Two-Compartment Basophil Cell Trafficking Model for Methylprednisolone Pharmacodynamics

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Received September 18, 1990-Final May 31, 1991

A two-compartment closed model was used to characterize the movement of basophils between blood and extravascular sites resulting from methylprednisolone (MP) exposure. This model is consistent with the view that corticosteroids cause a decrease in the recirculation of these cells from peripheral compartments. Methylprednisolone (Solu-Medrol) was given to healthy males at doses of 10, 25, and 40 mg. Blood samples were collected and assayed for MP by HPLC for pharmacokinetic analysis. Whole blood histamine, an index of circulating basophils, was assessed by RIA over 32 hr. Nonlinear least-squares analysis was carried out to solve for the model parameters reflecting cell movement between compartments and sensitivity (IC_{50}) to the steriod. This model quantitates the fall and return pattern of biologic response to corticosteroids with a minimal number of parameters which jointly fit several dose/response curves and yields a mean IC_{50} value of 8.1 ng/ml similar to receptor binding of MP. Properties of the temporal and integrated response curve and model extrapolations over a wide dose range were explored with simulations. Because corticosteroids exert similar effects on other cells in blood, this model may be applicable to various regulatory and immunosuppressive effects.

KEY WORDS: methylprednisolone; pharmacodynamics; cell trafficking; corticosteroids; glucocorticoid receptors; modeling.

INTRODUCTION

Corticosteroids such as methylprednisolone (MP) are widely utilized for their diverse array of effects. Clinically evident immunosuppression and anti-inflammation are the sum of multifarious corticosteroid activities. In

This work was supported in part by Grants GM 24211 and 150-1885-0 from the National Institute of General Medical Sciences, NIH.

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addition to decreased synthesis and release of arachidonic acid metabolites (1) and cytokines (2), corticosteroids alter the circulating patterns of leukocytes such as basophils (3), generally resulting in a net movement of cells, out of their functional domain in blood, to extravascular sites.

Basophils, constituting a relatively small fraction of total leukocytes, are major contributors to the development of allergic and anaphylactic reactions. Basophilic granules contain histamine, slow-reacting substance of anaphylaxis, platelet activating factor, eosinophil attracting factor, kallikrein, and large amounts of heparin (4). Degranulation occurs upon exposure to antigens, releasing these substances into the bloodstream and at sites of inflammation. Because at least 98% of circulating histamine is contained within basophils (3,5), decreases in circulating basophils are directly paralleled by decreases in whole blood histamine concentrations (WBH) (3,5-8).

Kong et al. (8) used an approximate pharmacodynamic model to characterize MP pharmacokinetics and its effect on WBH in six human subjects. The present basophil cell trafficking model is thus a secondgeneration pharmacodynamic model; it has been developed to more accurately define and extrapolate corticosteroid-induced alterations in the distribution of circulating cells. Furthermore, it provides parameters for sensitivity to steroid and apparent cell movement. Because many other leukocytes exhibit similar responses to MP and other corticosteroids, this model is potentially applicable to a variety of perturbations in steady state cell recirculation phenomena.

THEORETICAL

Methylprednisolone-induced basopenia is paradigmatic for a variety of cell trafficking phenomena seen immediately following corticosteroid exposure. Lymphocytes, monocytes, and eosinophils all exhibit corticosteroid-induced cytopenia (9-11). Leonard and Skeel (6) and Fauci and Dale (10) have indicated that a transient selective depletion of basophils and lymphocytes from blood to other body compartments accounts for corticosteroid effects. Characteristics of this effect are a rapid diminution of circulating cells, a nadir occurring several hours after steroid administration, followed by repopulation of the bloodstream well after plasma concentrations of drug have declined to subdetectable levels.

The basophil cell trafficking model, shown in Fig. 1, is a pharmacodynamic model structured with physiological analogy, which characterizes corticosteroid-induced basopenia over a range of doses using a minimum number of parameters. It is assumed that *WBH* is directly proportional to the number of blood basophils and that this ratio remains constant. In this

Fig. 1. Diagrammatic representation of the basophil cell trafficking model in which A_B is the number of basophils in the blood measured as whole blood histamine (*WBH*); k_{out} is a first-order rate constant for the movement of basophils from blood to extravascular sites; A_E is the number of circulating basophils in the extravascular pool; k_{in}^0 is the apparent zero-order return rate constant; IC_{50} is the MP concentration producing a 50% decrease in k_{in}^0 ; C_{MP} is the first-order decay rate constant for MP.

