

Chapter 4

AFM Imaging-Force Spectroscopy Combination for Molecular Recognition at the Single-Cell Level



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Abstract Molecular recognition at the single-cell level is an increasingly important issue in Biomedical Sciences. With atomic force microscopy, cell surface receptors may be recognized through the interaction with their ligands, inclusively for the identification of cell-cell adhesion proteins. The spatial location of a specific interaction can be determined by adhesion force mapping, which combines topographic images with local force spectroscopy measurements. Another valuable possibility is to simultaneously record topographic and recognition images (TREC imaging) of cells, enabling the mapping of specific binding events on cells in real time. This review is focused on recent developments on these molecular recognition approaches, presenting examples of different biological and biomedical applications.

Intermolecular recognition may be considered as the beginning for many biochemical processes. It involves several types of forces between single molecules. Different approaches have been developed to measure intermolecular forces, such as optical trapping [1–3], pipette suction [4] and surface forces apparatus (SFA) experiments [5]. Optical trapping is a very sensitive technique, but it is limited to measurements of less than tens of piconewtons and can only be applied to a small group of samples. Pipette suction and SFA experiments are sensitive techniques, but both have poor spatial resolution. The use of atomic force microscopy (AFM) in this context may overcome the problems associated to the previous techniques.

AFM is a very powerful technique, with great spatial resolution, which can probe surfaces maintaining their physiological environments and measure forces down to the piconewton range [6–10]. AFM can be used not only for imaging but, since the mid 1990's, with the first force spectroscopy study [10, 11], it can also be used to record force-distance curves of biological systems. This enables AFM to measure

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intermolecular forces between single molecules (*e.g.*, ligand-receptor interactions), which can be used for molecular recognition studies.

The combination of molecular recognition and topographic information has been studied by two different approaches: 1) adhesion force mapping mode, and 2) topographic and recognition (TREC) imaging.

1 Adhesion Force Mapping Using Force Spectroscopy

Adhesion force mapping can be performed by applying the force-volume mode or by collecting the topographic image with the maximum adhesion map on the retract part of a force-distance curve. On the force-volume mode, all force-distance curves are collected, leading to a huge amount of data, with difficult post-processing. The maximum adhesion map is created by recording whole force-distance curve(s) for every pixel of the scan. However, the ability to distinguish a molecule on the adhesion map is very limited as compared with the topography image; thus, usually no correlation between both images can be performed [12].

Force spectroscopy can be performed at a single sample spot, by selecting it on the AFM scanning image, or it can be record spatially in the x,y plane. Quantitative tip-sample adhesion maps may then be generated. The principle is to record spatially resolved force-distance curves by moving the AFM scanner across the biological samples over an area of a given size with $n \times n$ points to be probed (typically, 32, 64 or 128) [13–15]. The x,y AFM image is divided into a square grid of n^2 pixels and the system performs one or more approach/retract cycle(s) on the center of each square/pixel, with a common lateral resolution from a few tens to hundreds of nanometers per pixel (Fig. 4.1) [16]. At the same time, the system creates maps (of height, adhesion or elasticity), which data may be processed and quantified. Thus, for each force-distance curve, a given property of the sample can be extracted, quantified and displayed on maps. Color or grey scale can be used to display the pixels on the maps of each analyzed property of the sample. Brightness pixels reflect the magnitude of the measured property at a defined location [17–20]. Due to speed limitations and poorer spatial resolution on the most common atomic force microscopes, this method did not have significant scientific progress before the 2000's. Only after 2001, with the development of high-speed scanners, free of resonant vibrations up to 60 kHz, it was possible to build a high-speed AFM. This microscope was capable to capture a 100×100 pixel² images within 80 ms and, therefore, generate a movie of biological samples under physiological conditions [21]. This AFM provided a way to record and correlate data from structure, adhesion and elasticity maps of samples faster, achieving molecular resolution.

In 2008, Sahin et al. conducted a nanomechanical mapping by the real-time analysis of time-varying tip-sample forces in tapping-mode AFM [23]. For the first time, they constructed maps of local elastic modulus and adhesion forces, together with conventional phase and topography images, in tapping mode. This new approach allowed the nanomechanical analysis of samples with gentle forces and high spatial

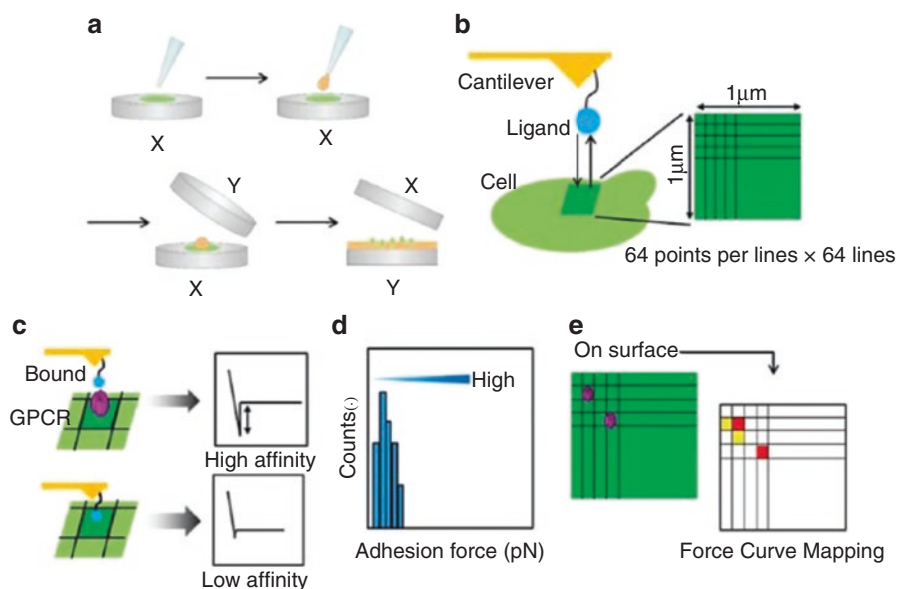


Fig. 4.1 Schematic representation of adhesion force mapping. (a) Immobilization procedure for a sample on a glass slide. (b) A cantilever derivatized with a ligand approaches the surface of a cell to conduct force measurements of $n \times n$ points within $1 \times 1 \mu\text{m}^2$. (c) Differences between high and low affinity systems. (d) Adhesion force histogram. (e) Force curve adhesion mapping, representing high (red), low (yellow) and very low (white) affinity binding measurements. Reprinted with permission from [22]

