

Chapter 9

Anthrax Toxin Protective Antigen Forms an Unusual Channel That Unfolds and Translocates Proteins Across Membranes

Bryan A. Krantz

Abstract Anthrax toxin is one of two major virulence factors secreted by pathogenic *Bacillus anthracis*, the etiologic agent of anthrax. Because inhalational anthrax is highly fatal, the agent has been weaponized for biowarfare and bioterrorism. Anthrax toxin is comprised of three individually nontoxic proteins, protective antigen (PA), lethal factor (LF), and edema factor (EF). But, to physiologically function, these individual subunits assemble into potent cytotoxins containing PA plus LF and/or EF. The PA component oligomerizes into a heptamer or octamer, which can insert into a host cell membrane to form a protein translocase channel. Under a transmembrane proton gradient driving force, LF and EF translocate through the narrow PA channel into the cytosol of the host cell. The narrowness of the channel necessitates that LF and EF unfold during translocation. This channel is unusual in this respect, because it contains its own unfoldase and translocase machinery. Highly nonspecific and dynamic clamp sites in the PA channel catalyze these activities. Anthrax toxin has been used extensively as a biophysical model to interrogate the molecular basis of translocation-coupled unfolding and translocation. It is being actively targeted by therapeutics to inhibit its function. New biotechnological adaptations use the toxin as a cancer therapy and generalized protein delivery vehicle.

Keywords Anthrax toxin • Protein translocation • Unfolding • Proton gradient

9.1 Anthrax

B. anthracis is the only pathogen in its genus known to cause epidemic disease in mammals, including humans. Attributed to its global reach are its names: Greek, ἀνθραξ (“anthrax” meaning “coal”); German, *Milzbrand* (“spleen fire”)

B.A. Krantz

Department of Microbial Pathogenesis, School of Dentistry,
University of Maryland – Baltimore, Baltimore, MD 21201, USA
e-mail: bkrantz@umaryland.edu

and *Hadernkrankheit* (“rag disease”); European, “Black Bane”; French, *charbon* (“charcoal”); Siberian Plague; Lodiana fever; and Indian, Pali Plague (Turnbull 1996). Anthrax was the first infectious disease to be linked to a specific bacterium, definitively establishing the Henle-Koch Postulates (Evans 1976). The disease is zoonotic and transmitted from animals to humans through three canonical infectious routes: cutaneous (~95 % of cases), inhalational (~5 %), and gastrointestinal (<1 %) (Mock and Fouet 2001; Koehler 2009).

9.1.1 Pathogenesis

Inhalation anthrax is the most pathogenic form of the disease. Inhaled *B. anthracis* spores germinate following phagocytosis, disseminating to nearby regional lymph nodes and the red pulp of the spleen. Lymphatic dissemination precedes hematogenous spread and terminal haemorrhagic septicemia. The high bacterial load of terminal anthrax ($\sim 10^9$ bacilli ml^{-1}) is favorable to its life cycle, especially given that it increases the probability that extremely stable infectious spores will be deposited into the soils surrounding an animal carcass for the next victim to contact, inhale, or ingest (Beyer and Turnbull 2009). Endowing *B. anthracis* with its extreme pathogenicity are its virulence plasmids, pXO1 and pXO2, which produce two major virulence factors, anthrax toxin and a poly- γ -D-glutamate (γ DPGA) capsule, respectively.

9.1.2 Vaccine

To thwart anthrax’s march at the start of the twentieth century timely vaccination programs were instituted. Modernity and industrial-scale agricultural processing and global and railway transportation of animals, hides, and furs led to the heightened severity of worldwide epidemics (Turnbull 1991). Pasteur’s prototypic bacterial vaccine worked as the encapsulation virulence plasmid, pXO2, was heat-cured, attenuating the bacillus’ virulence (Mikesell et al. 1983). Thus the anthrax toxin protective antigen (PA) was likely present in the earliest toxigenic cellular vaccine. More readily deployable and practical livestock vaccinations were required, and Max Sterne later isolated the toxigenic but “uncapsulated” 34 F2 strain (Sterne 1939), which today is the live-spore vaccine used for livestock (Turnbull 1991).

9.1.3 Biowarfare and Bioterrorism

Bioweaponization has again made anthrax an existential threat to civilization. Humankind’s tragic attraction to chemical and biological weapons is rooted in the Greek, τόξον (toxón, meaning bow or arrow) (Mayor 2008). Anthrax weaponization is not hard to imagine given its infamous history as a ravager of civilizations, its ability to manifest itself asymptotically in the early-stages of infection, its rapid

progression to acute disease, and its ability to be widely disseminated in the war theater as a highly infectious airborne aerosol of resilient spores. Correspondingly, the eminent threat of biowarfare intensified anthrax vaccinology research. Live-spore vaccines used in the former Soviet Union and China for military were not without risk. In Britain, an acellular culture filtrate of *B. anthracis* 34 F2 containing anthrax toxin PA, was prepared and combined with the adjuvant alum to make Anthrax Vaccine Precipitated (Belton and Strange 1954; Strange and Belton 1954; Wright et al. 1954). The American acellular vaccine, Anthrax Vaccine Adsorbed, now BioThrax (Pittman et al. 2002; Wasserman et al. 2003), is safe and is the best pre-exposure defense against inhalational anthrax (Friedlander et al. 1999).

Anthrax biowarfare and bioterrorism incidents throughout the twentieth century included clandestine German and highly organized Japanese (Williams and Wallace 1989) efforts in World War I and II, respectively. These incidents and subsequent bioweapons buildups during the Cold War led to the signing of the 1972 Biological Weapons Convention. Nonetheless, rogue nations, terrorist groups, and disturbed individuals unfortunately either maintained underground bioweapons efforts or carried out bioterrorist attacks. During the Amerithrax bioterrorism attack of 2001, spore-laden letters were sent in two separate mailings via the US Postal system to two US senators in Washington D.C., television and print media centers in New York City, NY, and a publisher in Boca Raton, FL, leading all told to 11 inhalation and 11 cutaneous infections, which ultimately caused 5 fatalities (Jernigan et al. 2002). Cleanup costs were \$1 billion due to the tenacity of the spores in the environment. Cutting-edge genomic evidence (Rasko et al. 2011) identified the strain and flask from which the spores were derived. After the prime suspect committed suicide, the FBI closed its case.

9.2 Anthrax Virulence Factors

B. anthracis would be a benign soil bacillus were it not for its two large virulence plasmids, pXO1 (Mikesell et al. 1983) and pXO2 (Green et al. 1985; Uchida et al. 1985). These plasmids express its two principle virulence factors: the tripartite toxin, anthrax toxin, encoded on pXO1; and a unique peptidoglycan-anchored γ DPGA capsule encoded on pXO2. The toxin dampens the innate and adaptive immune response in myriad of cell types, induces hypotension, assists in dissemination of the bacillus, and causes edema and a shock-like death (Baldari et al. 2006; Frankel et al. 2009; Moayeri and Leppla 2009). The capsule also functions to evade immune cell activities by thwarting phagocytosis.

9.2.1 Anthrax Toxin

Anthrax toxin, originally discovered by Harry Smith in the 1950s (Smith and Keppie 1954), is a binary toxin (Gill 1978; Barth et al. 2004) comprised of three ~80–90 kDa proteins, called lethal factor (LF), edema factor (EF), and protective antigen (PA)

(Frankel et al. 2009; Collier 2009). LF and EF are the two enzymatically active A moieties; PA is the cell-binding and channel-forming B moiety, making anthrax toxin an A₂B binary toxin. LF is a 90-kDa Zn²⁺ protease that cleaves numerous mitogen-activated protein kinase kinases (Duesbery et al. 1998; Vitale et al. 2000) and the innate immunity inflammasome sensor, NLRP1 (Levinsohn et al. 2012; Chavarría-Smith and Vance 2013), thus interfering with many host cell signaling pathways. EF is a 89-kDa Ca²⁺ and calmodulin-dependent adenylyl cyclase (Leppla 1982), which increases the concentration of cyclic-AMP, causing edema and facilitating dissemination (Dumetz et al. 2011). Crystal structures of LF and EF (Pannifer et al. 2001; Drum et al. 2002) and PA (Petosa et al. 1997) are known. PA is an 83-kDa Ca²⁺-binding proprotein that contains four domains, D1, D2, D3 and D4