Basophil Cell Trafficking Model



two-compartment closed model, the total number of basophils is assumed to remain constant.

Under normal conditions the circulating pool of basophils can be divided into two subsets, cells in the blood and cells at extravascular sites, the amount of each remaining essentially constant. Evidence from leukapheresis studies (6) indicates that the proportion of basophils occupying the blood is very small when compared to extravascular basophils. Assuming instantaneous transfer of extravascular basophils to the blood during leukapheresis, a maximal estimate of the fraction of the total cell pool contained in the blood is about 16%. In reality this number is likely to be smaller because repopulation of the blood is not instantaneous.

The movement of basophils from the blood to extravascular sites is governed by the rate constant, k_{out} , and is directly proportional to the amount of basophils in the blood, A_B . Likewise, the return of basophils to the blood is governed by a rate constant, k_{in} , and is directly proportional to the amount of basophils in the extravascular pool, A_E . Exposure to MP produces a concentration-dependent decrease in k_{in} resulting in a net decrease in A_B . Equations describing the above patterns are as follow:

$$\frac{dA_{\rm B}}{dt} = I(t) \cdot k_{\rm in} \cdot A_{\rm E} - k_{\rm out} \cdot A_{\rm B} \tag{1}$$

$$\frac{dA_{\rm E}}{dt} = -I(t) \cdot k_{\rm in} \cdot A_{\rm E} + k_{\rm out} \cdot A_{\rm B}$$
⁽²⁾

with initial conditions of $A_B(0) = A_B^0$, and $A_E(0) = A_E^0$, and where I(t) represents the fractional inhibition function (8)

$$I(t) = \left(1 - \frac{C_{\rm MP}}{C_{\rm MP} + IC_{50}}\right)$$
(3)

The IC_{50} equals the concentration of MP producing a 50% inhibition of the rate constant for return of basophils to the blood (k_{in}) .

Because the total circulating pool of basophils (A_T) is very large relative to A_B , A_E remains essentially constant with the addition of basophils from the blood. Therefore, the product of k_{in} and A_E generates an apparent zero-order rate constant, k_{in}^0 . Thus Eqs. (1) and (2) can be combined as

$$\frac{dA_{\rm B}}{dt} = I(t) \cdot k_{\rm in}^0 - k_{\rm out} \cdot A_{\rm B}$$
⁽⁴⁾

As observed by Kong *et al.* (8), the pharmacokinetics of MP after intravenous bolus administration may be described by

$$C_{\rm MP} = C_{\rm MP}^0 e^{-k_{\rm el} \cdot t} \tag{5}$$

where $C_{MP}^{0} = C_{MP}$ at time (t) = 0 and k_{el} is the first-order elimination rate constant for MP ($\bar{x} = 0.29 h^{-1}$). In characterizing MP pharmacodynamics with Eqs. (3) and (4), WBH is substituted for A_B and the time pattern for response is used to generate the rate constants k_{out} , k_{on}^{0} , and IC_{50} .

The initial estimates of some of the parameter values can be obtained by inspection of data curves. Figure 2 is representative of the basopenia and diminution of *WBH* observed following steroid exposure. This curve can be divided into four distinct regions, each providing insight to the model.

The initial slope of the cell number vs. time curve, when the first part of Eq. (1) is negligible (i.e., when $C_{\rm MP} \gg IC_{50}$), yields an approximation of $k_{\rm out}$

$$\lim_{t \to 0} \frac{dA_{\rm B}}{dt} = -k_{\rm out} \cdot A_{\rm B}^0 \tag{6}$$

As steroid concentrations decline to low values $(C_{MP} \ll IC_{50})$ providing little or no effect, the slope approaches zero at the nadir $(t = t_{min})$. The curve characterizing the return to baseline is a complex relationship of k_{out} , k_{in}^0 ,



Fig. 2. Depiction of blood basophil cell number as a function of time after methylprednisolone administration. The four major phases of the curve are marked where *ABEC* is the area between the baseline and effect curve.

