

Labile cochlear tuning in the mustached bat

I. Concomitant shifts in biosonar emission frequency

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Summary. The cochlea of the mustached bat (*Pteronotus parnellii*) has sharp tuning characteristics and pronounced resonance within a narrow band near the second harmonic, constant frequency (CF2) component of the animal's biosonar signals. That fine frequency discrimination occurs within this narrow band is evident from Doppler-shift compensation, whereby bats in flight lower the frequency of emitted CF2s to maintain returning echoes within this band. This study examined various factors capable of producing shifts in both the cochlear resonance frequency (CRF) and CF2s emitted by stationary bats and bats actively Doppler-shift compensating on a pendulum. Each of three experimental factors shifted the CRF in a reversible manner. Changes in body temperature produced an average CRF shift of 39 ± 18 Hz/°C. The CRF increased with flight by 150 ± 100 Hz and returned to baseline values within 10 min after flight. Contralateral sound exposure produced smaller (100 ± 20 Hz), rapid shifts in the CRF, suggesting that a mechanism different from the temperature- and flight-related shifts was involved. Changes in the CRF induced by temperature and flight were accompanied by shifts in the emitted CF2 of stationary and moving bats. Coupled with a companion study of associated shifts in neural tuning, the concomitant changes in CRF and CF2 provide evidence of cochlear tuning lability in the mustached bat.

Key words: Cochlea – Echolocation – Resonance – Body temperature – *Pteronotus*

Introduction

The mustached bat, *Pteronotus parnellii parnellii*, uses biosonar to obtain an acoustic image of its surroundings and to detect and track insect prey. The biosonar signals are 6–32 ms pulses that consist of at least 4 harmonics, the second of which is the most prominent (Novick and Vaisnys 1964; Henson et al. 1987; Gaioni et al. 1990). Each harmonic contains a long, constant frequency (CF) component bracketed by short initial, and terminal frequency sweeps. The CF of the second harmonic (CF2) is near 60 kHz, and is called the “resting frequency” when emitted from a stationary bat. The resting frequency varies from bat to bat (60 to 64 kHz); however, for an individual bat under constant conditions, it is relatively invariant.

Inherent in echolocation by mustached bats is a precise regulation of the biosonar signals in response to changing echo parameters (Schnitzler 1970a, b; Henson et al. 1980, 1982; Jen and Kamada 1982; Kobler et al. 1985; Suga et al. 1987; Gaioni et al. 1990). This is best exemplified by “Doppler-shift compensation,” whereby the frequency of the emitted CF2 is changed during flight to match the Doppler-shift in returning echoes. Thus, the echo CF2s are maintained within a narrow band, called the “reference frequency” (Schnitzler 1970a, b). As shown in Fig. 1, Doppler-shift compensation is easily observed by recording biosonar pulses and echoes from bats during forward swings on a pendulum.

It seems clear that Doppler-shift compensation requires a fine resolution of frequencies near 60 kHz. Therefore, it is not surprising that the cochlea of the mustached bat possesses many adaptations for sharp tuning. Relative to body size, the cochlea is much larger than that of most mammals, and for the matter, of most bats. The stimulated cochlea exhibits remarkably sharp tuning and pronounced resonance near the animal's CF2, and this resonance is thought to be a product of the mechanical properties responsible for sharp tuning in the 60 kHz portion of the cochlea (Pollak et al. 1972,

Abbreviations: CF2, second harmonic, constant frequency component of the biosonar signal; CM, cochlear microphonic; CRF, cochlear resonance frequency

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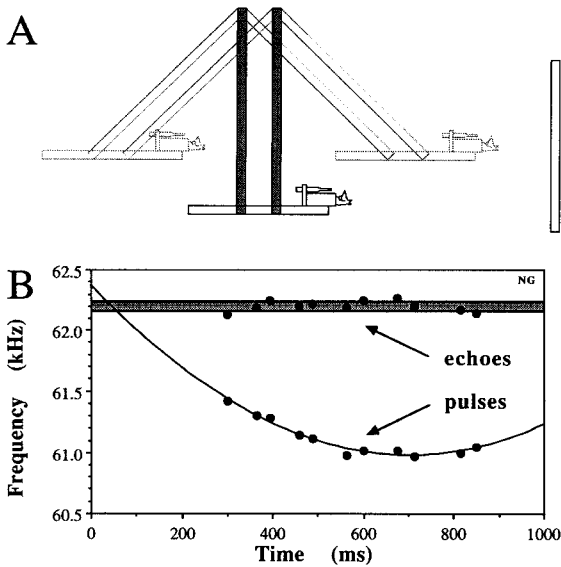


Fig. 1A, B. Doppler-shift compensation on the pendulum. **A** Pendulum design. During a forward swing, emitted pulses and echoes were recorded with a microphone mounted on the pendulum. For each forward swing, there was a period of positive acceleration as the pendulum approached the lowest point of its arc, followed by a negative acceleration as the pendulum approached zero velocity near the target. **B** Plot of the frequencies and times of occurrence of CF2 pulse-echo pairs for a single forward swing. Doppler-shift compensation is evident from the change in pulse frequency, which changes with the velocity of the pendulum. The relatively narrow, shaded band represents the mean reference frequency for this swing \pm one standard deviation (62.20 ± 0.04 kHz). The curve is a second order binomial regression of the pulse frequencies ($r^2 = 0.98$); $r = 0.99$ ($P < 0.001$, two-tailed t -test, $t = 21.0$, $\rho > 0.95$ for $P < 0.05$)

1979; Suga et al. 1975; Suga and Jen 1977; Henson et al. 1982, 1985, 1990; Kössl and Vater 1985a, 1990b; Vater 1988). Cochlear resonance and sharp tuning are easily revealed by recording cochlear microphonic (CM) potentials. The CM audiogram has an unusually sharp tuning curve, the tip of which is at the cochlear resonance frequency (CRF). Spectral analysis of the CM elicited by broadband noise shows that much of the spectral energy is at the CRF (Fig. 2). The sharply tuned portion of the cochlea is disproportionately long and densely innervated, and possesses several structural specializations (Kössl and Vater 1985b; Henson and Henson 1988, 1991; Zook and Leake 1989; Vater 1987). From anatomical and physiological evidence, it is clear that the narrow band centered around the bat's CF2 is overrepresented at the level of the cochlea and at every level of the auditory pathway (Suga and Jen 1976; Suga et al. 1975, 1987; Pollak and Bodenhamer 1981; Zook and Leake 1989; Zook et al. 1985; Ross and Pollak 1989; Ross et al. 1988; Kössl and Vater 1990a; Covey et al. 1991; Olsen and Suga 1991; Pollak and Casseday 1989).

