

An Overview of Quantitative Magnetic Resonance Imaging Analysis Studies in the Assessment of Alzheimer's Disease

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Abstract— Medical image analysis and visualization, can contribute in quantitative and qualitative analysis of Magnetic Resonance Imaging (MRI) towards an earlier diagnosis of Alzheimer's disease (AD). Moreover, the early detection of Mild Cognitive Impairment (MCI) has recently attracted a lot of attention. The main objective of this paper is to present a survey of recent key papers focused on the classification of MCI and AD and the prediction of conversion from MCI to AD using volume, shape and texture analysis. The most frequent anatomical features used in the assessment of AD, is the hippocampus, the cortex and the local concentration of grey matter. Shape analysis can identify the signs of early hippocampal atrophy, whereas volume analysis evaluates the structure as a whole. Shape analysis seems to be a more accurate technique both in classification of patients and in prognostic prediction. Compared to volume, shape and voxel based morphometry (VBM) techniques, texture analysis can be used to identify the microstructural changes before the larger-scale morphological characteristics which are detected by the other aforementioned techniques. We concluded that quantitative MRI measurements can be used as an *in vivo* surrogate for the classification of patients and furthermore, for the tracking the Alzheimer's disease progression.

Keywords— Alzheimer's disease; Mild Cognitive Impairment; quantitative MRI; temporal lobe; hippocampus; brain volume; prediction; classification.

I. INTRODUCTION

Mild Cognitive Impairment (MCI) represents a transitional period between normal ageing and clinical probable Alzheimer's disease (AD) [1]. Nowadays, the diagnosis of AD is based on Mini Mental State examination (MMSE) such as the criteria documented in the Diagnostic and Statistical Manual of Mental Disorders based on the revised recommendations of the National Institute of Neurological Disorders and Stroke–Alzheimer Disease and Related Disorders working group [2]. However, by the time a patient is diagnosed with AD using the standard clinical assessment, the brain tissue has already undergone widespread and irreversible synaptic loss [3]. AD is indicated by inevitable and insidious progression of atrophy which initially affects the

Medial Temporal Lobe (MTL) of the brain [4], a region of the brain which includes anatomically related structures that are essential for declarative memory [5]. The regions affected earlier by AD are the entorhinal cortex, followed by hippocampus, amygdala (see Fig. 1) and parahippocampal gyrus, a grey cortical region that surrounds hippocampus. With disease progression, these regions lose neuronal tissue with consequent brain atrophy [6].

There is a pressing need to identify the early signs of the disease using *in vivo* techniques, apart from the MMSE tests. In order to identify the MCI stage, suitable biomarkers need to be used. A biomarker is a biochemical or anatomical factor which can provide quantitative measurements of the pathophysiologic processes of a disease [2] thus, many researchers have been using neuroimaging to evaluate this possibility. The Alzheimer's disease Neuroimaging Initiative (ADNI) [7] is a multicenter collaborative effort created in 2003 by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, the Food and Drug Administration, private pharmaceutical companies and non-profit organizations. It is an open source database where a huge collection of Positron Emission Tomography (PET) and MRI images are available online. Apart from imaging data, other biological markers such as cerebrospinal fluid (CSF) of more than 2000 participants including AD patients, MCI subjects and elderly controls are available online. This paper focuses on studies derived mainly from the ADNI database, and more specifically on the studies where quantitative MRI analysis was used for the assessment of the disease.

Structural MRI is a non-invasive imaging modality that provides high resolution images of the brain in any plane. The high tissue contrast images provided by 3D T1-weighted acquisitions enables accurate structural neuroimaging analysis which can be used as a possible biomarker for both the assessment of the disease and the prediction of conversion from MCI to AD [8]. Furthermore, because MRI does not use any ionizing radiation it is a suitable technique for longitudinal studies, which are necessary in the investigation of AD. It has been proved by many volumetric and shape and thickness analysis studies [9]–[13] that structural

MRI based software tools allow the visualization of macroscopic tissue changes, and thus can help on the detection of neuronal loss in the initial stages of the disease. Features related to texture may have the potential to detect earlier and more subtle changes in neural tissue than other volumetric or shape analysis techniques [14].