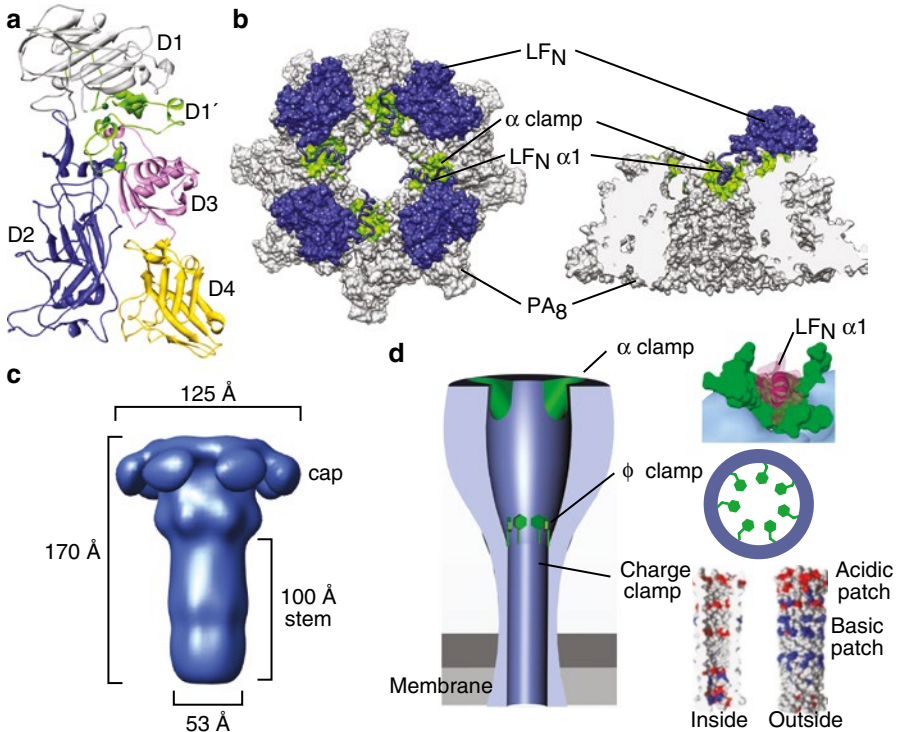


Fig. 9.1 Monomeric and oligomeric PA structures. (a) Ribbons depiction of the 83-kDa monomeric PA proprotein (Feld et al. 2012b) colored by domain: the prodomain (D1, gray); LF/EF binding domain (D1', green); channel-forming domain (D2, blue); oligomerization domain (D3, magenta); and receptor-binding domain (D4, gold). (b) *Left*, axial view of the PA₈ prechannel (gray space-fill) co-complex with four LF_N (blue) (Feld et al. 2010). LF_N α1 (blue ribbon) is docked into the α clamp (green space-fill). *Right*, sagittal section of the PA₈ prechannel with one LF_N shown for clarity. (c) PA₇ channel EM structure (blue surface) with indicated dimensions (Katayama et al. 2008). (d) *Left*, PA channel cartoon (gray) illustrating α- (green), φ- (green), and charge-clamp sites (Feld et al. 2012a). *Right*, clamp-site details and putative modes of action based on the structure/function of the α clamp-LF_N α1 interaction (Feld et al. 2010), functional and spectroscopic measurements of the φ clamp (Krantz et al. 2005), or functional analysis of an electrostatic model of the β-barrel charge clamp (Wynia-Smith et al. 2012)

(Fig. 9.1a). The D1' domain is what remains of the D1 prodomain upon proteolytic cleavage. Cleaved PA oligomerizes, assembles with LF and EF, and ultimately transforms into a translocase channel that delivers LF and EF into the cytosol of host cells. Hence, while PA, LF, and EF are individually nontoxic, the binary combinations, PA + LF and PA + EF, are toxic and known as anthrax lethal toxin (LeTx) and edema toxin (EdTx), respectively.

Holotoxin Assembly To function, LeTx or EdTx holotoxin complexes must first self-assemble. Two proposed assembly pathways are known: on cell-surfaces (Collier and Young 2003; Collier 2009) or in serum (Ezzell and Abshire 1992; Panchal et al. 2005; Moayeri et al. 2007; Ezzell et al. 2009; Kintzer et al. 2009, 2010a, b). In the former, PA binds to a host-cell-surface receptors, called the anthrax toxin receptors (ANTXR1 and ANTXR2) (Bradley et al. 2001; Scobie et al. 2003). PA is a proprotein that must be cleaved between D1 and D1' (Fig. 9.1a) by a furin or furin-like protease (Klimpel et al. 1992; Molloy et al. 1992) to produce the 20-kDa (PA₂₀) and 63-kDa (PA₆₃) fragments. Similar fragments are also observed with trypsin nicking (Blaustein et al. 1989; Christensen et al. 2005). PA₆₃ remains bound to the cell-surface receptor, allowing it to assemble at the cell surface to make ring-shaped heptameric (PA₇) (Milne et al. 1994; Petosa et al. 1997; Lacy et al. 2004a) and octameric (PA₈) (Kintzer et al. 2009, 2010a; Feld et al. 2010) prechannel oligomers (Fig. 9.1b). Prechannel oligomers then bind LF and EF to form holotoxin complexes.

In the serum of rabbits and guinea pigs, a protease resides there that can nick PA to form PA₆₃ (Ezzell and Abshire 1992; Panchal et al. 2005). In bovine serum, this cleavage can allow PA₆₃ to self-assemble with LF or EF to make assembled PA₇- and PA₈-prechannel LeTx or EdTx complexes (Kintzer et al. 2009, 2010a). The putative mammalian serum protease activity varies according to species (rats versus mice) (Moayeri et al. 2007), however, suggesting this mechanism may not be generalizable (Bann 2012). Nevertheless, several other highly active proteases are part of the *B. anthracis* secretome, and they can activate PA (Pflughoeft et al. 2014).

Host-Cell Receptor Binding Following assembly, LeTx or EdTx complexes bind to cells via an extremely tight, sub-picomolar interaction with the anthrax toxin receptor (ANTXR) (Wigelsworth et al. 2004), as recently reviewed (van der Goot and Young 2009). Two ANTXR have been described, tumor endothelial marker 8 (TEM8) (Bradley et al. 2001) and capillary morphogenesis protein 2 (CMG2) (Scobie et al. 2003), but these have been renamed to ANTXR1 and ANTXR2, respectively (Young and Collier 2007). Another potential receptor, heterodimeric integrin β 1, was also recently described (Martchenko et al. 2010). An ANTXR1/2 co-receptor was also described (Wei et al. 2006), albeit knockouts of the receptor show that it is not required in a mouse infection model (Young et al. 2007; Ryan and Young 2008). The widely studied receptors, ANTXR1 and ANTXR2, typically function as binding sites for the extracellular matrix, i.e., collagen type IV (Nanda et al. 2004) and basal lamina (Bell et al. 2001), respectively. Mutations in ANTXR2, for example, can lead to the rare genetic disorders juvenile hyaline fibromatosis and infantile systemic hyalinosis (Hanks et al. 2003). In vivo ANTXR2 is the major receptor mediating not only the pathology of toxemia but also the susceptibility to

spore infection (Liu et al. 2009). The affinity of PA for either of these receptors is much greater than the physiological substrates, allowing PA to compete with natural ligands. The structure of ANTXR2 is known both in isolation (Lacy et al. 2004b) and in complex with PA monomer (Santelli et al. 2004) and the PA₇ prechannel (Lacy et al. 2004a). ANTXR interactions are key to assembling (Kintzer et al. 2010b) and stabilizing holotoxin complexes (Miller et al. 1999; Lacy et al. 2004a; Kintzer et al. 2010b, 2012). A crystal structure of ANTXR1 (Fu et al. 2010) has also been reported.

Channel Formation Upon endocytosis, the toxin-bearing vesicles traffic to the lysosome. Subsequent acidification of the endosomal compartment is essential to toxin action (Friedlander 1986). Lower pH conditions drive a conformational change in the PA oligomer, transforming it from the prechannel to the channel state (Blaustein et al. 1989; Miller et al. 1999; Kintzer et al. 2012). Overall, the putative channel is mushroom-shaped in its architecture (Fig. 9.1c), sharing much in common structurally with the known prechannel structures, notably the pore-facing loops localize similarly (Krantz et al. 2005). However, there are two major differences: first, the phenylalanine-clamp (ϕ -clamp) pore-facing loop, most critical to facilitating protein translocation, converges from a wider 25–30 Å diameter opening in the prechannel to a much narrower <10 Å diameter opening in the channel (Fig. 9.1d) (Krantz et al. 2005); and second, additional loops in a Greek-key motif unfurl and refold into a large ~100-Å-long, 14- or 16-stranded β barrel (Petosa et al. 1997; Nassi et al. 2002). Models of the β barrel (Nguyen 2004) are consistent with it being 12–15 Å in diameter, or about as wide as an α helix (Krantz et al. 2004), as seen in an autotransporter structure (Oomen et al. 2004).

LF/EF Unfolding and Translocation Due to the aforementioned steric constraints, translocation of folded full-length LF and EF necessitates unfolding (Krantz et al. 2004, 2005). Endosomal acidification creates a destabilizing environment for LF and EF's amino-terminal domains (LF_N and EF_N), facilitating their unfolding (Krantz et al. 2004). Furthermore, endosomal acidification establishes a proton motive force (PMF), which is comprised of the proton gradient chemical potential (ΔpH) and an electrical potential ($\Delta\psi$) (Thoren et al. 2009; Brown et al. 2011). The ΔpH can drive the translocation of LF and EF (Krantz et al. 2006). Largely, in the endosomal context, where the latter $\Delta\psi$ is estimated to be minimal, it is the former ΔpH chemical gradient that drives translocation, and it was shown that the ΔpH on its own is sufficient (Brown et al. 2011). The ΔpH is critical to unfolding LF and EF as well as translocating their unfolded chains (Thoren et al. 2009). The mechanism of force transduction is largely consistent with a charge-state Brownian ratchet (Krantz et al. 2006; Basilio et al. 2009; Thoren et al. 2009; Pentelute et al. 2010; Pentelute et al. 2011; Brown et al. 2011; Wynia-Smith et al. 2012), albeit there are features of that model that do not explain all aspects of translocation, notably the high proton dependence of substrate unfolding (Thoren et al. 2009; Brown et al. 2011; Feld et al. 2012a). Following translocation into the cytosol, LF and EF refold and carry out their enzymatic functions, which serve to disrupt the host cell's normal physiology.