 IC_{50} , and the disposition of drug. However, as shown by Kong *et al.* (8), it can be approximated by

$$(A_{\rm B})_{t>t_{\rm min}} \approx A_{\rm B}^0 \cdot I(t) \tag{7}$$

Because the steady state flux of basophils is zero at baseline or time 0, the product of k_{out} and baseline WBH supplies an initial estimate of k_{in}^0 .

At the nadir (t_{\min}) of the cell number vs. time curve a pseudo steady state is achieved, hence

$$\lim_{t=t_{\min}} \frac{dA_{\rm B}}{dt} = I_{\min} \cdot k_{\rm in}^0 - k_{\rm out} \cdot A_{\rm B} = 0 \tag{8}$$

where I_{\min} , the inhibitory fraction at the nadir, is calculated from MP concentrations and estimates of IC_{50} (as will be described) according to Eq. (3). In turn, this equation can be rearranged to

$$I_{\min} = \frac{k_{\text{out}}}{k_{\text{in}}^0} \cdot A_{\text{B}}$$
(9)

Thus a plot of I_{\min} vs. WBH_{\min} values (i.e., A_B at the nadir) should yield a straight line with a slope of k_{out}/k_{in}^0 . Thus k_{in}^0 can be estimated after obtaining the initial slope estimate of k_{out} [Eq. (6)].

A summary parameter used to characterize the overall effect of the corticosteroid at each dosage level is the area between the baseline and the effect curve (ABEC) which was defined as

$$ABEC = WBH \cdot t_1 - AUHC_{0-t_1} \tag{10}$$

where WBH is the average baseline blood histamine concentration and AUHC is the area under the WBH vs. time curve after various doses of MP over the time interval of 0 to t_1 (see Fig. 2). In the present case, $t_1 = 32$. Integration of Eq. (4) (see Appendix) yields the following relationship:

$$ABEC = A_{\rm B}^0 \cdot t_1 - \frac{k_{\rm in}^0}{k_{\rm el} \cdot k_{\rm out}} \ln \left[\frac{IC_{50} + C_{\rm MP}^0 \cdot e^{-k_{\rm el} \cdot t_1}}{(IC_{50} + C_{\rm MP}^0) \cdot e^{-k_{\rm el} \cdot t_1}} \right]$$
(11)

When ABEC is plotted as a function of log AUC of the drug, it can be noted that the slope of the graph at high doses is $0.434k_{in}^0/k_{el} \cdot k_{out}$.

METHODS

The data fitted to the basophil cell trafficking model were originally reported by Kong et al. (8). Briefly, six healthy young males were given

intravenous injections of MP succinate (10, 20, and 40 mg of MP). Additionally, a control phase in which no steroid was given was included to assess the baseline values for WBH and cortisol. Blood samples were drawn at selected times over a 32-hr period. Plasma was analyzed for steroids by HPLC. Aliquots of whole blood were assayed for WBH by radioimmunoassay (BIOMERICA, Newport Beach, CA). It was necessary to omit the data from one subject because his WBH, before and after steroid, were typically near or below the minimum detectable concentration.

The model was fitted to the data using PCNONLIN (Statistical Consultants Inc, Lexington, KY). Initial parameter estimates and initial conditions were obtained from WBH vs. time plots. The values of k_{in}^0 , k_{out} , and IC_{50} were then obtained in the regression analysis. Simulations of model expectations were also carried out using the PCNONLIN program.

The general linear models procedure in SAS was utilized to detect significant variances in pharmacodynamic parameters estimated for different doses. The Tukey Multiple Comparison test was used to test for significance in the differences between means. All statistical procedures were performed with the p < 0.05 level indicating significant differences.

RESULTS

As discussed previously (8), the pharmacokinetics of MP were well described with a monoexponential equation [Eq. (5)]. The average values of V_{ss} and CL calculated by noncompartmental analysis were 1.23 (SD = 0.24) L/kg and 353 (53) ml \cdot hr/kg resulting in a $t_{1/2}$ of 2.37 (0.23) hr. The plasma protein binding of MP was constant and averaged 78% bound. There were no apparent dose-dependent differences in pharmacokinetic parameters for MP over this dose range.

