Chapter 16 Alendronate Liposomes for Antitumor Therapy: Activation of $\gamma\delta$ T Cells and Inhibition of Tumor Growth

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Abstract Circulating $\gamma\delta$ T cells are cytotoxic lymphocytes that are unique to primates. Recent studies have shown that amino-bisphosphonates (nBP) activate $\gamma\delta$ T cells to kill tumor cells in an indirect mechanism, which requires antigen presenting cells (APC). We hypothesized that selective targeting of nBP to monocytes would result in a more potent $\gamma\delta$ T cells activation in circulation, and in tissue associated macrophages (TAM) following monocytes-laden drug extravasation and liposomes accumulation at the tumor site. In addition, inhibition of TAM by alendronate liposomes (ALN-L) is expected. ALN was targeted exclusively to monocytes, but not to lymphocytes, by encapsulating it in negatively-charged liposomes. The proportion of human $\gamma\delta$ -T cells in the CD3⁺ population following treatment with ALN-L or the free drug was increased, from $5.6 \pm 0.4\%$ to $50.9 \pm 12.2\%$ and $49.5 \pm 12.9\%$, respectively. ALN solution and liposomes treatments resulted in an increased, and in a dose dependent manner, TNF α secretion from h-PBMC. Preliminary results showed that ALN-L inhibited tumor growth in a nude mouse breast tumor model. It is suggested that enhanced activation of $\gamma\delta$ T cells could be obtained due to interaction with circulating monocytes as well as by TAM endocytosing liposomal nBP leading to a potentiated anti-tumor effect of nBP. It should be noted that this could be validated only in primates/humans since $\gamma\delta$ T cells are unique in these species.

Keywords $\gamma\delta$ T cells • Liposome • Monocyte • nBP • TAM

Abbreviations

- DSPC 1,2-Distearoyl-sn-glycero-3-phosphocholine
- ALN-L Alendronate liposomes
- nBP Amino-bisphosphonate
- APC Antigen presenting cells
- BSA Bovine serum albumin
- CLOD-L Clodronate liposomes

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E. Zahavy et al. (eds.), *Nano-Biotechnology for Biomedical and Diagnostic Research*, Advances in Experimental Medicine and Biology 733, DOI 10.1007/978-94-007-2555-3_16, © Springer Science+Business Media B.V. 2012

DCs	Dendritic cells
DSPG	Distearoyl-phosphatidylglycerol
MHC	Histocompatibility complex
h-PBMCs	Human peripheral blood mononuclear cells
imDC	Immature DC
IPP	Isopentenyl pyrophosphate
mAbs	Monoclonal antibodies
MPS	Mononuclear phagocytic system
TAM	Tissue associated macrophages

16.1 Introduction

Human circulating $\gamma\delta$ T cells lymphocytes constitute of 1–5% of peripheral blood T cells (Hayday 2000) and exhibit major histocompatibility complex (MHC) unrestricted cytotoxicity against a large number of tumor types (Ferrarini et al. 2002). Most of the circulating $\gamma\delta$ T cells belong to the V γ 9V δ 2 subset that are unique to primates (Hinz et al. 1997). Recent studies have shown that amino-bisphosphonates (nBP), antiresorptive drugs utilized clinically in bone-related disorders (Rodan 1998a), activate $V\gamma 9V\delta 2$ T cells (Kunzmann et al. 2000). There has thus been interest in using nBPs in cancer immunotherapy, with promising results against B-cell malignancies (Wilhelm et al. 2003) and hormone refractory prostate cancer (Dieli et al. 2007). And in a very recent clinical trial, it was shown that a nBP (zolendronate) exerts a significant anticancer benefit when added to hormone therapy, reducing the risk of breast cancer returning by 36% (Gnant et al. 2009). Tumor cells are killed in an indirect mechanism, which requires antigen presenting cells (APC) (Caccamo et al. 2008; Kunzmann et al. 2000). nBP are internalized to some extent by mononuclear cells such as monocytes and dendritic cells (DCs) leading to intracellular accumulation of the isopentenyl pyrophosphate (IPP) metabolite (Roelofs et al. 2009). Consequently, this endogenous phosphoantigen is ultimately recognized by $\gamma\delta$ T cells with subsequent cell activation, proliferation, and the release of TNF α , IL6 and IFN γ (Mariani et al. 2005). However, the family of nBP is both highly hydrophilic and charged, and is rapidly eliminated from the circulation by binding to bone and via urine excretion (Rodan 1998a, b; Fleisch 1998). Therefore, peripheral monocytes and tumors are exposed only briefly and to a relatively low concentration of nBP. Thus, in order to potentiate the effect of nBP selective targeting of the drug to APCs is necessary.