Cochlear resonance in the mustached bat provides an attractive model for studies of cochlear micromechanics, and especially resonant components that appear to create sharp tuning (Davis 1983; De Boer 1983a, b, c; Kim et al. 1980; Neely and Kim 1983, 1986; Zwislocki 1980; Zwislocki and Kletsky 1980). Recent studies with

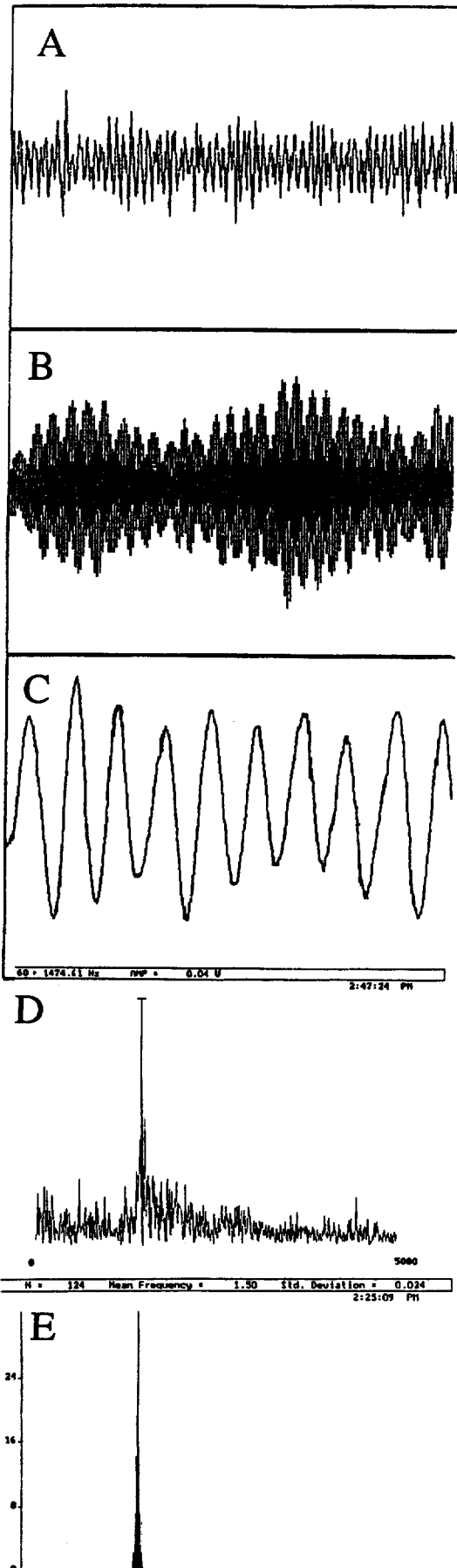
the mustached bat have found that flight activity and body temperature produce changes in the CRF, and that these changes are accompanied by shifts in the CF2 of emitted pulses (Henson et al. 1990; Huffman et al. 1991). In light of these findings, a precise understanding of CRF lability and its correspondence with changes in the CF2 is necessary if resonant features in this bat are to contribute further to general theories of sharp tuning, and to specific theories of biosonar signal processing. The purpose of this study was to expand these preliminary studies and provide quantitative descriptions of CRF and CF2 lability. This work was also the basis for developing methods to manipulate the CRF and examine its effects on the frequency tuning of auditory neurons. The neurophysiological data are presented in a companion paper (Huffman and Henson 1992).

Methods

This study reports data obtained from 23 mustached bats, *Pteronotus parnellii parnellii*, from Jamaica, W.I. For each type of experiment described (but not necessarily for each bat), 3 frequency measurements were routinely made: the CRF, the resting frequency and the reference frequency.

Cochlear resonance was measured in 11 bats with chronically implanted CM electrodes. For electrode implantation, hair was removed from the scalp with a depilatory agent (Nect) and the skin was cleaned. Bats were then anesthetized with an inhalant, methoxyflurane (Metofane, Pitman-Moore, Inc). A posterior skin incision was made over the dorsal part of the skull and the underlying part of the temporalis muscle was removed bilaterally. The bone was then cleaned, dried and coated with a thin layer of cyanoacrylic adhesive (Loctite, Superbond 409 gel). A tungsten ground electrode was implanted in the cerebral cortex. A hole was drilled near the lambda ridge, 2.4 mm from midline, and a teflon-coated tungsten electrode was stereotaxically advanced toward the cochlear aqueduct. When high amplitude CM potentials were evident in response to broadband acoustic stimuli, the electrode was glued in place. Care was taken not to penetrate the aqueduct. All experiments were conducted with bats that were awake and fully recovered from anesthesia and surgery. During CM recordings bats were held in a suspended, loose-fitting styrofoam mold to allow body movement, while the head was immobilized with a pin vise attached to the ground electrode.

Continuous cochlear resonance was evoked by low-level (approx. 35 dB SPL) broadband noise (Fig. 2). The CRF is known to be constant at low to moderate SPLs, but not at high levels (Henson et al. 1990); therefore, all measurements of CRF were conducted with stimulus levels which produced CM potentials just noticeable above the noise floor. The signal from a random noise generator (General Radio Co., Type 1390-B) was fed to a one-inch electrostatic speaker (Polaroid Corp.). The speaker was 15 cm from the pinna, 20° from midline, and positioned to yield the highest amplitude CM in response to low-level stimulation. The CM was amplified (EG&G Model 113 preamplifier, Princeton Applied Research), narrow-bandpass filtered (TTE, Inc. Model K18 E3007, 3 dB points at 59.65 and 64.0 kHz), and heterodyned with a signal near 60 kHz to increase frequency resolution and reduce the required sampling rate (Fig. 2C). The CRF was obtained from spectral analysis of the heterodyned output (spectrum analyzer/digital oscilloscope, Model R350, Rapid System Inc.). FFTs were collected at a rate of 200/min with a resolution of ± 10 Hz. Each FFT contained a single, sharp spectral peak (Fig. 2D). Spectral peak values were displayed as a histogram, and the CRF was determined by the mean of the histogram (Fig. 2E). The standard deviations of histograms normally ranged from 10 to 30 Hz. Each histogram established the CRF value for periods ranging from 15–120 s, and



several histograms were averaged to obtain mean CRF values for longer periods.