The suppression of *WBH* at three dosage levels of MP along with the model characterization of the data is shown in Fig. 3 for the average data and for a representative subject. Simultaneous curve-fitting of all three dosage levels were carried out. The curves show the classic suppression pattern as described in Fig. 2. The larger doses of MP produced a more profound and prolonged effect. Parameters of the pharmacodynamic model are listed in Table I. The values of k_{out} , k_{in}^0 , and IC_{50} were similar for the 3 dosage levels and for the simultaneous fitting. No statistically significant differences in these parameters were detected between these groups. The quality of the fitting (lack of systematic deviations between actual and fitted data) and the lack of differences in parameter values between doses indicates that the model successfully recreated the overall behavior of this biological response. However, with only 5 subjects it may not be possible to detect



Fig. 3. Composite graph showing whole blood histamine (*WBH*) vs. time for 3 dosage levels of *MP* with depiction of the average data $(\pm 1 \text{ SD})$ for 5 subjects (top), and one individual subject (bottom). Solid lines were generated by using nonlinear least-squares regression to fit the model to data from all dosage levels simultaneously.

Parameter	Individual means $(n = 5)^a$ Methylprednisolone (mg)			
	10	20	40	Simultaneous ^b
k_{out} (hr ⁻¹)	0.243	0.311 (0.132)	0.358	0.277 (0.052)
$k_{\rm in}^0 ({\rm ng}/{ m ml}{ m hr})$	5.55 (1.29)	7.55 (4.05)	8.25 (2.54)	6.10 (1.22)
$IC_{50} (ng/ml)$	5.96 ^c (6.89)	8.85 (5.58)	6.62 (6.31)	8.06 ^c (5.76)

Table I.	Pharmacodynamic Model Parameters for WBH	after
	Three Dose Levels of Methylprednisolone	

^aIndividual means (SD) were found by fitting the dosage groups individually. ^bAll data from each subject were fitted simultaneously.

 $^{c}IC_{50}$ from Subjects 2 and 3 excluded for 10 mg dose.

^d Differences between the fitting groups were not statistically significant.

only 3 dynamic and 2 kinetic parameters were needed to reasonably characterize the effects from all dosage levels simultaneously; i.e., k_{out} , k_{in}^0 , IC_{50} , V_{ss} , and CL.

Figure 4 is a correlation plot relating I_{\min} , the suppression factor, to the WBH at the nadir. In principle if the IC_{50} is known or can be estimated in order to calculate I_{\min} , a linear relationship is found with the slope approximately equal to k_{out}/k_{in}^0 . In the present case, the slope of the plot (0.0414) agrees well with the ratio obtained by simultaneous curve fitting $(k_{out}/k_{in}^0 = 0.0454)$. The graph also provides a method of assessing the general dynamic behavior of individual data from a group of subjects. Our subjects showed reasonably consistent responses.

The basophil cell trafficking model was used to extrapolate the net pharmacodynamic effects of MP over a broad range of doses (Fig. 5). When very low doses of steroid were simulated, the initial decline of WBH was not monoexponential as seen with higher doses. Because the IC_{50} is not exceeded for appreciable lengths of time with small doses, the initial slope is a hybrid of k_{out} and $k_{in}^0 \cdot I(t)$. With larger doses the duration of the monoexponential phase and the time until the nadir occurs (t_{min}) both



Fig. 4. The relationship of I_{\min} and WBH_{\min} at the nadir of basopenia following MP administration. This plot was derived from Eq. (9) and the least-squares slope of the plot equals 0.0414.



Fig. 5. Simulations of WBH concentrations vs. time (top), and methylprednisolone plasma concentrations (bottom) following doses of 1, 10, 20, 40, and 100 mg. Curves were generated from the basophil cell trafficking model using typical values for cell movement, IC_{50} , and MP pharmacokinetics. The triangles mark the time of occurrence of the IC_{50} value for each dosage level.

increase. There is also a dose-related decrease in the WBH at the nadir. It can be seen that the trough occurs at or somewhat before MP concentrations fall to the IC_{50} value. This provides a means of estimating the IC_{50} for use in Eq. (9). Very high doses will cause a maximum diminution of WBH to undetectable values with a broad and extended nadir; however, the duration of the response is prolonged until the steroid concentrations fall well below the IC_{50} and sufficient time elapses for k_{in}^0 to be fully operative.