resolution [23]. A new dynamic AFM method to quantitatively map the nanomechanical properties of live cells with a throughput 10 to 1000 times higher than that achieved with quasi-static AFM techniques was introduced in 2011 [24]. In 2015, a new fast scanning quantitative dynamic AFM method for nanomechanical imaging of heterogeneous live cells in solution was introduced, using the cantilever mean deflection as feedback signal, instead of standard amplitude reduction. This new method was able to achieve a 10 to 20-fold improvement in imaging throughput, compared to amplitude-modulation AFM [25].

Moreover, combining force spectroscopy mapping with an AFM-mounted fluorescence microscope enables dual fluorescence and AFM adhesion map imaging, allowing the detection and local determination of potential submicron-sized adhesive regions [26]. Nanoparticle tracking analysis and quantitative nanomechanical mapping AFM were also combined to determine size and nanomechanical properties of exosomes isolated from non-malignant and malignant (metastatic and non-metastatic) cell lines [27]. Authors revealed that malignant cell line exosomes have lower stiffness and adhesion compared to non-malignant cell line exosomes.

AFM-based adhesion nanomechanical mapping provides insights into the functions of different biological systems [28]. This technology has already been applied by different researchers to simultaneously image and quantify biophysical proper-

ties of complex samples, such as diatoms [29], lipid phases in supported bilayers [30], diverse membrane proteins [31–33], yeasts [34], virus capsids [35], human cells [25, 36–40] and neurodegenerative amyloid fibrils [41].

In 1998, Willemsen et al. demonstrated that the resolution of the topographical image in adhesion mode is only limited by tip convolution and, thus, comparable to tapping mode images. By comparing the high-resolution height image with the adhesion image, it is possible to show that specific molecular recognition is highly correlated with topography. This was possible by studying recognition events for individual antibody-antigen pairs when authors imaged individual ICAM-1 antigens both in tapping mode and the adhesion mode [42].

The characterization of the local mechanical properties of polymer cushioned membranes [43], as well as nanofibers [44], was also possible by applying force mapping methodologies. An AFM tip functionalized with cytochrome C2 molecules was also used to map native protein-protein interactions found in bacterial photosynthesis (electron donor/intrinsic membrane acceptor pair) [45]. AFM was also used to measure the adhesion force between targeting receptors and their ligands, and to map the targeting receptors (*e.g.*, Ste2p, a G protein-coupled receptor [22]). At the level of protein-protein interactions, the measurement of the binding force between glyceraldehyde-3-phosphate dehydrogenase (GAPDH) and Ras homologue enriched in brain (Rheb) was also performed [46]. By AFM-recognition mapping using specific DNA aptamers, it was possible to study the binding between human α -thrombin and vascular endothelial growth factor (VEGF), two proteins involved on the clotting cascade [47]. It is therefore possible to generate high resolution maps to spatially and temporally identify proteins at the molecular level on complex surfaces.

On other fields of research, such as crime scene investigations, PeakForce quantitative nanomechanical mapping (PF QNM) AFM has been used to study the variations in surface adhesion and topography of latent fingerprint droplets over time [48].

On this review, we will highlight the application of adhesion force mapping methodologies to study different types of cells.

In 2015, Rigato et al. performed AFM-based mechanical mapping on cells plated on micropatterns, demonstrating a pattern-specific reproducible mechanical response [49]. This yields the possibility of average the data of the elasticity maps allowing to specifically locate intracellular elasticity differences, which are maintained among cells, and to identify regions characterized by higher or lower mechanical stability [49].

One of the first studies that was performed with microbial cells was done by Gad et al. [20], whom focused on the distribution of mannan, a particular type of polysaccharides, on the surface of a living microbial cell. Specific AFM mapping molecular recognition events were only detected on specific areas of the cell surface, which was interpreted as reflecting a non-uniform distribution of mannan on the cell surface. Specific procedures are necessary to conduct these AFM measurements. Methods for: (i) functionalizing AFM tips with *Pseudomonas aeruginosa* or concanavalin A, (ii) for stretching specific polysaccharide molecules on live bacteria using single-molecule force spectroscopy with lectin-coated tips, and (iii) for

mapping the localization, adhesion and extension of individual polysaccharide chains were described in detail [50].

Experiments to measure the interaction forces of bacterial adhesins (HBHA) and for assessing their distribution on the surface of living cells (*Mycobacterium bovis* BCG cells) were successfully conducted by Dupres et al. [19, 51]. High-resolution image and adhesion force maps of a sodium dodecyl sulphate-treated *Aspergillus fumigatus* spore revealed high correlation between structural and hydrophobic heterogeneities [52].

In 2013, Alsteens et al. reported the correlation between structural, adhesion and elasticity images of complex biological samples, recorded at high temporal and spatial resolutions, and with biochemical specificity [18]. Using this method, they provided a direct visualization of the assembly machinery of bacteriophages on living cells, revealing that they localize near the septum, in the form of soft nanodomains surrounded by stiffer cell wall material [18]. The assessment of the electric charge distribution on the surface of the cell wall of Gram-positive bacteria was also proven to be feasible by AFM mapping images at a spatial resolution better than a few tens of nanometers [53].

On another report, the hydrophobic forces engaged in Epa6-mediated cell adhesion were successfully measured by AFM [54]. Using single-cell force spectroscopy, the authors conclude that *Candida glabrata* wild-type (WT) cells bind to hydrophobic surfaces via strongly adhesive macromolecular bonds, while mutant cells with impaired in Epa6 expression are weakly adhesive (Fig. 4.2).