Body temperature was controlled with a heat lamp positioned 30 cm from the bat. The lamp was adjusted to low heat levels with a rheostat to either sustain or increase the body temperature. Body temperature was kept within or near the range normally found in active mustached bats (37–42 °C). During experiments, each episode of heat exposure was limited to 50 min or less, and water and mealworms were offered every 1–2 h. Body temperature was monitored with a thermocouple probe (Sensortek, Inc., Models IT-18 and IT-21) and recording device (Sensortek, Inc., Model BAT-12) which allowed measurements with an accuracy of ± 0.05 °C. The probe was positioned in the midline of the deep skin fold between the occiput and the back. A control experiment was conducted to examine the accuracy of reported body temperature changes at this recording site. During trials similar to that shown in Fig. 3, body temperature was recorded simultaneously from two probes, one at the skin fold, and a second chronically placed in the parafloccular fossa of the cranial cavity. Although the absolute temperature values were slightly different, the changes in temperature recorded from these two positions were nearly identical (within 0.1 °C). Similar results were previously reported for a comparison between measurements in the skin fold and under the temporalis muscle (Henson et al. 1990). It should be noted that dorsal, subcutaneous probe placements have been found to provide accurate measures of deep body temperature in other small bats (Brown and Bernard 1991).

The resting frequency (CF2 emitted by stationary bats) was determined from the biosonar signals of bats placed in a small cylindrical cage (21.6 cm diameter; 21.6 cm long). Emissions were recorded with a 6.25 mm Brüel and Kjaer condenser microphone (Model 4135) and associated amplifier (Model 2608). Signals were treated in the same manner as the CM: they were narrow bandpass filtered to isolate the CF2, and then heterodyned with a signal near the CF2 to increase frequency resolution (to ± 10 Hz) and reduce the required sampling rate. Each filtered, heterodyned CF2 pulse triggered an FFT analysis of the pulse by the spectrum analyzer (mentioned above), which yielded a sharp spectral peak. In similar fashion to analysis of CM FFTs, 100–200 CF2 FFTs were collected and displayed as a histogram of spectral peaks to determine the mean resting frequency. Standard deviations normally ranged from 20 Hz to 50 Hz.

The reference frequency (CF2 of echoes returning to Doppler-shift compensating bats) was determined from bats placed on a pendulum and swung toward a target (Fig. 1A). Biosonar pulses and Doppler-shifted echoes were recorded with a microphone mounted on the pendulum. These signals were stored on a precision magnetic tape system (Racal Store 7DS, tape speed 15 or 30 inch/s). The filtered, heterodyned signals for each forward swing were collected by the spectrum analyzer and FFTs were performed on the CF2s of pulse-echo pairs. Individual values (± 10 Hz) were collected and graphed (Fig. 1B).

Results

CRF lability

The normally stable CRF could be reliably shifted by a number of physiological parameters, namely body temperature, flight and contralateral noise exposure. Of

Fig. 2A–E. Cochlear resonance and method of CRF determination. **A** Digitized sample of the low-level, broadband noise signal delivered to the ear. **B** Oscillographic display of the digitized, bandpass-filtered CM. **C** Waveform of the CM when heterodyned with a frequency near the CRF (10 kHz sample rate). **D** Single spectral peak of a 1024 point FFT of the heterodyned CM. **E** Histogram of 124 spectral peaks collected over 30 s

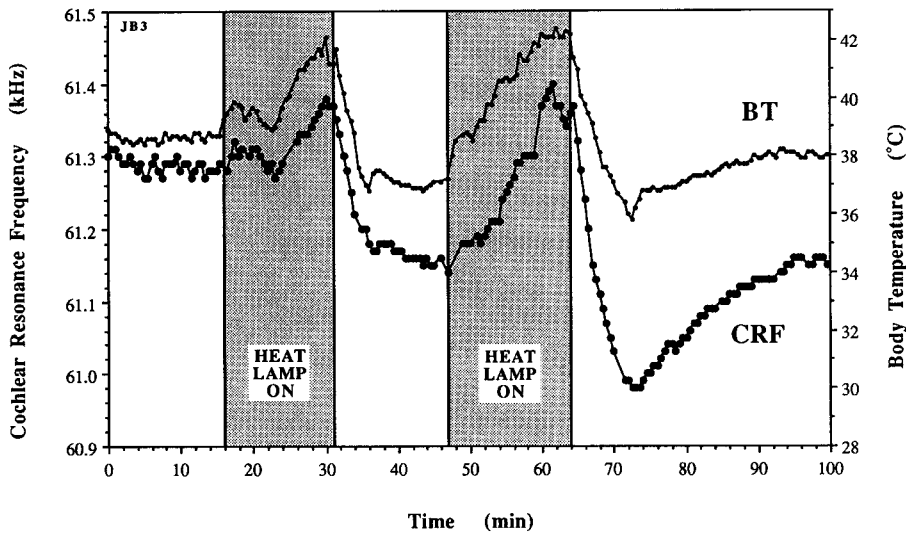


Fig. 3. Effect of heat lamp exposure on body temperature and the CRF. Body temperature was adjusted by turning a low-intensity heat lamp on and off for 2 consecutive trials