This paper also provides a very brief review of the most widely referenced medical image analysis techniques used in the assessment of AD. It focuses on selected studies published in the last decade, investigating the prediction of conversion from MCI to AD and the classification of MCI patients, using only structural MRI imaging and specifically volume, shape and texture analysis techniques. The results of the various ADNI studies might not be directly comparable; however, the data used are from the same database.

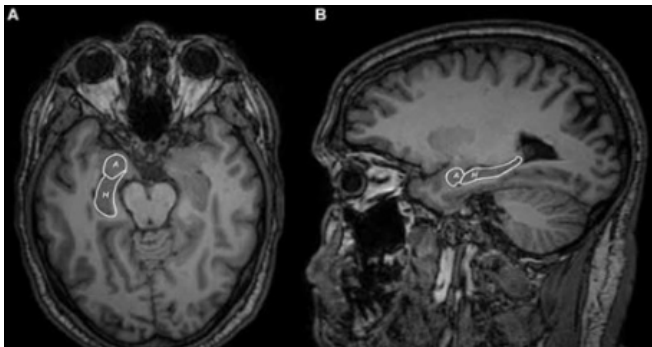


Fig. 1 Axial (A), sagittal (B) MRI views of hippocampus (H) and amygdala (A) segmentation [15]. Brain regions that are affected earlier by AD

II. QUANTITATIVE MRI STUDIES BASED ON VOLUME AND SHAPE CHARACTERISTICS

Table 1 and Table 2 tabulate quantitative MRI studies covering volume, shape and texture analysis for brain atrophy classification and prediction from MCI to AD, respectively. In each table the following data are presented: study, subjects, follow-up duration, region of interest (ROI) investigated, data type, classifier, accuracy, sensitivity and specificity.

II.A Classification of MCI and AD studies: One of the most common areas affected, at the very early stage of the disease, is the hippocampus [16], [17]. Several studies [5], [9], have used volume measurements and confirmed that hippocampus atrophy as seen in structural MRI can constitute a useful diagnostic biomarker. Desikan *et al.*, [18] carried out automated structural measurements of entorhinal cortex and supramarginal gyrus thickness. In conjunction with hippocampal volume, they classified MCI from AD patients with high accuracy. Gerardin *et al.* [19] used hippocampal shape features instead of volume analysis. Shape analysis methods can be used to reveal atrophy on local and non-global areas of the hippocampus, and according to the authors, the classification accuracy was superior to studies that used volume analysis. Specifically, they obtained a classification rate of 94%, with a sensitivity of 96% and a specificity of 92% for AD vs controls, and for MCI vs controls an accuracy of 83%, sensitivity 83% and specificity 84%. Kloppel *et al.*, [20] used SVM for the classification of

Table 1 Quantitative MRI studies in the classification of MCI and AD patients

| Study | Subjects | ROI | Volume and shape analysis | | | Classification | Acc. | Se. | Sp. |
|------------------------------------|----------------------|---|---------------------------|---------------------------|-------------|----------------|-------|-------|-----|
| | | | Data type | Classification method | | | | | |
| Desikan <i>et al.</i> , 2009 [18] | 49 NC, 48 MCI | Entorhinal cortex & supramarginal gyrus | Volume & Thickness | Logistic regression model | MCI | AUC: 0.91 | 74% | 94% | |
| | 94 NC, 57 MCI | | | | | AUC: 0.95 | 90% | 91% | |
| Gerardin <i>et al.</i> , 2009 [19] | 23 NC, 23 MCI, 25 AD | Hippocampus | Shape | SVM | NC vs AD | 94% | 96% | 92% | |
| | | | | | NC vs MCI | 83% | 83% | 84% | |
| Kloppel <i>et al.</i> , 2008 [20] | 20 NC, 20 AD | Grey matter | Thickness | SVM | NC vs AD | 95% | 95% | 95% | |
| | | | | | NC vs mAD | 81.1% | 60.6% | 93.0% | |
| | | | | | mAD vs FTLD | 89.2% | 94.7% | 83.3% | |
| Texture analysis | | | | | | | | | |
| Zhang <i>et al.</i> , 2012 [21] | 17 NC, 17 AD | Hippocampus & entorhinal cortex | 3D texture | Non-linear ANN | NC vs AD | 64.3% - 96.4% | - | - | |
| Simoes <i>et al.</i> , 2012 [22] | 15 NC, 15 MCI | Grey matter | Texture maps | SVM | NC vs MCI | 87% | 85% | 95% | |