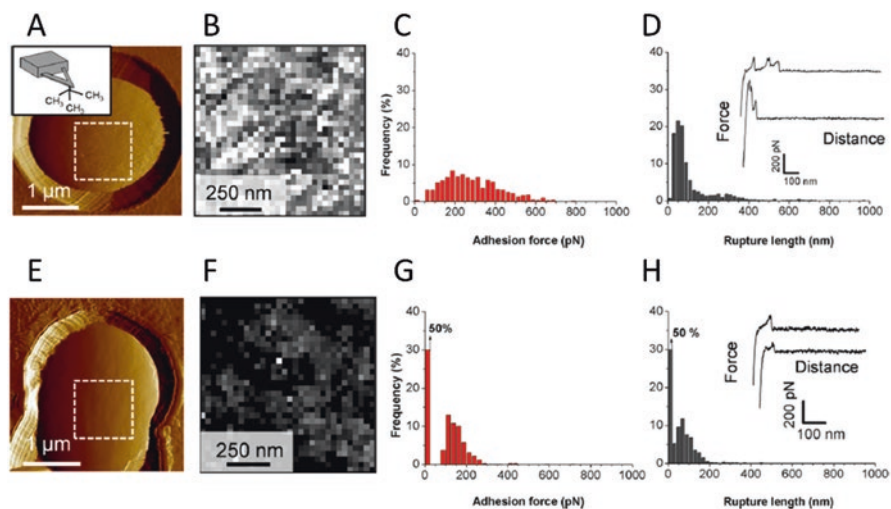


Fig. 4.2 Mapping and quantification of hydrophobic forces on *C. glabrata* cells using chemical force microscopy. AFM deflection images of WT (A) and Epa6 mutant (E) cells. The dashed white squares indicate the regions where the force maps were recorded. Adhesion force maps (1 $\mu\text{m} \times 1 \mu\text{m}$; bright pixels correspond to hydrophobic binding events) of WT (B) and mutant (F) cells; respective adhesion force (C, G) and rupture length (D, H) histograms. Adapted and reprinted with permission from [54]

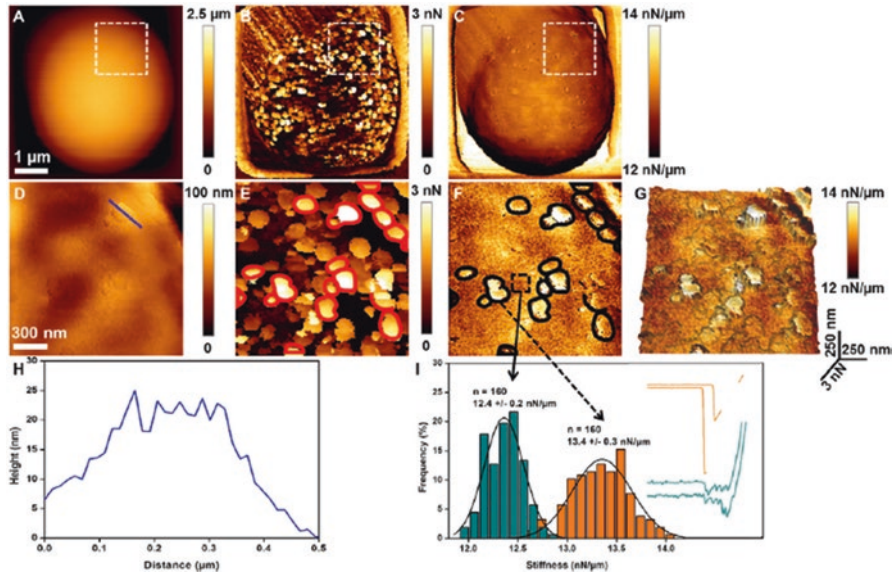


Fig. 4.3 Nanomechanics of the adhesive domains of *C. albicans* cells. Height image (A), and corresponding adhesion (B) and stiffness (C) images. Height (D), adhesion (E) and stiffness (F) images of a small area on top of the cell, corresponding to the white dashed square on A. Adhesive nanodomains circled in red on (E) are also found on the stiffness image (black circles on (F)). 3D-image of the adhesion mapped with the stiffness (G). Cross-section (H) taken along the blue line on (D). Distribution of the stiffness values (I) corresponding to the cell wall and the less adhesive domains (blue columns) or to the most adhesive domains (orange columns). Reprinted with permission from [55]

The observation that adhesins at the surface of *Candida albicans* cells are organized in nanodomains composed of free or aggregated mannoproteins was possible by AFM mapping of the adhesive properties of these cells (Fig. 4.3) [55].

Using a dynamic AFM technique operating in the intermittent contact regime to quantitatively map the local electro-mechanical force gradient, adhesion, and hydration layer viscosity within individual f29 virions, other authors provided new evidences of how bacteriophages like pressurized vessels, releasing DNA through any fracture present on the viral shell [56].

By studying the effect of plasma membrane receptor clustering on local cell mechanics, Almqvist et al. obtained adhesion force maps for the interaction between an antibody at the AFM tip and a specific VEGF receptor [17]. VEGF receptors were found to concentrate toward the cell boundaries and cluster rapidly, with local stiffness reductions (Fig. 4.4).

Mapping images of the distribution of sugar chains on epithelium and of the receptor associated protein (RAP) binding proteins on fibroblasts were also obtained [57, 58].

