conditions. No significant differences in vascular response to hypercapnia and acetazolamide stress were observed between the contralateral and ipsilateral cerebellum.

The CBF at rest, CBV, OEF, CMRO<sub>2</sub> and MTT values are given in Table 4. CBF at rest, CBV, and CMRO<sub>2</sub> were significantly lower in the contralateral (affected) side than in the ipsilateral (unaffected) side, whereas OEF was significantly higher in the contralateral cerebellum. No significant difference in MTT was observed between the two sides.

The contralateral to ipsilateral cerebellum ratios of



Fig. 2 Scatter plot of CBF at rest and CBV values of contralateral and ipsilateral sides of the cerebellum in all patients.

CBF at rest and during hypercapnia and acetazolamide stress, and the ratios of vascular responses to hypercapnia and acetazolamide stress are shown in Figure 1A. The ratio of CBF during all conditions was about 0.8. Therefore, the ratio of vascular response to hypercapnia and that of acetazolamide stress were about 1.

The contralateral to ipsilateral cerebellum ratios of CBF at rest, CBV, OEF, CMRO<sub>2</sub> and MTT are shown in Figure 1B. The ratio of CBF and that of CBV were about 0.8, so the resulting ratio for MTT was about 1.

The relations between CBF at rest and CBV values for the contralateral and ipsilateral side of the cerebellum for all patients are shown in Figure 2. The relation between CBF and CBV was determined by least squares analysis according to a previous study<sup>20</sup>: CBV = 0.29 CBF<sup>0.56</sup>.

### DISCUSSION

This is the first study to retrospectively examine data on CBF, CBV, OEF, CMRO<sub>2</sub> and vascular responses to hypercapnia and acetazolamide stress for CCD in which all measurements were conducted on the same day by the same modality. As in previous reports, we found that vascular responses to hypercapnia and acetazolamide stress were almost same between the CCD side and the unaffected side of the cerebellum (Table 3, Fig. 1A). We previously reported that tissue with increased CBF due to neural activation showed the same vascular response to change in P<sub>a</sub>CO<sub>2</sub> as that seen for resting CBF.<sup>21</sup> Inao et al. reported that despite a decreased vascular response to acetazolamide stress because of a steno-occlusive lesion of a major cerebral artery, normal CBF response to neural activation was observed.<sup>22</sup> These findings indicate that the mechanism of vascular response to neural activation is independent of that to either PaCO2 change or acetazolamide stress. No differences in vascular response to changes

in  $P_aCO_2$  or acetazolamide stress between the CCD and unaffected sides have been reported, and this supports the concept that the mechanism of CCD is secondary hypoperfusion due to neural deactivation.<sup>5,6</sup> Our present data confirm that the mechanism of CCD is secondary hypoperfusion due to neural deactivation.

In our present results, the CBF at rest and CBV were significantly lower on the CCD side than the unaffected side, and the degree of difference between CBF of the two sides was almost the same as that between CBV. This resulted in no difference in MTT between the CCD and unaffected sides (Table 4, Fig. 1B).<sup>4</sup> This indicates that vascular blood velocity does not change during neural deactivation. In our previous report, we noted that the increase in CBF during strong neural activation (8-Hz photic flicker) was caused primarily by the increase in vascular blood velocity rather than by the increase in CBV, but the increase in CBF was slightly greater than that in CBV during weak neural activation (2-Hz photic flicker).<sup>7</sup> These findings indicate that the change in CBF related to neural activity might be related to a change in CBV for the low or normal range of CBF and to change in vascular blood velocity for the high range of CBF.

In our present results, the relationship between CBF at rest and CBV of the CCD and unaffected sides was CBV =  $0.29 \text{ CBF}^{0.56}$  (Fig. 2). In our previous results, the relationship between CBF and CBV for the baseline and during visual stimulation by 2-Hz and 8-Hz photic flicker was  $CBV = 0.88 CBF^{0.30.7}$  According to Poiseuille's law, the flow of blood through a vessel is proportional to the fourth power of the vessel diameter. Blood volume is proportional to the square of the diameter. These show the relationship CBV = c CBF<sup>0.5</sup> (c: constant), which corresponds closely with our present relationship and the relationship during visual stimulation, although the CCD and the visual stimulation are different in the time scale. Both the present relationship between CBF and CBV and the relationship during visual stimulation closely corresponded with that during change in P<sub>a</sub>CO<sub>2</sub>,<sup>20</sup> suggesting that the regulation of CBF and CBV might be governed by a common microcirculatory mechanism during both change in neural activity and change in P<sub>a</sub>CO<sub>2</sub>.

