

Preventive and Personalized Strategies in Ambulatory and Clinical Cardiac Electrophysiology

Dariusz Jagielski, Przemysław Skoczyński, Andrzej Pawłowski, Bruno Hrymniak, Bartosz Skonieczny, Sebastian Stec, Dorota Zyśko, Waldemar Banasiak, and Halina Podbielska

Abbreviations

3PM Predictive, preventive, and personalized medicine AI Artifcial intelligence

Department of Cardiology, Center for Heart Diseases, 4th Military Hospital, Wrocław, Poland

P. Skoczyński

Department of Cardiology, Center for Heart Diseases, 4th Military Hospital, Wrocław, Poland

Department of Emergency Medicine, Faculty of Medicine, Wroclaw Medical University, Wrocław, Poland

e-mail: przemyslaw.skoczynski@umw.edu.pl

A. Pawłowski University of Science and Technology, Wrocław, Poland

Department of Mechanical and Industrial Engineering, University of Brescia, Brescia, Italy e-mail: andrzej.pawlowski@unibs.it

B. Hrymniak · B. Skonieczny Department of Cardiology, Center for Heart Diseases, 4th Military Hospital, Wrocław, Poland

S. Stec ELMedica, EP-Network, SKA, Skarżysko-Kamienna, Poland e-mail: smstec@wp.pl

H. Podbielska Department of Biomedical Engineering, Wrocław University of Science and Technology, Wrocław, Poland e-mail: halina.podbielska@pwr.edu.pl

© The Author(s), under exclusive license to Springer Nature Switzerland AG 2023 H. Podbielska, M. Kapalla (eds.), *Predictive, Preventive, and Personalised Medicine: From Bench to Bedside*, Advances in Predictive, Preventive and Personalised Medicine 17, [https://doi.org/10.1007/978-3-031-34884-6_11](https://doi.org/10.1007/978-3-031-34884-6_11#DOI)

199

D. Jagielski (⊠) · D. Zyśko · W. Banasiak

Faculty of Medicine, Wrocław University of Science and Technology, Wrocław, Poland e-mail: dariusz.jagielski@pwr.edu.pl; dorota.zysko@pwr.edu.pl[;](mailto:waldemar.banasiak@pwr.edu.pl) waldemar.banasiak@pwr.edu.pl

1 Electrophysiology as a Success Story of the Intersection of Biomedicine and Engineering

Contemporary electrophysiology encompasses two main felds. One uses the electrical activity of living cells to evaluate biological signaling processes for medical diagnosis; the other exploits various types of currents for treating numerous lesions, both in destructive and non-destructive manners. Both of these two aspects of

contemporary Electrophysiology require advanced technology equipment. That is why Electrophysiology is in the focus of many Biomedical Engineering education curricula worldwide (e.g. [[1–](#page-15-0)[4\]](#page-15-1)).

Electrophysiology in medicine relates mostly to two main areas: neurology and cardiology. In neurology, it is focused on an examination of brain signals, neuroimaging and neurostimulation. There are a plethora of reports describing the diagnostic and therapeutic potential of neurologic electrophysiology [\[5](#page-15-2)[–7](#page-16-0)].

In modern cardiology, both diagnostics and therapeutic procedures beneft from the electrophysiology approach. In this chapter, we will discuss some of them in view of 3P Medicine.

The main idea is illustrated in Fig. [1.](#page-2-0)

2 Preventive and Personalized Aspects of Atrial Fibrillation Diagnostic and Treatment Strategies

Atrial fbrillation (AF) is the most common type of heart-treated arrhythmia. It presents a completely irregular heart rate and is accompanied by an increased risk of thromboembolic and cardiovascular complications, hospitalizations, and deaths. A few percent of patients in the course of AF suffer from a stroke, apart from approx. 20% mortality rate carries complications in the form of chronic paresis, speech problems, and cognitive disorders. The above factors result in dramatic social consequences related to the costs of treatments burdening health care systems, leaving the labor market, and is a huge load for the economic systems of individual countries and societies. According to the offcial data, approx. 50–60 million people worldwide experience AF in its paroxysmal, persistent or permanent form [[8,](#page-16-1) [9\]](#page-16-2). There are many serious scientifc reasons to talk about the plague of AF, and the total number of patients is repeatedly greater [\[10](#page-16-3)]. The need for developing rational **predictive** and **prevention** strategies are of paramount importance. Only in the US annual treatment costs of atrial fbrillation are nearing \$26 billion [\[11](#page-16-4)].