In 2007, the local mechanical characteristics of different cell types (namely, muscle, endothelial, epithelial and glial cells, neurons, fibroblasts, osteoblasts,

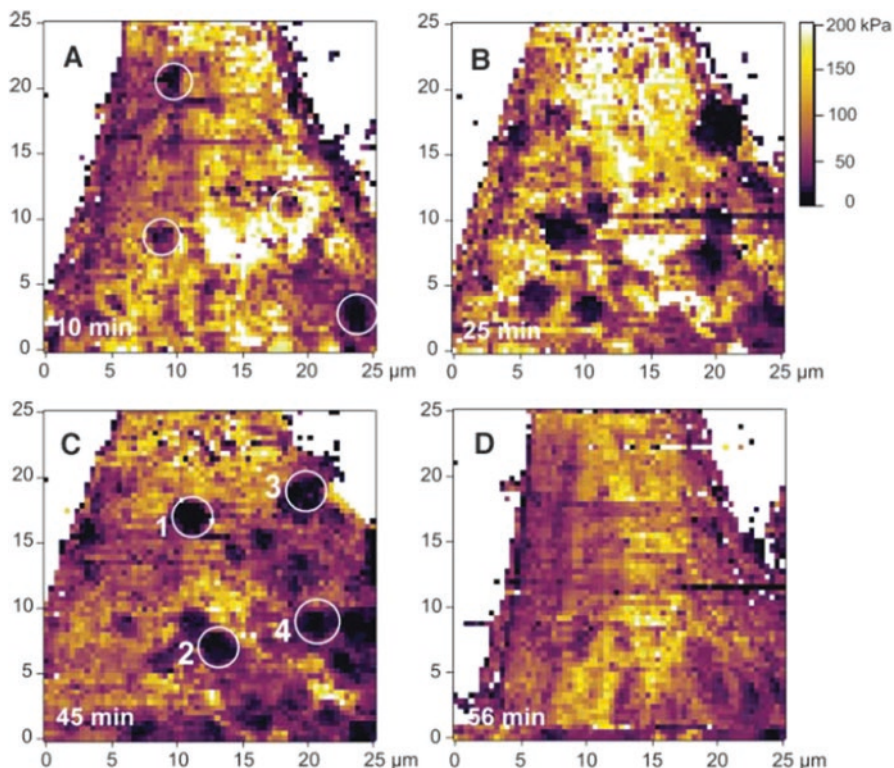


Fig. 4.4 Elasticity maps of the evaluated Young's modulus on endothelial cells in real-time, showing clustering of VEGF receptors on the cell surface. Images are colour-coded according to the bar, from 0 kPa (*dark*) to 200 kPa (*bright yellow*). Images show the elasticity at different time points after adding anti-flk-1 antibody: 10 min (**A**), 25 min (**B**), 45 min (**C**) and 56 min (**D**) after addition. A few regions with lower elasticity are marked with numbers 1–4 in (**C**). The regions underlying the receptor clusters appeared as less stiff. Reprinted with permission from [17]

blood cells and sensory cells) were analysed by Kuznetsova et al. [59]. According to this work, normal cells are one order of magnitude stiffer than cancer cells. Authors suggested that such change in elastic properties might be attributed to a difference in cytoskeleton organization. In another study, mapping of the local Young's modulus of a living astrocytes revealed that stiffer areas correspond to the sites where the cytoskeleton fibers are located (Fig. 4.5) [60].

Cassina et al. demonstrated that a peptide obtained from the cleavage of the neuroprotein VGF stimulates intracellular calcium mobilization in Chinese Hamster Ovary (CHO) cells [61]. The sub-cellular localization of the tyrosine kinase receptor (Met) for hepatocyte growth factor on hippocampal neurons was also studied by AFM force spectroscopy adhesion mapping. Authors found that multimeric activated Met is concentrated in the dendritic compartment, while the inactivated monomeric form of Met was prominent on the soma [62]. An adhesion force

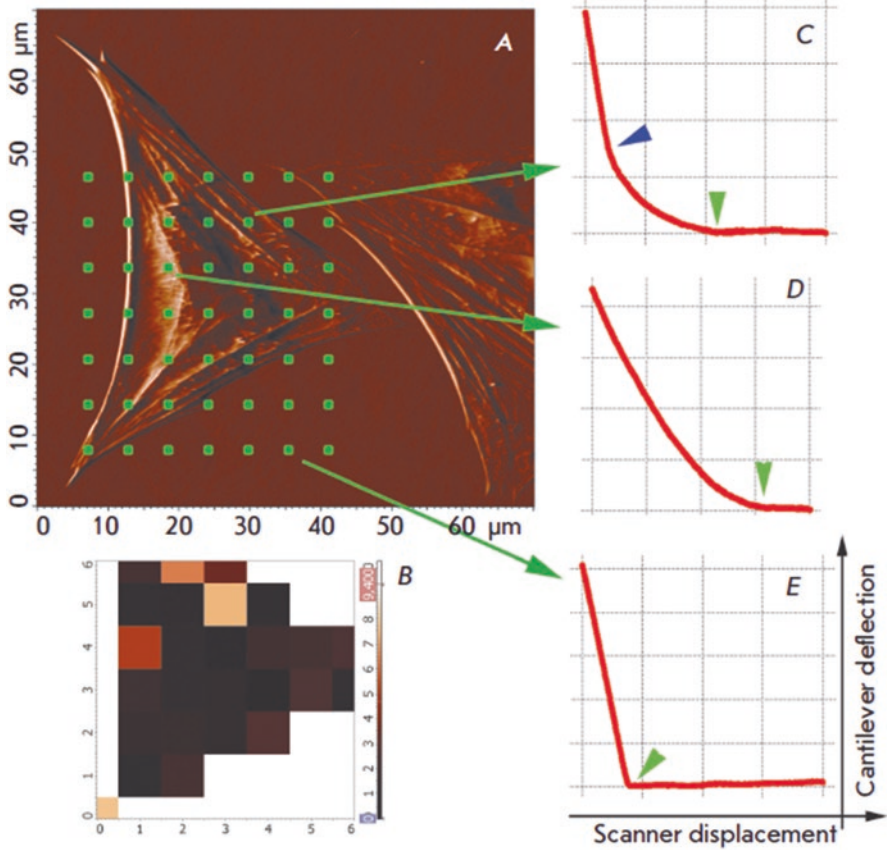


Fig. 4.5 Mapping the local Young's modulus of astrocytes. (A) Deflection image of a living astrocyte, with a grid of points indicating where the force curves were obtained. (B) Map of the local Young's modulus in the grid nodes (colour scale in kPa, with lighter squares corresponding to stiffer areas). (C) Force curve obtained in a point above the cell edge; the upper part of the curve coincides with the curve obtained on the substrate (E). Green arrows mark the contact point and the blue arrow the point where the cantilever touches the substrate. (D) Force curve obtained in a point above the cell nucleus. Reprinted with permission from [60]

mapping methodology was also applied to reveal the nanoscale distribution of Fc gamma receptors on local areas of macrophages, which have an important role in clinical cancer immunotherapy [38].

