



# Oxygen Transport and Tissue Utilization

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## 2.1 Introduction

Tissue oxygenation and regulation is a critical feature for survival of any cell and, by extension, to any organism. The maintenance of an adequate supply of oxygen ( $O_2$ ) is required to maintain normal cellular function through the production of adenosine triphosphate (ATP) [1] mainly by oxidative phosphorylation in the mitochondrial Krebs cycle [2]. This requires the coordinated action of the three major systems involved in oxygen transport: the cardiovascular system, the respiratory system, and the blood. The cardiovascular and respiratory systems are designed to carry the oxygen that is present in the atmosphere down to the mitochondria.

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## 2.2 Transport of Oxygen

The total amount of oxygen transported ( $DO_2$ ) can be calculated using the following formula:

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$$DO_2 = CaO_2 \times \text{Cardiac Output}$$

$$= [1.34 \times Hb \times SaO_2 + (0.003 \times PaO_2)] \times \text{Cardiac Output}$$

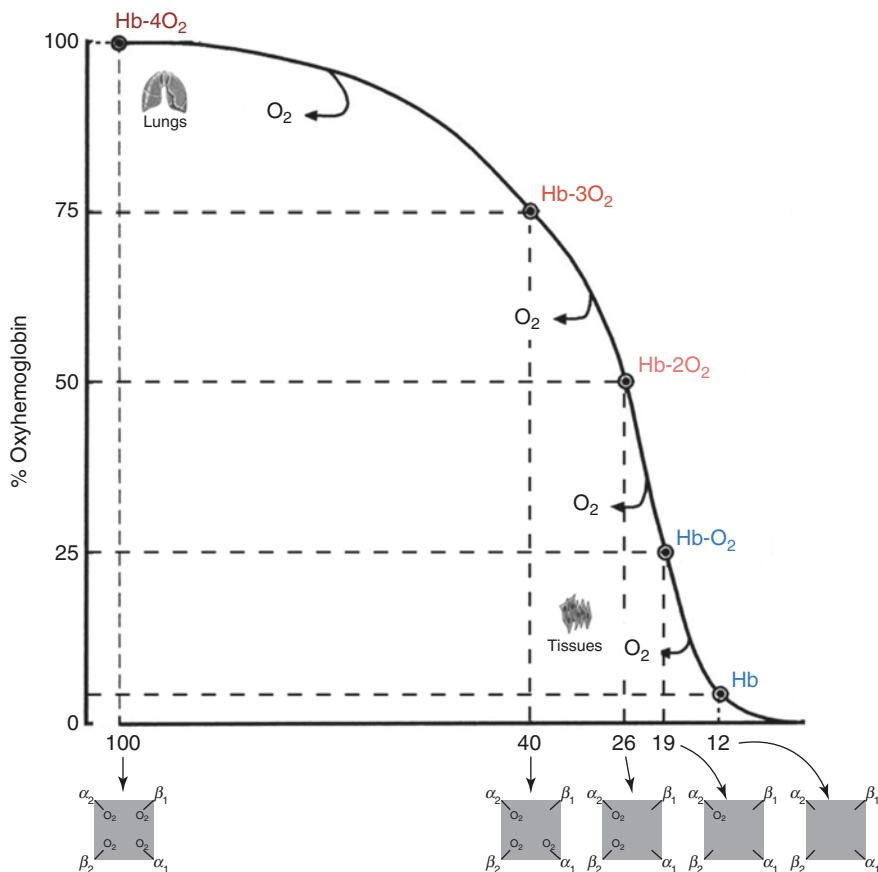
CaO<sub>2</sub> = arterial oxygen content