9.2.2 γ DPGA Capsule

Pathogenic strains of *B. anthracis* also secrete a γ DPGA virulence factor (Candela and Fouet 2006), which consists of long, linear polypeptides (50–200 kDa) of D-Glu linked via amide linkages between the γ -carboxylate and α -amino group of adjacent monomers (Bruckner et al. 1953). Several gene products, Cap A-E, on the pXO2 virulence plasmid produce the thick capsule layer of γ DPGA that surrounds the bacillus. While γ DPGA was first isolated from *B. anthracis*, the genes responsible for its synthesis were determined by homology to *B. subtilis* (Ashiuchi et al. 2001). Cap A, Cap B, Cap C, and Cap E form the membrane-embedded molecular machinery that produces and secretes γ DPGA (Candela and Fouet 2005; Candela et al. 2005). Cap D, anchors γ DPGA to the peptidoglycan cell wall, and it also cleaves γ DPGA into dissociable fragments; these function to greatly augment virulence and allow the bacillus to evade host innate immune defenses (Uchida et al. 1993; Candela and Fouet 2005). During infection, serum levels of γ DPGA polymers reach up to 1–2 mg ml⁻¹ in vivo (Boyer et al. 2009). The individual anthrax toxin components are secreted through the hydrogel layer of γ DPGA capsule surrounding the bacillus. The free capsule polymers can interact with PA in vivo (Ezzell et al. 2009), and PA, LF and EF in vitro, and these interactions can facilitate holotoxin assembly and stability (Kintzer et al. 2012). γ DPGA polymers can be either toxin-activating (Jang et al. 2011) or toxin-deactivating (Kintzer et al. 2012) depending on the molecular weight of the γ DPGA and its preparation procedures.

9.3 PA Oligomerization

Assembled anthrax toxin complexes have been studied for many years with some controversy surrounding their stoichiometry and heterogeneity. Nevertheless, recent research has determined two possible PA oligomer stoichiometries and demonstrated new biochemical methods to isolate and detect particular complexes for physiological and biophysical studies.

9.3.1 PA Heptamer

The earliest work showed that the 83-kDa PA component can be cleaved by trypsin to make nicked PA (nPA); and nicking yields 63-kDa and 20-kDa fragments, called PA₆₃ and PA₂₀, respectively (Blaustein et al. 1989). PA₆₃ was isolated from PA₂₀ via mono Q anion-exchange chromatography; and PA₆₃, but not PA₂₀, formed cation-conducting channels in planar lipid bilayers (Blaustein et al. 1989). Anion-exchange purified PA₆₃ also yields a stable oligomer, which was homoheptameric (PA₇) by electron microscopy (Milne et al. 1994). Furthermore, PA oligomers were also

observed in cell extracts, although the stoichiometry of the cell-surface-assembled complexes was not characterized (Milne et al. 1994). The oligomer was subsequently crystallized initially to low resolution (Petosa et al. 1997) and then to 3.6-Å resolution (Lacy et al. 2004a) and shown in either case to be a homoheptamer. The crystal structure reveals a large surface comprised of the D1' domain and the twin Ca^{2+} -ion-binding sites, where LF and EF were known to bind. There is extensively buried surface between D1', D2, and parts of D3 between PA monomers. The inside of the oligomeric ring is defined by D2 and key pore loops shown to be critical for protein translocation via the PA channel. The D4 domains are located on the outside of the oligomer, and the D4 metal ion-dependent adhesion site, which is key for binding to the anthrax toxin receptor, is located on the bottom face opposite of the D1' LF/EF-binding face (Lacy et al. 2004a).

To determine the PA:LF holotoxin co-complex stoichiometry, PA₇ oligomers were extensively characterized by radioisotope-labeling, light-scattering, and ultracentrifugation studies (Mogridge et al. 2002a; Wigelsworth et al. 2004; Phillips et al. 2013). To simplify matters, the PA-binding, amino-terminal domain of LF (LF_N) was used. When PA₇ oligomers form co-complexes with LF_N or LF the stoichiometry is consistent with 7:3 and the PA₇LF₃ complex (Mogridge et al. 2002a). Mutagenesis studies on PA revealed that binding interactions between PA and LF_N occurred at PA₂ dimer interfaces (Cunningham et al. 2002; Mogridge et al. 2002b), hence explaining the observed 7:3 stoichiometry. A prior study using native polyacrylamide gel electrophoresis, however, suggested that nPA and LF form co-complexes with a 1:1 stoichiometry (Singh et al. 1999).

9.3.2 PA Oligomer Heterogeneity

Electrospray ionization mass spectrometry (ESI-MS) determined that when nPA co-assembles with LF_N it forms two distinct oligomers, the well-known heptamer (PA₇) and a unique octamer (PA₈), at 7:3 and 8:4 PA:LF_N stoichiometries, respectively (Kintzer et al. 2009). Two even-numbered intermediates, PA₂LF_N and PA₄(LF_N)₂, were also observed by ESI-MS. The unique PA₈ species was not observed in prior radioisotope-labeling, light-scattering, crystallographic, and EM studies, because Q anion-exchange purified PA oligomers (the dominant form studied) are >95 % PA₇ and contain only a small percentage (~5 %) of PA₈ oligomers (Kintzer et al. 2009).

The PA₈ oligomer assembly mechanism was characterized further by EM and electrophysiology. EM was used to estimate the ratio of PA₇:PA₈ oligomers, which was ~2:1 when nPA was co-assembled with LF_N, EF_N, or dimeric anthrax toxin receptor (Kintzer et al. 2009). Moreover, when carboxy-terminal His₆-tagged PA was assembled upon Chinese hamster ovary (CHO) cells and subsequently purified by His₆-affinity chromatography, it was also found that it formed a similar 2:1 ratio of PA₇:PA₈. Planar lipid bilayer electrophysiology studies showed that PA oligomer samples enriched in the PA₈ species revealed a 20–30 % subpopulation of channels that had ~10 % greater conductance (Kintzer et al. 2009). These larger channels

translocate LF_N, EF_N, LF and EF at similar rates to the PA₇ oligomer, revealing PA₈ oligomers are physiologically active translocases.

9.3.3 PA Octamer

The PA₈ crystal structure was solved to 3.2 Å using a membrane-insertion loop deleted construct (PA^{ΔMIL}) (Kintzer et al. 2009). PA^{ΔMIL} unlike wild-type PA enabled purification of a high population (28 %) of free PA₈ oligomers by Q anion-exchange. A unique property of the PA₈ complex is that it is more pH and thermostable than the PA₇ complex, and hence (PA^{ΔMIL})₇ complexes were removed from (PA^{ΔMIL})₈ by precipitating them away from a heterogeneous mixture by treatment with ~10 % ethanol and mildly acidic conditions (pH 5.7). This procedure yielded homogeneous (PA^{ΔMIL})₈ complexes that crystallized in a square-planar architecture. (PA^{ΔMIL})₈ contains more extensively buried interface between adjacent PA subunits than the PA₇ structure, when accounting for the difference in the MIL between the two constructs. Based on the known PA₇ oligomer structure, it was suspected that the interaction of the MIL with neighboring PA subunits at the D4-D2 inter-PA interface could alter the oligomeric stoichiometry. This hypothesis was tested by chemically cross-linking the D4-D2 intra-PA interface. Depending upon the cross-link length, different oligomeric ratios could be produced, which favored the PA₈ architecture (Feld et al. 2012b). An innovative synthetic octamerization strategy was devised by mutating the known D2-D3 oligomerization interface (Mogridge et al. 2001) in two separate PA monomer constructs, which could form a mutant, but functional, PA-PA interface (Phillips et al. 2013). When these two mutant PA are combined then only the even-numbered PA₈ oligomers can form. This method works well and supports the physiological activity previously reported for WT PA₈ complexes (Kintzer et al. 2010a).

9.3.4 Unique Serum Stability of PA₈

Currently, WT PA₈ oligomers can only be isolated as co-complexes with LF_N, EF_N, LF and EF. For example, a heterogeneous 2:1 mixture of PA₇(LF_N)₃ and PA₈(LF_N)₄ is first produced by co-assembling nPA with LF_N at pH 8, 0 °C. Then the mixture is pH- and temperature-challenged at pH 7, 37 °C, causing the PA₇(LF_N)₃ complexes to precipitate as prematurely formed, insoluble channels (Kintzer et al. 2010a). EF_N, LF and EF co-complexes with PA₈ can be produced by ligand exchange using purified PA₈(LF_N)₄ and an excess of the former (Kintzer et al. 2010a, 2012). Due to this stability difference, PA₈LF₄ predominated over PA₇LF₃ complexes in defibrinated bovine serum at physiological pH and temperature (37 °C) (Kintzer et al. 2010a). Moreover, the macrophage cytolysis activities of the PA₇LF₃ and PA₈LF₄ complexes were compared after incubations in defibrinated bovine serum finding that the PA₈LF₄ complex exhibited a 30-min half life, whereas the PA₇LF₃ complex was

significantly less stable with a <5 min half life (Kintzer et al. 2010a). Hence, PA₈ toxin complexes are more thermostable than the PA₇ toxin complexes under conditions encountered in mammalian serum.