The morphology and the elastic properties of live cultured, non-malignant human mammalian epithelial cells (HMEC) and cancerous breast epithelial cells (MCF7) were also investigated through AFM force mapping [40]. The quantification of the surface density and the spatial organization of CXCR4 on breast cancer cell membranes were also assessed by AFM, leading the authors conclude that the CXCR4 density, spatial organization, and matrix stiffness are paramount to achieve strong binding [63].

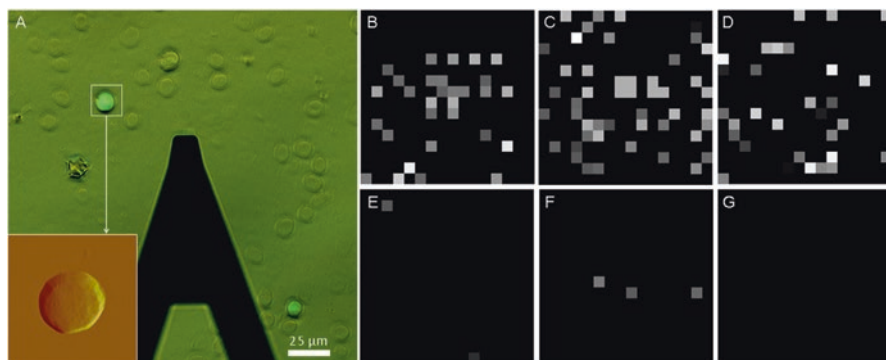


Fig. 4.6 Detection of specific CD20-rituximab interactions on cancer cells. (A) Fluorescence image of a clinical bone marrow cell sample, with the AFM image of a single cell as inset. (B, C, D) CD20 distribution maps on the cancer cells. (E, F, G) CD20 distribution maps on the cancer cells after blocking with rituximab, a monoclonal antibody against CD20. Grayscale is from black to white, up to 200 pN. Reprinted with permission from [39]

Specific molecular-receptor interactions on living human colorectal cancer cells were also already tested as *in vitro* models for gut epithelium [36]. On this study, authors measured the binding of wheat germ agglutinin to the surface of living Caco-2 human intestinal epithelial cells.

Using fast scanning dynamic AFM, it was possible to observe the nanomechanical spatio-temporal response of the cortical actin cytoskeleton, including the formation and movement of lateral actin bands [25]. These bands are characteristic of the retrograde actin flow machinery rapidly formed by inhibiting Syk expression in MDA-MB-231 breast cancer cells.

AFM was also applied to map the nanoscale distribution of CD20 molecules on the surface of cancer cells from clinical B-cell non-Hodgkin's lymphoma (NHL) patients, with the assistance of ROR1 (a cell surface marker expressed exclusively on cancer cells) fluorescence recognition (Fig. 4.6) [39]. The membrane protein CD20 is an effective target for treating B-cell NHL, as demonstrated in clinical practice. That study provided a new approach to directly investigate the nanoscale distribution of a target protein on individual clinical cancer cells.

2 Topographic and Recognition (TREC) Imaging

The second approach to study molecular recognition is a very powerful technique, which combines imaging at high resolution and single-molecule interaction measurements [64–66]. TREC imaging is a dynamic approach that uses an oscillating tip close to its resonant frequency [65, 67]. This technique is faster and has better lateral resolution (few nanometers) than adhesion force mapping [15, 65, 66]. Topographic and recognition images are obtained at the same time, allowing to

distinguish sites of receptors in the recognition image, spatially correlating them with features of the topographic image. TREC imaging uses a molecule (ligand) covalently attached to the AFM tip, usually via a flexible crosslinker (*e.g.*, poly(ethylene glycol) – PEG) [68–70]. During the scanning of the surface, the functionalized tip oscillates close to its resonance frequency. The binding sites are evident from the reduction in the oscillation amplitude, as a result of specific recognition during the lateral scan. Enhanced signal processing, in combination with a modified feedback loop [64], provides a recognition image simultaneously acquired alongside the topography image. The separation of topographical and recognition signals is achieved by splitting the cantilever’s oscillation amplitude into lower and upper parts (relative to the cantilever’s resting position), containing solely topography and recognition information, respectively. The maxima of these parts are then used to record the topography (lower part) and recognition image (upper part) at the same time (Fig. 4.7) [71, 72].

TREC imaging on AFM offers different advantages [73]: (i) high resolution of samples and high tracking capacity of target molecules on cells; (ii) high recognition specificity; (iii) less sample damage and no sample pre-treatment; and, (iv) simple and clear output, demonstrating the exact location of target molecules on the surface of the scanned sample. The use of TREC imaging offers a wide range of biological applications. It enables the study of the real location of single molecules on a tissue or cell surface, providing new perceptions of cell physiological mechanisms.

Applying TREC imaging, it is possible to investigate interactions of single molecules with their specific receptors, while simultaneously recording a high-resolution topography image. The combination of topographic and recognition images has been demonstrated on different biological systems with great success. This technique has already been useful to study chromatin structures [65], receptor-ligand pairs [64, 66, 72], proteins [75], isolated erythrocyte membranes [76] and cells [77, 78].

Radmacher et al. reported one of the first adhesion mapping studies, which was done by mapping lysozyme aggregates adsorbed onto mica [79]. A decrease of the adhesion of the tip with the lysozyme compared to mica was observed. This study was performed with a non-functionalized tip and the adhesion map was based on the physicochemical properties of the molecule and the substrate, rather than on specific biomolecular interactions. Ludwig et al. used a biotin-functionalized tip to map a streptavidin pattern and, with specific high-affinity interaction measurements, were able to create an adhesion map [80].

