Hypoxia as a Biomarker and for Personalized Radiation **Oncology**

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Abstract

Tumor hypoxia is a clinically relevant cause of radiation resistance. Direct measurements of tumor oxygenation have been performed predominantly with the Eppendorf histograph and these have defined the reduced prognosis after radiotherapy in poorly oxygenated tumors, especially head-and-neck cancer, cervix cancer and sarcoma. Exogenous markers have been used for immunohistochemical detection of hypoxic tumor areas (pimonidazole) or for positron-emission tomography (PET) imaging (misonidazole). Overexpression of hypoxia-related proteins such as hypoxiainducible factor-1 α (HIF-1 α) has also been linked to poor prognosis after radiotherapy and such proteins are considered as potential endogenous hypoxia markers.

Keywords

Tumor hypoxia \cdot Tumor oxygenation \cdot Pimonidazole \cdot Hypoxia-inducible factor- 1α

1 Introduction

Intratumoural hypoxia is a clinically relevant condition causing radiation resistance of tumour cells. The insufficient supply of fast-growing tumours with blood vessels and the pathologic structure of intratumoural vessels, respectively, have been

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associated with two mechanisms of tumour hypoxia. Specifically, these are diffusion-limited hypoxia caused by long distances of individual tumour cells from the nearest blood vessel versus perfusion-limited tumour hypoxia which can also occur close to (non-perfused) blood vessels due to the presence of vascular leaks, thrombosis or shunts. These two types have also been referred to as "chronic" and "acute" hypoxia, respectively. However, oxygenation of a tumour is considered a dynamic process, and in many tissues, intermittent changes of oxygen concentration are observed ("cyclic hypoxia").

The classic explanation of hypoxia-associated radioresistance in tumour cells is the interference of molecular oxygen with DNA repair. Oxygen has been shown to bind to sites of radiation-induced DNA damage, thereby causing fixation of DNA lesions and preventing repair. In in vitro experiments, an oxygen-enhancement ratio (OER) of 2–3 has been determined, meaning that compared to a reference dose of ionizing radiation under normoxic conditions, 2–3 times this dose has to be given to achieve equivalent cell kill under anoxic (0 % oxygen) conditions.

In vivo, an additional mechanism causing treatment resistance of hypoxic tumours is the selection of tumour cells with increased anti-apoptotic, proliferative and metastatic characteristics by conditions of hypoxia (Graeber et al. [1996](#page-14-0)). This chapter will discuss currently available methods to detect intratumoural hypoxia and their clinical applicability.

2 Direct Measurements of Tumour Oxygenation

Probably, the most direct method for identifying hypoxia in tumours involves inserting electrodes into the tissue and monitoring the actual oxygenation status. This approach was first applied to human tumours in the 1960s using "home-made" glass electrodes. These early polarographic electrodes were, however, generally cumbersome and fragile, and only a few $pO₂$ values 3–4 mm below the surface of the tumour were possible. Nevertheless, clinical data were obtained in cervix (Kolstad [1968](#page-15-0)) and head-and-neck (Gatenby et al. [1988](#page-14-0)) cancer patients that clearly demonstrated a relationship between the oxygenation measurements and outcome to radiation therapy, in that those patients with tumours that were better oxygenated had a significantly superior local response to irradiation.

This whole area was revolutionized with the development of the Eppendorf histograph, which had two distinct improvements. The first was having a more robust electrode with the oxygen sensor protected inside a metal needle. A second improvement was the attachment of this needle to a stepping motor that allowed for multiple measurements along the needle track through the tumour; thus, detailed oxygen partial pressure $(pO₂)$ distributions were possible. Numerous clinical studies were thus undertaken in a variety of human tumour types. The results clearly showed that hypoxia was a characteristic feature of virtually all human tumours investigated, although the degree of hypoxia could be variable (Vaupel et al. [1989\)](#page-19-0). Probably, the most significant finding from these studies was the confirmation that hypoxia influenced outcome to therapy. This has been reported for head and neck

Fig. 1 Relationship between tumour oxygenation estimated prior to therapy using the Eppendorf histograph and eventual outcome to that therapy. **a** Overall survival for 89 cervix patients given surgery or radiotherapy with curative intent in which the median $pO₂$ values were above or below 10 mmHg. b Freedom from distant failure in 22 patients with soft tissue sarcomas receiving preoperative irradiation and hyperthermia in which the tumour median $pO₂$ values were above or below 10 mmHg. c Overall survival for 397 head-and-neck cancer patients after primary radiation therapy in which the percentage of $pO₂$ values less than or equal to 2.5 mmHg was above (more hypoxic) or below (less hypoxic) the median value of 19 %. **d** Freedom from biochemical failure for 57 prostate patients treated with brachytherapy in which the prostate/muscle (P/M) mean $pO₂$ ratio was above or below 0.10. Composite figure derived from Hoeckel et al. ([1996](#page-15-0)) (a); Brizel et al. [\(1996](#page-13-0)) (b); Nordsmark et al. [\(2005](#page-17-0)) (c); and Turaka et al. [\(2011\)](#page-18-0) (d)

