Osteoclastic Resorption of Ca-P Biomaterials Implanted in Rabbit Bone

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Summary. The nature of the multinucleated cells involved in the resorption processes occurring inside macroporous calcium-phosphate biomaterials grafted into rabbit bone was studied using light microscopy, histomorphometric analysis, enzymatic detection of tartrate-resistant acid phosphatase (TRAP) activity, scanning, and electron microscopy. Sampies were taken at days 7, 14, and 21 after implantation. As early as day 7, osteogenesis and resorption were observed at the surface of the biomaterials, inside the macropores. Resorption of both newly formed bone and calcium-phosphate biomaterials was associated with two types of multinucleated cells. Giant multinucleated cells were found only at the surface of the biomaterials; they showed a large number of nuclei, were TRAP negative, developed no ruffled border, and contained numerous vacuoles with large accumulation of mineral crystals from the biomaterials. Osteoclasts exhibited TRAP positivity and well-defined ruffled border. They were observed at the surface of both newly formed bone and biomaterials, around the implant, and inside the macropores. In contact with the biomaterials, infoldings of their ruffled border were observed between the mineral crystals, deeply inside the microporosity. The microporosity of the biomaterials (i.e., the noncrystalline spaces inside the biomaterials) increased underneath this type of cell as compared with underneath giant cells or to the depth of the biomaterials. These observations demonstrate that macroporous calciumphosphate biomaterials implanted in bone elicit osteogenesis and the recruitment of a double multinucleated cell population having resorbing activity: giant multinucleated cells that resorb biomaterials and osteoclasts that resorb newly formed bone and biomaterials.

Key words: Osteoclast - Giant multinucleated cell **-** Biomaterials – Ceramics – Morphometry – Bone.

Various porous synthetic or natural calcium-phosphate (Ca-P) materials have been developed and used as bone substitute for clinical applications [1]. When grafted in a bone site, ingrowth of vascularized connective tissue into the macropores of the implant is followed by osteogenesis, with bone deposition at the surface of the biomaterial [2–4]. It was reported that such biomaterials cannot induce bone formation in heterotopic site, however, osteogenesis was observed in subcutaneous implant when the biomaterial was combined with bone marrow cells [5].

Resorption of the newly formed bone and of the Ca-P ceramics also occurs, and multinucleated cells are found in contact with the biomaterial. However, the nature and origin of these multinucleated cells remain incompletely elucidated and even conflicting. It was reported that the multinucleated cells elicited in contact with synthetic hydroxyapatite implanted in bone [6] or with mineralized bone particles subcutaneously implanted in rat [7] developed some morphological and functional features of osteoclast such as tartrateresistant acid phosphatase (TRAP) activity and ruffled border with clear zones. In contrast, the multinucleated cells recruited in contact with hydroxyapatite implanted in human periodontium or in contact with mineralized bone particles subcutaneously implanted in rabbit, lack TRAP activity, cell surface aspects, and functional features of osteoclasts [8, 9]. So, the term "multinucleated cell" may be confusing as it often includes osteoclast and giant cell of the foreign body reaction.

Osteoclasts are the main cells involved in the resorption of mineralized bone tissue. They differentiate in contact with bone from mononucleated medullar precursors [10, 11], and a lot of systemic and local factors have demonstrated an effective influence on their differentiation [11-13]. However, morphological and histochemical features usually provide sufficient support for cell identification.

Giant multinucleated cells also termed "Langhans cells" or "foreign body giant ceils," containing a large number of nuclei, have been described in chronic inflammatory tissue reaction (granuloma). They do not show a ruffled border or TRAP activity and they originate by fusion of mature monocytes or macrophages [14-17].

In the present study we have attempted to determine the nature of the cells involved in the resorption processes observed in such Ca-P ceramics, after implantation in corticomedullar defects drilled in tibiae of young rabbits. Two types of Ca-P biomaterials were used to test the specificity of the cellular and tissular reactions to implantation in bone. Histological and electron microscopic examination of resorbing cells were completed by histomorphometric analysis, histoenzymatic determination of the tartrate-resistant acid phosphatase activity, and measurement of the microporosity of the biomaterials.