Several modern monitoring technologies aim to diagnose various cardiac arrhythmias as standard ECG and prolonged 24–48 h ECG Holter monitoring. Due to the fact that some episodes of AF appear relatively seldom (e.g., a few times a year), the critical issue is the recording duration. The application of a monitoring framework based on the concept of chronic registration 24 h/365 days is a gold standard of ECG registration in the shape of the implantable loop recorder (ILR) technique [\[12](#page-16-5)]. Unfortunately, this is an invasive procedure with obvious limitations. Numerous efforts have been taken to develop a system for continuous non-invasive long-term ECG monitoring [[13,](#page-16-6) [14\]](#page-16-7). The projects concerning a variety of hardware, software, and algorithms as a part of artifcial intelligence and machine learning processes are still under development. The continuous ECG monitoring is becoming not only a modern technological solution but also constitutes a necessity to broaden **preventive** actions aiming to limit the enormous impact of AF on health, social, and economic aspects of our life globally.

There are two main strategies to treat AF episodes, i.e., rate or rhythm control therapy [[15](#page-16-8)]. With growing evidence supporting early rhythm control also for asymptomatic and new-onset AF patients, we observe a change in the paradigm of AF treatment. Nevertheless, many factors infuence the fnal decision to undertake invasive activities, such as age, comorbidities, echocardiographic parameters, potential success rate, patient's understanding of the clinical situation, etc. Because many factors infuence the decision to fnally undertake invasive activities like catheter ablation technologies, the effectiveness of chosen treatment method, age and category of patients, special **personalized** AF Heart Teams are established to discuss and decide about the selection decision criteria for the patients [[16\]](#page-16-9). Sometimes they may range from specialist cardiologists (electrophysiologist, heart failure specialist, echocardiographist, etc.) to multidisciplinary teams (cardiologist, cardiac surgeon, endocrinologist, hematologist, nephrologist, neurologist, and others) who plan AF treatments jointly depending on individual patient needs and availability of services. Considering the signifcant impact of AF on a variety of aspects of our health, social and economic milieu, there is substantial space for **predictive**, **preventive,** and **personalized** actions as described previously [[17](#page-16-10)].

3 Preventive Leadless Pacemaker Implantation in Patients After Tavr Procedure

Aortic stenosis (AS) is the most common valve lesion, often requiring transcatheter aortic valve replacement (TAVR) or surgical aortic valve replacement (SAVR) due to the increased risk of sudden cardiac death [\[18\]](#page-16-11). The AS prevalence increases with the aging of the population. Till the TAVR era, the interventional approach of the elderly and frail patients was associated with high operational risk. It changed in 2002, with the proof-of-concept frst TAVR procedure performed by Cribier, which created a new treatment approach for the highest-risk patients [[19](#page-16-12)]. The indisputable safety profle of the procedure mentioned above led to creating TAVR strong recommendation (IA) in ESC/EACTS Guidelines for the management of valvular heart disease from 2021 for all patients above 75 years or those with high operational risk (STS-PROM/EuroSCORE II $> 8\%$) [\[18\]](#page-16-11). Since the first case, TAVR use in the elderly population has only risen. Moreover, the procedure's indications are also spreading among the younger population. It results in increase

by 2.7 times the number of TAVR procedures in patients <65 years old between 2015 and 2021. That said, the TAVR procedure count reached nearly equal volume as SAVR by 2021 [[20\]](#page-16-13).

The safety profile in patients with severe AS presenting low operation risk was recently evaluated in the PARTNER 3 trial. In the mentioned research, study participants were randomized into groups undergoing TAVR with SAPIEN 3 system and SAVR procedure. The primary composite endpoint was death, stroke or rehospitalization at 1 year. Both 30 days and 1 year after the procedure, SAPIEN 3 system proved the safety procedure profile and was superior to SAVR in the case of the primary endpoint. Moreover, the SAVR procedure was associated with a significantly higher rate of new-onset atrial fibrillation at 30 days, a more extended index hospitalization, and a higher risk of a poor treatment outcome (death or a low KCCQ score) at 30 days compared to TAVR [[21\]](#page-17-0). Developing the newer TAVR systems significantly reduced complications, which may explain the eagerness to involve younger and lower-risk patients in the TAVR procedure.

Nevertheless, new-onset or worsening conduction disturbances remain one of the most common complications after TAVR. They are found in 34.8% of patients at hospital discharge, with the Left Bundle Branch Block (LBBB) as the most common conduction disorder [[22\]](#page-17-1). Randomized trials and registries show that such complications require pacemaker (PM) implantation in up to 25.9% of patients with consequent conduction disorders [[23\]](#page-17-2). However, what needs to be emphasized is that AS per se increases the risk of conduction disturbances.