(Nordsmark et al. [1996](#page-17-0), [2005](#page-17-0); Brizel et al. [1997](#page-13-0); Stadler et al. [1999](#page-18-0); Rudat et al. [2001\)](#page-18-0), cervix (Hoeckel et al. [1993,](#page-15-0) [1996](#page-15-0); Knocke et al. [1999](#page-15-0); Fyles et al. [1998](#page-14-0), [2006;](#page-14-0) Lyng et al. [2000\)](#page-16-0), soft tissue sarcomas (Brizel et al. [1996](#page-13-0); Nordsmark et al. [2001\)](#page-17-0), and prostate (Turaka et al. [2011](#page-18-0)). Examples of the typical results obtained in each of these clinical sites are illustrated in Fig. 1 and clearly show that patients with more hypoxic tumours had a poorer outcome to therapy. Perhaps the most striking results were those made in cervix and sarcomas that showed hypoxia to influence outcome in patients in which surgery was the primary or only treatment (Hoeckel et al. [1996](#page-15-0); Nordsmark et al. [2001](#page-17-0)), suggesting that hypoxia could also influence malignant progression, especially metastatic spread. In fact, one other study in cervix was able to show that the primary tumours of patients with metastases were indeed more poorly oxygenated than those of patients without metastases (Sundfør et al. [1998](#page-18-0)).

Today, the Eppendorf electrode is no longer commercially available, and there are a number of reasons for this. Without using concurrent imaging during the oxygen measurements, it was impossible to state whether the values obtained were from viable tissue, and even where this was done one could not state whether the cells in the hypoxic regions were clonogenic; the tumours themselves had generally to be easily accessible; and the technique was invasive. Furthermore, despite the positive findings between the Eppendorf measurements and treatment outcome, the machine was never predictive of response on a patient-to-patient basis. This was clearly illustrated in one of the first clinical studies using head-and-neck cancer patients (Nordsmark et al. [1996\)](#page-17-0). Here, the 35 patients in which tumour oxygenation measurements were performed could be separated into two distinct groups with those patients having the more hypoxic tumours showing a significantly lower local tumour control following conventional radiation therapy. However, some 40 % of the patients did not fall within the correct category; they were hypoxic but controlled or had no hypoxia yet failed. Despite the various limitations, the results obtained from the Eppendorf studies must still be considered positive in that it supplied us with a tremendous level of information about tumour hypoxia and its importance.

Another approach that may have the potential to measure tumour oxygenation status involves the use of fibre optic probes. Unlike the Eppendorf histogram electrode, these do not consume oxygen with each measurement; thus; continuous observations of oxygenation status in the same tumour region is possible (Griffiths and Robinson [1999](#page-14-0)). Preclinical studies comparing the commercially available Oxford-Optronix OxyLite sensor with the polarographic techniques (Collingridge et al. [1997;](#page-13-0) Braun et al. [2001](#page-13-0); Seddon et al. [2001;](#page-18-0) Wen et al. [2008](#page-19-0)), or classical paired survival curve estimates of radiobiological hypoxia (Urano et al. [2002\)](#page-18-0), reported similarities and differences depending on the tissue type, tumour size or the changes observed using various modifiers of tumour hypoxia. Although fibre optic probes have the potential to not only measure the pretreatment level of tumour hypoxia, but also to monitor tumour oxygenation status continuously during and after treatment, there has as yet been no clinical application in cancer.

Other less invasive attempts to directly measure tumour oxygenation have involved phosphorescence tomography- or magnetic resonance (MR)-based approaches. The former requires the infusion of water-soluble phosphor probes into the vasculature (Vikram et al. [2007\)](#page-19-0) and has been used to map oxygen concentration in preclinical tumour models (Wilson and Cerniglia [1992](#page-19-0); Fukumura et al. [2001\)](#page-14-0), but again has not been used in patients. The MR approaches include monitoring oxygen-sensitive reporter molecules $(^{19}$ F-oximetry). Several such molecules have been developed including perfluorochemical emulsions and hexafluorobenzene (Pacheco-Torres et al. [2011\)](#page-17-0). The latter approach allowed for actual quantification of the MR signals and conversion into oxygen concentrations at the pixel level (Zhao et al. [2005\)](#page-19-0). However, systemic toxicity required the imaging agent to be injected directly into tumours limiting its potential clinical application. An alternative MR method is electron paramagnetic resonance (EPR),

which detects paramagnetic materials that have been injected into tissues (Krishna et al. 2012). It can provide quantitative and repeated 3D estimates of oxygenation and has been extensively used in preclinical studies and even in patients for a range of different clinical problems (Swartz et al. [2004\)](#page-18-0). Although many of the preclinical studies have focused on tumour hypoxia, the clinical application of EPR in cancer has, however, been somewhat limited (Krishna et al. [2012\)](#page-16-0).