The overall response measured as *ABEC* [Eqs. (10) and (11)] versus the *AUC* of MP (equivalent to C_{MP}^0/k_{el}) is shown in Fig. 6. In each case t_1 allowed for return of cells to baseline. The *ABEC* exhibited an initial curved portion with an apparent threshold. Subsequently, *ABEC* increased as a linear function of the logarithm of MP *AUC*. There is no plateau in the response curve: larger steroid doses simply cause a more prolonged effect (see Fig. 5).

The mathematical definition of *ABEC* was confirmed using differential equations to simulate the response pattern as a function of dose or C_{MP}^0 .



Fig. 6. The area between the baseline and effect curve (ABEC) a measure of net response, is plotted vs. the log of MP AUC. The solid line depicts the model expectations for ABEC over a broad range of MP doses. Symbols show average $(\pm SD)$ data from two studies: \bigcirc (ref. 8) and \blacktriangle (ref. 21).

In turn, the upper linear slope of Fig. 6 (plotted as log AUC) was identified as $0.434 \cdot k_{in}^0/k_{el} \cdot k_{out}$, and is thus a function of two intrinsic parameters of the cells and two of the drug (i.e., $k_{el} = CL/V_{ss}$).

DISCUSSION

The basophil cell trafficking model was devised to quantitatively assess the time course and extent of corticosteroid-induced basopenia and define parameters of cell movement and steroid sensitivity following MP administration. The model has flexibility in potentially allowing any dosing or disposition function to be used as the pharmacokinetic input. Thus, it can be used to characterize the effects of complicated dosing regimens, other corticosteroids, or changes in pharmacokinetics caused by disease states and drug interactions. However, such applications require use of the differential Eq. (4) with insertion of the appropriate pharmacokinetic function in the I(t) relationship [Eq. (3)]. An integrated relationship such as Eq. (A3) is cumbersome to use and would require rederivation for non-iv bolus administration of drug.

The teleological derivation of this model predicts that if the plasma steroid concentration reflects the free (cytosolic) drug concentration at the receptor site then the IC_{50} value will reflect the receptor dissociation constant (K_D) . The average IC_{50} value from simultaneous fittings (Table I) is about

22 nM. Literature values for MP K_D in human tissues are 9.8 and 43 nM (12,13). This close correspondence between IC_{50} and K_D indicates that the physiological response to corticosteroids in the basophil cell trafficking model may reflect intrinsic receptor binding.

The mechanism by which corticosteroids affect basophil trafficking is not known (4). However, the first level of traffic control for other leukocytes involves binding to venular endothelium (14). The extravasation process is highly specialized for different cell types. The processes involved with respect to lymphocytes include the presence of a number of adhesion molecules on the cell and the occurrence of tissue address signals termed "vascular addressins." In addition, other cells express homing receptors for peripheral lymph nodes. We assume that corticosteroid binding to basophils results in some type of altered affinity of the cells for extravascular tissues causing a transient retention. Schleimer (15) hypothesized that glucocorticoids act by preventing the release of factors that initiate basophil recruitment rather than the adhesive response per se. However, this does not explain the present responses that occur in the absence of inflammation. In any case, the therapeutic benefit may include a reduction in histamine release by prevention of basophil access to inflammatory sites such as the lung in asthmatic patients.

Simulations using this model can be a useful tool for predicting the response to corticosteroids under a variety of conditions; however, extrapolating to larger or chronic doses requires caution. Considerations such as synthesis and/or loss of cells from the circulating pool, down-regulation of steroid receptor content, and the contribution of endogenous steroids need to be more closely examined. Interpretation of the model parameters must also be done with caution, particularly the significance of k_{in}^0 and k_{out} . The value of k_{out} most likely reflects the major rate-limiting process for cells exiting the blood. Presumably, k_{in}^0 is a hybrid consisting of cells returning to the bloodstream from a collection of nonhomogeneous tissue compartments, the sum of which constitutes the extravascular compartment in the model. Individual tissue sites may exhibit unique characteristics.