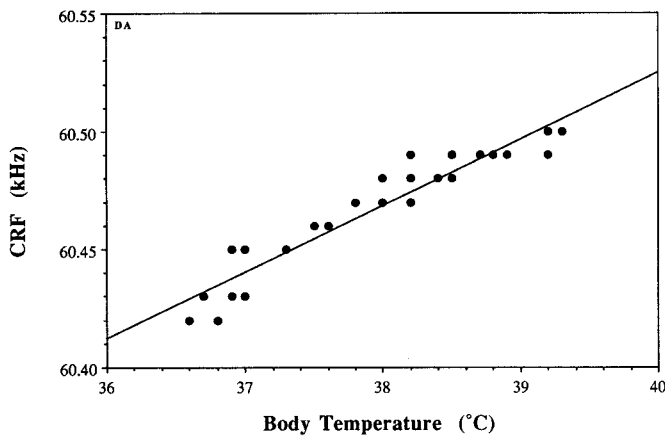


Fig. 4. Correlation of the CRF and body temperature ($r=0.96$; $P<0.001$, two-tailed t -test, $t=16.4$, $n=25$; $\rho>0.91$ for $P<0.05$). Data were obtained from a heat lamp experiment like that shown in Fig. 3. The slope of a simple regression line of the data ($r^2=0.92$) was used to estimate the rate of change in the CRF with body temperature ($28 \text{ Hz}/^\circ\text{C}$)

these, body temperature was the most easily controlled factor for effecting quantifiable shifts in the CRF. In all experiments where bats were exposed to a heat lamp, increases in body temperature were accompanied by upward shifts in the CRF; subsequent removal of the heat lamp produced downward shifts in body temperature and CRF ($n=11$ bats). Figure 3 shows typical results. In such trials, there was a high, positive correlation between CRF and body temperature for all bats (e.g. Fig. 4). Regressions like the one shown in Fig. 4 were calculated for 25 trials among 6 bats, for which data was sufficient to test the statistical significance of correlation (r) and regression (m) coefficients ($P<0.05$; two-tailed t -test). The mean shift in CRF (determined from regression slopes) was $39 \pm 18 \text{ Hz}/^\circ\text{C}$ ($N=25$; range = $18\text{--}74 \text{ Hz}/^\circ\text{C}$; $P<0.05$ in t -tests of r and m for each data set).

The effect of flight on the CRF was examined in 8 bats. In all cases, 5–15 min flights produced an increase

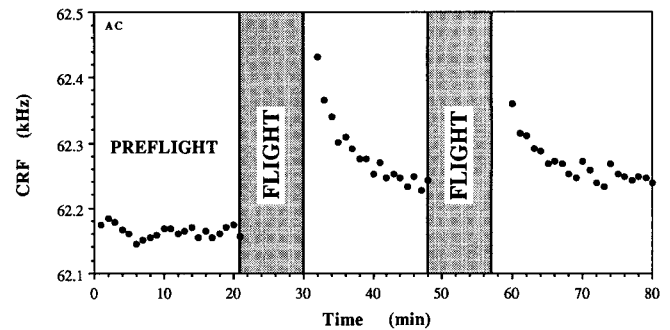


Fig. 5. Shifts in the CRF with flight. The CRF was elevated from preflight values, and decreased after each period of flight

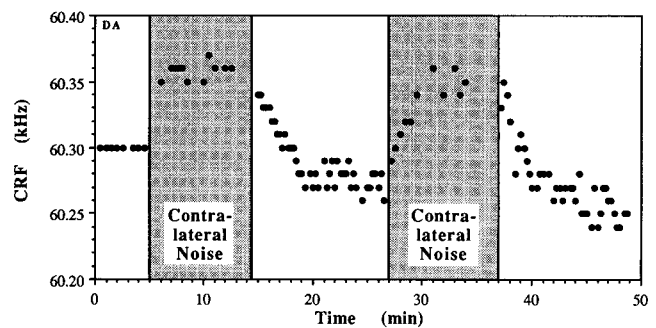


Fig. 6. Effect of contralateral noise exposure on the CRF. The CRF was shifted upward during periods of high-level noise presented to the contralateral ear. (See text for description.)

in the CRF from preflight values (Fig. 5). Initial CRF determinations after flight undoubtedly underestimated the size of the shift in resonance because of a 1–2 min delay necessary to attach the CM leads immediately after capture of the flying bat. The mean CRF shift measured 1–2 min after flight was $150 \pm 100 \text{ Hz}$ ($N=8$; range = $40\text{--}280 \text{ Hz}$). After each flight, the elevated CRF decayed to a new baseline level, usually within a 10 min period (mean decay = $180 \pm 80 \text{ Hz}$; $N=10$; range = $80\text{--}370 \text{ Hz}$).

Shifts in the CRF were also induced in 5 bats exposed to loud noise presented to the contralateral ear. Figure 6

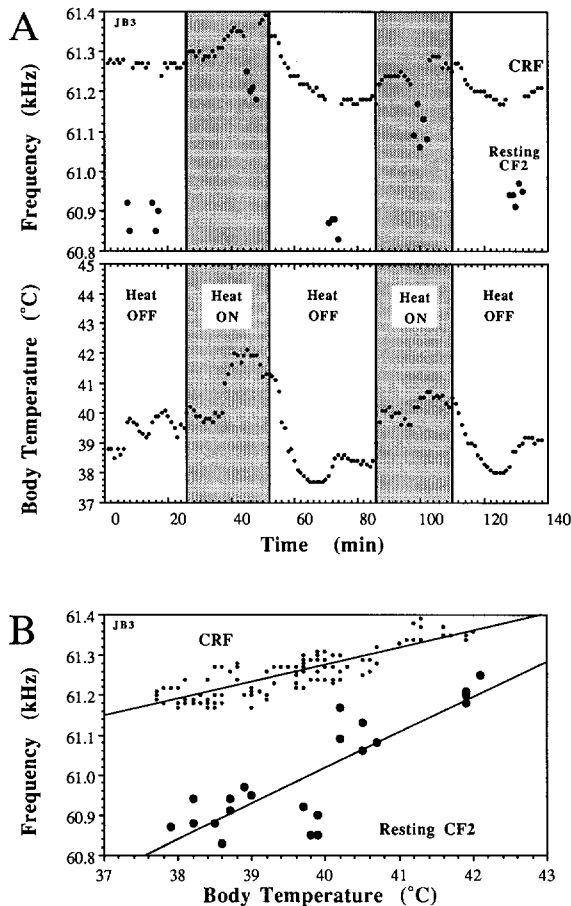


Fig. 7A, B. Concomitant shifts in the CRF and resting frequency with changes in body temperature. **A** Results of a single experiment in which the CRF and resting frequency were measured (top) as body temperature (bottom) was adjusted for 2 consecutive trials. **B** Correlations of the CRF ($r=0.84$; $P<0.001$, two-tailed t -test, $t=18.5$, $n=145$; $0.79<\rho<0.89$ for $P<0.05$) and resting frequency ($r=0.84$; $P<0.001$, two-tailed t -test, $t=7.09$, $n=23$; $0.65<\rho<0.94$ for $P<0.05$) with body temperature (data is from the experiment shown in A). In A and B, each CF2 data point represents 50–100 pulses