On cell surfaces, by contrast, PA oligomer complexes contact the soluble integrin-like domain of the anthrax toxin receptor (Lacy et al. 2004b). This interaction occurs via ANTXR2 and D2 and D4 of PA (Lacy et al. 2004a; Santelli et al. 2004). Since D2 and D4 are effectively stapled together by the ANTXR2 interaction, PA is unable to form the channel state readily unless the pH is dropped to about 5.5 (Lacy et al. 2004a). Receptor stabilization is roughly equivalent for PA₇ and PA₈ complexes; therefore, the stabilization advantage of the PA₈ architecture over the PA₇ architecture resides only within the milieu of the serum (Kintzer et al. 2010b). Since all of the observed PA in the serum of animal infection models late in infection is proteolytically activated as PA₆₃ (Ezzell and Abshire 1992; Panchal et al. 2005; Ezzell et al. 2009), then significant serum-based assembly of anthrax toxin is possible, and octamer formation in the serum is another potential route of anthrax toxin assembly (Kintzer et al. 2009, 2010b). Detailed examination of serum-based assembly and the oligomeric architecture of toxin complexes in anthrax infection models are future areas of research.

9.4 Holotoxin Assembly

LF and EF bind to PA through a homologous ~250-residue PA-binding domain (referred to as LF_N and EF_N, respectively), and these domains share 35 % sequence identity and 55 % similarity (Quinn et al. 1991). The stoichiometry of assembled co-complexes with LF, EF, LF_N, or EF_N depends on the identity of the PA oligomer, where PA₇ binds three LF and/or EF (Mogridge et al. 2002a; Wigelsworth et al. 2004; Kintzer et al. 2009, 2010a) and PA₈ binds four LF and/or EF (Fig. 9.1b) (Kintzer et al. 2009, 2010a; Feld et al. 2010). Heterologous fusions to the C-terminal end of the PA-binding domain, LF_N, was sufficient to deliver proteins into host cells in a PA-dependent manner, suggesting that the domain is necessary and sufficient for translocation (Arora and Leppla 1993; Milne et al. 1995). However, later studies, determined that amino-terminal His₆, poly-lysine, and poly-arginine tags were also sufficient to deliver heterologous proteins into cells in a PA-dependent manner, albeit higher concentrations of heterologous substrate were required than with the LF_N fusions (Milne et al. 1995; Blanke et al. 1996). While not understood at the time, these seemingly opposing sets of results revealed that PA oligomers contain two distinct binding subsites for LF and EF. One subsite was the tight-affinity site specific for the homologous folded domains of EF_N and LF_N, and the other subsite was a lower-affinity site that was *far less specific* and could bind unstructured peptides (like His₆ tags).

LeTx Prechannel Core Complex Structure Many subsequent mutagenesis studies confirmed that the binding sites comprised of specific contacts between PA and LF_N and EF_N (Cunningham et al. 2002; Lacy et al. 2002; Mogridge et al. 2002b;

Lacy et al. 2005; Melnyk et al. 2006; Feld et al. 2010). Hydrogen exchange mass spectrometry (Melnyk et al. 2006) and rigid-body computational docking algorithms (Schueler-Furman et al. 2005; Lacy et al. 2005) were used to deduce the structure of a co-complex between PA oligomers and LF_N. These models did not resolve why poly-cationic sequences (by themselves) were sufficient to localize heterologous proteins to PA oligomers. Also the computationally-docked model (Lacy et al. 2005) did not reconcile why PA point mutations (notably R178A) disrupted LF_N binding (Cunningham et al. 2002).

The PA₈ oligomer was exploited as a structural platform to answer these questions due to its enhanced thermostability and C4 symmetry. The structure (Fig. 9.1b) solved to 3.1 Å was representative of the PA₈(LF_N)₄ co-complex (Feld et al. 2010). Unlike the isolated structure of LF_N (Pannifer et al. 2001), the LF_N subunits in the PA₈(LF_N)₄ co-complex are in a partially unfolded conformation. This co-complex is one of the few examples, where the unfolding process has been visualized. The first α helix (α1) and β strand (β1) of LF_N are in a partly unfolded conformation that is dissociated about 40 Å from the remainder of the folded structure (Feld et al. 2010). Hence, there are two distinct binding subsites for each LF_N on the surface of the PA₈ oligomer. In one subsite, the α1/β1 portion of LF_N docks into a deep cleft between PA subunits, called the “α clamp”; and in the other subsite, the carboxy-terminal portion of LF_N binds in a separate subsite contained within a single PA subunit (Feld et al. 2010). While the latter subsite was well defined in mutagenesis and computer modeling studies (Lacy et al. 2005), the former α-clamp site was not. This discrepancy was due to the fact the modeling approach employed (Schueler-Furman et al. 2005) did not allow for conformational changes, such as partial unfolding.

The walls of the α-clamp cleft are comprised of the twin Ca²⁺ binding sites, which are fully-conserved within all known PA homologs (in other *Clostridium* and *Bacillus* binary toxins). The twin Ca²⁺ binding sites are such that their side chains are pointed inward toward the Ca²⁺ ions, leaving mostly backbone surface area contacts with the α1 helix. By virtue of the larger than average backbone exposure, the interactions with the α clamp are very nonspecific (Feld et al. 2010). The proposed mechanism of nonspecific helix recognition is consistent with the broad substrate specificity of calmodulin, a well known adapter, which uses a pair of twin Ca²⁺ sites to recognize α helices (Meador et al. 1992, 1993; Shen et al. 2005). Hence nonspecific and nonhomologous poly-cationic sequences also bind to the α-clamp cleft remarkably well (Feld et al. 2010), explaining prior observations that poly-cationic tracks are necessary and sufficient for heterologous protein delivery (Blanke et al. 1996).

9.5 PA Channel

Recent biophysical efforts have elucidated the basic structural features of the PA channel (Fig. 9.1c, d). The suggested resemblance of the PA channel to staphylococcal α hemolysin (Song et al. 1996; Benson et al. 1998) was based on morphological similarities not homology. The PA channel also possesses a ring-shaped

oligomeric architecture, is SDS-resistant, and utilizes a hollow β -barrel domain to penetrate the membrane (Benson et al. 1998; Nassi et al. 2002). From modeling studies (Nguyen 2004), the β -barrel stem is extended, and it likely can accommodate structures as wide as an α helix (10–15 Å-wide) (Krantz et al. 2004; Oomen et al. 2004). The inward-facing pore loops within the soluble prechannel oligomer are also inward-facing within the cap of the channel (Krantz et al. 2005). By EM, the PA₇ channel is indeed mushroom-shaped and approximately 170 Å tall \times 125 Å wide at its maximum dimensions (Fig. 9.1c) (Katayama et al. 2008). The wider, cap is about 70 Å long, and like the prechannel, the topmost surface contains the LF/EF binding sites. The 100 Å long stem beneath the cap inserts into the membrane bilayer (Fig. 9.1d) (Katayama et al. 2010).

9.5.1 Peptide Clamps as Unfoldase and Translocase Active Sites

Functional electrophysiology studies laid the early groundwork in mapping the major active sites in the PA translocase, referred to collectively as “peptide clamps” (Fig. 9.1d) (Thoren and Krantz 2011; Feld et al. 2012a). These peptide-clamp sites have been empirically shown to catalyze the translocation of LF and EF into cells (Krantz et al. 2005; Feld et al. 2010; Wynia-Smith et al. 2012). Based on the locations of these clamps, the PA translocase channel can be divided into three sections: (i) the substrate docking surface on the top of the cap, which contains the “ α clamp” (Feld et al. 2010); (ii) a critical hydrophobic constriction point with an opening near the base of the cap containing a ring of F427 residues, called the “ ϕ clamp” (Krantz et al. 2005); and (iii) the highly anionic charged region in the solvophilic β -barrel stem portion, called the “charge clamp” (Wynia-Smith et al. 2012). Nonspecific substrate recognition is a key feature of a peptide translocase, because as the protein translocates, the segment of polypeptide sequence within the transporter will change continuously during translocation (Krantz et al. 2005; Thoren and Krantz 2011; Brown et al. 2011; Feld et al. 2012a; Wynia-Smith et al. 2012). In general, these clamps allow the PA channel to interact with a translocating polypeptide substrate via broad chemical or morphological features, imparting a high degree of nonspecificity (Thoren and Krantz 2011; Feld et al. 2012a). It is no surprise, therefore, that functional clamp sites are observed throughout the length of the channel.

Peptide-Clamp Paradox The observed peptide clamp sites (Fig. 9.1d) may on their surface appear paradoxical: on one hand tight binding to clamp sites may impede protein translocation; on the other, when clamp sites are functionally disrupted, protein unfolding and translocation are kinetically inaccessible at physiological driving forces (Krantz et al. 2005; Feld et al. 2010; Thoren and Krantz 2011; Brown et al. 2011; Wynia-Smith et al. 2012). Because functioning clamp sites lower the activation energy of protein translocation, then these sites likely bind and release the translocating chain in a dynamic manner, much like an enzyme binds its substrate and releases

product during catalysis. A protonation and deprotonation dynamic of the substrate, for example, could modulate interaction between the channel and a charge-clamp site. Under these conditions, a clamp site, therefore, is not a static binding site found in a more simplistic antibody-epitope interaction. Rather, a clamp site more closely resembles a dynamic binding site for polypeptide, where, for example, a clamp site can be modulated from a higher-affinity binding mode to a lower-affinity binding mode. Considering the structural plasticity of polypeptides and molecular machines, these putative dynamics are reasonable.