Also, reports that the total circulating pool of basophils consists of two subsets containing differing amounts of histamine (6) and different sensitivities to prednisolone (7) should be addressed in further studies.

Oosterhuis *et al.* (16) used a variation of the Sheiner hypothetical effect compartment model to characterize the lymphopenic effect of prednisolone. In this approach, the hysteresis of the effect versus drug concentration curve was accounted for as the time required for diffusion of drug into an effect compartment. The time at which peak concentrations in this compartment occurs is the same independent of dose, hence the maximum effect (nadir) should occur at the same time regardless of dose. This is not consistent with the data observed in our study or theirs; the changes in their parameter values related to dose reflect this inconsistency. Hysteresis in the basophil model is more aptly attributed to the efflux and return of cells.

Kong *et al.*'s (8) direct effect model used the sum of an exponential exit of cells from the blood and the product of baseline *WBH* and a sigmoidal fractional effect term to characterize this response. This model works for larger iv bolus of methylprednisolone but is handicapped by the requirement that C_p^0 must be well in excess of the IC_{50} . The present model produces a slightly larger estimate of the IC_{50} than that of Kong *et al.* (8 vs. 3 ng/ml).

Bloemena et al. (17) adapted a two-compartment pharmacokinetic model with peripheral elimination to account for the distribution of circulating lymphocytes and effects of prednisolone in rabbits. Although they did not apply a response function such as our I(t) equation, they arrived at a similar conclusion to ours that prednisolone reduces the influx of circulating cells from peripheral sites to blood.

The onset of steroid-induced basopenia is rapid with diminution of WBH seen immediately following dosing. Conversely, gene-mediated effects of corticosteroids, such as tyrosine aminotransferase induction (18), typically exhibit a lag time in which gene transcription and *de novo* protein synthesis occur. Various authors (19, and reviewed in ref. 8) have discussed immediate steroid effects which act through the receptor but occur too rapidly to be the result of new protein synthesis. The rapid onset of basopenia is attributed to the drug-receptor complex rapidly preventing cell return to blood (8).

A high incidence of side effects (20) necessitates caution in corticosteroid dosing. Clinicians often prescribe large single daily doses. In accordance with Figs. 5 and 6, the response pattern is dictated by the time that MP plasma concentrations exceed the IC_{50} . A steroid dose-sparing effect may also be achieved from two or more smaller doses which reduce total steroid exposure. We tested and confirmed this hypothesis in a limited clinical study (21).

An important extrapolation of this model is that the dose-response curve for corticosteroid effects has no upper plateau (Fig. 6). Indeed, larger doses of corticosteroids simply prolong the cell trafficking response by maintaining plasma concentrations above the IC_{50} (Fig. 5). Although our study employed only a limited dosage range of MP, support for the profile seen in Fig. 6 was found by Derendorf *et al.* (22) who used much greater dosages of MP to assess various blood cell response patterns.

The proposed cell trafficking model has the potential to characterize steroid-induced changes in the distributional patterns of a variety of circulating cells. The time course of the diminution of eosinophils, monocytes,

and lymphocytes is identical in pattern to basopenia. Neutrophils, which increase in circulating numbers, might be described by an altered version of the model in which the movement of cells into the blood is enhanced by corticosteroids.

The basophil cell trafficking model presents equations, estimation techniques, and extrapolations to evaluate the non-gene-mediated dose/response relationship of corticosteroids. This approach of physiological pharmacodynamic modeling may be used to evaluate alterations in the kinetics and dynamics of various steroids in the presence of disease states and drug interactions. We have extended this work to other cell types such as T-helper (CD4⁺) lymphocytes, incorporating their baseline circadian patterns in the model (23).