Encapsulating a BP in a particulate delivery system, such as liposomes, deviates these bone-seeking molecules to circulating monocytes and macrophages of the mononuclear phagocytic system (MPS) (van Rooijen and van Kesteren-Hendrikx 2003; Danenberg et al. 2002). The anti-inflammatory effect resulting from macrophage depletion by clodronate liposomes (CLOD-L; a non nBP) has been documented in experimental arthritis (Richards et al. 2001), delayed graft rejection (Slegers et al. 2000), CNS inflammation (Zito et al. 2001), and tumor angiogenesis (Zeisberger et al. 2006), and restenosis (Danenberg et al. 2002, 2003a; Epstein-Barash et al. 2010). Previous studies in our group demonstrated the high efficacy of alendronate liposomes (ALN-L; a nBP) in inflammatory-related disorders such as restenosis (Danenberg et al. 2002, 2003b; Epstein et al. 2007, 2008; Epstein-Barash et al. 2010) and endometriosis (Haber et al.. 2009, 2010).

Macrophages populate the microenvironment of most if not all solid tumors, representing >50% of the tumor mass in certain breast cancers (Lewis and Pollard 2006). Monocytes are recruited into solid tumor stroma where they differentiate into tumor-associated macrophages (TAM). Depletion of TAM by long-circulating CLOD-L, exploiting the enhanced permeability of the tumor microcirculation, has been reported (Banciu et al. 2008). A more potent activation of $\gamma\delta$ T cells could be achieved by a liposomal delivery system due to the preferential uptake by circulating monocytes (Monkkonen et al. 1994; Monkkonen and Heath 1993; Epstein et al. 2008). The indirect therapeutic effect of BP in tumor

is mediated by two different mechanisms, stimulatory effect on $\gamma\delta$ T cells and the inhibition of TAM. We hypothesized that a potent therapeutic effect could be achieved by a liposomal delivery system of nBP, mediated by the two mechanisms. Selective targeting of nBP to monocytes by liposomes would result in a more potent $\gamma\delta$ T cells activation in circulation, and at the tumor tissue by TAM following both, monocytes-laden drug extravasation and passive liposomes accumulation at the tumor site. In addition, inhibition of TAM by liposomal ALN is expected. Liposomal ALN is expected to be more potent than liposomal CLOD since this delivery system is more potent in depleting monocytes and macrophages (Danenberg et al. 2003a; Epstein-Barash et al. 2010). It should be noted that since ALN-L depleting effect on circulating monocytes is noted 36–48 h following treatment (Afergan et al. 2008; Epstein et al. 2007, 2008; Epstein-Barash et al. 2010), activation of $\gamma\delta$ T cells can be achieved during this period.

Herein, we examined the effect of monocytes targeted ALN-L on $\gamma\delta$ T cells activation and on tumor growth. To the best of our knowledge there are no reports in the literature exploiting circulating monocytes for the activation of $\gamma\delta$ T cells by liposomal nBPs. Furthermore, the inhibitory effect of ALN-L on tumor growth has not yet been studied. It should be noted that the indirect mechanism of tumor inhibition mediated by $\gamma\delta$ T cells activation couldn't be elucidated in the current study, because $\gamma\delta$ T cells are unique to primates (Hinz et al. 1997).