Materials and Methods

Two types of cylindrical Ca-P ceramic (60 samples), 4 mm in length

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and 2.5 mm in diameter, were implanted in 15 young adult New Zealand white rabbits, each of them receiving two implants in the left tibiae and two implants in the right (one type of ceramic by tibia): (1) macroporous biphasic calcium phosphate (MBCP, 30 implants) consists of a 60/40 mixture (weight ratio) of synthetic hydroxyapatite $Ca_{10}(PO_4)_6(OH)_2$ and β tricalcium phosphate $(Ca_3(PO_4)_2$ compacted and sintered, at 1100°C, in macroporous blocks $(40-50\%$ macroporous, macropores from 400 to 600 μ m in diameter); (2) bovine hydroxyapatite (Bonap, 30 implants), a bovine bone hydroxyapatite, was prepared by deproteinization of trabeculax bovine bone and hydrothermal transformation of the inorganic phase into hydroxyapatite (this biomaterial was a gift from Dr. R. Legeros, College of Dentistry, New York University).

Implantations were performed, under sterile conditions and general anesthesia, in tibial cortico-medullar defects drilled at low speed under sterilized saline coolant, at about 15 mm from the proximal metaphyseal plate. Biopsies containing the implants were harvested 3, 7, 14, and 21 days after implantation.

Histological studies were carried out on 48 samples (24 MBCP, 24 Bonap), 4% paraformaldehyde-fixed, 7.5% buffered-EDTA decalcified, and paraffin embedded. The $7-\mu m$ sections were used for histological observation, histomorphometric analysis, and TRAP detection.

Light microscopic observations were done on sections stained with hematoxylin and eosine $(H & E)$ and Masson's trichrome, using a photomicroscope Nikon UFX II.

Histomorphometric measurements of the implants were carried out using a Zeiss microscope equipped with an integratory 100 points eyepiece reticule. The following measurements were carried out and expressed according to the ASBMR Histomorphometry Nomenclature Committee, using implant volume $(Imp.\hat{V})$ as referent: biomaterial volume (Bm.V/Imp.V) and thickness of trabeculae (Bm.Th.) of the biomaterials, and volume of the newly formed bone (NFB.V/Imp.V). These measurements were performed, before implantation (day 0), on undecalcified and methylmethacrylateembedded specimens, because decalcification of the nonimplanted samples led to the dissolution of the biomaterials.

TRAP activity was identified using naphtol AS BI phosphate (Sigma) as substrate with freshly diazotized Fast Garnet GBC (Sigma), in the presence of 50 mM tartrate. The number of multinucleated cells, either $TRAP +$ or $TRAP -$, in contact with newly formed bone or with biomaterials, was determined and expressed per $mm²$ of the implant area (Imp.Ar.).

Electron microscopic observation was done on biomaterials before implantation and on samples, taken at days 7, 14, and 21. Specimens were fixed for 90 mn, at $+4$ °C, in a 4.5% glutaraldehyde solution in pH 7.4 phosphate saline buffer and washed in phosphate buffer. These specimens were then processed for either transmission electron microscopy (TEM) or scanning electron microscopy (SEM).

SEM examination was done by two sequential methods: (1) after fixation and rinsing, fragments were dehydrated in a series of graded ethanol and acetone, critical-point dried, gold coated, and examined in a Jeol JSM 35 SEM; (2) after observation, fragments were rehydrated in distilled water, placed in a 10% sodium hypochlorite aqueous solution for about 6 hours, washed in distilled water, dehydrated, and then processed as above; this treatment removes the organic fraction. The same procedure was applied to two nonimplanted samples to serve as controls and to six implanted samples (3 MBCP and 3 Bonap).

TEM observation was carried out on two nonimplanted specimens used as controls and on six implanted samples (3 MBCP, 3 Bonap), broken up into fragments about 1 mm³ and separately embedded, undecalcified, in 812 resin epoxy. Multiple semiserial, ultrathin sections, 40-60 nm thick, were obtained using a diamond knife, stained with uranyl acetate and lead citrate, and observed using a 100 C Jeol electron microscope. The microporosity was calculated for each biomaterial, before implantation and on samples taken at day 14. Microporosity expressed the percentage of the surface area of the biomaterial not occupied by the mineral crystals. Image analysis was performed, on photographs (A4 format) at the original magnification of \times 5000, using a point-counting method. Measurements were done in the region underneath multinucleated cells and in the depth of the biomaterial.

All values are expressed using mean \pm SD. Comparisons between groups were done with Student's t test.

Results

Light microscopic examination of samples at day 3 after implantation showed loose connective tissue inside the superficial macropores of both biomaterials. Neither bone formation nor multinucleated cells were found in contact with the surface of the biomaterials. Histomorphometric analysis showed no significant variation in Bm.V/Imp.V or Bm.Th. when compared with preimplantation condition (results not shown).