9.5.2 *Transition to the Channel State*

As the details of the structure of the PA channel have become apparent, much interest has been given to the acidic pH-induced conformational change from the pre-channel to the channel (Bann 2012). Mutagenesis studies established a series of dominant-negative inhibitor (DNI) point mutations in PA that could allow for PA assembly into prechannel oligomers but would prevent formation of the channel state (Sellman et al. 2001b; Mourez et al. 2003). These possess therapeutic potential as a single copy of a DNI PA in an otherwise wild-type PA oligomer rendered the toxin harmless in vitro (Janowiak et al. 2009) and in a toxemia animal model (Sellman et al. 2001a). Hence DNI mutations provided the insight that certain molecular interactions occur in the channel that are less critical to prechannel oligomerization. 2-fluorohistidine substitution, however, did not effect the pH dependence of PA channel formation (Wimalasena et al. 2007), contrary to prior expectations that His residues sensed endosomal acidification to trigger the channel transition (Blaustein et al. 1989; Petosa et al. 1997).

Among the DNIs, the more notable D425K, F427A, and K397D mutations localize within the known PA₇ and PA₈ prechannel structures in adjacent pore-facing loops: the ϕ -clamp loop (2 β 10-2 β 11 loop) and the 2 β 7-2 β 8 loop. Biophysical characterizations of these sites demonstrate considerable inward narrowing and convergence of these loops as the channel forms. Electron paramagnetic resonance spectroscopy showed Cys-spin-labeled ϕ -clamp sites collapsed to a narrow pore of dimensions <10 Å (Krantz et al. 2005). Furthermore, bilayer-electrophysiology (Krantz et al. 2005), circular-dichroism (CD) spectroscopy (Kintzer et al. 2012), and liposome-pore-formation (Sun et al. 2008) assays revealed many mutations (such as F427A) slowed, but did not prevent, channel formation, whereas others (F427G, F427D, and F427R) blocked pore formation (Sun et al. 2008). Phylogenetic comparisons to the *Clostridium* binary toxins revealed covariance at two positions (D426Q and K397Q). PA K397Q channels were less functional translocases, but they could be complemented with the D426Q mutation, suggesting that the ϕ -clamp site and the 2 β 7-2 β 8 loop engaged each other through inter-PA contacts (Melnik and Collier 2006). In summary, a major step in channel formation is the collapse and assembly of the ϕ clamp and adjacent 2 β 7-2 β 8 loop.

ϕ -clamp assembly, however, does not appear to be the only rate-limiting aspect of the mechanism of channel formation. The interfacial D2-D4 contacts on the periphery also must be disrupted not only within each individual PA subunit (intra-PA) but also between the membrane-insertion loop and a D4 in an adjacent PA subunit (inter-PA) (Kintzer et al. 2012). The intra-PA D2-D4 contacts occur in a water-coordinated interface between the two domains, where mutations in the interface can increase the pH threshold for channel formation in bilayers and by CD (Kintzer et al. 2012). Consistent with this view ANTXR2 (Lacy et al. 2004a; Sun et al. 2007; Kintzer et al. 2010b, 2012) or γ -DPGA (Kintzer et al. 2012) binding to PA oligomers stabilizes the intra-PA D2-D4 interface, and either of these ligands can significantly limit the rate of channel formation. Not surprisingly the loss of structure in intra- and inter-D2-D4 contacts is needed, because the membrane-insertion loops ($2\beta_2$ – $2\beta_3$) situated between D2 and D4 must detach, unfold, and refold into the membrane-spanning β -barrel. The final step of PA channel formation involves the penetration of the β -barrel across the hydrophobic lipid bilayer as deduced from the D315A point mutation, which does not block channel formation in solution by CD, but does block insertion into planar lipid bilayers (Kintzer et al. 2012).

Thus while other pathways have been suggested (Bann 2012), a possible mechanism of prechannel-to-channel conversion (Kintzer et al. 2012) first requires the detachment of the various intra- and inter-D2-D4 interfaces in the oligomer; this dissociation or unfolding is followed by the collapse and proper organization of the ϕ -clamp site; an organized ϕ -clamp site then initiates the folding of the β -barrel; lastly, the barrel must penetrate the bilayer to form a functional translocase channel. The logic of the proposed scheme is not only based on functional mutagenesis studies but also on the idea that the prechannel must partially unfold before it can refold into the channel.

9.6 Translocation

Anthrax toxin is an excellent model system to study transmembrane protein translocation in part because the three subunits of the toxin can be expressed recombinantly and worked on in isolation. PA channels can be studied using whole-cell (Wolfe et al. 2005) and planar lipid bilayer electrophysiology (Finkelstein 2009) using a painted-membrane technique (Mueller et al. 1963). Single PA channels, when inserted into planar bilayers, form an open and ungated cation-conducting channel at modest potentials (Blaustein et al. 1989, 1990; Krantz et al. 2005). But when small molecule blocking ions (Blaustein and Finkelstein 1990; Blaustein et al. 1990; Orlik et al. 2005; Krantz et al. 2005) or protein substrates, such as LF_N , are added, the conductance is blocked (Zhang et al. 2004a, b; Krantz et al. 2006; Thoren et al. 2009; Basilio et al. 2011b). Upon raising the driving force, substrate translocation may be monitored as the time-dependent increase in conductance. In an LF_N translocation experiment under symmetrical pH 5.6, PA_7 oligomer is added to the

cis side to form channels; upon stabilization of the current, the cis compartment is perfused; LF_N is added to block conductance and the cis compartment is perfused a second time, removing excess LF_N ; and finally the voltage is raised, driving LF_N unfolding and translocation (Fig. 9.2a). Translocation is observed as PA channel conductance is restored and can be replotted to show a kinetic time course (Fig. 9.2b). With this method, the applied driving force can be externally controlled and continuously adjusted to identify key barriers in the translocation pathway (Zhang et al. 2004b; Krantz et al. 2006; Thoren et al. 2009; Thoren and Krantz 2011; Brown et al. 2011; Wynia-Smith et al. 2012).

A second and perhaps more powerful technique has emerged to study protein translocation at the single-channel level (Kintzer et al. 2009; Thoren et al. 2009; Basilio et al. 2011b). With this method, a single PA channel can be inserted into a planar lipid bilayer, and peptide or protein substrate translocations can be inferred from the step-like openings and closings of the channel (Fig. 9.2c). Dwell times (τ) can be determined for when the channel is closed (τ_C) or open (τ_O). The τ_C values report on unblocking processes, including translocation and dissociation of the protein from the channel, whereas τ_O values report on the binding kinetics of the substrate to the channel. While individual measured τ values are stochastic, they can be analyzed statistically using the cumulative distribution function (CDF) (Fig. 9.2d). When combined with a driving-force analysis, translocation can be studied independently of dissociation. Single-channel assays have been used to determine pore size of the PA channel to deduce relative populations of PA_7 and PA_8 oligomers and determine their ability to translocate proteins (Kintzer et al. 2009); they have been used to observe transient intermediates during docking (Brown et al. 2011) and translocation (Thoren et al. 2009); and they have been employed to dissect the unusual S-shaped kinetics of translocation (Basilio et al. 2011b). The only disadvantage of single-channel analyses of translocation is the time investment of the investigator in the assays. Otherwise, there are tremendous advantages: single-channel assays, for example, can elucidate more complex chemical kinetic mechanisms, observe intermediate conductance states, and determine the order of transient kinetic intermediates.

Topologically, LF and EF initiate translocation starting from their unstructured 20–30 residue-long amino-terminal ends (Zhang et al. 2004a). Albeit when polycationic tracks are added to the carboxy-terminal end of LF_N or heterologous fusions (Milne et al. 1995), the protein can also enter the PA channel and translocate into cells at 10- to 100-fold reduced efficiency (Sharma and Collier 2014). Nevertheless, because the amino-terminal ends are unstructured, it is unlikely LF and EF translocate to any significant extent from their carboxy-terminal ends, since the latter would require their unfolding to produce significant unstructured carboxy-terminal peptide to initiate translocation. Initiation (or docking) is charge and sequence (Pentelute et al. 2010, 2011; Brown et al. 2011; Wynia-Smith et al. 2012); length (Zhang et al. 2004a); pH (Brown et al. 2011); and PA-channel dependent at both the ϕ - (Krantz et al. 2005) and α -clamp sites (Feld et al. 2010). Empirically, LF, EF, LF_N and EF_N translocation kinetics are highly complex and cannot be fit to