16.2 Materials and Methods

16.2.1 Liposome Preparation

Liposomes were prepared by the modified thin-film hydration method (Danenberg et al. 2002; Epstein et al. 2008; Epstein-Barash et al. 2010) with 1,2-distearoyl-sn-glycero-3-phosphocholine (DSPC, Lipoid, Ludwigshafen, Germany), the negatively charged distearoyl-phosphatidylglycerol (DSPG, Lipoid), and cholesterol (Sigma-Aldrich, Israel). Liposomes were prepared at a molar ratio of 3:1:2. The lipids were dissolved in t-butanol and lyophilized overnight. The lyophilized cake was hydrated with an aqueous solution containing 200 mM ALN or CLOD at 55–60°C, and left to stand for 1 h. Blank liposomes were prepared by the same technique, with buffer instead of the drug. Fluorescent liposomes were prepared similarly with 0.025% w/w DSPE-rhodamine (Avanti Polar Lipids, Alabaster, AL) and 15.3% w/w dextran-FITC (Sigma-Aldrich, Israel), membrane and core markers, respectively (Afergan et al. 2008; Epstein-Barash et al. 2010). For small-sized liposomes, the ethanol injection method was used (Epstein et al. 2008; Epstein-Barash et al. 2010). The obtained liposomes were homogenized to a desired size by means of an extruder. To remove un-encapsulated drug, the liposomes were passed through a Sephadex G-50 column and were eluted with buffer.

16.2.2 Liposome Characterization

Liposome size and zeta potential were determined at room temperature after appropriate dilution with MES/HEPES buffer by photon correlation spectroscopy (ALV-GmBH, Langen, Germany) and NanoZ (Malvern Instruments, Malvern, UK), respectively. The phospholipid content was determined colorimetrically with the Bartlett assay (Bartlett 1959; Danenberg et al. 2002; Epstein et al. 2007), cholesterol content was measured by means of HPLC (Lang 1990), and ALN and CLOD content was determined by spectrophotometric assay of their complex with copper (II) ions at λ =240 nm (Danenberg et al. 2003a; Epstein-Barash et al. 2010).

16.2.3 Ex Vivo Cell Culture

16.2.3.1 Human Peripheral Blood Mononuclear Cells (h-PBMCs)

h-PBMCs were isolated from human buffy coat using Ficoll-Hypaque (Amersham-Pharmacia, Uppsala, Sweden) density gradient centrifugation. h-PBMCs were cultured in RPMI media supplemented with 100 U/ml penicillin, 100 μ g/ml glutamine, 10% fetal calf serum (Biological Industries, Beit Haemek, Israel), and 10 U/ml rhIL-2 (Chiron B.V., Amsterdam, The Netherlands).

16.2.3.2 Generation of Monocyte-Derived Immature DC (imDC)

ImDC were generated from monocytes, separated from adhered h-PBMC, by incubation in RPMI 1640 with 10% heat-inactivated human AB serum, supplemented with 1,000 U/ml IL-4 and 1,000 U/ml GM-CSF (R&D, Minneapolis, MN, USA) on days 1 and 4. ImDC were harvested on day five and phenotypically defined by FACS by the following monoclonal antibodies (mAbs): anti-CD14-PE (Dako, Glostrup, Denmark), anti-CD11C-FITC, anti-CD83-FITC and anti-HLA-DR-FITC (Beckman Coulter, Fullerton, CA, USA); and anti-86-PE (BD bioscience, San Jose, CA, USA). Isotype matched mAb were utilized as control (Beckman Coulter and BD bioscience).

16.2.4 Liposome Uptake by h-PBMC and imDC

Freshly isolated h-PBMCs and monocyte-derived imDC were incubated with fluorescent liposomes. Following 4 h of incubation, cells were harvested for assessment of liposomes cellular uptake by confocal microscopy (Zeiss LSM 410) and quantitative uptake by means of FACS (FACScan, Becton Dickinson, USA).

16.2.5 Quantification of TNFα Release

h-PBMCs were cultured at a density of $1 * 10^6$ cells/ml in 96-well u-shaped plates and treated with ALN solution or liposomes for 48 h in the presence of 10 U/ml rhIL-2. The medium was removed after centrifugation of the plate at 1,500 g, and levels of TNF α were quantified with ELISA kit (Peprotech EC Ltd, London, UK) according to the manufacturer's instructions.