In 2005, Agnihotri et al. used binary recognition images to differentiate specific from unspecific interactions between fibrinogen on the surface and its specific antibody [81]. The number of recognition events had a major decrease after blocking the surface with anti-fibrinogen antibodies. The positive events observed in the recognition image were considered as specific antibody-fibrinogen interactions.

An adaptation of this technique was proposed by Wang et al. which used an AFM tip with two tethered antibodies and sequential blocking to identify two types of proteins in single AFM images of compositionally complex molecules [82]. By

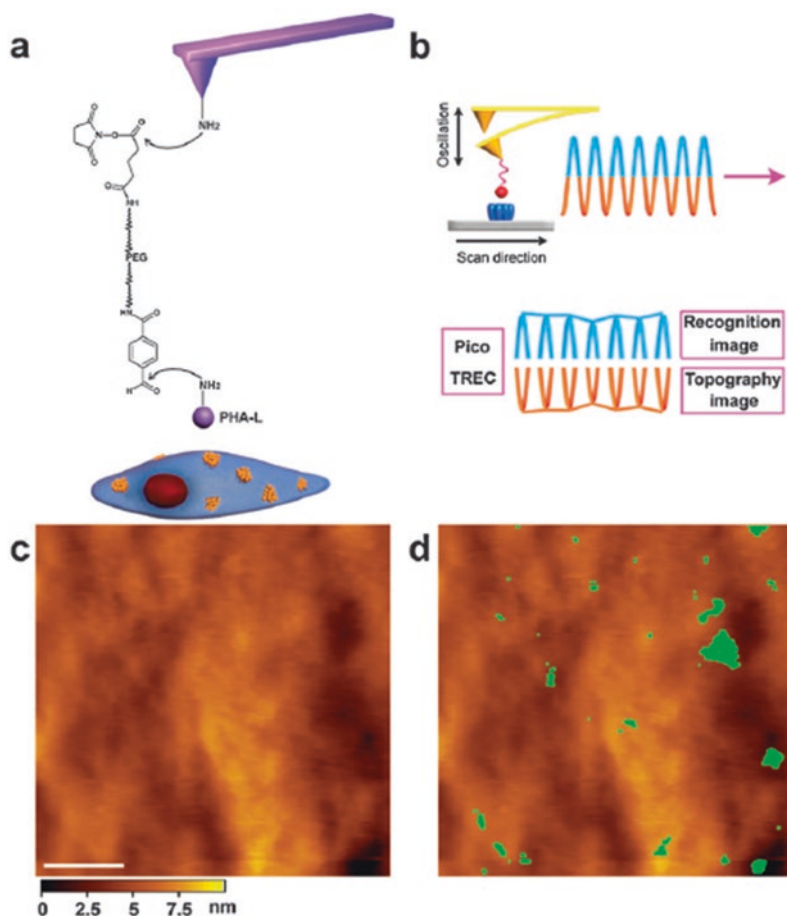


Fig. 4.7 TREC molecular recognition imaging of galactose on the surface of HeLa cells. (a) Scheme of the AFM tip modified with a lectin (PHA-L). (b) Principles of TREC imaging, scanning the cell with the modified tip (scale bar: 300 nm). (c) Topography image. (d) Topography image with the recognition signal superimposed. Adapted and reprinted with permission from [74]

applying this methodology, authors were able to analyse two specific components, BRG1 and β -actin, of the human Swi-Snf ATP-dependent nucleosome remodelling complex and two types of histones, H2A and H3, on the chromatin samples (Fig. 4.8).

Sotres et al. proposed other mode of performing force scanning by AFM, named jumping mode [12]. Topographic and tip-sample adhesion maps are acquired simultaneously. Lateral resolved adhesion maps of avidin-biotin unbinding forces highly correlated with single avidin molecules in the corresponding topographic map were achieved after testing this method.

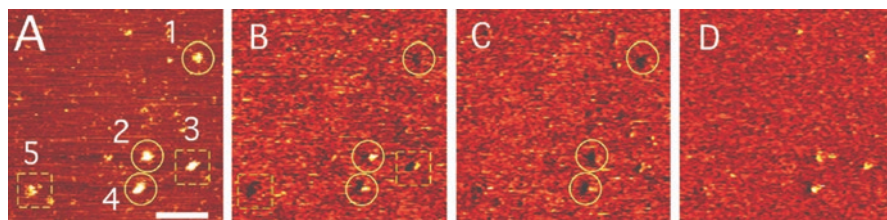


Fig. 4.8 Identification of different subunits in a multiprotein complex. Human Swi-Snf ATP-dependent nucleosome remodelling complexes were deposited and scanned with an AFM tip with both anti-BRG1 and anti- β -actin antibodies, rescanned in the presence of β -actin blocking peptide, and then rescanned in the presence of BRG1 and β -actin blocking peptides. (A) Topographic image from the initial scan. (B) Corresponding recognition image (no blocking). (C) Recognition image obtained after blocking with β -actin peptide. (D) Recognition image obtained when both BRG1 and β -actin blocking peptides are present. Dashed squares identify complexes whose recognition disappears after blocking with β -actin peptide and solid circles identify complexes whose recognition disappears only when BRG1 blocking peptide is present. Squares and circles are shown only when molecular recognition occurs, *i.e.*, in (B) and (C). Reprinted with permission from [82]

A simple procedure for adjusting the optimal amplitude for TREC imaging was described by Preiner et al. [71]. This method takes advantage of the sharp localization of the TREC signal within a small range of oscillation amplitudes. Using this procedure, authors imaged single avidin molecules immobilized on a mica substrate with an AFM tip functionalized with a biotinylated IgG.

In 2014, van Es et al. presented a new way to look at AFM TREC data. TREC imaging was used on a model system comprising an S-layer surface modified with Strep-tag II for binding sites and Strep-Tactin bound to the AFM tip [83]. They have shown that high resolution TREC images contain information on binding and unbinding rates for surface bound molecules. They also presented a method to analyse the TREC images to extract these rates as a function of distance between the AFM tip and the binding site. The authors concluded that high resolution TREC imaging is a valid method to determine k_{on} values at the single-molecule level [83].