GLOSSARY: ROI: Region of interest; Acc: accuracy; Se: sensitivity; Sp: specificity; MCIc: MCI converters; MCInc: MCI non converters; SVM: support vector machine; AUC: area under curve; NC: Normal controls; ANN: Artificial neural network; mAD: mild AD; FTLD: frontotemporal lobar degeneration.

patients (from 3 different groups) by using two different types of analysis: in the first model they used data from the whole brain and on the second they used data from an ROI within the hippocampus. Their results were comparable with other techniques which restrict their analysis only to medial temporal lobe structures. However, shape analysis used in [19] resulted in a better classification accuracy for both AD vs NC and MCI vs NC.

II.B Prediction of conversion from MCI to AD studies: Many studies have been investigating the prediction of conversion from MCI to AD (see Table 2). Chupin *et al.*, 2009 [10] used automated segmentation techniques in order to calculate hippocampal volume in an attempt to predict the conversion from MCI to AD. In their study, they achieved an overall classification accuracy of 64%, showing that global hippocampal volume evaluation may not be a very accurate measure, mainly due to the fact that hippocampal volume is as variable in young as in older adults, thus this may have implications on the final results [23]. In a recent study, Costafreda *et al.*, [24] used a fully automated procedure to extract 3D hippocampal shape morphology in order to predict conversion from MCI to AD. Their predicting model had an accuracy of 80% (sensitivity 77%, and specificity 80%) which was competitive with other predictive models which used non automated measurements. In their prediction model, only hippocampus was used, which interestingly achieved a predictive performance comparable or superior to those employing a multi-region or whole brain approach [14],[15]. In [25], the authors used VBM analysis to evaluate the volume of white matter (WM) and grey matter (GM) of 103 MCI patients which they followed up for 15 months in order to predict which individuals will convert to AD. They evaluated their results via cross-validation and achieved an accuracy of 81.5% which is the one of best results published. Plant *et al.*, 2010 [17] in order to predict the conversion from MCI to AD from atrophic changes across the brain, they used 3 different classifiers including Support vector machine (SVM), Bayes statistics, and Voting Feature Intervals (VFI). When the anterior cingulate gyrus and orbitofrontal cortex was included in their measurements, they obtained their best predictive accuracy which was 75%. Bakkour *et al.*, [27] applied measures on cortical thickness of nine ROI's to test the predictive performance of this model. Among the other ROI's, MTL, cortical thickness had the best peak performance, predicting conversion to mild AD with 83% sensitivity and 65% specificity. Querbes *et al.*, [28] used mean cortical thickness within 22 ROI's and they obtained an accuracy of 73% and a sensitivity of 75% by applying their Normalized Thickness Index (NTI) on subjects from the ADNI database. In a very similar study [13], cortical thickness was measured, and based on the results, it was noticed that atrophy patterns

differ with the disease progression, thus by learning these differences, the prediction accuracies can be improved. The aforementioned ROI and whole brain studies successfully discriminated the individuals who converted from MCI to AD. The study by Desikan *et al.*, [29] attempted to predict the time to progress from MCI to AD. They used automated MRI-based software tools to apply measurements of medial temporal cortex thickness and volume on 64 ROI's among the two hemispheres of 324 MCI patients. Furthermore, they compared their results with CSF samples and PET measures and interestingly, their results revealed that structural MRI could better predict the disease progression rather than CSF biomarkers and metabolic changes detected from PET.

In a very similar study by Vemuri *et al.*, [30] where structural MRI and CSF biomarkers on 399 subjects were used, the results were similar to the study in [29] as it was found that MRI could predict with higher accuracy the time to conversion from amnesic MCI to AD, compared to CSF biomarkers.