From day 7 after implantation, seams and trabeculae made of newly formed bone, covered by layers of plump osteoblasts, were observed in the macropores, bound to the surface of the biomaterials in both types of implants (Fig. 1). Multinucleated cells were present as early as day 7, at the surface of both newly formed bone and biomaterials.

Most of the resorption cell profiles contained 2-10 nuclei; $TRAP +$ activity was detected in these cells and in the underlying biomaterial (Fig. 2). These cells, observed at the surface of the newly formed bone (NFB) and of the biomaterials, were similar to host osteoclasts found in the bone tissue distant from the implant or in the metaphyseal growth plates, and were designated as osteoclast-like cells (OLC). Some giant multinucleated cells (GMNC), containing more than 20 nuclei and showing no TRAP activity, were observed but only at the surface of the biomaterials (Fig. 3).

Histomorphometric analysis showed, before implantation, that in MBCP, $(n = 4)$, Bm.V/Imp.V = 49.6 \pm 4.1%, Bm.Th. = 345 ± 61 um; in Bonap, (n = 4), Bm.V/Imp.V = $48.1 \pm 3.2\%$, Bm.Th. = 295 \pm 35 μ m). After implantation, Bm.V/Imp.V progressively decreased in both biomaterials, whereas newly formed bone NFB.V/Imp.V increased (Fig. 4). In Bonap, Bm.Th. decreased to 163 ± 25 µm at day 21 after implantation ($P < 0.001$). Because of the partial dissolution of MBCP, occurring during the histological procedures, trabecular thickness could not be calculated for this biomaterial.

The total number of TRAP+ multinucleated cells $(OLC_{Total}/Imp.Ar.)$ progressively increased in both implants. The number of OLC in contact with the biomaterials $(OLC_{Bm}/Bm.Ar.)$ or with the newly formed bone $(OLC_{NFR}/Bm.Ar.)$ NFB.Ar.) increased in MBCP from day 7 to day 14, was similar at day 14 and day 21, and, in Bonap, increased progressively from day 7 to day 21. In both biomaterials, the number of GMNC (GMNC/Imp.Ar.; GMNC/Bm.Ar.) increased from day 7 to day 14 and decreased from day 14 to day 21 (Fig. 5).

Scanning electron microscopic observation showed, from day 7 after implantation, numerous cells, some reaching $100 \mu m$ in length, lying at the surface of the biomaterials in the macropores (Fig. 6). After treatment with sodium hypochlorite, new bone tissue was observed in the form of layers or trabeculae bound to the surface of the biomaterials (Fig. 7). Large zones of resorption with multiple pits were observed at the surface of the newly formed bone, and small pits $10-20 \mu m$ in diameter were also found at the biomaterial surfaces (Fig. 8).

Transmission electron microscopic study showed that the giant multinucleated cells in contact with the biomaterials contained numerous vacuoles in which a large accumulation of mineral crystals was observed (Fig. 9). No ruffled border was observed in this type of giant ceils on the multiple ultrathin sections. A ruffled border, with clear zones, was found in smaller multinucleated cells in contact with the biomaterials (Fig. 10). Infoldings of the ruffled border were found inside the biomaterial itself, in the spaces left between the mineral crystals (Fig. 11). In these cells, nuclei were irregularly shaped, mitochondria were numerous, and no or few vacuoles containing mineral crystals were present. A

Fig. 1. Light microscopy of samples taken at day 7 after implantation. Newly formed bone is visible (\rightarrow) at the surface of the macropores, inside the biomaterial (Bm): (A) MBCP $(\times 70)$ and (B) Bonap (×250). Masson's Trichrome.

well-defined ruffled border was also observed in osteoclasts resorbing newly formed bone (Fig. 12).

After implantation, the microporosity of the ceramics increased underneath OLC in both biomaterials, compared with before implantation, to the region underneath GMNC

Fig. 2. Enzymatic detection at day 14 of the TRAP in osteoclast-like cells at the surface of (A) MBCP Bm $(\times 200)$ and (B) Bonap biomaterial $(\times 250)$.

Fig. 3. Light microscopy at day 14 of giant multinucleated cell in contact with MBCP Bm. Note the semicircular disposition of nuclei $(x400)$ H & E.