16.2.6 Proliferation of $\gamma \delta T$ Cells

h-PBMCs were cultured at a concentration of $1 * 10^6$ cell/ml in 24/well plates. Cells were treated for 9 days with BP solution or liposomes with or without 0.5 µg/ml LPS (LPS, E. coli, serotype 0127:B8, Sigma, Saint Louis, Missouri, USA) in the presence of 10 U/ml rIL-2. On day 4 and 7 of the culture period, one half of the medium was replaced with fresh medium containing rIL-2 and treatments. On day 9 non-adherent cells were harvested and aliquots of $1 * 10^6$ cells were washed with FACS buffer (1% w/v bovine serum albumin (BSA) and 0.02% w/v sodium azide in PBS pH 7.4) and stained with 10 µl anti-CD3-FITC and 5 µl anti-pan-γδ-TCR-PC5 Abs, or the respective isotype-matched controls

(Beckman Coulter, Fullerton, CA, USA) for 30' at 4°C in a final volume of 100 μ I FACS buffer. Adherent cells were detached using 0.25% trypsin/EDTA solution (Biological Industries, Beit Haemek, Israel) and aliquots of 1 * 10⁶ cells were washed with FACS buffer and stained with anti-CD14 Ab (Dako, Glostrup, Denmark) for 30' at 4°C in a final volume of 100 μ I FACS buffer. Dead cells exclusion was done by adding 1 μ g/ml topro3 (Invitrogen, California, USA) to a sample tube of both nonstained adherent and non-adherent cells. Cells were analyzed using BD FACS DIVA LSR II System (Becton Dickinson, USA) and FCS express (Denovo software) was used for quantitative analysis.

16.2.7 Murine Breast Cancer Model

Animal care and procedures were in accordance with the standards for care and use of laboratory animals of The Hebrew University of Jerusalem. Animals were fed with standard laboratory chow and tap water ad libitum. Female athymic nude mice (Harlan Laboratories, Jerusalem, Israel), 6 weeks old, were anaesthetized by isoflurane (Minrad International, USA), and were inoculated subcutaneously in the right flank with human MDA-231 (ATCC, Rockville, MD, USA) breast cancer cells $(1 * 10^6 \text{ cells in } 200 \,\mu\text{l} \text{PBS})$. The injected cancer cells were allowed to grow for 14 days into tumors in the host animals before treatment. The animals were randomly assigned to a treatment of 20 mg/kg free ALN, 20 mg/kg ALN-L or empty liposomes (mean size of $85 \pm 20 \,\text{nm}$), by 3 lateral tail vain injections, on day 14, 16 and 18 (n=4/group). The maximum and minimum diameters of the tumors were measured using a sliding caliper on day 14, 16 and 18. The volume of the tumors was calculated using the formula: $0.5(\text{short axis})^2(\text{long axis})$ (Geran et al. 1972).

16.2.8 Data Analysis

All data are expressed as the mean \pm standard deviation. Comparisons among treatment groups were made by 2-way analysis of variance (ANOVA) followed by Tukey test, and unpaired two-tailed *t*-test when necessary. Differences were termed statistically significant at p<0.05.

16.3 Results

16.3.1 Liposomes Characteristics

The physicochemical characteristics of ALN-L, used for $\gamma\delta$ T cells activation and tumor growth inhibition, are summarized in Table 16.1. The liposomal formulations obtained were negatively charged and in two nano-sizes of 190±24 and 85±20 nm.

Liposome composition (molar ratio)	ALN conc. (mg/ml)	Lipid conc. (mg/ml)	Mean diameter (nm)	Zeta potential (mV)	
DSPC:Chol:DSPG (3:2:1)	5.6±0.51	28.2±2	190±24	-30 ± 2.5	
DSPC:Chol:DSPG (3:2:1)	5.2 ± 0.34	32.9 ± 1.7	85 ± 20	-31.5 ± 1.2	

Table 16.1 Characterization of ALN-L formulations



Fig. 16.1 Uptake of blank liposomes by h-PBMCs. Representative FACS images (**a**), calculated mean \pm SD, N=3 (**b**), and confocal images (**c**). h-PBMCs were incubated with fluorescent liposomes labeled with DSPE-rhodamine (membrane marker) and dextran-FITC (hydrophilic core marker). Following 4 h of incubation cells were harvested for assessment of liposomes internalization by confocal microscopy and FACS analysis (**p<0.01)