For example, the stenotic process of aortic valve severe calcifcation may involve a near-located heart conduction system. Such situation is usually observed in patients with low-fow, low-gradient AS with preserved ejection fraction. This is because the atrioventricular (AV) node is located in the triangle of Koch's apex, near the aortic valve's non-coronary cusp. Three positions of the AV node can be listed with the most common right-sided. However, the left-sided AV node, especially superfcial to the endocardium, seems to be particularly vulnerable to calcifcation and TAVR post-procedure-related conduction disturbances.

Another heart conduction structure—the left bundle branch of the AV node—is a superficial structure positioned on the crest of the interventricular septum. It is located at the base of the interleaflet triangle, separating the aortic valve's noncoronary and right-coronary leafets, which the TAVR procedure can easily harm. Both situations can lead to PM implantation.

3.1 Permanent Pacemaker Implantation as a Preventive Strategy

ESC Guidelines on cardiac pacing and cardiac resynchronization therapy clearly recommend: asymptomatic patients or those who do not require pacemaker implantation due to standard indications do not need a permanent pacemaker implantation preventive strategy (PPIPS) before the TAVR procedure [\[23](#page-17-2)].

However, due to the post-TAVR risk of further conduction disturbances advancing in the future, early PPIPS after TAVR should be considered in several cases. With pre-existing right bundle branch block, developing any other conduction disturbances during or after TAVR, even transient high-degree atrioventricular block (AVB), PR prolongation, or QRS axis change, is a clear indication of a PPIPS. Another case when PPIPS should be implemented for patients >48 h after TAVI are:

- New LBBB with QRS > 150 ms.
- Pre-existing conduction abnormality who develops prolongation of QRS or $PR > 20$ ms.
- $PR > 240$ ms.

Yet, before the PM implantation decision, one should have an electrophysiological study (EPS) that measures the His bundle -Ventricular interval. The nominal value that justifes the implantation procedure should be at least 70 ms. Those who developed bifascicular block after TAVR and did not meet above mentioned criteria, yet have had syncope after the procedure, should also be considered for PPIPS. It has been proven that in elderly patients with unexplained, recurrent syncope and bifascicular block (for example, LBBB or RBBB with left anterior fascicular block), PPIPS signifcantly reduces the risk of symptoms recurrence [[24\]](#page-17-3). However, one in eight patients with a transvenous pacemaker (TV-PM) may experience peri- and post-procedural complications [[25\]](#page-17-4). The risk of complications rises with such burdens as age, BMI, and frailty syndrome, which are all often in the characteristic spectrum for a patient after the TAVR procedure.

3.2 Leadless Pacemakers in TAVR Population

The arrival of leadless pacemakers (LPs) (Fig. [2](#page-5-0)) in 2012 became a cornerstone in the treatment of bradycardia and atrioventricular (AV) conduction disorders as an alternative to TV-PMs. Currently, the only available LPs on the market are Micra VR (MVR) and the newly developed Micra AV (MAV), which allows AV synchronous ventricle pacing (VDD mode).

However, their external construction is similar. With a low mass of 1.75 g, dimensions of 25.9 mm \times 6.7 mm, and volume of 0.8 cc Micra occupies around 1% of the hearts' right ventricle volume. MVR and MAV longevity is estimated between 8 and 13 years, which depends on the pacing mode, ventricle pacing percentage, and

Fig. 2 Leadless Pacemaker—Micra (own picture)

implanted place's electrical parameters. Even though Micra is considered an unremovable device after a couple of months since implantation due to encapsulation [\[26](#page-17-5)], another implantation of Micra in the same patient is feasible and safe. However, due to the expected limited lifespan in TAVR-related, elderly and frail populations, it seems to be a relatively rare need.

The most common conduction disturbance after TAVR—the newly developed LBBB—has a relatively high long-term recovery rate to normal conductive function $(26.2\%$ at long-term follow-up [\[27](#page-17-6)]). Thus, such situation allows LP to work often as a backup mode extending battery life.

One of the reasons behind LP technology development was the improvement of the safety profle in cardiac pacing. The pocket and leads account for two-thirds of transvenous PM complications, and their lack in LP technology is one of their most signifcant advantages. Reducing the risk of infective endocarditis is essential from the point of view of a person with an artifcial aortic valve.