Hb = hemoglobin level

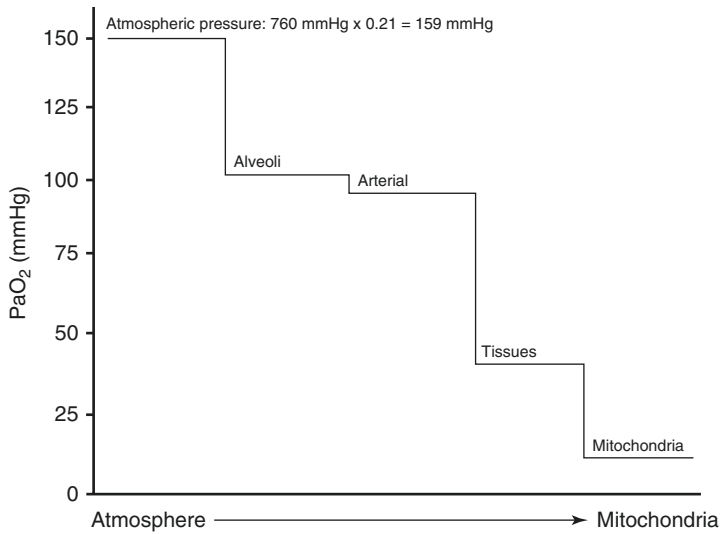
PaO<sub>2</sub> = arterial oxygen partial pressure

SaO<sub>2</sub> = arterial oxygen saturation

From this it is clear that the majority of oxygen is transported to the tissues bound to hemoglobin. Hemoglobin has an oxygenbinding capacity of 1.34 mL O<sub>2</sub> per gram, where the oxygen content mainly depends on oxygen saturation and hemoglobin concentration, as the amount of dissolved oxygen in the blood is minimal. The oxygen partial pressure at sea level is approximately 160 mmHg. From this high initial pressure in the lungs, there is an abrupt fall of about 4–8 mmHg at the mitochondrial level (Fig. 2.1). The level



**Fig. 2.1** Oxygen fall. Respiration is a cellular phenomenon. Intracellular oxygen partial pressure must be maintained between 5 and 8 mmHg



**Fig. 2.2** Hemoglobin's oxygen dissociation curve is sigmoidal. The four-subunit arrangement in hemoglobin ( $\alpha_1$ ,  $\alpha_2$ ,  $\beta_1$ ,  $\beta_2$ ) accomplishes a specific function when hemoglobin flows from high oxygen tension in the lungs to the low oxygen tension areas in the tissues and back to the lungs. Oxygen remains tightly bound to hemoglobin in the lungs but will be progressively released as partial oxygen pressure drops in the tissues of the body. The release of the second, and even more so the third, oxygen molecule requires a smaller drop in pressure as the erythrocyte moves farther from the lungs, whereas the reverse occurs when the erythrocyte moves to the lungs (figure constructed from [4])

of saturated hemoglobin ( $SaO_2$ ) is determined by the oxygen–hemoglobin dissociation curve, where the proportion of hemoglobin in its saturated form is plotted against the prevailing oxygen tension on the horizontal axis. This curve is an important tool for understanding how the blood carries and releases oxygen. This curve is such that when  $SaO_2$  drops to less than 90%, even small variations in  $PaO_2$  are associated to important changes on  $SaO_2$  [3]. Generally speaking, a  $SaO_2$  of about 50% ( $P_{50}$ ) associates to a  $PaO_2$  of 26 mmHg (Fig. 2.2, [4]). Shifts in the oxygen dissociation curve (resulting in changes in the  $P_{50}$ ) are related to changes in the off-loading of oxygen. A right shift of the curve (increase in  $P_{50}$ ) as seen in acidosis, hypercapnia, and fever facilitates oxygen off-loading. Normal  $DO_2$  is approximately 1000 mL/min or 500 mL/min.M<sup>2</sup> if cardiac index is substituted for cardiac output:

Oxygen consumption ( $VO_2$ ) is the rate at which  $O_2$  is taken up from the blood and used by the tissues. It can either be directly measured or calculated.  $VO_2$  is defined by the Fick equation as the difference between the content of oxygen in the arterial and mixed venous compartment (equaling the amount of oxygen taken up by the periphery) multiplied by the cardiac output (the flow through the system).

$$VO_2 = (CaO_2 - CvO_2) \times \text{Cardiac Output}$$

$$SvO_2 = [1.34 \times Hb \times SvO_2 + (0.003 \times PvO_2)] \times \text{Cardiac Output}$$