shows 2 consecutive trials for which the CRF was monitored during and after noise exposure. The CRF was measured continuously during alternating periods of low-level broadband noise (approx. 35 dB SPL output) presented to the ipsilateral (implanted) ear alone from a speaker 20 cm away, versus high-level noise (approx. 90 dB SPL output) presented to the contralateral ear alone from a funneled speaker 5 cm away. During the noise exposure condition, cochlear resonance was evoked by the contralateral noise; the small amplitude of the CM indicated that this stimulus level was comparable to the low levels of the ipsilateral stimulus alone. Contralateral noise produced a comparatively small and sustained increase in the CRF (mean = 100 ± 20 Hz; $N=10$; range = 70–130 Hz). Within several minutes after cessation of contralateral exposure, resonance evoked by low-level, ipsilateral noise returned to a baseline frequency.

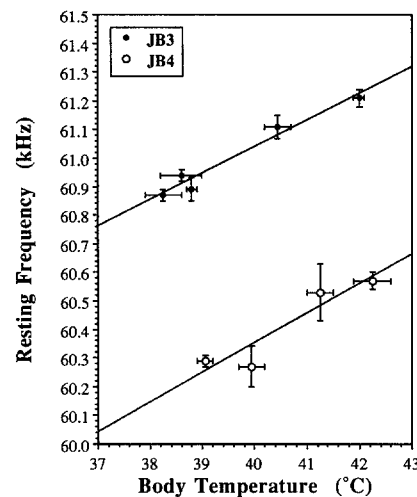


Fig. 8. Changes in the mean resting frequency throughout the day with fluctuations in body temperature for 2 bats. Each data point represents 100–200 pulses. Correlation coefficients are 0.98 ($P<0.005$, two-tailed t -test, $t=8.49$) and 0.94 ($0.05<P<0.1$, two-tailed t -test, $t=3.90$) for bats JB3 and JB4, respectively. Regressions were used to estimate the amount of shift in the resting frequency with respect to body temperature. The slopes of the regression lines are 93 Hz/°C ($r^2=0.96$) and 104 Hz/°C ($r^2=0.89$) for bats JB3 and JB4, respectively

Concomitant shifts in CRF and CF2

Factors that shifted the CRF, such as body temperature changes and flight activity, also caused shifts in the resting frequency of stationary bats, and in the reference frequency of Doppler-shift compensating bats. For example, in body temperature experiments like those mentioned above, where resting frequency was measured in addition to the CRF ($N=5$ bats), both CRF and resting frequency shifted with changing body temperature in all cases. Figure 7A shows typical results of these experiments, in which the CRF and resting frequency were positively correlated with body temperature (Fig. 7B). Trials with a sufficient number of data points to test for statistical significance of both correlation (r) and regression (slope) coefficients ($P<0.05$; two-tailed t -test) were used to estimate the amount of shift in resting frequency with body temperature. The mean shift in resting frequency (determined from regression slopes) was 93 ± 33 Hz/°C ($N=8$; range = 32–124 Hz/°C). In addition, the resting frequency was examined throughout the day in relation to fluctuating body temperature. As shown in Fig. 8, higher resting frequencies were associated with higher body temperatures; these shifts were equivalent (per °C) to the shifts observed with the heat lamp experiments.

Shifts in the resting frequency also occurred with periods of flight ($N=12$ bats). In cases where both the CRF and resting frequency were recorded, both were elevated after flight, and subsequently showed decreases to baseline values; these values were often below previous baseline levels (Fig. 9). The mean flight-induced shift from preflight values was 210 ± 100 Hz ($N=14$; range = 100–

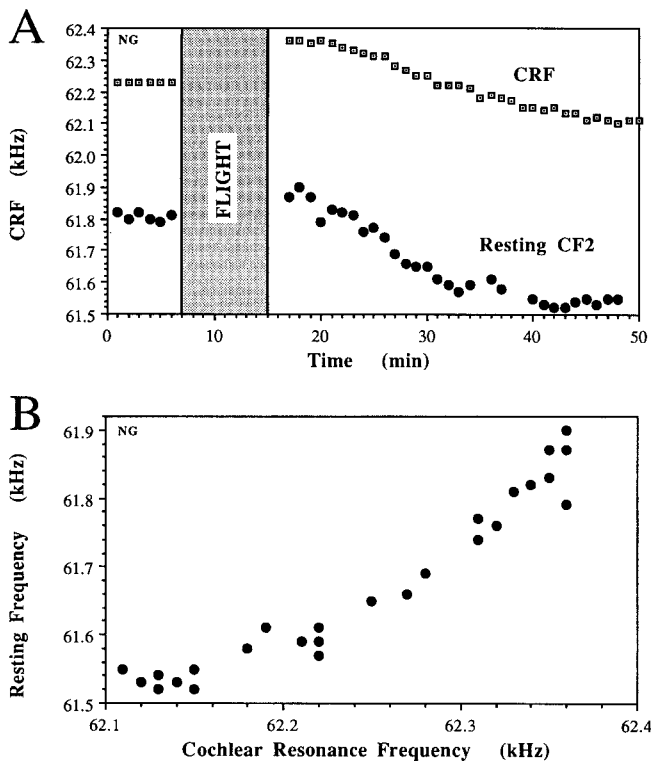


Fig. 9A, B. Concomitant shifts in the CRF and resting frequency with flight. **A** Preflight and postflight CRFs and resting frequencies for a single flight trial. **B** Correlation of the resting frequency and the CRF (postflight data from the experiment shown in **A**); $r=0.96$ ($P<0.001$, two-tailed t -test, $t=17.8$, $n=29$; $0.92<\rho<0.99$ for $P<0.05$). In **A** and **B**, each CF2 data point represents 20–50 pulses