The frst study exploring the MVR safety profle was Investigational Device Exemption (IDE). The IDE study showed 48% (HR 0.52; 95% CI 0.35–0.77;) fewer complications compared to TV-PMs, a high implant success rate (99.2%), and stable low pacing thresholds at 6 months in 98.3% of patients [[28\]](#page-17-7). The second one— The Post-Approval Registry—proved a low rate of major complications throughout 12 months (2.7% CI:2.0–3.6%) with no device-related infections. Major complications were mainly reduced by a 47% relative risk reduction in hospitalizations and an 82% relative risk reduction in system revisions. The all-cause mortality does not differ at 2-year follow-up in groups of LPs and TV-PMs, even though patients obtaining LP are usually burdened with more comorbidities [\[29](#page-17-8)]. Micra's implantation safety, performance, and post-procedural complications were also evaluated in patients who underwent MAV implantation after the TAVR procedure between November 2020 and June 2021. The short-term safety and performance of the LP were once again proved with a 1-month follow-up [\[30](#page-17-9)]. Most of LP's indications are similar to the TAVR population. Thus, LP should be considered for patients with frailty syndrome and chronic kidney disease, especially those on dialysis, with less than 10 years of life span, hindered access to the TV-PM, but also with a history of cardiac device-related infective endocarditis (CDRIE). The MAV should be preferred over MVR in patients with AV block but without bradycardia or persistent supraventricular arrhythmia, due to the VDD pacing mode.

This demonstrates how important is a **personalized** approach before taking a decision about the procedure to be employed.

4 Prediction, Prevention, and Personalization: A Strategy for Managing Patients with Symptomatic Bradycardia

Management of sinus node dysfunction or atrioventricular conduction disorders leading to symptomatic bradycardia remains a diagnostic and therapeutic challenge. According to the guidelines of the European and American cardiological societies ESC/EHRA/ACC/AHA/HRS, if these disorders are of internal origin and are irreversible, the treatment of choice is PM implantation [\[23,](#page-17-2) [31\]](#page-17-10). The method has been proven and improved for many years. However, it is burdened with signifcant limitations and not without the risk of complications. The recent rapid development of technology has signifcantly increased diagnostic possibilities and expanded the number of therapeutic options, from optimizing the stimulation itself to techniques to avoid it. Such a variety of options create a possibility to **personalize** the therapy to reduce complication risk and improve the quality of life. Saving lives, although still a priority, is no longer the only goal, and a specifc therapeutic option may be an optimal solution for one patient but a diffcult or unacceptable compromise for others.

It becomes possible to:

- consider the patient's individual preferences, plans, and professional and private activities.
- anticipate what limitations of potential solutions will be relevant in individual cases.
- **prevent** or minimize cumulative risk throughout chronic therapy.

Developing an optimal therapeutic strategy often requires a multidisciplinary approach and the inclusion of the patient in the decision-making process [[32\]](#page-17-11). Both to know their preferences and share responsibility for decisions made.

Until recently, the only therapeutic option for a patient with symptomatic bradycardia, if it was not reversible, was PM implantation, a prosthesis of the heart's physiological pacemaker/conduction system. This method has been successfully used for many years. Subsequent PM generations are becoming more reliable and their capabilities more excellent. With new implantation technics, cardiac pacing became more physiological, i.e., His-bundle pacing or its left branch [[33,](#page-17-12) [34\]](#page-17-13). However, the main limitations of this method remain the same. The generator must be replaced every few years and systematically checked by professional medical personnel.

Moreover, one should remember the possible infectious complications of implanted PMs due to periprocedural and blood–borne origin or lead damage. The risk increases with the duration of therapy. No less crucial, the PM—by itself—limits the quality of everyday life and physical activity and sometimes can force one to change a professional life. The risk of complications from PPM signifcantly increases in young patients with a long-life expectancy. On the other hand, often, it is the only available therapy form. Implantation procedures last shorter and shorter, and consequently, the periprocedural risk is signifcantly reduced. New pacing options, such as resynchronization with a left ventricle electrode, physiological pacing in the region of the His-bundle or its left branch, or the recently introduced implantation of LP, enable an individualized approach to each patient.

Cardioneuroablation (CNA)—a new therapeutic option for patients with symptomatic bradycardia—has been available for several years [\[35](#page-17-14), [36\]](#page-18-0). A procedure involves modifying the heart's parasympathetic part of the autonomic nervous system of the heart's physiological pacemaker/conducting system. The vagus nerve, which belongs to the parasympathetic nervous system, has an inhibitory effect on the sinus node responsible for generating the heart rhythm and the atrioventricular junction responsible for conduction. CNA is an invasive procedure involving damage through radiofrequency electric energy to the ends of the vagal nerve (postganglionic neurons and interneurons), located in the epicardium, in the left atrium in the vicinity of the pulmonary venous ostia, interatrial septum and the mitral annulus, also in the area of the roof of the right atrium and the coronary sinus ostium. CNA is a benefcial method of bradycardia treatment caused by excessive vagal nerve tension-functional bradycardia. The rising evidence suggests that it should be a frst-choice treatment in such cases [\[37](#page-18-1)]. It can be used in particular cases of structural damage to the heart's physiological pacemaker/conduction system, releasing its functional reserves from the vagal nerve infuence. This procedure is more complicated than the implantation of a PM and, unlike it, requires general anesthesia.