16.3.2 Internalization of Liposomes by h-PBMCs Ex Vivo

In order to validate that the liposomes target specifically phagocytic cells, h-PBMCs, were incubated with fluorescent liposomes. The fluorescent liposomes were double-labeled with DSPE-rhodamine (red, membrane marker) and dextran-FITC (green, hydrophilic core marker). Following incubation with h-PBMCs, which comprise of monocytes and lymphocytes, the cells were analyzed by means of FACS. Treatment of h-PBMCs with blank liposomes resulted in internalization by $83 \pm 1.8\%$ of the monocyte cell population, whereas only $6 \pm 0.6\%$ of the lymphocytes internalized the liposomes (Fig. 16.1b). In agreement with the FACS results, confocal microscopy showed specific internalization of liposomes into monocytes (Fig. 16.1c, lower panel), and no liposomes were traced in association with lymphocytes (Fig. 16.1c, upper panel). Co-localization of the lipophilic membrane marker with the hydrophilic core marker (Fig. 16.1c right column, orange color) indicated the uptake of intact liposomes.

16.3.3 ALN Loaded Liposomes Bioactivity Ex Vivo

16.3.3.1 Proliferation of γδ T Cells

In cultures of h-PBMCs, the proportion of $\gamma\delta$ T cells in the CD3⁺ cell population was determined following various treatments in the presence of IL2 (Fig. 16.2). The control group, non-treated h-PBMCs, had 5.6±0.4% $\gamma\delta$ T cells in the CD3⁺ cell population. Treatment with ALN in solution or encapsulated in liposomes (1 µM) significantly increased the proportion of $\gamma\delta$ T cells,



Fig. 16.2 The effect of bisphosphonates (clodronate, CLOD) and amino BP (alendronate, ALN) and liposomes (liposomal CLOD and ALN, CLOD-L and ALN-L, respectively) on $\gamma\delta$ T cells proliferation. (a) FACS profiles of the T cells gated population. (b) Proportion of CD3⁺ $\gamma\delta$ -T cells (%). h-PBMCs were double stained with anti-CD3 and anti $\gamma\delta$ TCR Abs before FACS analysis of the T-cell–gated population. (c) h-PBMCs viability by TO-PRO-3 staining and (d) CD3⁺ counts. h-PBMCs were cultured for 9 days with 1 μ M of various formulations in the presence of IL-2. Data shown is the mean ± SD of experiments with h-PBMCs from 4 to 7 independent donors (**p<0.01)

 $50.9 \pm 12.2\%$ and $49.5 \pm 12.9\%$ of the CD3⁺cell population, respectively. Empty liposomes, CLOD (a non nBP) in solution and encapsulated in liposomes did not affect $\gamma\delta$ T cells proliferation. The similar increase of the $\gamma\delta$ T cell population following treatment with ALN as a free drug and in liposomes was associated with no changes in both cells' viability (Fig. 16.2c) and CD3 expression (Fig. 16.2d).

16.3.3.2 TNFα Secretion

After verifying the selective targeting of liposomes to monocytes in h-PBMCs cultures, the potential of the delivered ALN to exert its bioactivity on $\gamma\delta$ T cell was studied by examining TNF α activation. Treatment with ALN in solution or in liposomes resulted in an increased, dose-dependent, TNF α secretion from h-PBMCs (Fig. 16.3).

16.3.3.3 Proliferation of γδ T Cells in LPS-stimulated Monocytes

Proliferation of $\gamma\delta$ -T cells was evaluated in the presence of LPS-induced activation of monocytes. Elevated proportions of $\gamma\delta$ -T cells were found in LPS treated h-PBMCs with or without ALN solution, in comparison with to no LPS, $56.4 \pm 4.5\%$, $15.2 \pm 3.2\%$ and $44.6 \pm 12.2\%$, $6.1 \pm 3.4\%$ of the CD3⁺cell population, respectively. The stimulatory effect of ALN-L on $\gamma\delta$ T cells proliferation was diminished when the h-PBMCs were co-treated with LPS, $52.5 \pm 12\%$ and $24.3 \pm 4.8\%$ of the CD3⁺cell population, respectively (Fig. 16.4).