SYMBOLS

A_{B}	Number of cells in blood compartment
$A_{\rm E}$	Number of cells in extravascular compartment
A_{T}	Total number of cells $(A_{\rm B} + A_{\rm E})$
ABEC	Area between the baseline and decline in cell number curve
AUHC	Area under the WBH versus time curve
AUC	Area under the drug concentration versus time curve
$C_{\rm MP}$	Plasma concentration of drug
CL	Clearance of drug
I(t)	Fractional inhibition function
I_{\min}	Inhibitory fraction at the nadir
IC_{50}	Concentration of drug causing 50% inhibition of k_{in}
$k_{\rm in}, k_{\rm in}^0$	Rate constant for return of basophils to blood
kout	Rate constant for efflux of basophils from blood
$k_{\rm el}$	Rate constant for drug elimination
t	Time
t_1	Time at completion of cell trafficking response
t _{min}	Time at occurrence of nadir in blood cell number
$V_{ m ss}$	Volume of distribution of drug
WBH	Whole blood histamine concentration

ACKNOWLEDGMENTS

We appreciate the participation of Prof. Richard Slaughter and Drs. Ah-Ng Kong, Elizabeth A. Ludwig, Providence M. DiStefano, James DeMasi, William G. Reiss, and Elliott Middleton, Jr. in the original clinical pharmacodynamic studies (refs. 8 and 21). Ms. Nancy Pyszczynski provided technical assistance.

APPENDIX

An integrated solution to define the determinants of ABEC can be found as follows. Combining Eqs. (3) to (5) yields

$$\frac{dA_{\rm B}(t)}{dt} = \frac{IC_{50} \cdot k_{\rm in}^0}{IC_{50} + C_{\rm MP}^0 e^{-k_{\rm el}t}} - r_{\rm out} \cdot A_{\rm B}(t)$$
(A1)

Multiplying both sides of Eq. (A1) with dt yields

$$dA_{\rm B}(t) = \frac{IC_{50} \cdot k_{\rm in}^0 dt}{IC_{50} + C_{\rm MP}^0 e^{-k_{\rm ef}t}} - k_{\rm out} \cdot A_{\rm B}(t) dt$$
(A2)

Integrating both sides of Eq. (A2) from time 0 to t yields

$$A_{\rm B}(t) - A_{\rm B}(0) = \frac{k_{\rm in}^0}{k_{\rm el}} \cdot \ln \frac{IC_{\rm 50} + C_{\rm MP}^0 e^{-k_{\rm el}t}}{[IC_{\rm 50} + C_{\rm MP}^0] \cdot e^{-k_{\rm el}t}} - k_{\rm out} \cdot \int_0^t A_{\rm B}(t) dt \quad (A3)$$

Since $A_B(t) = A_B(0)$ at $t = t_1$, from Eq. (A3) it follows that

$$\int_{0}^{t_{1}} A_{\rm B}(t) dt = \frac{k_{\rm in}^{0}}{k_{\rm el} \cdot k_{\rm out}} \cdot \ln \frac{IC_{\rm 50} + C_{\rm MP}^{0} e^{-k_{\rm el}t_{\rm I}}}{[IC_{\rm 50} + C_{\rm MP}^{0}] \cdot e^{-k_{\rm el}t_{\rm I}}}$$
(A4)

Thus, by definition

$$ABEC = A_{\rm B}(0) \cdot t_1 - \int_0^{t_1} A_{\rm B}(0) dt$$
$$= A_{\rm B}(0) \cdot t_1 - \frac{k_{\rm in}^0}{k_{\rm el} \cdot k_{\rm out}} \cdot \ln \frac{IC_{50} + C_{\rm MP}^0 \cdot e^{-k_{\rm el}t_1}}{[IC_{50} + C_{\rm MP}^0] \cdot e^{-k_{\rm el}t_1}}$$
(A5)

In the above ln quotient, $IC_{50} \gg C_{MP}^0 \cdot e^{-k_{el} \cdot t_1}$ in the numerator at late times when the trafficking change is back to baseline. Also, for large doses of drug, $C_{MP}^0 \gg IC_{50}$ in the denominator. Further, $C_{MP}^0 = AUC \cdot k_{el}$. This allows Eq. (A5) to simplify to

$$ABEC \approx A_{\rm B}(0) \cdot t_1 + \ln IC_{50} + \ln k_{\rm el} - k_{\rm el} \cdot t_1 + \frac{k_{\rm in}^0}{k_{\rm el} \cdot k_{\rm out}} \cdot \ln AUC \quad (A6)$$

While the combination of constants constituting the intercept is not meaningful, the slope of a plot of *ABEC* vs. log *AUC* (for larger doses) yields an estimate of $0.434 \cdot k_{in}^0/k_{el} \cdot k_{out}$.

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