III. QUANTITATIVE MRI STUDIES BASED ON TEXTURE ANALYSIS

Texture analysis, is a less frequently used compared to volume and shape analysis. The information provided by texture analysis cannot be visible through volume and shape properties [22] thus, texture analysis techniques may have the advantage of detecting earlier, subtle changes [31]. There exist different methods for texture analysis: (i) structural methods, (ii) statistical based methods, (iii) model based methods [32] and (vi) transform based methods [33]. Quite frequently, the features are extracted from the grey level co-occurrence matrix (GLCM) methods which computes how often pair of pixels with specific values occur in an image [34].

III.A Classification of MCI and AD studies: In [21], Zhang *et al.*, used 3D texture features to identify normal controls from AD patients. They used over 100 texture features which were extracted from spherical ROIs placed within the area of the hippocampus and the entorhinal cortex, using image histograms, gradients, co-occurrence matrices and Run Length matrices (RLM). However, the classification accuracy of the method varied significantly, from 64.3% to 96.4%, depending on the chosen ROI. Not many studies applied texture analysis on MCI patients. One such study was that of Oliveira *et al.*, [35] where texture analysis was carried out only in the thalamus and corpus callosum of the brain. Because of the small number of subjects (17 MCI, 16 mild AD patients and 16 NC) the segmentation of corpus callosum and the thalamus was carried out manually and 44 texture parameters were extracted. The analysis was carried

out separately for the two types of ROI's (and not on the whole brain) using the MaZda program [36]. According to the authors that method was more reliable than other techniques, where they analyze the brain texture as a homogeneous structure. The aim of their study was to classify normal aging subjects from MCI and AD patients. In a similar study [37], where only corpus callosum was evaluated using 3D texture analysis on AD, MCI and normal controls, it was found that the 3D texture features had significance differences between the 3 groups of subjects. Because microstructural changes on the brain tissue start to develop years before the larger- scale alterations, Simoes *et al.*, [22] used a whole-brain voxel-wise approach by applying local statistical texture maps for the classification of MCI patients from NC. In order to classify the two groups they used SVMs and they obtained a mean accuracy of 87%, with a sensitivity at 85% and a specificity at 95%. However, the number of samples used in the study was very small as they used only 15 NC and 15 MCI patients.

III.B Prediction of conversion from MCI to AD studies:

One of the few recent studies that carried out texture analysis to predict MCI to AD progression was that of Martinez Torteya *et al.*, [38]. In their study, they used Magnetization-Prepared Rapid Acquisition with Gradient Echo (MP-RAGE) images from the ADNI database and they include six features, one related to genotyping, three related to

image signal distribution and two related to texture features. In order to apply ROI's for every image, they used it's corresponding segmentation mask provided by [39]. For each ROI they used 9 texture-related features together with 13 morphological features and 28 signal distribution related features. They presented an MCI to AD progression biomarker which yielded a mean blind accuracy of 0.79.

IV. MAGNETIC RESONANCE SPECTROSCOPY AND DIFFUSION TENSOR IMAGING IN THE ASSESSMENT OF MCI AND AD

Magnetic Resonance Spectroscopy (MRS) is a non-invasive technique, which can be used to measure metabolites [40]. The concentration of N-acetyl aspartate (NAA) in cortical tissue has been associated with neuronal density and consequently, with AD patients [41]. MRS was used previously in order to test its ability in the distinction of normal older subjects and AD patients. However, the results were variable and dependent on the anatomic region analysed. MRS it was found to be ineffective in clinical practice [42].

Diffusion tensor imaging (DTI) is MRI technique which studies the orientation and integrity of WM tracts by measuring the diffusion of water molecule in neural tissue [43].