Fig. 16.4 The effect of alendronate (ALN) and liposomal ALN (ALN-L) on $\gamma\delta$ T cells proliferation in the presence of LPS. The proportion of CD3+ $\gamma\delta$ T cells was determined 9 days following h-PBMCs incubation with 1 μ M ALN solution or liposomes in the presence of IL-2 with or without 0.5 μ g/ml LPS. h-PBMCs were double stained with anti-CD3 and anti $\gamma\delta$ TCR Abs before FACS analysis of the T-cell-gated population. Data shown is the mean±SD of experiments with h-PBMCs from two independent donors

16.3.3.4 Interplay Between γδ T Cells and APCs

After assessing the bioactivity of ALN-L on $\gamma\delta$ T cells, its effect on monocytes was further examined. Following treatment of h-PBMCs with ALN solution or liposomes, the proliferation of $\gamma\delta$ T cells and the proportion of monocytes in the h-PBMCs culture were quantified (Fig. 16.5). In order to avoid monocytes depletion, a low concentration of ALN was used (<1 μ M). Treatment with both ALN solution and liposomes resulted in elevated counts of $\gamma\delta$ T cells in the CD3⁺cell population, and in a dose dependent manner (Fig. 16.5a). The proliferation of $\gamma\delta$ T cell was inversely correlated with CD14⁺ expression in the adherent cells (Fig. 16.5b). It should be noted that lymphocytes and monocytes viability was similar in all treatments (data not shown).

Down regulation of the CD14 receptor could suggest differentiation of monocytes to dendritic cells (DC) following $\gamma\delta$ T cell stimulation. In order to validate that liposomes also target DC, human imDC were incubated with fluorescently labelled liposomes. Human imDC were phenotypically defined as



CD14⁻, CD11c⁺, CD83⁻, CD86⁺ and HLA-DR⁺ (Fig. 16.6 left). Following 4 h incubation with fluorescent liposomes, 48±3% of the imDC, gated as Cd11C⁺, were fluorescently stained (Fig. 16.6 right).

16.3.4 Effect of ALN-L on Tumor Growth In Vivo

The effect of ALN-L on tumor growth was studied *in vivo* (Fig. 16.7). Athymic nude mice were inoculated with human MDA-231 breast cancer cells, and blank liposomes, ALN and ALN-L were IV administered at day 14, 16 and 18. Animals treated with ALN solution exhibited necrosis at the injection area, and the animals were euthanized before the end of the experiment. This phenomenon was not observed in liposome treated animals, either empty or ALN loaded. Tumor growth inhibition was observed following treatment with ALN-L, but the results did not reach statistical significance due to the small number of animals.

16.4 Discussion

We demonstrate here that selective targeting of ALN to monocytes by conventional liposomes resulted in $\gamma\delta$ T cells proliferation *ex vivo*. Furthermore, we show preliminary results of tumor growth inhibition *in vivo* by ALN-L in a mechanism not involving $\gamma\delta$ T cells activation.

Activated $\gamma\delta$ T cells display distinct natural killer functions and directly eliminate transformed cells, a feature that is successfully being exploited in immunotherapy trails in cancer patients (Dieli et al. 2007; Wilhelm et al. 2003). Intravenous stimulation by nBP of $\gamma\delta$ T cells in patients for cancer immunotherapy is thought to involve accumulation of IPP in APCs (Eberl et al. 2009; Miyagawa et al. 2001; Roelofs et al. 2009). The full clinical impact of these drugs efficacy is impeded due to rapid urine elimination and bone accumulation (Rodan 1998a; Fleisch 1998). Moreover, due to their high charge and hydrophilicity, free BP do not easily cross cell membranes. We hypothesized that selective



Fig. 16.6 Human derived imDC phenotype characterization and uptake of liposomes. FACS images of imDC phenotypes (*left*) and quantitative uptake of fluorescently labeled liposomes (*right*). imDC were generated from CD14⁺ h-monocytes treated with GMCSF and IL4 for 5 days. imDC were incubated with fluorescent liposomes labeled with DSPE-rhodamine (membrane marker). Following 4 h of incubation cells were harvested for assessment of liposomes cellular uptake of CD11C gated cells (mean \pm SD)