3 Exogenous Markers of Hypoxia

The oxygen mapping techniques described above involve injecting exogenous agents to directly ascertain oxygen values that are low and equivalent to hypoxia. A more widely studied method for indirectly detecting tumour hypoxia involves the administration of exogenous compounds that under hypoxic conditions undergoes a chemical change from a non-reactive species to a highly reactive product that then binds to macromolecules within the cell. Subsequent application of techniques that can identify this bound product will allow us to demonstrate the presence of hypoxia. The most popular agents used in this context have been 2-nitroimidazole-based markers. These nitroimidazole compounds were originally developed as hypoxic cell radiosensitizers, with the 2-nitroimidazoles being the most effective agents for enhancing radiation response in preclinical models (Adams and Cooke [1969](#page-13-0)). Such compounds are characterized by having an $NO₂$ grouping attached to the imidazole ring structure. This $NO₂$ group can undergo a 6-electron intracellular reduction to produce NH_2 , and although the NO_2 and NH_2 moieties are generally inactive, one of the formed intermediates is highly reactive and can bind to any macromolecule within the cell (Horsman et al. [2012](#page-15-0)). In the presence of oxygen, typically above 10 mmHg, the first electron reduction species formed reacts with oxygen and returns to the $NO₂$ moiety with the subsequent production of oxygen radicals that ultimately form hydrogen peroxide, and it is this lack of further reduction that gives rise to the hypoxia specificity. The bound product formed under hypoxia can be identified either using an antibody to the product or by labelling the original compound with a radioactive tracer such as ${}^{1}H$ or ${}^{14}C$. The most commonly used nitroimidazole is pimonidazole, the binding of which in preclinical studies was found to correlate with radiobiological hypoxia (Raleigh et al. [1999](#page-17-0)). Additional clinical studies showed that the degree of pimonidazole binding was related to radiation-induced local tumour control in head-and-neck cancer (Kaanders et al. [2002](#page-15-0)), but not cervix (Nordsmark et al. [2006](#page-17-0)). Similar positive findings for head-and-neck cancer patients were reported between radiotherapy outcome and the degree of hypoxia estimated using another nitroimidazole marker, EF5 (Evans et al. [2007](#page-14-0)).

By labelling the nitroimidazole compound with 18 F will allow for the hypoxia produced bound product to be identified using positron emission tomography (PET). The first tracer developed for hypoxia PET imaging was a $[{}^{18}F]$ -fluorinated version of the radiosensitizer misonidazole (FMISO) and was found to be capable of identifying hypoxia in a range of human tumours (Rasey et al. [1996\)](#page-17-0). It was followed by a group of compounds based on another radiosensitizer, etanidazole

(i.e. EF3/5). These markers have a relatively high lipophilicity which allows for easy penetration of cell membranes and diffusion into tumour tissue, but simultaneously limited the clearance of unbound tracer, thus leading to relatively low tumour-to-reference tissue ratios. Other fluorinated nitroimidazole compounds have been developed which are more water soluble than FMISO and therefore easier to clear from non-hypoxic tissue. These have included fluoroetanidazole (FETA), fluoroerythronitroimidazole (FETNIM), fluoroazomycinarabinofuranoside (FAZA) and HX4, of which the latter two are currently in clinical evaluation (Schuetz et al. [2010;](#page-18-0) van Loon et al. [2010\)](#page-19-0). It is difficult to say whether one tracer is superior to another in identifying tumour hypoxia, since there has never been any systematic examination of all the 2-nitroimidazoles tracers in the same tumour model or patient population. The ideal tracer would be one in which clearance of unbound tracer is complete at the time of imaging; thus, only bound material indicative of hypoxia is measured. This can take many hours and even days to achieve, but such measurements have to take into account decay of the radioactive marker and normal clinical schedules. As a result, static scans are typically made 2–4 h after tracer administration, which results in low inter-tissue and intratumour contrast. An alternative approach involves labelling the nitroimidazoles with long-lived radionuclides, for example $[1^{24}I]$ -iodoazomycin arabinoside $(1^{24}I-AZA)$ and $[$ ¹²⁴I]-iodoazomycin galactoside (¹²⁴I-AZG), allowing for delayed scans up to 24 and 48 h after tracer administration. Unfortunately, the results have been disappointing with no improvement in image contrast and poor counting statistics (Rischin et al. [2006;](#page-18-0) Reischi et al. [2007](#page-17-0)), and it is unlikely that the problems inherent to hypoxia PET can be solved exclusively by better tracers. One small study in head-and-neck cancer patients (Thorwarth et al. [2005](#page-18-0)) demonstrated that pharmacokinetic analysis of the shape of tumour time activity curves (TACs) obtained from dynamic PET scans increased prognostic accuracy compared to traditional analysis of static PET images. However, dynamic scans are cumbersome and expensive, and cause inconvenience to patients; the analysis is complex; and different estimates of hypoxia can be obtained depending on the kinetic model and tumour type used.