Fig. 4. Histomorphometric evolution after implantation of (A) volume of biomaterials (Bm.V/Imp.V), and (B) volume of newly formed bone (NFB.V/Imp.V) in MBCP and Bonap (NS = nonsignificant difference. * $P < 0.05$, * * $P < 0.01$, * * * $P < 0.001$.

or to the depth of the trabeculae. In Bonap, the microporosity was $56.0 \pm 4.6\%$ before implantation and increased at day 14 up to 77.2 \pm 4.8% underneath OLC, but it remained at $61.7 \pm 4.5\%$ underneath GMNC and $60.8 \pm 3.9\%$ in the depth of the trabeculae. In MBCP, the microporosity was 54.1 \pm 3.7% before implantation and increased at day 14 up to $70.7 \pm 5.2\%$ underneath OLC. Microporosity remained at 59.8 \pm 4.9% underneath GMNC and 58.7 \pm 4.1% in the depth (Fig. 13).

Discussion

Osteoclasts are the major cells responsible for the physiological resorption of mineralized bone [11, 12, 18]. These cells show morphological and functional characteristics: they are multinucleated, they develop a typical ruffled border in contact with mineralized bone matrix [11, 19, 20], they are capable of acidifying the extracellular compartment leading to extracellular dissolution of the Ca-P crystals [21-23], they show TRAP and ATPase activity [24, 25] although the

Fig. 5. Histomorphometric evolution after implantation of (A) number of osteoclast-like cells $(OCL_{Total}/Imp.Ar.)$ and (B) giant multinucleated cells (GMNC/Imp.Ar.) in MBCP and Bonap implants. (NS: nonsignificant difference, $*P < 0.05$, $**P < 0.01$.)

Fig. 6. SEM at day 14 of a large cell in resorption lacunae at the surface of MBCP Bm (\times 280).

Fig. 7. SEM at day 21 of (A) layer $(\times 800)$ and (B) trabeculae of newly formed bone (x240) bonding to the surface of MBCP Bm and observed after treatment with sodium hypochlorite.

value of this activity as a reliable marker for osteoclast in culture is discussed [26, 27], and they possess receptors for calcitonin [12, 28]. Recently, specific antibodies were raised against some osteoclast cell surface antigens, and immunohistochemical methods were proposed for osteoclast identification [29-32].

Fig. 8. SEM at day 21, after sodium hypochlorite treatment, of a resorption lacunae found at the surface of (A) Bonap biomaterial $(\times 2300)$ and (B) newly formed bone $(\times 380)$ onto Bonap implant.

Giant cells elicited in contact with mineralized bone particles have some morphological features of osteoclasts, such as multinuclearity, but do not show a ruffled border or TRAP activity [9, 17, 33, 34]. Moreover, they break down bone particles by a process resembling phagocytosis.

In our study, implantation in bone of two types of Ca-P macroporous ceramics was followed by osteogenesis inside the implant and by remodeling of the newly formed bone and resorption of the biomaterials. The resorption processes appeared to involve at least two distinct multinucleated cell types. The first type, OLC, observed as soon as day 7 after implantation, includes cells with some features of osteoclasts: multinuclearity, TRAP activity, and ruffled border. These cells were found to be associated with erosion pits at the surface of both biomaterials and newly formed bone. Moreover, TRAP+ activity and increased microporosity were found in the biomaterials underneath these cells suggesting an extracellular dissolution of the biomaterials underneath OLC. However, the ruffled border appeared somewhat different in the cells resorbing the newly formed bone or the biomaterials. A typical ruffled border was observed in the osteoclasts in contact with the newly formed bone. The

Fig. 9. TEM of a GMNC found, at day 14, at the surface of Bonap Bm. Note the presence of numerous vacuoles with large accumulation of mineral crystals $(\times 3900)$.

Fig. 10, TEM of an osteoclast-like cell observed at day 14, in contact with the surface of Bonap Bm. Note the absence of mineral crystal inside the cell $(\times 3300)$.

Fig. 11. TEM showing details of the cytoplasmic membrane differentiation of OCL cell found, at day 14, in contact with MBCP Bm. (A) Detail of the clear zone $(\times 14,800)$ and (B) detail of the ruffling zone with infoldings inside the microporosity, between mineral crystals $(\times 13,000)$.

osteoclast-like cells in contact with the biomaterial showed characteristic clear zones and ruffling with infoldings threading between the mineral crystals of the biomaterial. These results suggest that the morphological appearance of the ruffled border depends on the mineralized matrix to be resorbed.