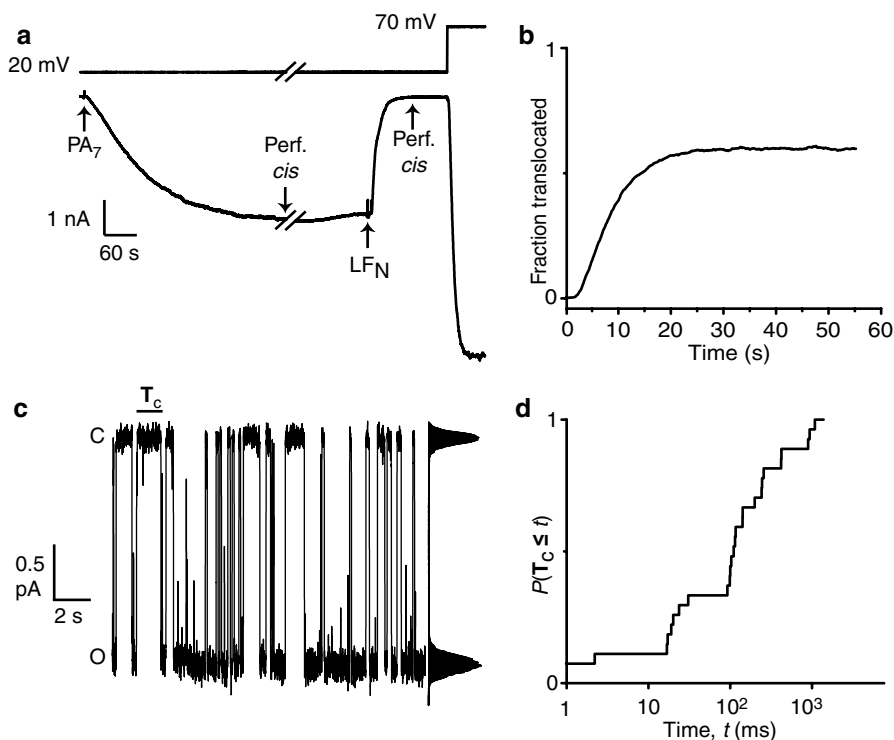


Fig. 9.2 Electrophysiological studies of translocation. **(a)** Ensemble planar lipid bilayer translocation experiment is shown for a bilayer formed between 1 mL chamber volumes and bathed in symmetric universal bilayer buffer (UBB) at pH 5.6 (Thoren et al. 2009). PA₇ channel formation was recorded as the increase in conductance at a $\Delta\psi$ of 20 mV (cis positive). Upon stabilization, the cis side was perfused (perf.) with 10 mL of fresh UBB. Then LF_N was added to the cis side, causing an exponential decrease in current as LF_N docks inside the PA channels. Following a second perfusion of the cis side, the voltage was raised, driving the translocation of LF_N. **(b)** To better observe the S-shaped translocation kinetics, the translocation phase from panel **(a)** is replotted. Time zero is set to the time when $\Delta\psi$ was raised to 70 mV. Fraction translocated is given as the level of current observed divided by the expected current, assuming a linear current-voltage relationship. **(c)** A single-channel translocation experiment under a 2-unit Δ pH and $\Delta\psi$ of 0 mV in asymmetrical KCl and pH conditions: cis buffer was 100 mM KCl, pH 5.6; trans buffer was pH 7.6 with no added KCl. A synthetic peptide (LF residues 1–50) was added to a single PA channel, and two-state opened (O) and closed (C) channel conductances were observed where a closed dwell time (τ_c) is highlighted. **(d)** τ_c from the recording in panel **(c)** were statistically analyzed as the CDF, $P(\tau_c \leq t)$, or probability a τ_c is less than or equal to time, t

simple single-exponential functions; rather these kinetics are S-shaped (Fig. 9.2b) and indicative of many consecutive steps (Zhang et al. 2004b; Krantz et al. 2005, 2006; Thoren et al. 2009; Brown et al. 2011; Wynia-Smith et al. 2012). The relative lifetime of these complex kinetic records has been quantified by measuring the time for half of the substrate to translocate ($t_{1/2}$) (Krantz et al. 2006).

9.6.1 Driving Forces and Barriers

For anthrax toxin, protein unfolding and translocation are driven by the PMF comprised of a $\Delta\psi$ and a ΔpH (Thoren et al. 2009). The electrical potential, $\Delta\psi$, relates to the activation energy of translocation, $\Delta G^\ddagger(\Delta\psi)$

$$\Delta G^\ddagger(\Delta\psi) = \Delta G^{\ddagger\circ} + zF\Delta\psi \quad (9.1)$$

$\Delta G^{\ddagger\circ}$ is the ΔG^\ddagger when $\Delta\psi$ is 0 mV; F is Faraday's constant; and z is the charge required to cross the limiting barrier. Similarly, a chemical potential-modulated energy barrier, $\Delta G^\ddagger(\Delta\text{pH})$, relates to ΔpH

$$\Delta G^\ddagger(\Delta\text{pH}) = \Delta G^{\ddagger\circ} + 2.3nRT\Delta\text{pH} \quad (9.2)$$

$\Delta G^{\ddagger\circ}$ is the ΔG^\ddagger when ΔpH is 0 units; n is the number of protons used to cross the limiting barrier; R is the gas constant; and T is the temperature. $\Delta G^\ddagger(\Delta\psi, \Delta\text{pH})$ values can be estimated by computing $t_{1/2}$ values (in seconds) extracted from primary kinetic records under different applied potentials, $\Delta\psi$ or ΔpH , where c is a one-second constant

$$\Delta G^\ddagger(\Delta\psi, \Delta\text{pH}) = RT \ln t_{1/2} / c \quad (9.3)$$

In principle and in practice, either of these driving forces can affect the activation energy of the two major barrier-crossing steps in the mechanism of translocation (Thoren et al. 2009). A pure $\Delta\psi$ can drive the translocation of the small substrate, LF_N (Zhang et al. 2004b; Krantz et al. 2005, 2006; Thoren and Krantz 2011). However, EF_N , LF , and EF translocate poorly under a pure $\Delta\psi$ (Krantz et al. 2006; Wynia-Smith et al. 2012), and efficient translocation of these substrates also requires a ΔpH (Krantz et al. 2006; Kintzer et al. 2009; Feld et al. 2010). A diode-like rectifying blockade of PA channels with LF was reported under a pure $\Delta\psi$, even at high driving potentials, demonstrating inefficient translocation under that condition (Halverson et al. 2005). The ΔpH by itself, on the other hand, is sufficient for translocation, and mutagenesis of LF_N suggests protonation and deprotonation of Asp and Glu residues play a key role in harnessing the ΔpH (Brown et al. 2011). Hence the PA channel is a proton/protein symporter (Krantz et al. 2006; Brown et al. 2011; Wynia-Smith et al. 2012).

Overall, in the translocation mechanism, there are two major limiting barriers (Thoren et al. 2009). In $\Delta G^\ddagger(\Delta\psi, \Delta\text{pH})$ versus driving force ($\Delta\psi$ or ΔpH) plots, the observed curves are not linear as would be expected for a simple single-barrier crossing kinetic mechanism. (Of course, a single-barrier model cannot be expected to fully describe translocation records that are S-shaped.) Instead, ΔG^\ddagger versus $\Delta\psi$ or ΔpH plots are boomerang-shaped with two asymptotic linear extremes, indicating that there are two major limiting barriers in the translocation mechanism (Thoren

et al. 2009). One barrier has a high driving-force dependence, i.e., a high z value or n value for $\Delta\psi$ -dependent and ΔpH -dependent translocation, respectively. The second has a ~ 10 -fold lower driving-force dependence. A two-major-limiting-barriers model was fit using mean-transit-time theory for two sequential first-order reactions (Fersht 1998; Thoren et al. 2009). From a series of destabilizing point mutations in LF_N , the high driving-force-dependent barrier was shown to be limited by protein unfolding, but the lower-force-dependent barrier was not dependent on unfolding. This two-barrier model pertains only to the steps following substrate docking and initiation as deduced from single-channel experiments (Thoren et al. 2009). The oversimplification of the two-major-limiting-barriers model is that the folding and translocation processes could have multiple similar height barriers in succession, which is likely the case for the latter lower-force unfolding-independent translocation barrier. (See arguments below).

Barrier-less Drift-diffusion Model of Translocation An alternative barrier-less model of translocation, the drift-diffusion model, has been applied to LF_N translocation (Basilio et al. 2011b). Based on electrodiffusion, the model represents LF_N as a rigid and positively charged rod dominated by Brownian motion and an applied $\Delta\psi$. Over a narrow $\Delta\psi$ range (45–60 mV) the model fits the S-shaped single-channel translocation records remarkably well. Yet, fits to the semi-natural-log $t_{1/2}$ versus $\Delta\psi$ plot are crudely linear. By comparison, when a larger dynamic range of $\Delta\psi$ records (from 30 to 150 mV) are analyzed, however, the empirical data are not linear on a semi-log plot ($RT \ln t_{1/2}$ versus $\Delta\psi$), but rather the empirical relation is boomerang shaped with two linear extrema (Krantz et al. 2006; Thoren et al. 2009; Brown et al. 2011; Wynia-Smith et al. 2012). The experimental results of Basilio (Basilio et al. 2011b) are important in that they imply the post-unfolding step(s) contain many small barriers. But, the barrier-less drift-diffusion model, while a nice addition, is overly simplified, since it ignores unfolding, a process shown to limit translocation (Wesche et al. 1998; Zhang et al. 2004b; Thoren et al. 2009).

Toward a Unifying Barrier Model A unifying interpretation is that translocation is universally barrier limited. This hypothesis is cogent with myriad of biochemical processes: protein folding and unfolding, peptide binding and dissociation, and enzyme catalysis (Fersht 1998). At low potentials < 50 mV, the major limiting barrier(s) is (are) dominated by unfolding (Thoren et al. 2009; Brown et al. 2011). This notion is evident in that destabilizing point mutations shift the observed ΔG^\ddagger versus $\Delta\psi$ curves at voltages < 50 mV but not at higher potentials (Thoren et al. 2009). At higher potentials, translocation is not limited by unfolding, but rather it is logically hypothesized to be limited by the movement of the unfolded chain through the channel (Thoren et al. 2009). To maintain S-shaped kinetics, i.e., when the latter translocation barrier is limiting at higher potentials, a unifying picture may be that translocation requires the crossing of many equivalent height barriers, which must be traversed in serial/consecutive order. Kinetic schemes comprised of a series of irreversible steps with similar lifetimes may be analyzed using a gamma-function (Feller 2008), and these models yield lag-phase S-shaped kinetics (Floyd et al. 2008). A multi-barrier-limited interpretation also explains the use of an extremely slow diffusion constant (D) of

10^{-11} cm s⁻¹ in the drift-diffusion model (Basilio et al. 2011b) (much slower than the D of 10^{-8} cm s⁻¹ expected for free diffusion through a narrow pore (Simon et al. 1992; Chauwin et al. 1998)). The slower D estimated by the drift-diffusion model for PA suggests the channel binds and releases the peptide chain (likely at the peptide-clamp sites) in a repetitious manner along the length of the protein substrate (Krantz et al. 2005; Thoren and Krantz 2011; Feld et al. 2012a). Consistently, other slow D constants of 10^{-15} cm s⁻¹ have been estimated for mitochondrial protein import and were rationalized as being due to peptide-pore interactions (Chauwin et al. 1998). In summary, binding and release steps are barrier-limited events immediately analogous to peptide-protein binding and dissociation reactions.