Regardless of whether static or dynamic assessment is applied, one of the major issues with PET markers is that the cells must be hypoxic for significant time periods to be detected, which means that such markers are more likely to identify diffusion-limited chronic hypoxia rather than acute hypoxia resulting from transient fluctuations in blood flow (Horsman et al. [2012\)](#page-15-0). Another significant problem facing the application of PET hypoxia markers is one of resolution in which the voxel sizes identified in the PET scans are much larger than most of the hypoxic structures (Horsman et al. [2012\)](#page-15-0). Thus, the actual PET image does not accurately reflect the true hypoxia heterogeneity at the microregional level.

Several of the nitroimidazole-based PET markers have undergone clinical evaluation with respect to correlating the hypoxia estimates with outcome to radiation therapy. The majority of studies involved FMISO measurements in head-and-neck cancer patients (Rajendran et al. [2006;](#page-17-0) Rischin et al. [2006](#page-18-0); Thorwarth et al. [2006;](#page-18-0) Eschmann et al. [2007;](#page-14-0) Dirix et al. [2009](#page-14-0); Lee et al. [2009](#page-16-0); Kikuchi et al. [2011;](#page-15-0)

Fig. 2 Results from four different clinical trials showing the relationship between hypoxia imaging and outcome to therapy. a Disease-free survival in 40 head-and-neck cancer patients based on the preradiation therapy estimate of hypoxia as determined by a tumour-to-muscle ratio of $>$ 1.4 from $\binom{18}{1}$ FAZA PET measurements. **b** Progression-free survival in 38 cervical cancer patients receiving radiotherapy and chemoradiotherapy in which the tumour/muscle (T/M) levels of 60 Cu-ATSM were above or below the threshold dose of 3.5. c Overall survival for 32 non-small-cell lung cancer patients in which the tumour-to-normal tissue (T/N) ratio measured with ^{99m}Tc-HL91 SPECT before radiation therapy was above/below 1.47. d Disease-specific survival in 98 cancer patients based on the level of perfusion measured with DCE-MRI either before or before and during radiation treatment. Composite figure derived from Mortensen et al. ([2012\)](#page-17-0) (a); Dehdashti et al. [\(2008](#page-14-0)) (b); Li et al. ([2006\)](#page-16-0) (c); and Mayr et al. [\(2010](#page-16-0)) (d)

Zips et al. [2012\)](#page-19-0). Two other studies in head and neck used either FETNIM (Lehtio et al. [2004](#page-16-0)) or FAZA (Mortensen et al. [2012](#page-17-0)). Results from the latter study using FAZA as the imaging agent are illustrated in Fig. 2 and clearly show that like all the other head-and-neck studies, patients with hypoxic tumours had a significantly poorer outcome. Similar findings were found using FETNIM in lung (Li et al. [2010\)](#page-16-0) and oesophagus (Yue et al. [2012\)](#page-19-0), FAZA in sarcomas (Khamly et al. [2008](#page-15-0)) and cervix (Scheutz et al. [2010\)](#page-18-0) and FMISO in central nervous system tumours (Spence et al. [2008\)](#page-18-0). Despite the positive findings obtained with all these nitroimidazole-based hypoxia PET markers, the situation remains the same as seen with the oxygen electrode methods in that although we can verify the presence of hypoxia in human

tumours and demonstrate that it influences outcome to therapy, we still cannot use the results to select those patients that are hypoxic on an individual basis.