Force clamp force mapping (FCFM), an AFM-based technique for measuring the viscoelastic creep behaviour of live cells with sub-micrometer spatial resolution, can also be successfully applied [84].

A study from 2009 evaluated the changes in surface topography, surface adhesion, indentation depth and Young's modulus on a metal-tolerant marine bacterium after its exposure to cobalt (II) ions [85]. An overall increase on the elasticity of the bacterial membrane and an increase in adhesiveness were observed.

Detailed procedures for all stages of TREC experiments with cells (*e.g.*, vascular endothelial cells), from tip and sample preparations to the operating principles and visualization, were described by Chetchevlova et al. [86].

The distribution of osteopontin (OPN) over pre-osteogenic cell membrane was tracked by mapping the adhesion forces between an anti-OPN coated probe and the cell surface. Authors were able to recognize specific OPN nanodomains on the cell membrane (Fig. 4.9) [73].

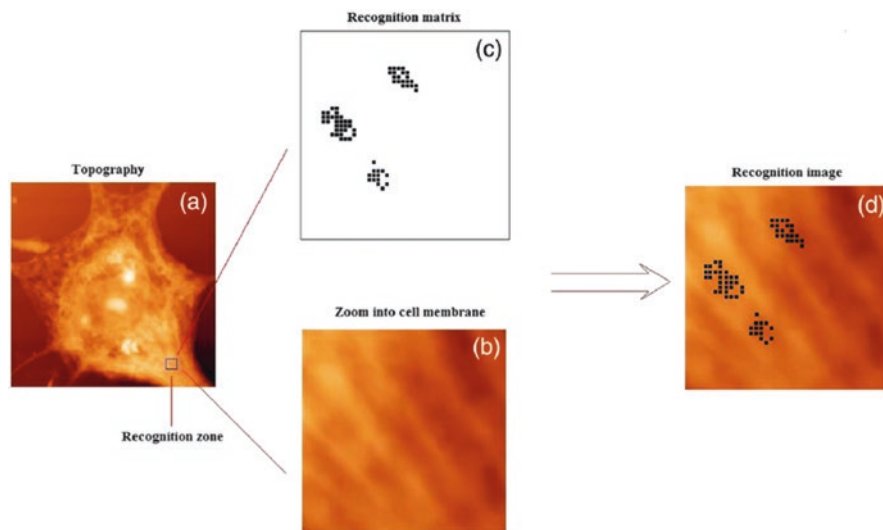


Fig. 4.9 (a) Topographic AFM image of a pre-osteogenic cell (the black frame on the right corner shows the chosen recognition zone). (b) High resolution topography image of the recognition zone. (c) Recognition matrix demonstrates the location of all specific binding events between anti-OPN tip and the OPN proteins on the cell surface. (d) The recognition image was created by merging the binary matrix image (c) and the high resolution topography image of the recognition zone (b). The image reveals the location of all OPN sites over the recognition zone. Each black square indicates the location of an OPN site. AFM images of $30 \times 30 \mu\text{m}^2$ (a) and $1 \times 1 \mu\text{m}^2$ (b–d). Reprinted with permission from [73]

On another TREC imaging study, galactose was detected and localized on the surface of cancer and normal cells [74]. Authors revealed that there are more galactose residues on cancer cells than on normal ones, and that the stability of galactose-lectin binding on cancer cells is much lower than that on normal cells.

Recently, the interaction of the specific DNA aptamer *sgc8c* immobilized at the AFM tip with its corresponding receptor, protein tyrosine kinase-7 (PTK7), embedded in the membrane of acute lymphoblastic leukaemia (ALL) cells (Jurkat T-cells) was investigated [87]. A homogeneous distribution of PTK7 molecules on the outer regions of ALL cells with a surface density of 325 ± 12 PTK7 receptors (or small receptor clusters) per μm^2 was demonstrated (Fig. 4.10).

TREC mapping was also applied to the imaging of α actinin-4 filaments and mapping of the epitopic region within α actinin-4 molecule using an antibody functionalized tip [88]. To gain a comprehensive view of the structural and chemical properties of *Staphylococcus epidermidis*, four different strains (biofilm positive and biofilm negative strains) were also analysed using the same methodology [89]. On this study, force measurements performed using bare hydrophilic silicon nitride tips disclosed similar adhesive properties for each strain. However, the use of hydrophobic tips showed that hydrophobic forces are not the driving forces for adhesion

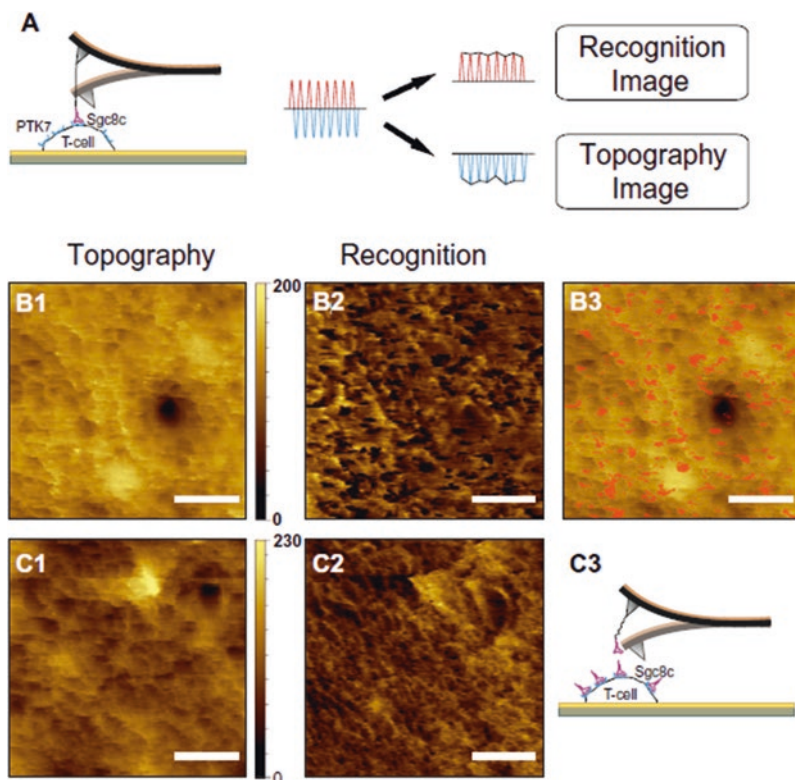


Fig. 4.10 (A) Schematic representation of the TREC setup. Simultaneously acquired topography (B1) and recognition (B2) images on a T-cell membrane using *sgc8c* functionalized tips. A superimposition of topography and recognition is also shown (B3). After addition of free aptamers, the topography image (C1) remains unchanged, whereas the recognition spots (C2) are completely abolished, as a result of blocked PTK7 receptors, as illustrated in (C3). Scale bars: 500 nm. Reprinted with permission from [87]