Moreover, the periprocedural risk is higher, and the qualifcation process for CNA is more complex and time-consuming. In the short term, it requires more signifcant commitment and acceptance of the risk of complications and possible failure of therapy by a patient. However, in many cases, it allows for avoiding or postponing the prosthesis of the heart's physiological pacemaker/conduction system, which is PM implantation, yet not excluding this option in the future [[38,](#page-18-2) [39\]](#page-18-3).

The abovementioned options allow physicians to offer a more **personalized** approach to bradycardia therapy. Knowing the advantages and limitations of individual therapeutic strategies—the patient's lifestyle and preferences, as well as the estimated lifespan—allows for risk complications **prediction** and estimation related to the considered therapies. Such awareness leads to preventing and minimizing adverse events. For example, the younger the patient, with a less incriminating medical history, the longer lifespan, which entails a signifcant increase in the cumulative risk of long-term complications of therapy with implantable devices. However, the increased short-term periprocedural risk is more acceptable. PM implantation at a young age presupposes more PM replacement procedures in the future. Each procedure is associated with an increased risk of infectious complications. Also, the lifetime of the electrodes in pacing systems is limited due to physical damage, which can come with patient activity. It is crucial to consider the patient's lifestyle and occupational activity, i.e., transvenous pacemaker precludes some activities, such as sports involving the shoulder girdle. It also excludes the possibility of working with an electric arc and forces the avoidance of strong electromagnetic felds. It binds the patient to the center controlling the implanted device and makes him strictly, chronically dependent on the healthcare system. For this, the acceptance of an individually increased risk associated with a more complicated and arduous CNA procedure and a more complicated procedure qualifcation process may be accepted. The number of variables necessary to consider in this case requires a more detailed analysis of individual therapy options, optimally with the participation of a multidisciplinary team: electrophysiologists, other specialists in the case of comorbidities, a psychologist, or a career counselor (EP Heart Team) (Fig. [3](#page-9-0)).

Most importantly—the patient needs to be actively involved in this decisionmaking process, understanding and accepting both the short-term risk associated with the PM implantation or CNA procedure itself and the cumulative long-term risk and possible limitations resulting from such a choice. Even within the same age group, optimal therapy strategies may vary depending on other factors. The patient

Fig. 3 The decision-making process and a strategy for personalized management of patients with symptomatic bradycardia (own scheme)

may ultimately prefer the well-established medical procedure – the PM, with all its limitations.

A more considerable challenge is the 3P Medicine approach to optimize the already implemented pacing system. An individual-**personalized** approach to each patient requires a reassessment of indications for permanent cardiac pacing. The guidelines of European and American cardiological societies ESC/EHRA/ACC/ AHA/HRS [\[23](#page-17-2), [31](#page-17-10)] reassures with such a procedure, requiring a reassessment of indications for continued PM therapy with PPM before each pacemaker replacement, electrode extraction and replacement and during the entire long-term follow-up.

Patients who had a conventional cardiac PM implanted a few years ago might now be qualifed for physiological pacing or can avoid PPM by CNA procedure. In a study of a Danish population of patients who had a pacemaker implanted before the age of 50, it was shown that vasovagal syncope, resulting from an exaggerated refex, the efferent arm of which is the vagus nerve, was in 5% of cases. If it is a cardioinhibitory type of refex, i.e., when it results in bradycardia or even a pause in the heart rhythm, CNA would be a causal treatment and would avoid PM implantation. In the same population, it was shown that in 50% of patients qualifed for PPM, the cause of atrioventricular node dysfunction could not be determined [[40\]](#page-18-4). Continuous development of diagnostic tools, the autonomic nervous system tests improvement, or the use of implanted loop recorders undoubtedly expand the possible medical solutions for patients whose diagnostics were completed several years ago. This group would include patients who could beneft from a different therapy. Reassessment of indications for continuing PPM therapy or its possible optimization to physiological is not burdensome and should be performed in each case. However, changing the current therapy is a much more complex issue. There are various options: continuation of the current PPM, replacing it with more physiological pacing of the His-bundle or its left branch, or CNA, and discontinuation of PM therapy (Fig. [4\)](#page-10-0).