460 Hz). The mean decrease observed in the period that followed flight was 230 ± 100 Hz ($N=14$; range = 80–470 Hz).

Changes in body temperature also caused shifts in the reference frequency of Doppler-shift compensating bats. Five bats were swung on a pendulum before and after exposure to a heat lamp, and temperature-dependent shifts in emitted pulses and echoes were recorded. Figure 10 shows examples of data acquired from pendulum swings. Shifts in reference frequency accompanied temperature-dependent changes in the CRF (Fig. 11). The mean shift in reference frequency was 90 ± 38 Hz/ $^{\circ}$ C ($N=6$; range = 49–136 Hz/ $^{\circ}$ C). Shifts in reference frequency and CRF were also observed for bats swung on the pendulum before and after flight (Fig. 12). The mean flight-induced shift from preflight values was 310 ± 180 Hz ($N=6$; range = 100–440 Hz).

In summary, temperature, flight and contralateral noise exposure induced reproducible shifts in the CRF. CRF shifts were matched by concomitant shifts in the CF2 emitted during echolocation, either from stationary or moving bats. This was best illustrated by the cases where the cochlear resonance, resting and reference frequencies were recorded concurrently from a single bat, for two different body temperatures (Fig. 13).

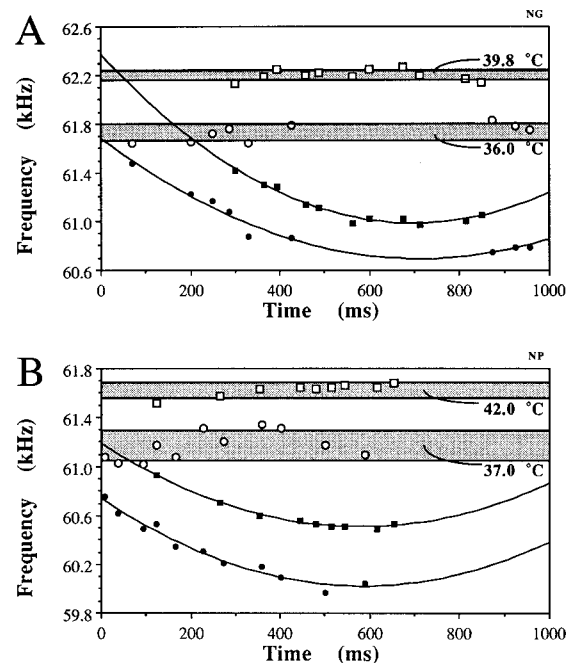


Fig. 10A, B. Two examples of the effect of body temperature on the reference frequency of bats swung on the pendulum, showing that bats maintain higher reference frequencies with increases in body temperature. The CF2s of pulses (filled symbols) and echoes (open symbols) are shown for forward swings recorded at 2 body temperatures (squares and circles, respectively). Shaded bands represent mean reference frequencies \pm one standard deviation. Curves are second order binomial regressions of the pulse frequencies (**A**: $r^2=0.97$ for both curves; **B**: $r^2=0.996$ and 0.97 for pulses at 42.0° C and 37.0° C, respectively; $P<0.001$ (two-tailed t -test) for r in all cases)

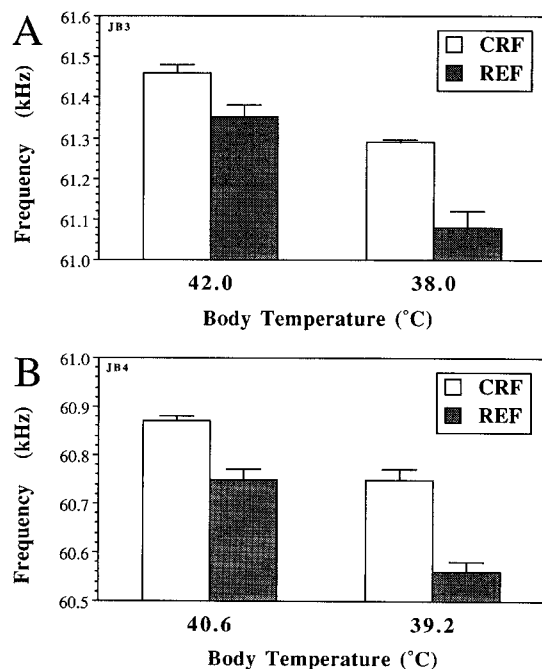


Fig. 11A, B. Shifts in the CRF and reference frequency (REF) with changes in body temperature for two bats. Reference frequency values represent the mean of echoes from 3–5 pendulum swings. Error bars indicate one standard deviation from the mean. Shifts in CRF and reference frequency are statistically significant ($P<0.05$, one-tailed t -test)