of the four strains. Treatment of two biofilm positive strains with two chemical inhibitor compounds leads to a loss of adhesion, suggesting that AFM could be a valuable tool to screen for anti-adhesion molecules.

Studying the binding affinity of peptides binding to various materials is also possible with quantitative force mapping methods [90].

TREC can be combined with other techniques. One example of this was presented by Zhu *et al.*, which used native-protein nanolithography (NPNL) and TREC to synergistically use AFM tips to write and image nanoscale protein patterns on a surface [91]. The approach was validated using surface-bound biotinylated bovine serum albumin (BSA) and AFM tips carrying streptavidin tethered via a flexible PEG linker. Another example is the combination of AFM with scanning electrochemical microscopy (SECM) in peak force tapping (PFT) mode, thereby offering spatially correlated electrochemical and nanomechanical information

paired with high-resolution topographical data under force control [92]. The development of this approach may also be used to study complex biological samples, such as bacterial cells. Hinterdorfer et al. have shown that AFM combined with near-field scanning optical microscopy (NSOM) provide a broad range of possibilities for mapping the distribution of single molecules on the surfaces of cells with nanometer spatial resolution, thereby shedding new light on their highly sophisticated functions, namely on the study of the adhesion of *C. albicans* to proteins (Fig. 4.11) [93, 94].

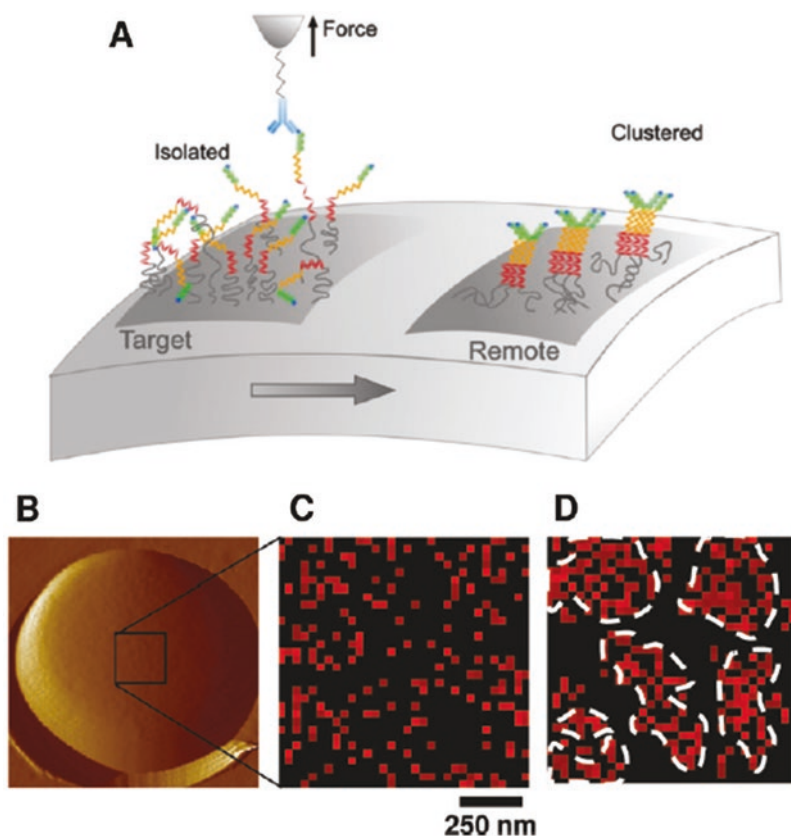


Fig. 4.11 Single-molecule AFM imaging unravels the dynamic clustering of cell adhesion proteins on yeast cells. (A) Single Als proteins from *C. albicans* were localized and stretched using an AFM tip bearing specific antibodies. (B) AFM topographic image of a single live cell. (C) Adhesion force map recorded on a cell that was never subjected to force. Red pixels document the detection of single proteins. Most proteins were isolated and evenly distributed, without any clear evidence for clustering. (D) Subsequent mapping recorded on the same cell after mechanical stimulation. Unlike native cells, cells that had been preactivated by force displayed adhesion nanodomains referred to as “nanoadhesomes” (A). Reprinted with permission from [93, 94]

3 Conclusions

The molecular recognition of the specific interactions between two molecules, proteins, membranes, or the entire surface of cells is essential to understand both structure and function(s). The recent advances on single-molecule imaging approaches, as for atomic force microscopy, allowed researchers to take advantages of these methods, with high improvements in spatial/temporal resolution, cell imaging speed, ease of use, higher throughput analysis and maintenance of *in vivo* cell physiological conditions.

Here, two different methods that combine AFM imaging and force spectroscopy were explained in detail: adhesion force mapping and TREC imaging. Both methods have expanded AFM beyond basic imaging studies, giving researchers the possibility to record and correlate data from structure, adhesion and elasticity maps, as well as to quantify molecular recognition events on different biological samples. Several applications of both methods led to numerous discoveries in cell biology, immunology, pharmacology and medical field. Some of the most recent studies are compiled on this review. We believe that the evolution and extension of the use of both methods will lead to important scientific discoveries and future developments in Biology and Medicine.

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Conflict of Interest Disclosures The authors declare no competing financial interests.

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