Fig. 16.7 The anti-tumor effect of liposomal alendronate (ALN-L) in athymic mouse model of human breast cancer. Shown is the tumor volume following treatment with ALN-L (20 mg/kg) and control (blank liposomes) by 3 IV injections (on day 14, 16, and 18) 14 days post tumor cells inoculation. Results are presented as the mean \pm SD (n=4)

targeting of nBP to monocytes would result in a more potent $\gamma\delta$ T cells activation. We utilized liposomes to deliver encapsulated ALN to APCs for optimizing ALN efficacy due to increased uptake. Since ALN-L depleting effect on circulating monocytes is noted 36–48 h following treatment (Afergan et al. 2008; Epstein et al. 2007, 2008; Epstein-Barash et al. 2010), activation of $\gamma\delta$ T cells can be achieved during this period. In this study we have used 'conventional' liposomes endowed with preferable physicochemical properties for monocyte-targeting; negatively charged membrane, that enhances the internalization of liposomes into phagocytic cells (Epstein-Barash et al. 2010; Patel 1992; Patel and Moghimi 1998), and in a mean diameter size of <200 nm, for maximizing both efficacy and safety (Allen and Hansen 1991; Epstein-Barash et al. 2010; Rodrigueza et al. 1993; Torchilin 2005).

Since $\gamma\delta$ T cells are unique to primates (Hinz et al. 1997) our study on the effect of liposomal formulations was limited to ex vivo experiments. We first assessed the selective targeting of conventional liposomes to monocytes in ex vivo cultures of h-PBMCs, which comprise of monocytes and lymphocytes. It should be noted that the specific uptake by DC in the PBMC culture was not determined. Liposomes were selectively internalized intact by $83 \pm 1.8\%$ of h-monocytes, whereas only $6 \pm 0.6\%$ of the lymphocytes internalized liposomes following 4 h of incubation (Fig. 16.1). The scant uptake of liposomes by lymphocytes is attributed to B cells, and not T cells, as previously demonstrated for nanoparticles (Sela et al. 2010). The intracellular accumulation of IPP in monocytes, caused by nBP inhibition of FPP synthase of the mevalonate pathway, subsequently activates cytotoxic $\gamma\delta$ T cells proliferation and secretion of pro-inflammatory cytokines (Hewitt et al. 2005). As expected from a non nBP (Kunzmann et al. 2000), treatment with CLOD-L or the free drug had no effect on $\gamma\delta$ T cells proliferation (Fig. 16.2b). The similar stimulatory effect of liposomal and free ALN on $\gamma\delta$ T cells proliferation (Fig. 16.2b) and TNFa secretion (Fig. 16.3) is most likely due to a similar uptake of free and ALN-L by monocytes in culture. The significantly increased cellular uptake, in tissue cultures, of particulated dosage forms of BPs in comparison to free BPs is not observed when the free BP concentration is low (<1 μ M) (Monkkonen et al. 1994). This is because the cellular uptake of free BPs by monocytes/macrophages in vitro is mediated probably by a calcium complex formed in the culture media (Monkkonen and Heath 1993; Monkkonen et al. 1994). At low BPs concentration the calcium to BP ratio is high, enabling enhanced complexation of free ALN and internalization.

Human $\gamma\delta$ T cells recognition of LPS is predominately presented by CD1 on APCs resulting in increased $\gamma\delta$ T cells proliferation (Hava et al. 2005; Cui et al. 2009). ALN in liposomes and as a free drug increases the secretion of inflammatory cytokine by LPS-stimulated monocytes (Epstein-Barash et al. 2010; Makkonen et al. 1999). However, treatment by LPS reduced the stimulatory effect of ALN-L (Fig. 16.4), which is in contrast to the expected synergistic stimulation of $\gamma\delta$ T cells by LPS and ALN co-treatment. The molecule through which IPP is presented to the $\gamma\delta$ T cell receptor is still unknown (Clezardin 2010). It could be suggested that the presentation of LPS and phospholipids on monocytes hindered the presentation of IPP resulting in the reduced stimulatory effect of $\gamma\delta$ T cells proliferation.