Changing the current therapy, i.e., cardiac pacing to a different mode or stopping it, is not easy, even when the new method seems to be better. **Personalization** of the approach to this problem is inevitable in this case. The potential risk is no longer only due to implementing a new treatment method but also possible complications resulting from abandoning the current treatment method. Changing the pacing method to physiological or its complete cessation after a successful CNA procedure is associated with an additional risk of removal of the existing pacing system. Treatment by transvenous lead extraction (TLE) carries a 2–3% risk of severe periprocedural complications. This risk can be minimized by performing TLE in

Fig. 4 Reassessment processes for permanent pacing, cardioneuroablation, and transvenous lead extraction (own scheme)

hi-volume centers [[41,](#page-18-5) [42](#page-18-6)]. However, there are only a few, and they often require transporting a patient to a different center in another city for the procedure. It is an additional diffculty and stress during the treatment process. Abandonment of an inactive pacing system is not a good solution. It is associated with a long-term risk of infective endocarditis. Such a solution can be accepted only in the case of the patient's refusal to undergo the TLE procedure or a very high risk associated with this procedure.

The consideration of the potential benefts and risks of changing treatment should also be based on a multi-professional assessment by EP Heart Team and the patient. Patients who have already received PPM are more aware of its limitations and potential risks. Estimating and anticipating the risks resulting from individual options, **preventing**, and eliminating already existing limitations, such as impairment of physical activity, professional activity or social exclusion, is indispensable.

5 Automatic Control of Anesthesia for Pulmonary Vein Isolation and Cardioneuroablation Procedures

Pulmonary vein isolation (PVI) is a technique of catheter ablation of atrial fbrillation, the most often diagnosed arrhythmia worldwide and, as such, an important treatment option in modern cardiologist's armamentarium. The concept of PVI emerged after the publication of a landmark paper by Haïssaguerre et al. [[43\]](#page-18-7). Nowadays, it is an established AF treatment modality, both as the frst-line therapy and as a bail-out after failed drug therapy $[16]$ $[16]$. It can be performed using two energy sources: cryoballoon and catheter ablation with radiofrequency (RFA) current. The effcacy of both techniques is comparable, at least as a frst procedure in the paroxysmal form of AF [\[44](#page-18-8)]. Cryoballoon PVI, compared to RFA, results in shorter procedure time and seems to be better tolerated by patients [[45\]](#page-18-9). As a result, lower levels of anesthesia during cryoballoon PVI can be safely used. However, a few patient's and procedural characteristics, such as redo procedure or left atrial enlargement, favor RFA over cryoballoon [[46,](#page-18-10) [47](#page-18-11)]. As RFA PVI results in longer procedural time, which is invariably associated with patient spending prolonged time motionless in a recumbent position, it is less well tolerated. Movement of patients during the procedure can result in disturbance of the electroanatomical mapping system and inadvertent damage of the cardiac tissue, even leading to cardiac tamponade. The aforementioned obstacles favor deeper levels of anesthesia during RFA PVI. Findings from 2010 randomized clinical trial support the use of general anesthesia over conscious sedation during RFA PVI [[48\]](#page-18-12). Unfortunately, performing PVI under general anesthesia is more challenging regarding electrophysiology lab workfow and the availability of anesthesiologists. In Japan, only 0.5% of patients undergo general anesthesia during RFA PVI [[49\]](#page-18-13). To address these logistic obstacles, a trial on total intravenous anesthesia (TIVA) provided by cardiologists with support from anesthesiologists was performed. TIVA using intravenous propofol and fentanyl was administered by cardiologists in the EP lab in 160 consecutive

patients. Airway support was provided via i-gel, and all patients were ventilated in synchronized intermittent mandatory ventilation mode provided by a standard respirator. Doses of anesthetic were titrated to maintain a bispectral index (BIS) between 30 and 50. Only in 3% of cases the intervention of a supporting anesthesiologist was needed, and in 2%, TIVA was abandoned. There were no anesthesiarelated complications [[50\]](#page-19-0). This study supports the feasibility of TIVA administered by a cardiologist during RFA PVI, which is especially important in the face of an anesthesiologists' shortage.

In recent years, a novel therapy for bradyarrhythmias emerged – endocardial ablation of the vagal nerve postsynaptic neurons, i.e., CNA. During the procedure, monitoring of residual vagal innervation is essential. The monitoring can be performed by solely observing an increase in heart rate, evoking vagal reactions during high-frequency stimulation, or by direct transvenous stimulation of vagal nerve extracardiac vagal nerve stimulation (ECVS) [[51\]](#page-19-1). Due to the proximity of the accessory nerve, ECVS leads to head rotation while performed without a neuromuscular blocking agent. This unpredictable movement can result in loss of effcient vagal stimulation and even vascular damage by pacing electrode, so ECVS is generally performed after the neuromuscular blockade. However, it complicates further course of CNA, as neuromuscular blockade decreases the excitability of the diaphragm and monitoring of the phrenic nerve cannot be reliably performed so long as effect of the neuromuscular blocking agent is sustained. The remarks mentioned above makes anesthesia of patients undergoing CNA especially challenging. Method for simplifed, more reliable and reproducible general anesthesia to prevent complications and ease management of patients in EP lab is sorely needed. Considering the introduced procedure, the use of the automated control system for anesthesia can be seen as the supplementary tool for support medical staff in this challenging intervention.