A chemically different group of putative PET markers that may have the potential to identify tumour hypoxia includes Cu-ATSM $[Cu(II)$ -diacetyl- $bis(N^4$ -methylthiosemicarbazone)], which can be labelled with a variety of positron-emitting isotopes of copper. Cu-ATSM has been shown to have high membrane permeability and fast tumour uptake, thus allowing for rapid imaging after injection (Dearling et al. [1998\)](#page-14-0), but its exact retention mechanism is still not completely understood. The hypoxia specificity is believed to occur because while the Cu^{2+} moiety can easily pass across cell membranes, under low oxygen conditions the $Cu²⁺$ is converted to $Cu¹⁺$ which is then trapped within cells (Vävere and lewis [2007](#page-19-0)). A good correlation between Cu-ATSM and $pO₂$ measurements (Lewis and Welch [2001;](#page-16-0) O'Donoghue et al. [2005\)](#page-17-0) and nitroimidazole-based hypoxia markers (O'Donoghue et al. [2005;](#page-17-0) Dence et al. [2008](#page-14-0)) have been shown in preclinical studies, although these effects are time- and tumour-dependent (O'Donoghue et al. [2005\)](#page-17-0). Measurements in patients with lung (Dehdashti et al. [2003](#page-14-0)), cervix (Dehdashti et al. [2008](#page-14-0)), rectal (Dietz et al. [2008\)](#page-14-0) or head-and-neck (Minagawa et al. [2011](#page-16-0)) cancer support the possibility of using Cu-ATSM as a marker of outcome to radiotherapy. The results from the cervix trial (Dehdashti et al. [2008](#page-14-0)) are shown in Fig. [2](#page-6-0) and clearly demonstrate that those patients with a higher tumour uptake of Cu-ATSM, and presumably more hypoxic, had a lower progression-free survival. However, additional studies have shown Cu-ATSM to be affected by mechanisms other than hypoxia and that it is also insensitive to treatments that modify tumour oxygenation (Yuan et al. [2006](#page-19-0)); thus, its potential to be used as a specific marker for tumour hypoxia remains unclear.

The use of alternative radioactive labels allows for the possibility to use other non-invasive imaging techniques to identify hypoxia in tumours. Such an approach has been achieved with a number of $\int_0^{123} I^{125}$. iodoazomycin derivatives which can be detected using single-photon emission computer tomography (SPECT). Of these, only $\lceil^{123} \rceil$ -iodoazomycin arabinoside (IAZA) has undergone clinical evaluation (Urtasun et al. [1996](#page-19-0)), and it was found that head-and-neck cancer patients with positive IAZA scans had a poorer outcome to radiotherapy than those patients with negative scans. Other potential SPECT markers for hypoxia that have been developed include ^{99m}Technetium-labelled compounds, such as BMS 181321 and BRU59-21, and complex ligands, specifically HL91. BRU59-21 was investigated in a phase I study in patients with head-and-neck cancer, and a significant correlation was found with pimonidazole binding (Hoebers et al. [2002\)](#page-15-0). HL91 uptake was studied in non-small-cell lung cancer patients prior to radiation therapy, and the results, as shown in Fig. [2](#page-6-0), demonstrated that those patients with the highest uptake had a significantly poorer response (Li et al. [2006\)](#page-16-0). Various $[1^9F]$ -labelled nitorimidazole compounds have also been developed which can be detected using MR. To-date, two $[1^9F]$ -labelled nitroimidazoles have been developed, namely $[$ ¹⁹F]-EF5 and $[$ ¹⁹F]-SR 4554. Of these, only $[$ ¹⁹F]-SR 4554 underwent some clinical evaluations (Seddon et al. [2003\)](#page-18-0), but there has not been any real follow-up.

An alternative MR approach that utilizes measurements made after injecting an exogenous marker is dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI). This involves intravenously injecting a contrast agent and then monitoring its extravasation over several minutes from a region of interest (Nielsen et al. [2012](#page-17-0)). The focus with these estimates is actually on tumour perfusion, but this may still be an excellent method for identifying tumour hypoxia; oxygen delivery occurs via the vascular supply so the measurements could reflect chronic hypoxia, and changes in perfusion are clearly responsible for fluctuating hypoxia (Horsman et al. [2012\)](#page-15-0). Clinical studies have been performed with DCE-MRI and reported that the parameters obtained actually correlated with oxygen electrode measurements in cervix (Cooper et al. [2000;](#page-13-0) Lyng et al. [2001\)](#page-16-0), pimonidazole binding in head and neck (Newbold et al. 2009 ; Donaldson et al. 2011) and $\binom{18}{1}$ -FMISO uptake in glioblastoma multiforme (Swanson et al. [2009](#page-18-0)) and head-and-neck nodal metastases (Jansen et al. [2010\)](#page-15-0). Several studies have also attempted to correlate the DCE-MRI measurements with radiotherapy outcome in patients with cervical cancer (Loncaster et al. [2002](#page-16-0); Mayr et al. [2010](#page-16-0); Andersen et al. [2012\)](#page-13-0) and reported that those patients with supposedly more hypoxic tumours had a poorer response to radiotherapy, as illustrated in Fig. [2.](#page-6-0) Tumour perfusion can also be estimated with PET following administration of $\binom{15}{0}$ -labelled water. However, the clinical studies that used this method in head-and-neck cancer have produced conflicting results. One study reported that the $[15O]$ -labelled water perfusion estimates correlated reasonably well with $\left[{}^{18}F\right]$ -EF5 measurements of hypoxia (Komar et al. [2008](#page-15-0)), but another study found that poor local tumour control and survival after radiation therapy were associated with high blood perfusion rather than the low perfusion one would expect to be indicative of hypoxia (Lehtio et al. [2004\)](#page-16-0).