In the present study, CBF and CMRO<sub>2</sub> were significantly lower on the CCD side than on the unaffected side, but the degree of difference between CMRO<sub>2</sub> on the two sides was less than that between CBF, resulting in a significant increase in OEF on the CCD side (Table 4, Fig. 1B). To the best of our knowledge, only one report showed a significantly higher OEF on the CCD side than on the unaffected side.<sup>4</sup> This increased OEF was not due to ischemia since CBV did not increase and vascular responses to hypercapnia and acetazolamide stress were intact.<sup>18,19,23</sup> The higher OEF with the lower CBV on the CCD side than on the unaffected side might indicate that neural deactivation primarily causes vasoconstriction rather than a reduction in oxygen metabolism.<sup>24</sup> Wenzel et al. has reported that the neural deactivation caused by saccades induced focal hypooxygenation, in which CBF was more reduced than oxygen delivery.<sup>25</sup> Although the CCD and the saccadic suppression were different in the time scale, similar phenomena were observed. In addition, no significant correlations were observed between the duration from the onset of stroke and hemodynamic parameters (CBF, CBV, OEF, and CMRO<sub>2</sub>) of CCD (data not shown). Fox et al. reported that the increase in regional CBF was greater than that in regional CMRO<sub>2</sub> during neural activation, which would result in decreased regional OEF.<sup>26</sup> This finding is opposite to that observed during neural deactivation.

In conclusion, vascular responses to hypercapnia and acetazolamide stress were nearly equivalent between the CCD and unaffected sides of the cerebellum. This finding supports the concept that the mechanism of CCD is secondary hypoperfusion due to neural deactivation. The degree of difference between CBF values on the CCD and unaffected sides was almost the same as that between CBV values on the two sides, indicating that vascular blood velocity does not change during neural deactivation. The relationship between CBF and CBV of the CCD and unaffected sides was  $CBV = 0.29 CBF^{0.56}$ . The degree of difference between CMRO<sub>2</sub> values on the two sides was less than that between the CBF values, resulting in significantly higher OEF on the CCD side. The increased OEF with the decreased CBV in the CCD side might indicate that neural deactivation primarily causes vasoconstriction rather than a reduction in oxygen metabolism.

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#### REFERENCES

- Lenzi GL, Frackowiak RS, Jones T. Cerebral oxygen metabolism and blood flow in human cerebral ischemic infarction. J Cereb Blood Flow Metab 1982; 2: 321–335.
- Martin WR, Raichle ME. Cerebellar blood flow and metabolism in cerebral hemisphere infarction. *Ann Neurol* 1983; 14: 168–176.
- Pantano P, Baron JC, Samson Y, Bousser MG, Derouesne C, Comar D. Crossed cerebellar diaschisis. Further studies. *Brain* 1986; 109: 677–694.
- Yamauchi H, Fukuyama H, Kimura J. Hemodynamic and metabolic changes in crossed cerebellar hypoperfusion. *Stroke* 1992; 23: 855–860.
- Bogsrud TV, Rootwelt K, Russell D, Nyberg-Hansen R. Acetazolamide effect on cerebellar blood flow in crossed cerebral-cerebellar diaschisis. *Stroke* 1990; 21: 52–55.
- 6. Ishii K, Kanno I, Uemura K, Hatazawa J, Okudera T,

Inugami A, et al. Comparison of carbon dioxide responsiveness of cerebellar blood flow between affected and unaffected sides with crossed cerebellar diaschisis. *Stroke* 1994; 25: 826–830.