Recently we have witnessed an unprecedented international effort to improve the quality and availability of medical care. In this regard, researchers in clinical automation have focused on novel solutions in the feld of physiological closed-loop control systems. This scientifc area requires a multidisciplinary approach combining specialist knowledge to tackle the problem in a holistic manner. In this context, automated control **in personalized** therapies is one of the most promising research areas, where the application of new research techniques and cutting-edge technologies, such as artifcial intelligence (AI), can expand the frontiers of this challenging feld [[52,](#page-19-2) [53](#page-19-3)]. Automatic control engineering has become an important enabling technology in many areas of medicine and biomedical technology. Prominent examples include the artifcial pancreas, closed-loop anesthesia, and **personalized** drugdosing strategies in neurology, oncology, endocrinology, and psychiatry [\[52](#page-19-2)]. It is a testament to the power of control systems that allow individualizing treatment by providing mechanisms for linking treatment goals to treatment regimens, thus achieving the desired therapeutic effect. Consequently, the arrival of control systems engineering in the clinic makes the visionary concept of "treat the patient, not the disease" technologically and economically feasible. In this regard, it is desirable to develop automated drug-dosing techniques to prevent under or overdosing issues

and to provide a more personalized solution. Additionally, continuous advances in medical sensors, medical equipment and AI have created propitious conditions for incorporating closed-loop systems. For this, patient-dynamics models can be used to predict the patient's pharmacological/biological response to the drug/substance administered, which can be incorporated into the individualized control system design and tuning [\[52](#page-19-2)[–54](#page-19-4)]. This issue is one of the open research questions that can be explored to personalize the control system in the context of model individualization.

In the setting of previously described interventions, an important aspect is related to an anesthesia process required for the proper execution of the surgery. The total intravenous anesthesia (TIVA) process generally refers to the loss of sensation. It can be described as the absence of recall and response to a noxious stimulus as the effect of the used drugs. Usually, the medications applied during intravenous anesthesia can be split into three groups: analgesic, hypnotic and those providing a neuromuscular blockade. Those drugs have a physiological effect on the loss of sensitivity to pain and loss of consciousness, interpreted as the depth of hypnosis and caused paralysis of affected skeletal muscles, respectively [\[52](#page-19-2)[–54](#page-19-4)]. The anesthesia process is usually divided into three stages, induction, maintenance, and emergence. The simplest TIVA considers only one hypnotic drug, propofol, and its effect is measured by the depth of the hypnosis level. This scheme can be extended to a multivariable case, where more than one drug is infused, having mutual interaction between them. Nevertheless, here we will focus on the simplest case, where the potential benefts could be interpolated to even more complex control system confgurations. Figure [5](#page-13-0) shows the closed-loop control system where the main components of the analyzed scheme are indicated.

In the classical approach, the anesthesiologist observes the monitors representing patients' vital signs and manually regulates the infusion pump's rates based on their experience. While in automated control, the main idea consists of applying the control algorithm (designed software) that computes the required amount of the drug based on patient state measurements (obtained through clinical monitors equipped with specifc sensors). Calculated infusion rates are applied using the computer-controlled infusion pump (actuator). Using an automated system can relieve a medical staff from continuously monitoring and modifying the drug dosage, which is a highly demanding task, especially during long interventions where

Fig. 5 Automated drug administration in anesthesia—schematic closed-control-loop for depth of hypnosis (own scheme)

it is challenging to maintain the necessary concentration for a long time. The purpose of such an automated control system is to support the anesthesiologist in this difficult process and not to replace them $[53, 54]$ $[53, 54]$ $[53, 54]$ $[53, 54]$ $[53, 54]$. In this way, the anesthesiologist becomes a supervisor of the process, acting only in critical situations, which permits them to focus on high-level tasks.