A unifying model of unfolding and translocation will be broadly relevant to understanding transmembrane protein translocation in the cell and mitochondrion (Simon et al. 1992; Chauwin et al. 1998; Huang et al. 1999) and the unfolding and translocation by ring-shaped oligomeric ATP-dependent disaggregase, unfoldase, and degradase molecular machines (Burton et al. 2001; Kenniston et al. 2003). At the very highest potentials, the observed rate of PA translocation begins to plateau in a way consistent with the maximal rates observed in many other ATP-dependent molecular machines that unfold and translocate proteins in the cell (Thoren et al. 2009). Of particular note, single-molecule translocation studies, which measure displacements and forces, show step-wise displacement, consistent with nm-length movements during translocation (Aubin-Tam et al. 2011; Maillard et al. 2011). Step-wise displacements in the anthrax toxin translocation mechanism would manifest in a series of consecutive barrier crossings and hence the empirically observed S-shaped kinetics.

9.6.2 *Translocation-Coupled Unfolding*

The earliest indication that protein unfolding limited protein translocation came from cellular studies of anthrax toxin translocation using heterologous LF_N fusions (Wesche et al. 1998). Addition of fold-stabilizing ligands and disulfide bonds further supported this view that unfolding was required prior to translocation (Wesche et al. 1998; Zhang et al. 2004b; Juris et al. 2007). Protons, on the other hand, are likely a key physiological ligand that serves to assist in unfolding LF_N and EF_N through the destabilization of their native states (Krantz et al. 2004). Correspondingly, ΔG^\ddagger values for translocation at low driving forces (~50 mV) correlate with equilibrium changes in stability (Krantz et al. 2006). Because the unfolding-limited barrier coincides with the force-dependent barrier, the unfolding transition state (TS) was mapped onto the structure of LF_N using 21 different destabilizing point mutations (Thoren et al. 2009). Upon applying protein folding ϕ analysis (Fersht 1998), it was found that the unfolding TS is asymmetrically localized in the β -sheet subdomain of LF_N; hence, the β -sheet subdomain is the “mechanical breakpoint” (Thoren et al. 2009) (according to nomenclature used in mechanical unfolding studies (Crampton and Brockwell 2010)). Once the rate-limiting β -sheet-subdomain structure is ruptured the rest of the LF_N unfolds (Thoren et al. 2009).

The aforementioned translocation-coupled unfolding mechanism deduced from the study of the destabilized LF_N mutants (Thoren et al. 2009) is also supported well by the crystal structure of the PA₈(LF_N)₄ prechannel core complex (Feld et al. 2010). The α 1 helix and β 1 strand of LF_N are unfolded in that prechannel structure, and this partially unfolded starting state was verified in the channel-LF_N co-complex using planar bilayer electrophysiology (Feld et al. 2010). One interesting destabilizing mutation in LF_N (M40A), the only outlier in that study, exhibited an unusually negative translocation-coupled unfolding ϕ value (Thoren et al. 2009). The negative ϕ value was indicative of slow translocation despite the fact that LF_N M40A is destabilized. This residue is in the center of the α 1 helix, which is situated in the α -clamp site on the surface of the PA₈(LF_N)₄ structure. Mutations in this site affect the stability of the co-complex, where M40A caused LF_N to bind more tightly to the PA channel (Feld et al. 2010). Tight binding correlated with slower translocation for multiple substitutions at M40. Furthermore, B-factor analysis and fluorescence anisotropy studies corroborated that the partial unfolding of the α 1/ β 1 structure leads to increased disorder in the β -sheet subdomain (Feld et al. 2010). Therefore, prior to translocation, these interactions with the α clamp initiate some destabilization to the key rate-limiting structure in the LF_N substrate.

9.6.3 Brownian-Ratchet Mechanism

A Brownian-ratchet (Astumian 1997), or charge-state-ratchet (Krantz et al. 2006), model of translocation is one possible explanation for how the Δ pH may be harnessed by the PA channel to produce physical force on the substrate protein (Fig. 9.3a). In this mechanism, acidic residues in the substrate protonate on the lower pH side upon entering the PA channel. Protonation is required because the channel is cation-selective (Blaustein et al. 1989) and hence anion-repulsive to deprotonated Asp/Glu residues (Krantz et al. 2006). Brownian motion then dominates the chain within the channel allowing it to move past the major cation-selective site. As protonated acidic groups emerge beyond the major cation-selective (i.e., anion-repulsive) site in the channel via Brownian motion, they then deprotonate down gradient to the higher pH side, thus reforming a net anion-anion repulsion between the chain and the channel. Therefore, the asymmetric Δ pH condition effectively enforces the direction of protonation and deprotonation, providing directionality to translocation.

Empirical evidence for the Δ pH-driven charge-state ratchet has come from 2-sulfonato-ethyl-methanethiosulfonate (MTSES) modification of Cys residues or semisynthetic chemistry, either of which added an SO₃⁻ modification to LF_N (Basilio et al. 2009; Pentelute et al. 2010). These modifications are effectively non-protonatable anionic sites at physiological pH. Many, but not all, of these SO₃⁻-modified LF_N showed significant decreases in the rate of translocation and suggested anionic sites were blocked by the strong anion-repulsive features of the channel. The positional effects of these SO₃⁻ modifications were complex, appearing to combine sterics and local electrostatics (Basilio et al. 2009). Additional semisynthetic peptide ligation studies showed positive and negative charges were required to utilize the Δ pH (Pentelute et al. 2011).

Detailed mutagenesis of LF_N showed replacement of all anionic residues on the amino terminus up to residue 85 slowed the relative rate of ΔpH -driven translocation 100–1000 fold (Brown et al. 2011). An LF_N with an uncharged amino terminus (i.e., no D, E, H, K, or R residues) was similarly deficient, but when only Asp/Glu residues were reintroduced at various positions, especially between residues 20 and 30 (the “20s cassette”), then translocation could be restored. Reintroduction of positively charged residues on their own did not stimulate ΔpH -driven translocation. The position of the 20 cassette is critical to driving the unfolding of LF_N. When an uncharged spacer was inserted between the 20s cassette and the folded portion of LF_N, then the rate of translocation was greatly impeded. However, this uncharged-spacer defect could be reversed with the LF_N L145A (Thoren et al. 2009) destabilizing point mutation (Brown et al. 2011). A chimera study was conducted, which recombined the amino-terminal ends of LF_N and EF_N, with the goal to understand why EF_N translocated 100-fold slower than LF_N (Wynia-Smith et al. 2012). The major difference in the ΔpH -driven translocation of EF_N is a general lack of negatively charged residues in EF_N's effective “20s cassette” (using LF_N residue numbering). When too many Asp/Glu residues were added to EF_N's effective “20s cassette”, however, translocation slowed; therefore, an appropriate balance of charges is needed in the force-generation cassette (Wynia-Smith et al. 2012). Thus the highly charged 20 cassette is the ΔpH force-transduction cassette, and its position and Asp/Glu charge composition are required for ΔpH -driven translocation.

A charge-clamp site was electrostatically modeled to the upper portion of the β barrel; and when the strongly anionic clamp was mutated to neutral residues, cation-selectivity was reduced, and $\Delta\psi$ - and ΔpH -driven translocation was impeded (Wynia-Smith et al. 2012). While the major electrostatic sites both in the substrate and the channel have been identified, there are some curious deficiencies with the Brownian-ratchet mechanism when applied to anthrax toxin translocation. First, the location of the 20s cassette relative to the folded domain greatly affected ΔpH -driven translocation, suggesting mechanical force generation has significant positional requirements (Brown et al. 2011). A positional requirement is not anticipated in a Brownian-ratchet model, because this ratchet does not generate large enough force to unfold proteins, and the channel would need to wait for the protein to unfold prior to translocation (Glick 1995). However, if the channel were to wait for unfolding to equilibrate prior to translocating (as suggested (Basilio et al. 2011b)), then the location of the 20s cassette would not greatly influence the translocation kinetics (Brown et al. 2011). The next section considers these perceived deficiencies and provides an update to the overall mechanism.

9.6.4 Molecular Basis of Force Transduction

A key aim in the investigation of ΔpH -driven protein translocation is to understand the molecular basis of force transduction. The charge-state Brownian ratchet (Krantz et al. 2006) is compelling, but the energies garnered from a Brownian ratchet are near RT . These energies are lower than what may be needed to unfold LF and EF on

a reasonable timescale. The protein unfolding step is more highly proton dependent than the subsequent translocation step; moreover, unfolding possesses a strong positional requirement for anionic, proton-binding residues in the 20s cassette of LF_N . A complementary view is that there are two phases to this force-transduction mechanism (Brown et al. 2011; Feld et al. 2012b; Wynia-Smith et al. 2012). The first phase is a proton-binding step that manifests in a force-generating power stroke required for unfolding, and the latter phase contains the salient features of the charge-state Brownian ratchet.