- 7. Ito H, Takahashi K, Hatazawa J, Kim SG, Kanno I. Changes in human regional cerebral blood flow and cerebral blood volume during visual stimulation measured by positron emission tomography. *J Cereb Blood Flow Metab* 2001; 21: 608–612.
- Iida H, Miura S, Kanno I, Ogawa T, Uemura K. A new PET camera for noninvasive quantitation of physiological functional parametric images: Headtome-V-dual. In *Quantification of Brain Function Using PET*, Myers R, Cunningham V, Bailey D, Jones T (eds), San Diego; Academic Press, 1996, 57–61.
- Martin WR, Powers WJ, Raichle ME. Cerebral blood volume measured with inhaled C<sup>15</sup>O and positron emission tomography. J Cereb Blood Flow Metab 1987; 7: 421–426.
- Mintun MA, Raichle ME, Martin WR, Herscovitch P. Brain oxygen utilization measured with O-15 radiotracers and positron emission tomography. *J Nucl Med* 1984; 25: 177– 187.
- Herscovitch P, Mintun MA, Raichle ME. Brain oxygen utilization measured with oxygen-15 radiotracers and positron emission tomography: Generation of metabolic images. J Nucl Med 1985; 26: 416–417.
- Iida H, Jones T, Miura S. Modeling approach to eliminate the need to separate arterial plasma in oxygen-15 inhalation positron emission tomography. *J Nucl Med* 1993; 34: 1333– 1340.
- Lammertsma AA, Jones T. Correction for the presence of intravascular oxygen-15 in the steady-state technique for measuring regional oxygen extraction ratio in the brain: 1. Description of the method. J Cereb Blood Flow Metab 1983; 3: 416–424.
- 14. Iida H, Kanno I, Miura S, Murakami M, Takahashi K, Uemura K. Error analysis of a quantitative cerebral blood flow measurement using  $H_2^{15}O$  autoradiography and positron emission tomography, with respect to the dispersion of the input function. *J Cereb Blood Flow Metab* 1986; 6: 536– 545.
- 15. Iida H, Higano S, Tomura N, Shishido F, Kanno I, Miura S, et al. Evaluation of regional differences of tracer appearance time in cerebral tissues using [<sup>15</sup>O] water and dynamic positron emission tomography. J Cereb Blood Flow Metab

1988; 8: 285–288.

- Raichle ME, Martin WR, Herscovitch P, Mintun MA, Markham J. Brain blood flow measured with intravenous H2<sup>15</sup>O. II. Implementation and validation. *J Nucl Med* 1983; 24: 790–798.
- Kanno I, Iida H, Miura S, Murakami M, Takahashi K, Sasaki H, et al. A system for cerebral blood flow measurement using an H<sub>2</sub><sup>15</sup>O autoradiographic method and positron emission tomography. *J Cereb Blood Flow Metab* 1987; 7: 143–153.
- Kanno I, Uemura K, Higano S, Murakami M, Iida H, Miura S, et al. Oxygen extraction fraction at maximally vasodilated tissue in the ischemic brain estimated from the regional CO<sub>2</sub> responsiveness measured by positron emission tomography. J Cereb Blood Flow Metab 1988; 8: 227–235.
- Powers WJ, Grubb RL Jr, Raichle ME. Physiological responses to focal cerebral ischemia in humans. *Ann Neurol* 1984; 16: 546–552.
- Grubb RL Jr, Raichle ME, Eichling JO, Ter-Pogossian MM. The effects of changes in P<sub>a</sub>CO<sub>2</sub> on cerebral blood volume, blood flow, and vascular mean transit time. *Stroke* 1974; 5: 630–639.
- Shimosegawa E, Kanno I, Hatazawa J, Fujita H, Iida H, Miura S, et al. Photic stimulation study of changing the arterial partial pressure level of carbon dioxide. J Cereb Blood Flow Metab 1995; 15: 111–114.
- Inao S, Tadokoro M, Nishino M, Mizutani N, Terada K, Bundo M, et al. Neural activation of the brain with hemodynamic insufficiency. *J Cereb Blood Flow Metab* 1998; 18: 960–967.
- Kuwabara Y, Ichiya Y, Sasaki M, Yoshida T, Fukumura T, Masuda K, et al. PET evaluation of cerebral hemodynamics in occlusive cerebrovascular disease pre- and postsurgery. *J Nucl Med* 1998; 39: 760–765.
- 24. Raichle ME. Behind the scenes of functional brain imaging: A historical and physiological perspective. *Proc Natl Acad Sci USA* 1998; 95: 765–772.
- 25. Wenzel R, Wobst P, Heekeren HH, Kwong KK, Brandt SA, Kohl M, et al. Saccadic suppression induces focal hypooxygenation in the occipital cortex. *J Cereb Blood Flow Metab* 2000; 20: 1103–1110.
- Fox PT, Raichle ME. Focal physiological uncoupling of cerebral blood flow and oxidative metabolism during somatosensory stimulation in human subjects. *Proc Natl Acad Sci USA* 1986; 83: 1140–1144.