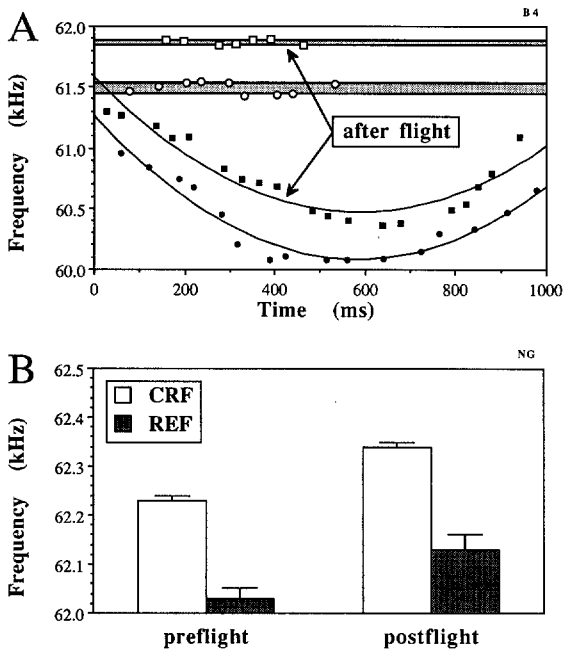


Fig. 12A, B. Shifts in the CRF and reference frequency with flight. **A** Flight-associated shifts in emitted pulses and echoes of bats swung on a pendulum. CF2s of pulses (*filled symbols*) and echoes (*open symbols*) are shown for forward swings recorded before (*circles*) and after (*squares*) flight. *Shaded bands* represent mean reference frequencies \pm one standard deviation. (For this case, the frequencies of echo CF2s in the second half of the forward swing were not measurable). *Curves* are second order binomial regressions of the pulse frequencies; $r^2 = 0.89$ and 0.94 for preflight and post-flight pulse CF2s, respectively ($P < 0.001$, two-tailed t -test, for r in both cases). **B** Correspondence of shifts in the CRF and reference frequency (*REF*) before and after flight. Reference frequency values represent the mean of echoes from 3–5 pendulum swings. Error bars indicate one standard deviation from the mean. Shifts in CRF and reference frequency are statistically significant ($P < 0.05$, one-tailed t -test)

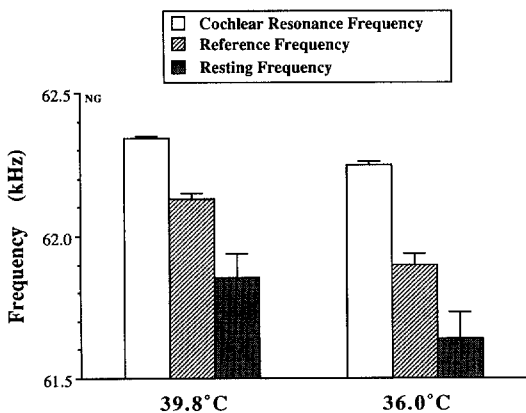


Fig. 13. Shifts in the CRF, reference frequency and resting frequency with a change in body temperature for a single trial. Reference frequency values represent the mean of echoes from 3–5 pendulum swings. Resting frequency values represent the mean of 100–200 pulses. *Error bars* indicate one standard deviation from the mean. Shifts in CRF, reference frequency and resting frequency are statistically significant ($P < 0.05$, one-tailed t -test)

Discussion

CRF lability

A major purpose of this study was to provide new data on CRF lability in response to body temperature, flight and contralateral noise exposure. The principal findings were (1) each of these parameters produced a reversible change in the CRF (Figs. 3, 5, 6 and 14); (2) the amount of change was different for each parameter (see Fig. 14); (3) post-trial recoveries in the CRF often returned to a new baseline value (Figs. 3, 5, 6); and (4) both temperature-dependent and -independent factors affect the CRF. These results substantiated the variability of the CRF which has been noted in earlier reports from our laboratory (Henson et al. 1989, 1990; Huffman et al. 1991).

Changes in body temperature proved to be the most reliable method for shifting the CRF (Figs. 3, 4, 7). The data suggest that elements of the cochlear partition which contribute to cochlear mechanical tuning are affected by temperature such that a shift in the frequency response of outer hair cells tuned at the resonance frequency occurs. In agreement with the finding that the CRF shifts with temperature, Kössl and Vater (1985a) showed that localized cooling of the head reversibly decreased the frequency of a prominent otoacoustic emission (OAE) tuned near the CRF. They have suggested that the OAE is related to the morphological specializations responsible for cochlear resonance in the mustached bat. Interestingly, temperature-dependent changes in the frequencies of spontaneous OAEs have been demonstrated for the guinea pig (Ohyama et al. 1992) as well as for nonmammalian vertebrates (Wilson et al. 1986; van Dijk and Wit 1987; van Dijk et al. 1989; Manley and Köppl 1992). Furthermore, spontaneous OAEs are prevalent in humans (see Probst et al. 1991, p. 2036), and several recent studies have shown that spontaneous OAE frequencies are sensitive to a number of physiological variables (Mott et al. 1989; Haggerty 1989, 1990; Bell 1992).

Flight-associated physiological changes tended to induce more pronounced CRF shifts than heat exposure, yet both factors were capable of producing marked changes in the CRF (Fig. 14A, B). The change in the CRF with flight may be due to a combination of temperature-dependent and -independent factors. For some neotropical bats it has been shown that body temperature is elevated during flight, and dramatic temperature increases in the first minutes of flight are common (Thomas and Suthers 1972; Thomas 1987). Physiological factors other than body temperature may influence the CRF during flight, however, since instances of flight-induced shifts which were independent of body temperature have been recorded (Henson et al. 1990). In this case, it is compelling to ask if these, and otherwise temperature-dependent factors, are cumulative, and account for the more robust effects of flight on the CRF.

The CRF shifts produced by contralateral sound exposure differed quantitatively from those produced by temperature changes or flight (Fig. 14C). For example,

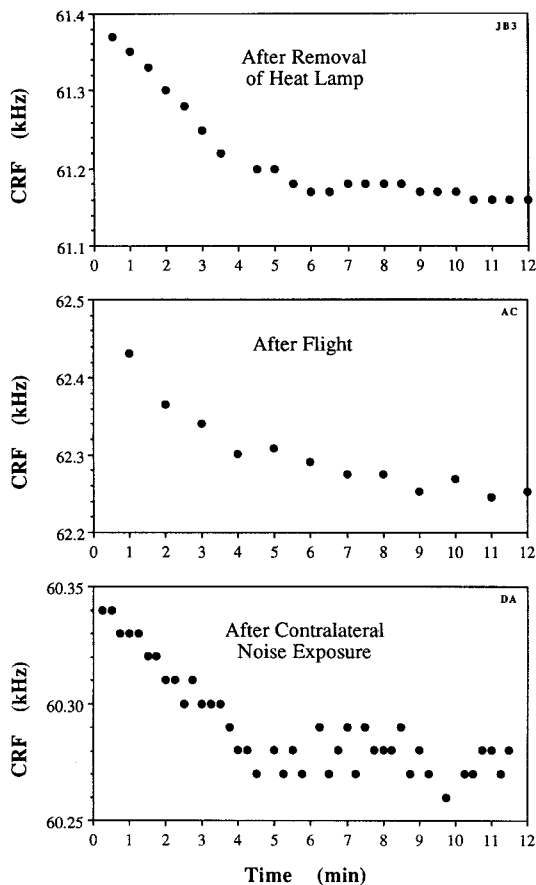


Fig. 14. Comparison of decreases in the CRF with a drop in body temperature (*top*; from trial 1 in Fig. 3), after flight (*middle*; from trial 1 in Fig. 5) and after contralateral noise exposure (*bottom*; from trial 1 in Fig. 6). Note the different frequency scale for the bottom panel