$CvO_2$  = arterial oxygen content

$PvO_2$  = mixed venous oxygen partial pressure

$SvO_2$  = mixed venous oxygen saturation

Oxygen extraction ratio ( $ERO_2$ ) is the relationship between  $DO_2$  and  $VO_2$ , and it normally ranges from 0.25 to 0.30. When we reduce the formula for  $ERO_2$  to its main components, we are left with

$$ERO_2 = (CaO_2 - CvO_2) / (CaO_2) \\ \approx 1 - SvO_2$$

Therefore, mixed venous oxygenation (or its surrogate, central venous oxygenation) is clinically used to estimate the balance between oxygen delivery and oxygen demand. Under normal conditions oxygen demand equals oxygen consumption. However, when central venous oxygenation falls, it reflects an imbalance between the demand and supply. This is not equal to inadequate oxygen consumption (as this would reflect a state of tissue hypoxia) but rather a compensation for a decrease in delivery either due to a decrease in oxygen content or cardiac output. The transport of oxygen does not equal the delivery of oxygen to the tissues. For this local blood flow is regulated by several tissue factors mainly related to the metabolic rate. So, cardiac output is redistributed among the tissues depending on their relative requirements, where this regulation occurs in the microcirculation [5]. Thus, under normal conditions, cardiac output is demand driven.

Once oxygen reaches the tissues, a part of it passes to the interstitial space and freely diffuses to the intracellular space and mitochondria. The site within the mitochondria at which oxygen is consumed is cytochrome c oxidase, the terminal electron acceptor in the electron transport chain. Mitochondria appear to be able to sustain normal oxygen consumption needed for generating ATP at a maximum rate, until the amount of oxygen in their immediate vicinity acutely falls below a critical value of 4–6 mmHg [6, 7]. In chronic hypoxemia conditions, this threshold is significantly higher, and suppression of oxygen consumption may already start below 40 mmHg [8].

Tissue oxygenation is typically described by one of the following three terms: first, normoxia, being a state where cellular  $PO_2$  is greater than the critical value; second, hypoxia, where some tissue regions have less than adequate oxygen levels and in consequence mitochondria produce ATP at a submaximal rate; and third, anoxia, which is the absence of oxygen in the tissue where mitochondria cease to produce ATP [9].  $CO_2$  diffuses rapidly through the tissues and across peripheral capillary walls due to its greater solubility. Because of this  $CO_2$  elimination from tissues is seldom a concern of diffusion but rather dependent on the perfusion of the tissues. Therefore, changes in cardiac output relate to changes in central venous  $CO_2$  levels in many disease states [10–12].

Oxygen exchange occurs not only across the walls of capillaries but can be exchanged between any two regions in which a partial oxygen pressure difference occurs or where a gradient is present. Therefore, a significant transarteriolar  $O_2$

gradient is generally present. It was Krogh who presented a more accurate model and description of oxygen transport in tissues. Since all capillaries were assumed to be identical and uniformly spaced, he devised a simple tissue model for oxygen transport and consumption constituted by a single capillary with continuous blood flow, surrounded by a concentric cylinder of oxygenconsuming tissue. This model was refined over time to take into account the variations in capillary hematocrit, the low solubility of  $O_2$  in the plasma, and the resistance to oxygen diffusion between the blood and tissue due to the particulate nature of the blood [13]. Diffusion is the mechanism by which oxygen passes from blood to tissue cells. As red blood cells (RBC) pass through capillaries in single file due to their similar size to the capillary caliber, oxygen is continuously released from the RBC hemoglobin and eventually diffuses to the mitochondria where it is consumed. Although most ( $\approx 98\%$ ) of the oxygen in the blood is reversibly bound to hemoglobin, the vector or the “driving force” for oxygen movement from the blood to tissue is the  $PO_2$  difference that exists across the vascular wall, not hemoglobin level or arterial oxygenation levels [1, 2].