The mechanics of force transduction requires some consideration of the conformation of the translocating polypeptide chain. There are two different views. One view, the “extended-chain model” (Basilio et al. 2011a), is that the translocating chain is acted upon in the extended-chain configuration, where ϕ/ψ angles would be $180^\circ/180^\circ$. In that model for significant force to be applied to the load (the folded protein) the chain would need to be fully extended. Another view, the “helix-compaction model” or “proton-helix engine model” (Feld et al. 2012a) considers that the translocating chain could bind protons and convert from a more extended conformation to a more helical one (Fig. 9.3b). This interconversion would substantially contract the end-to-end length of a polypeptide about 1.5-2 Å per residue, allowing for force to be applied to the load. Alternatively a formed helix may be electrostatically pulled into the channel via interactions with the positive end of its helical dipole and other residue charges induced upon protonation. Either mechanism would yield a similar net favorable displacement on the load. While the former extended-chain model considers the chain to remain in a single conformation, the latter model considers that the translocating chain cycles between contracted α -helical and extended conformations in myriad serial steps along the length of the substrate chain.

The helix-compaction model (Fig. 9.3b) has emerged from recent data showing helical structure in the α clamp of the prechannel co-complex with LF_N (Feld et al. 2010). Also surprisingly slow kinetics (orders of magnitude slower than LF_N translocation) are observed in streptavidin-trapping experiments of a highly extended 33-residue portion of LF_N in the PA channel (Basilio et al. 2011a). In the current picture, the various peptide-clamp sites in the PA channel coordinate their activities to promote the cyclic turnover of translocating chain from the extended-chain state to the collapsed and compacted helical state. Proton binding would either lead to helical compaction of a small portion of the translocating chain into the PA channel or the net attraction of a preformed helix deeper into the channel. For either possibility, proton-driven compaction or attraction may then be the major force generation step or “power stroke” (Glick 1995) in this mechanism, explaining the positional effects of the 20s cassette observed in the unfolding of LF_N (Brown et al. 2011). Subsequently, the now helical segment would then have to convert to a more extended state. This transition could be driven by a putative conversion of the ϕ -clamp site to a more constricted state (only accommodating to extended chain). This conversion is suggested by work done on the ϕ -clamp-loop network in the PA channel (Melnik and Collier 2006), and also by the fact that the ϕ -clamp loop has been solved in two different structures in the two different PA_8 complexes (3HVD

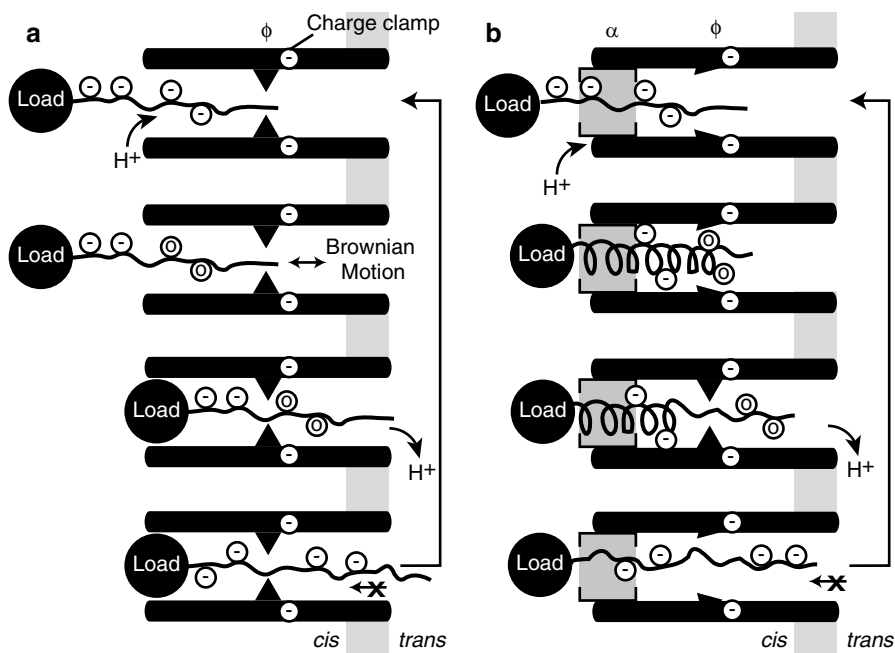


Fig. 9.3 Δ pH force-transduction models. (a) Charge-state Brownian ratchet (Krantz et al. 2006) as described in the text. The ϕ clamp constriction, charge clamp, proton binding (H^+), and Brownian motion (\leftrightarrow) are indicated. Peptide chain is solely in the extended-chain configuration (Basilio et al. 2011a). (b) Helix-compaction model as described in the text (Feld et al. 2012a). The α clamp is also indicated. Peptide chain is either α -helical (coiled loops) or extended chain. The displacement of the “load” (black sphere) in either model is illustrative and meant only to indicate application of a productive force that could unfold or translocate a protein substrate

(Kintzer et al. 2009) and 3KWV (Feld et al. 2010)) (Feld et al. 2012a). Once in the extended-chain state, the charge-state Brownian-ratchet phase of the mechanism ensues. Interaction at the the α -clamp and ϕ -clamp sites may serve as backstops to prevent retrotranslocation during chain extension past the charge clamp, thus favoring that the polypeptide release its protons down gradient instead (Fig. 9.3b). The now anionic peptide will be trapped as the charge-clamp will repel the peptide, preventing its retrotranslocation (Krantz et al. 2006; Brown et al. 2011; Wynia-Smith et al. 2012). The transport cycle can then repeat on the next segment of polypeptide.

Allosteric associations between proton binding and the α , ϕ , and charge clamps may be likely pivotal to the latter mechanism (Feld et al. 2012a). For example, the ϕ clamp may be triggered to change state when the α clamp is either occupied or vacated; and/or the degree of protonation of the substrate or clamp site may trigger a change in state. If proton binding directly drives clamp transitions, then uncharged sequences could be moved through the channel, albeit without the benefit of the charge clamp acting to prevent backsliding. Overall, this conceptualization should serve as a framework for continued experimentation. Future work should address

the allostery and mechanics of the ϕ -, α - and charge-clamp sites both structurally through EM, NMR and crystallography and functionally through single-channel electrophysiology.

9.7 Co-translocation Factors from the Host

The PA channel is sufficient to translocate LF and EF in a fully reconstituted planar bilayer electrophysiology assay at room temperature (Zhang et al. 2004b; Krantz et al. 2005, 2006; Thoren et al. 2009; Feld et al. 2010; Brown et al. 2011; Wynia-Smith et al. 2012). However, ATP-dependent and -independent cytosolic factors (including heat shock protein 90, thioredoxin reductase and the β subunit of the coat protein complex) can expedite diphtheria toxin A domain (DTA) translocation (Ratts et al. 2003, 2005) and the heterologous LF_N-DTA fusion substrate (Tamayo et al. 2008). Yet the role of these chaperones in anthrax toxin LF and EF translocation is less clear; the enhancement of DTA enzyme activity may be peculiar to DTA; it could either indicate that chaperones assisted unfolding and translocation or chaperones functioned post-translocationally to refold the heterologous substrate. For instance, in cellular assays, drug compounds, which inhibit the chaperones, heat shock protein 90, and cyclophilin, block LF_N-DTA but not LF translocation (Dmochewicz et al. 2011). If host-cell chaperones significantly assist LF and EF translocation, it is unlikely that cellular chaperones could operate in pure isolation because a portion of LF or EF must translocate via the PA channel in order to then allow a host chaperone to engage and complete translocation.

9.8 Therapeutics and Biotechnologies

There are many technologies poised to either inhibit or exploit the PA channel as a new protein-delivery platform. Since the studies of tetraalkylammonium ion blockade (Blaustein and Finkelstein 1990), a variety of other tetra-substituted ammonium and phosphoniums and other cationic small molecules have been tested as potential inhibitors of the channel (Orlik et al. 2005; Krantz et al. 2005). Derivatives of β -cyclodextrin have been successfully utilized as potent inhibitors of the staphylococcal α -toxin pore-forming channel (Gu et al. 1999). Numerous similar β -cyclodextrin derivatives (Nestorovich and Bezrukov 2014) were synthesized with multiple cationic sites to complement the anionic charge of the PA channel; and channel blockade appears to be a primary mode of action (Karginov et al. 2005). The β -cyclodextrin approach is applicable to other homologous *Clostridium* binary toxin channels (Bezrukov et al. 2012). The PA channel is also being exploited: to treat cancer through targeted cytotoxicity (Wein et al. 2013; Phillips et al. 2013; McCluskey and Collier 2013), to deliver antigens and active proteins into T cells (Shaw and Starnbach 2008), and to dissect innate immune sensing pathways (Kofeod

and Vance 2011; Zhao et al. 2011; von Moltke et al. 2012). New protein engineering approaches with native peptide ligation will allow this protein-delivery science to scale to highly flexible screening platforms (Liao et al. 2014). These are just some of the many new and exciting PA channel therapeutics and biotechnologies.

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