whereas postflight decreases in CRF of 200^+ Hz over 7–10 min were common, CRF shifts from contralateral noise were usually 100 Hz over 3–4 min. The difference in magnitude and time scale of the sound-induced shift may point to a different cochlear mechanism than those responsible for the temperature- and flight-related shifts. This mechanism is likely to involve the medial olivocochlear efferent system (for review see Wiederhold 1986; Warr 1992), which is well developed in the mustached bat (Bishop and Henson 1987). Numerous studies on other mammals have provided evidence that activation of olivocochlear efferents alters the micromechanical properties of the cochlea (see Brown 1988; LePage 1989; Mott et al. 1989). It is of interest to note here that, in humans, contralateral acoustic stimulation produces an abrupt, upward shift in the frequency of spontaneous OAEs (Mott et al. 1989), suggesting a similar effect from efferent activity in the human cochlea.

Concomitant shifts in CRF and CF2

A principal finding of this study was that the CF2 changed concomitantly with CRF shifts during flight

and with changes in body temperature. These data substantiate earlier reports from our laboratory (Henson et al. 1990; Huffman et al. 1991) and provide an opportunity for quantitative analysis of CF2 shifts associated with CRF lability. The directions of CRF and CF2 shifts were identical in all cases; however, the amount of shift in the CF2 was often greater than that of the CRF (see Fig. 7). The heat lamp experiments produced mean shifts in resting and reference frequencies of 93 ± 33 Hz/°C and 90 ± 38 Hz/°C, respectively, yet the mean CRF shift was 39 ± 18 Hz/°C. In contrast, the amounts of shift in the CF2 and CRF due to flight were more equivalent than the temperature-related shifts. For example, the mean changes in resting frequency and CRF with flight were 210 Hz and 150 Hz, respectively. Similarly, the mean postflight decays in resting frequency and CRF were 230 Hz and 180 Hz, respectively. It is not presently clear why the CF2 is more labile than the CRF.

It would be of interest to determine if the CRF shifts with sound exposure are accompanied by shifts in biosonar emission frequency. This study was attempted, but several problematic factors made the interpretation of the data difficult. First, although the CRF shift could be maintained during noise exposure, restrained bats were reluctant to emit biosonar signals; furthermore, the rapidity of decay in the CRF shift after exposure prevented accurate CF2 determinations, which require a suitable number of emissions. Second, the shift in the CRF with noise was comparatively small; it would be expected that shifts in the CF2 would also be small, making a significant change difficult to show.

There are numerous examples of specialization of cochlear structures responsible for sharp tuning in the CF2 portion of the partition (Henson 1973, 1978; Henson and Henson 1988, 1991; Henson et al. 1977, 1984, 1985; Vater 1988; Zook and Leake 1989). It is likely that, because these features are exaggerated, small physiological changes in this band impart significant and measurable effects on tuning properties of the partition, which are evident from the change in the CRF. Labile cochlear tuning is corroborated by the finding that parallel tonotopic shifts in neural tuning result from changes in the CRF (Huffman and Henson 1991, 1992). It is apparent from the temperature- and flight-induced shifts in both the CRF and the CF2 that continuous adjustment of the CF2 is an important process that may facilitate fine frequency resolution. The mustached bat, like many small neotropical bats, experiences significant changes in body temperature throughout the day, depending on changes in ambient temperature, activity, and proximity to other bats (McNab 1969; Thomas 1987). Furthermore, the shifts in cochlear tuning observed before and after flight represent changes that are likely to occur under natural conditions.

The ability to Doppler-shift compensate, and to match shifts in cochlear tuning with complementary shifts in biosonar emission frequency, implies some exchange of precise frequency information between auditory and vocalization systems. The auditory-vocal interface in bats is apparently complex in its anatomical distribution (e.g. Schuller and Radtke-Schuller 1988). Not-

withstanding, it has been demonstrated that brain regions for which microstimulation elicits vocalization receive and process auditory information that is frequency-specific, indicating discrete tonotopic input. For example, in the mustached bat, neurons in "vocalization centers" have sharp tuning characteristics in response to frequencies near the CF2 (Suga and Yajima 1988), and for one region of the cerebral cortex, the representation of evoked-CF2 emission frequencies is organized tonotopically in a manner similar to the bat's auditory system (Gooler and O'Neill 1987).

The adjustment of biosonar emission frequencies to match changes in cochlear tuning cannot be explained, however, with a neural system that is composed solely of hardwired, feedforward input of frequency information to the vocalization system. To the contrary, such feedforward input, if tonotopically shifted, would consistently create a mismatch between vocal output and frequencies represented in the band of sharp tuning. Thus, it is likely that a feedback mechanism exists which detects the coincidence of both the activation of the narrow band to which the cochlea is most sensitive, and the frequency of emitted CF2s. How this match is encoded is an open question; a neural model would likely include a "set point" of neural activity in vocal centers (and subsequent motor instructions to laryngeal muscles) that is achieved when auditory feedback to these centers is consistent with stimulation of the sharply tuned band.

In conclusion, the CF2 emission frequencies of moving and stationary bats shift with the CRF such that echo CF2s are kept in the sharply tuned, 60 kHz band. The concomitant shifts in CRF and CF2 strongly suggest that the change in CRF reflects a lability of frequency tuning within this sensitive, high-resolution portion of the cochlea. Coupled with neurophysiological data which shows labile tuning of central auditory neurons with shifts in the CRF (Huffman and Henson 1992), this study provides additional evidence that the mustached bat's biosonar signal is adjusted to accommodate normally occurring shifts in cochlear tuning.

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