Table 2 Quantitative MRI studies in the prediction of conversion from MCI to AD

| Volume and shape analysis | | | | | | | | | |
|---------------------------------------|--------------------------|--------------------|------------------------|---------------------------|--------------------------|-----------------------|----------------------|------------|------------|
| Study | Subjects | Follow-up (months) | ROI | Data type | Converters/total MCI | Classification method | Acc. | Se. | Sp. |
| Chupin <i>et al.</i> , 2009 [10] | 210 MCI | 0-18 | Hippocampus & amygdala | Atlas based | 76/210 | k-means | 64% | 60% | 65% |
| Costafreda <i>et al.</i> , 2011 [24] | 71 AD, 103 MCI 88 NC | 0-12 | Hippocampus | Shape | 22/103 | nSVM | 80% | 77% | 80% |
| Misra <i>et al.</i> , 2009 [25] | 103 MCI | 0-36 | Whole brain | VBM - Grey & White matter | 27/103 | nSVM | 81.5% | - | - |
| Plant <i>et al.</i> , 2010 [26] | 32 AD, 24 MCI 18 NC | 0-30 | Whole brain | VBM - Grey matter | 9/24 | VFI | 75% | 56% | 87% |
| Querbes <i>et al.</i> 2009 [28] | 130 AD 122 MCI 130 NC | 0-24 | Cortex | Thickness | 77 /122 | LDA | 73% | 75% | 69% |
| Desikan <i>et al.</i> , 2010 [29] | 324 MCI | 0-36 | Neocortex | Volume and Thickness | TC: 60/162 VC: 58/162 | Factor analysis | AUC:0.82 AUC:0.84 | 74% 87% | 84% 66% |
| Texture analysis | | | | | | | | | |
| Martinez-Torteya <i>et al.</i> , 2010 | 62 MCI | 0-24 | Whole brain | Signal and texture | - | Risk analysis | AUC: 0.79 | - | - |

GLOSSARY: ROI: Region of interest; Acc: accuracy; Se: sensitivity; Sp: specificity; QAD: questionable AD dementia; ROC: receiver operating characteristic; LDA: linear discriminant analysis; nSVM: non Support Vector Machine; VFI: voting feature interval; TC: Testing cohort; VC: Validation cohort; AUC: area under curve; NC: Normal controls.

DTI studies have been used to detect the levels of Fractional Anisotropy (FA) of water molecules in order to detect changes of white matter in AD. FA was found to be decreased in specific regions of the brain in AD and MCI patients compared to controls [44].

However, both MRS and DTI techniques are beyond the scope of this paper and they are not included in the National Institute on Aging and Alzheimer's Association criteria for preclinical, MCI, and AD [45].

V. CONCLUDING REMARKS

The challenge for modern neuroimaging is to provide early diagnosis of Alzheimer's disease. Quantitative structural MRI is sensitive to the neurodegeneration that occurs in mild AD as it reveals the atrophy of the structures within the MTL, thus it can be used as a diagnostic marker in the assessment of early AD or the MCI stage.

The techniques compared can be grouped into three categories. In the first category volume or shape analysis methods are being used, mainly on the hippocampus. The second category, used VBM analysis measurements on the cortical surface and mainly on the cortical thickness. The methods of the third category included features extracted from texture analysis. All the studies used automatic classification methods and most of them discriminate with high accuracy the normal from AD subjects. However, their sensitivity appears to be lower for the classification of MCI subjects. Perhaps, if additional data from other biomarkers such as CSF or PET can be combined with quantitative MRI, the accuracy could improve. Similar results were observed when morphometric pattern analysis was used in order to predict the prognostic conversion from MCI to AD as the results of shape analysis, were more accurate than volumetric measures.

The main findings can be summarized as follows:

1. MRI could predict with higher accuracy the time to conversion from amnesic MCI to AD, compared to CSF biomarkers [29], [30].
2. Shape analysis appears to be a more sensitive technique than volume analysis [19], [24].
3. There is a lack of research in the assessment of AD using texture analysis. However, it has a very important role in image analysis research and may develop into a useful clinical imaging tool [21].
4. Image analysis needs to be applied on images acquired from 3.0 Tesla MRIs in order to investigate if both structure and texture features perform differently.
5. As the structures vulnerable to AD have been identified and used for the prediction of conversion from MCI to AD, further investigations is required in order to evaluate if the same structures can be used to predict the onset of cognitive impairment.

CONFLICT OF INTEREST

"The authors declare that they have no conflict of interest".

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