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### 2.3 Some Clinical Considerations

From the formula for  $DO_2$ , it may seem that manipulating oxygen content (oxygen saturation and hemoglobin levels) is as effective as manipulating cardiac output or its distribution. As already mentioned earlier, adaptation to the changing need for oxygen of tissues, these tissues do not influence oxygen content but rather change the flow. In addition, increasing oxygen levels have been associated with adverse effects on tissue oxygenation and outcome [14–16]. Therefore, the judicious use of oxygen has been challenged [17] and clinicians are increasingly willing to apply conservative supplemental oxygen strategies [18]. Although the same holds for blood transfusion given the results from older studies [19–21], more recent studies focusing on the microcirculation have shown beneficial in recruiting the microcirculation [22–24]. Therefore, a transfusion strategy should probably not focus on a static hemoglobin level but rather on the state of the microcirculation.

For almost three decades,  $DO_2$  optimization has been one of the fundamental strategies to improve tissue oxygenation during acute circulatory dysfunction, particularly in high-risk surgical or septic patients. And in the majority of studies, the main manipulated variable was cardiac output next to blood pressure. The pioneer studies by Shoemaker et al. identified an  $O_2$  debt in these patients that was related to organ failures and mortality [25]. In a subsequent study, Shoemaker et al. showed that a strategy of  $DO_2$  maximization to supranormal levels with fluids and vasoactive agents aimed at decreasing or preventing this  $O_2$  debt decreased mortality [10]. Other investigators confirmed that increasing  $DO_2$  to high levels not only increased  $VO_2$  but also improved survival in patients with severe sepsis [26–28]. However, other large studies showed no benefit where one study even showed increased mortality associated with this approach [29, 30].

Although not specifically targeting  $VO_2$  but incorporating all the elements of increasing  $DO_2$ , Rivers et al. [31] showed that therapy aimed to improve cardiac

output and oxygen content significantly increased survival in early severe sepsis in emergency department patients. A redo of the concepts of Rivers many years later did not show to have a survival benefit [32–34]. However, the patient population in these studies (among other characteristics) was markedly different from the original study [35]. Nevertheless, it seems obvious that in patients with a risk of under-resuscitation, like postsurgical patients, the concept of early hemodynamic optimization (that mainly manipulates  $DO_2$ ) is related to improved survival [36, 37].

The resuscitation of patients with hemodynamic dysfunction is more than normalizing hemodynamics as an approach like that might prove to be inadequate [38], but also the therapies might have inherent negative effects. More recently, the risk of fluid overload has been highlighted [39, 40], and it has been recognized that fluid resuscitation to fixed static hemodynamics might induce harm [41, 42]. Therefore, these static clinical endpoints of fluid resuscitation have been removed from the latest sepsis guidelines [43]. Like in the discussion on blood transfusion earlier, aiming for fixed endpoints for fluid resuscitation, cardiac output, and blood pressure, it seems more physiological to aim for the ultimate target: improving microcirculatory perfusion. Although some studies have shown that the microcirculation as the target of resuscitation might be a relevant endpoint [22, 44–46], larger clinical studies incorporating holistic protocols, covering all aspects of tissue perfusion, are necessary.

Another important aspect is that some therapies aimed at improving  $DO_2$  or  $VO_2$  in clinical practice could be harmful not only in terms of toxicity but also detrimental for the purpose for which they were indicated.

Especially the use of vasoactive agents (vasopressors, vasodilators, inotropes) may have unwanted side effects.

Dobutamine increases myocardial  $VO_2$  and might enhance maldistribution of flow between different organs due to unbalanced vasodilatory effects that could be associated with increased mortality [30, 47]. In general, the vasopressor load and the use of multiple vasopressors has been associated with adverse outcome [48–50]. Although vasodilators might improve the microcirculation and have been associated with an increase in oxygen consumption (as a marker of improved tissue perfusion) [51–54], there may be decreases in blood pressure [52] that may have negative [55] or even positive effects [56, 57] in some patients.

Therefore, the management of a patient in shock with the theoretical concepts of the main drivers for transport of oxygen and the subsequent delivery of oxygen to the tissues might lead to a structured approach that might benefit the patient more than using static clinical endpoints for these variables.

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