4 Endogenous Markers of Hypoxia

As an alternative to invasive electrode measurements or exogenously applied hypoxia markers, molecules expressed under (patho)physiological conditions of low oxygenation have been studied as potential "endogenous" or "intrinsic" hypoxia markers. Most of these studies are related to hypoxia-inducible factor- 1α $(HIF-1\alpha)$, a transcription factor subunit considered to be the main regulator of the hypoxia response in mammalian cells. HIF-1 α protein accumulates in the nucleus under hypoxic conditions and binds to hypoxia-responsive elements in the promoter regions of hypoxia-regulated genes, including erythropoietin (EPO), carbonic anhydrase IX (CA IX), glucose transporter 1 (GLUT1) and vascular endothelial growth factor (VEGF). Therefore, both HIF-1 α protein itself and mRNA or protein of HIF-1-regulated genes could serve as indicators of tumour hypoxia.

An appropriate marker of hypoxic radioresistance should become overexpressed or accumulate at a level of hypoxia which is relevant for cellular radiosensitivity. The half-maximal oxygen effect on radiosensitivity is observed at about 0.5 $\%$ O₂ (Hall [1988](#page-15-0)). HIF-1 α protein has been shown to be detectable in HeLa cells after 4 h at 20 % O_2 with a moderate increase between 20 and 6 %, a strong increase below

6 % and a maximum expression at 0.5 % (Jiang et al. [1996\)](#page-15-0). In U87 MG human glioma cells, a constant increase in HIF-1 α protein could be shown between 2 and $< 0.02 \%$ O₂, for *in vitro* hypoxia durations between 1 and 18 h (Vordermark and Brown [2003](#page-19-0)).

The temporal response of HIF-1 α protein response to hypoxia (and reoxygenation) has been described as rather rapid: in HeLa cells, induction of HIF-1 α protein was observed after 2 min of hypoxia, a maximum expression was seen after 1 h, and after 32 min of reoxygenation, the protein was again undetectable (Jewell et al. [2001](#page-15-0)). These data indicate that HIF-1 α protein expression in tissue can occur already at higher oxygen concentrations where radiosensitivity of cells is not yet compromised and that care must be taken in processing of surgical/biopsy tissue to account for the immediate response to changes in oxygenation. Colocalization studies of HIF-1 α and injectable hypoxia markers in xenograft tumours have supported the assumption that HIF-1-related hypoxia markers accumulate at higher $O₂$ concentrations (i.e. closer to perfused blood vessels) than exogenous markers such as EF5 (Vukovic et al. [2001\)](#page-19-0).

Among the HIF-1-regulated genes, the membrane enzyme carbonic anhydrase IX (CA IX) has received the most attention as a potential endogenous hypoxia marker for use in radiotherapy. In vitro, a continuous increase of CA IX protein expression has been described in A-549 lung carcinoma cells exposed to decreasing $O₂$ concentrations from 5 to 0.1 % (Wykoff et al. [2000](#page-19-0)). Long-term hypoxia (24 h) at 1.5 % O_2) was found to result in higher CA IX levels than exposure for up to 10 h, suggesting that CA IX indicates predominantly prolonged exposure of cells to hypoxia (Lal et al. [2001\)](#page-16-0). In FaDu head-and-neck squamous cell carcinoma, expression of CA IX increased over a radiosensitivity-relevant range of oxygen concentrations, resulting in a correlation of CA IX protein and cellular radioresistance (Vordermark et al. [2005](#page-19-0)).

The possibility to detect HIF-1 α protein and related proteins such as CA IX in archival tumour material from patients with an already known clinical course of disease has motivated researchers to analyse the relationship of marker expression on immunohistochemistry and clinical outcome (e.g. survival and local control) after cancer treatment, especially radiotherapy. In early histopathological series investigating a number of different tumour types, $HIF-1\alpha$ has been detected in 40– 82 % of prostate cancers, 80–100 % of colon adenocarcinomas and 29–83 % of breast adenocarcinomas (Zhong et al. [1999](#page-19-0); Talks et al. [2000](#page-18-0)), with respective corresponding numbers for CA IX protein of 0, 100 and 26 % (Ivanov et al. [2001\)](#page-15-0).