It is usually accepted that osteoclast progenitors are related to mononuclear hematopoietic precursors [10-12, 35]. Thus, osteoclasts or their precursors could migrate, with ingrowth of vascularized connective tissue, from the medullar spaces to the lacunae inside the biomaterials.

The second type of multinucleated cells, GMNC, are huge, containing numerous nuclei and large vacuoles with accumulation of mineral crystals. They show no TRAP activity and develop no ruffled border. They were observed only in contact with the biomaterials and never in relationship with the newly formed bone. Microporosity in the biomaterials under these cells was not significantly increased. These cells were comparable to the giant ceils found in the

Fig. 12. TEM of the cytoplasmic membrane differentiation in an osteoclast observed, at day 21, in contact with newly formed bone. Note lower mineral density in bone tissue underneath the ruffled border and presence of hydroxyapatite crystals between infoldings $(\times 15,000)$.

inflammatory tissue of the foreign body reaction. It is usually accepted that they generate by fusion of mature cells of the monocyte/macrophage lineage [15, 16]. However, in our experiment, GMNC were not observed in association with any inflammatory tissue.

Tissue response to implantation of mineralized materials seems to differ according to host species, receiving tissue and chemical composition of the implant, particularly the presence of bone proteins [36]. In this study, the results observed were similar in both types of biomaterials. However, intensity of the response in terms of osteogenesis and number of OCL differed at day 7 and 14 between the two types of biomaterial, but was similar at day 21. Differences in the architectural organization of the materials, particularly in the connections between the macropores, may modify the spreading of the connective tissue and the migration of precursor cells. However, this factor was not studied in this experiment.

Thus, the true role of the implanted material in the cell differentiation is not clear, and controversial results have been reported. When implanted subcutaneously in the rat or onto chorioallantoic membranes of chick embryos [36, 37], devitalized mineralized or demineralized bone particles elicited the recruitment of multinucleated cells. They exhibited some phenotypic features of osteoclasts such as multinuclearity and membrane specializations (clear zones and ruffled borders), TRAP activity, inhibition of resorption by calcitonin, and presence of receptors for this hormone [7, 36-39]. In contrast, multinucleated cells recruited in subcutaneous implants of mineralized bone particles and slices in rabbits showed a TRAP activity considerably weaker than in host

Fig. 13. The microporosity inside (A) MBCP and (B) Bonap biomaterials was measured before and at day 14 after implantation, in the depth of the biomaterials and in the superficial regions underneath GMNC and OCL. In both biomaterials, the microporosity significantly increased only under OCL cells.

osteoclasts, no tartrate-resistant acid ATPase activity, and did not stain with an osteoclast-speciflc monoclonal antibody [9].

The discrepancy between these studies may be related to host species and/or to differences in the nature or preparation of the implanted mineralized matrix. It was demonstrated that chemical composition of the implanted material influences the degree of osteoclast differentiation. The formation of mineral matrix complexes by the adsorption to hydroxyapatite of bone extract or osteocalcin enhanced ruffled border formation and the presence of specific osteoclast antigen on elicited multinucleated cells [36]. When implanted subcutaneously, synthetic crystalline apatite was reported to generate multinucleated cells showing osteoclastic features, but only when associated with osteocalcin [40].

Osteoblasts synthesize collagenous and noncollagenous proteins of the bone matrix. Among them, osteocalcin was hypothesized to favor differentiation of the ruffled border of the osteoclast [36, 40] and osteopontin to help the binding of this cell to hydroxyapatite $[41-43]$.

Consequently, the resorption events occurring in Ca-P ceramics implanted in bone cannot be dissociated from the simultaneous bone formation. In our experiment, new bone was observed as early as day 7 after implantation onto the surface of biomaterials. Amount of bone proteins, synthesized by osteoblasts, could circulate with biological fluids in the microporosity of the implant. Thus, the Ca-P ceramics progressively enriched in bone proteins could then favor osteoclastic differentiation. This could explain that the number of OLC resorbing the biomaterials increased from day 7 after implantation in both biomaterials.

From these data we conclude that osteogenesis occurs inside macroporous Ca-P ceramics implanted in bone. Remodeling of the newly formed bone and resorption of the biomaterials appeared to be associated with at least two types of multinucleated cells. Osteoclast-like cells could remodel newly formed bone and resorb the biomaterials progressively enriched in bone proteins, according to an extracellular mechanism, similar to that observed in physiological osteoclastic resorption of bone; giant multinucleated cells could resorb the biomaterials by phagocytosis.

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