Down regulation of CD14 in monocytes (adherent cells), by both ALN as a free drug and in liposomes, correlated conversely with the proliferation of $\gamma\delta$ T cells (Fig. 16.5), suggesting that activated $\gamma\delta$ T cells may have induced this phenotypic change. This notion is supported by the pronounced reciprocal effect of $\gamma\delta$ T cells stimulation on APCs (Devilder et al. 2006). Activated $\gamma\delta$ T cells secrete cytokines such as TNF- α , which in turn down regulate CD14 expression, and cause differentiation of monocytes into DC (Eberl et al. 2009). Recently, it has been shown that amplified activation of $\gamma\delta$ T cells can be achieved by another nBP (zolendronate) treated DC (Cabillic et al. 2010). The liposomes ability to target human imDC (Fig. 16.6 right) suggests that a positive feedback could be obtained for the amplification of $\gamma\delta$ T cells. ALN-L will activate $\gamma\delta$ T via monocytes, which in turn will stimulate monocytes differentiation into DC, an the latter will engulf liposomes further activating $\gamma\delta$ T cells (Takahara et al. 2008).

We observed an anti-tumor effect of liposomal ALN in mice (Fig. 16.7), with no overt infection or side effects. A growing body of evidence suggests that the anti-tumor effect of nBP is mediated by both direct and in-direct mechanisms (Caraglia et al. 2010; Clezardin 2010; Clezardin and Massaia 2010).

Since activation of $\gamma\delta$ T cell is excluded in mice, the anti-tumor effect in our study should be attributed to passive tumor targeting as has been demonstrated for <200 nm liposomes in a murine bearing human breast cancer (Mayer et al. 1990). A direct cytotoxic effect on tumor cells is also unlikely since no significant accumulation of non-targeted liposomal formulations is expected in tumor cells (Kirpotin et al. 2006; Shmeeda et al. 2010). Thus, it is reasonable to assume that the tumor growth inhibition by ALN-L was mediated by TAM depletion, and possibly the induced differentiation of M2 into M1 (Veltman et al. 2010). The depletion of TAM and blood monocytes by liposomal formulations of CLOD and tumor growth inhibition has been reported (Banciu et al. 2008; Hiraoka et al. 2008; Zeisberger et al. 2006). ALN-L may possess a stronger anti-tumor effect than CLOD-L since it is more potent in depleting monocyte/macrophages (Danenberg et al. 2003a; Epstein-Barash et al. 2010), and at the same time, can stimulate $\gamma\delta$ T cells activation since it is an nBP.

In attempts to increase the circulation time of nBP, Zhang et al. synthesized lipophilic pyridinium BP, which exhibit a pronounced $\gamma\delta$ T cells stimulatory effect following incubation with h-PBMCs ex vivo (Zhang et al. 2010). However, systemic side effects were noted following the activation of $\gamma\delta$ T cells (Adami et al. 1987; Hewitt et al. 2005), and the uptake of these compounds by APCs in vivo has not been determined. Recently, Shmeeda et al. reported that folate-targeted liposomes containing zolendronate has a potent *in vitro* cytotoxic activity on tumor cells (Shmeeda et al. 2010). In another study it was found that zolendronate activates $\gamma\delta$ T cells to lyse tumor cells in cell culture (Li et al. 2009). Thus, it can be assumed that treatment with a combined formulation of targeted and conventional liposomes encapsulating nBP may result in a synergistic anti-tumor effect mediated by activation of $\gamma\delta$ T cells as well as by depletion of tumor cells and monocytes/TAM. In light of our results that ALN-L activate $\gamma\delta$ T cells *ex vivo*, we can envisage the following picture *in vivo*: Enhanced activation of $\gamma\delta$ T cells would be obtained due to interaction with circulating monocytes as well as by TAM endocytosing liposomal nBP, leading to a potentiated anti-tumor effect of nBP. It should be noted that this scenario is speculative since $\gamma\delta$ T cells are unique to primates (Hinz et al. 1997). The potential anti-tumor activity of ALN-L by activating cytotoxic $\gamma\delta$ T cells and the resultant inhibition of tumor growth, presented in this study, could be assessed by investigations in primates correlating depletion of TAM and $\gamma\delta$ T cells activation.

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