The HIF-1 α immunohistochemical staining pattern observed in sections of human tumour material is not consistent across tumour types and individual studies. In oropharyngeal carcinoma, a typical staining pattern of "diffusion-limited hypoxia" (i.e. positive cells in ring shape at a distance from a central blood vessel) was described in 65 % of positive tumours, with more diffuse patterns in the remainder (Aebersold et al. [2001](#page-13-0)). Other authors characterized the area of HIF-1 α -positive cells as close to a blood vessel (compatible with perfusion-related or "acute" hypoxia) versus distant from a vessel versus unspecific pattern (Haugland et al. [2002](#page-15-0)). A so-called perinecrotic staining pattern (i.e. accumulation of the marker in the zone most distant from a blood vessel, near regions of necrosis) was also reported in studies of CA IX expression in cervical carcinoma, head-and-neck cancer and non-small-cell lung cancer (Beasley et al. [2001;](#page-13-0) Giatromanolaki et al. [2001;](#page-14-0) Loncaster et al. [2001\)](#page-16-0). The use of the term "endogenous hypoxia marker" has been criticized, since immunohistochemical studies of $pO₂$ electrode measurement tracks in cervix cancer tumour tissue have shown no direct correlation of overexpression of the proteins HIF-1 α , CA IX or GLUT1 with the corresponding pO₂ reading (Mayer et al. [2006](#page-16-0)). This suggests that in vivo additional mechanisms other than the mere oxygenation level modulate expression of the putative endogenous hypoxia markers and that their expression is at least not hypoxia-specific.

However, a vast body of clinical literature suggests that a high level of expression of HIF-1-related proteins is related to poor outcome after cancer treatment. In head-and-neck cancer, several groups reported an association of $HIF-1\alpha$ overexpression and reduced overall survival or disease-specific survival following surgery or radiotherapy or combination treatment (Aebersold et al. [2001](#page-13-0); Beasley et al. [2002](#page-13-0); Winter et al. [2006](#page-19-0)). The association of high CA IX expression with poor prognosis in head-and-neck cancer was seen to a lesser extent in comparable studies, and some groups found this marker to be prognostic only in combination with other potential hypoxia markers (Hui et al. [2002;](#page-15-0) De Schutter et al. [2005\)](#page-14-0) or not at all (Eriksen and Overgaard [2007;](#page-14-0) Nordsmark et al. [2007\)](#page-17-0).

Cervix cancer, the other tumour entity with strong evidence from oxygen electrode studies of a relationship between tumour oxygenation and clinical response to radiotherapy, has been studied extensively regarding endogenous hypoxia marker expression. In three of the largest series treated with radiotherapy and/or surgery, $HIF-1\alpha$ expression was also significantly associated with overall survival or disease-specific survival on multivariate analysis (Birner et al. [2000;](#page-13-0) Bachtiary et al. [2003;](#page-13-0) Burri et al. [2003](#page-13-0)). Similar associations were found in some, but not all studies of CA IX expression in cervix cancer (Loncaster et al. [2001](#page-16-0); Lee et al. [2007](#page-16-0)).

Other cancer types have been studied extensively regarding endogenous hypoxia marker expression, but with a stronger therapeutic focus on surgery and less impact of radiotherapy, among them breast cancer and lung cancer. Predominant associations of high marker expression and poor survival were observed here as well (review in Bache et al. [2008\)](#page-13-0).

5 Plasma Hypoxia Markers

In theory, the measurement of a hypoxia-related protein secreted from hypoxic tumour cells into the plasma could permit an integrated assessment of both the total tumour burden ("number of cells") and their oxygenation level ("percentage of hypoxic tumour cells"). The best-studied secreted hypoxia-related protein is osteopontin (OPN), a tumour-associated glycoprotein secreted into bodily fluids and in the plasma of tumour patients. Plasma OPN level was shown by Le et al. [\(2003](#page-16-0)) to correspond with Eppendorf electrode measurements of tumour oxygenation in patients with head-and-neck cancer, suggesting a role for OPN as an

endogenous marker of tumour hypoxia. In a landmark study, Overgaard et al. [\(2005](#page-17-0)) showed that only patients with high plasma levels of OPN (upper tertile) significantly benefitted from the addition of nimorazole, a hypoxic radiosensitizer, compared to standard radiotherapy in patients with head-and-neck cancer. OPN may therefore serve as a marker by which to select head-and-neck cancer patients for intensified, hypoxia-specific, treatment. A molecular mechanism for the intracellular accumulation of OPN under hypoxia has been described (Sorensen et al. [2005;](#page-18-0) Zhu et al. [2005](#page-19-0)), although secretion of OPN may require additional steps (Said et al. [2005](#page-18-0); Lukacova et al. [2006\)](#page-16-0).

Elevated plasma or serum levels of OPN have been reported for several human cancer types including pancreatic, hepatocellular, colon, breast, prostate and lung cancer (Fedarko et al. [2001](#page-14-0); Koopmann et al. [2004](#page-16-0); Zhang et al. [2006\)](#page-19-0). An association of high OPN plasma levels with poor prognosis has been established for different clinical situations. For instance, Isa et al. ([2009\)](#page-15-0) demonstrated that low plasma OPN measured before treatment correlated with improved overall survival and progression-free interval after chemotherapy for non-small-cell lung cancer. Mack et al. ([2008\)](#page-16-0) reported an association of elevated OPN plasma levels and inferior overall survival after carboplatin-/paclitaxel-based chemotherapy for advanced non-small-cell lung cancer. Blasberg et al. ([2010\)](#page-13-0) could show that OPN plasma levels significantly decreased after resection of early stage lung cancer and increased with later relapse, supporting the potential value of OPN as a biomarker for monitoring the treatment response in lung cancer. Recently, a pilot study of plasma hypoxia markers has also suggested a prognostic role of osteopontin response to radiotherapy of locally advanced non-small-cell lung cancer (Ostheimer et al. [2013](#page-17-0))

Given the strong association with both electrode-measured oxygenation (Le et al. [2006\)](#page-16-0) and response of tumour to surgery or chemotherapy in non-small-cell lung cancer, the prognostic potential of plasma OPN in radiotherapy of non-small-cell lung cancer was recently studied. Ostheimer et al. ([2013\)](#page-17-0) found in a pilot study of 55 patients with locoregionally advanced non-small-cell lung cancer that a panel of plasma biomarkers (OPN, CA IX and VEGF) in combination was an independent prognostic factor for overall survival in multivariate analysis. Early data on repeated measurements of OPN suggest a prognostic value of increasing plasma OPN over time in patients undergoing radiotherapy. In malignant glioma patients, OPN plasma levels did not decrease after surgical resection which may in part be explained by the fact that resection of such tumours is microscopically incomplete by nature, but also suggests that tumour-unrelated factors, such as wound healing, may contribute to total plasma osteopontin levels (Güttler et al. [2013](#page-15-0)). Nevertheless, a low plasma level of osteopontin at the end of postoperative radiotherapy identified patients with significantly improved overall survival in this pilot study. In patients with head-and-neck cancer, pretreatment OPN plasma levels were evaluated for outcome after surgery, radiotherapy, combined chemoradiation or sequential combinations. An adverse effect of high pretreatment OPN levels on survival and tumour control was confirmed for the different treatment arms (Petrik et al. [2006](#page-17-0)). In a separate series, lower pretreatment OPN levels were in favour of better tumour response and superior survival in head-and-neck cancer patients after radiotherapy alone (Snitcovsky et al. [2009\)](#page-18-0).

6 Conclusions and Future Perspectives

Hypoxia is a characteristic feature of human tumours that has a major negative influence on determining tumour response to conventional therapy and is also an important factor in influencing malignant progression, both in terms of the aggressive growth of the primary tumour and its ability for metastatic spread. What is now needed is a method that allows us to identify those individual patients that have tumours containing significant levels of hypoxia, so that we can predict their outcome to therapy and where necessary select alternative treatments to eliminate that hypoxia.

Of course, one of the problems here is that hypoxia is often considered as a single entity when in fact we know that the degree and type of hypoxia found in tumours are very heterogenous (Horsman et al. [2012\)](#page-15-0). At the very least, we have chronic and acute hypoxia, and it is not known whether both types respond equally well to therapy. Even if we could identify regions of both chronic and acute hypoxia within tumours, it is often difficult to state whether the cells in those hostile environments are actually viable and clonogenic. The situation becomes even more complicated because we also know that other microenvironmental factors such as intermediate hypoxia, low pH and glucose deprivation can influence malignant progression and thus outcome. The ideal imaging method must be able to identify all the critical factors. Furthermore, it must also give accurate, reliable and reproducible measurements, be easy to use on a routine basis and be applicable to any tumour type regardless of location. A non-invasive method would also be preferable. Clearly, no one technique that is currently available can achieve all these criteria. We must, therefore, either rely on measurements made with the best method there is or begin to combine modalities that can give us a better indication of the relevant parameters.

Once we have decided on the most relevant technique for imaging hypoxia, then there is the question of how do we deal with that hypoxia? Numerous preclinical studies have demonstrated a variety of methods that can be applied to eliminate hypoxia (Horsman et al. [2011](#page-15-0)), and many of these have been successfully applied in the clinic (Horsman and Overgaard [2007;](#page-15-0) Overgaard [2007](#page-17-0)), but none is currently in routine clinical use. It has also been suggested that in situations where we can actually image the distribution of hypoxia in tumours, we can then use that information to increase the radiation dose delivered to the tumour (Ling et al. [2000;](#page-16-0) Søvik et al. [2009;](#page-18-0) Bentzen and Gregoire [2011\)](#page-13-0). But, whether that should be an increase to the gross tumour volume in which a substantial hypoxic volume has been identified or simply increase the dose to the biological target volume defined by the hypoxic area is not clear.

At present, we have a wealth of information about tumour hypoxia from a variety of clinically relevant techniques. Although we are not yet in a position to use that data to help us predict outcome on an individual patient basis or decide what we should do to tackle the hypoxia problem, the amount of effort being applied to this area would suggest that it is only a matter of time before we achieve those goals and the hypoxia problem eventually becomes obsolete.

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