Nowadays, many control techniques that have been proposed for depth of hypnosis control in anesthesia process have been widely proven, e.g., A Proportional-Integrative-Derivative (PID) controllers, regulators based on fuzzy logic as well as model predictive control (MPC) techniques, to name a few [\[52](#page-19-2), [55–](#page-19-5)[60\]](#page-19-6). However, in the context of **personalized** medicine in anesthesia process, the MPC techniques have the greatest potential since they could use an individualized patient's model. As an example, a pharmacokinetic/pharmacodynamic (PK/PD) model for propofol could be indicated, which relates the drug infusing with its clinical effect represented by the bispectral index cale (BIS) [\[61](#page-19-7)]. This model is derived from the compartmental model, where some of its parameters are related to patients' physical characteristics (like; age, height, weight and gender). Finally, it should be highlighted that the **personalized** model can be exploited to predict the effect of the drug on each individual resulting in a powerful and fexible toll. When combined with an appropriate control technique, like the MPC, the resulting control action takes into account the specifc patient's response to the infused drug provided by the personalized model [\[56](#page-19-8)[–61](#page-19-7)]. The control algorithm uses this **predictive** feature to compute the optimal drug dosage, considering limitations and constraints indicated by the type of intervention and clinical practice. As a consequence, the control algorithm is able to provide the right value of the drug dosage. Simultaneously, it reduces the possibility of the drug's over/under dosage, where both could have a negative impact on the patient. The under dosage could result in the regaining consciousness and, consequently, provoking severe traumatic experiences. Whereas overdosage could result in postoperative complications such as postoperative nausea and vomiting (PONV), resulting in a longer recovery [\[62](#page-19-9)[–65](#page-19-10)].

With these characteristics, a personalized control scheme assures the **preventive** measure to reduce postoperative complications and to limit the infuence of a human factor [[66–](#page-20-0)[69\]](#page-20-1). Moreover, automated anesthesia is able to provide a more unifed procedure due to the limited role of the subjective decision of the anesthesiologist [\[57](#page-19-11)[–59](#page-19-12)].

6 Conclusions

Continuous ECG monitoring based on the 24 h/365 days concept could be extremely effective in clinical practice for diagnosing atrial fbrillation episodes and other arrhythmias. This might change the paradigm of recognizing not only supraventricular arrhythmias but also brain infarcts sources, syncopal episodes and infuence a strategy for anticoagulation therapy.

Dedicated **personalized** AF Heart Team is of crucial importance for decisions concerning diagnostic and therapeutic options in patients with AF and numerous other arrhythmias. Such attitude will presumably infuence health, social and economic policies in different countries and systems. PPM implantation **preventive** strategy after transcatheter aortic valve replacement is emphasized by cardiology guidelines and should be widely used. Not yet registered device-related infective endocarditis in patients with leadless pacemakers, a signifcantly lower risk of periprocedural and post-procedural complications in LPs compared to the transvenous pacemaker—also proved in a TAVR population—seems to favor the LP in frail and elderly patients. Proceeding according to the idea of **personalization**, **prediction,** and **prevention** in treating symptomatic bradycardia and its optimization should no longer be an option but a common practice. Routine application of the guidelines recommendations facilitates everyday practice but often leads to diffculty accepting and unnecessary compromises. The patient's age, occupation, plans for the future, the cumulative risk of long-term complications and diffculty in estimating other preferences cannot be easily summarized in recommendations IA or IIIA arbitrarily presented in the guidelines of cardiological societies. Each patient should be considered individually, and the decision as to the therapy method in seemingly similar cases may vary. Automatic control of anesthesia process, as described above, fts into paradigms of 3P Medicine addressing **personalized**, **predictive**, and **preventive** aspects. These properties can be of added value in the context of cardiologic surgeries, improving the overall patient state after the intervention and thus reducing their postoperative recovery time. However, it must be highlighted that signifcant effort must be dedicated to developing new technologies and techniques, making them reliable and widely accepted modalities that will be used in clinical practice.

Acknowledgments This work has been partially supported by EU-H2020 funds under MSCA Individual Fellowship—Grant holder: A. Pawłowski, ACTAN project ID: 837912.

References

- 1. University of Alabama, Department of Biomedical Engineering. [https://www.uab.edu/](https://www.uab.edu/engineering/bme/research/ce) [engineering/bme/research/ce](https://www.uab.edu/engineering/bme/research/ce)
- 2. University of Central Florida.<https://mae.ucf.edu/research-areas/electrophysiology/>
- 3. The University of Bologna. [https://corsi.unibo.it/2cycle/BiomedicalEngineering/](https://corsi.unibo.it/2cycle/BiomedicalEngineering/notice-board/advanced-training-course-bioengineer-and-the-new-technologies-in-the-electrophysiology-room) [notice-board/advanced-training-course-bioengineer-and-the-new-technologies-in-the](https://corsi.unibo.it/2cycle/BiomedicalEngineering/notice-board/advanced-training-course-bioengineer-and-the-new-technologies-in-the-electrophysiology-room)[electrophysiology-room](https://corsi.unibo.it/2cycle/BiomedicalEngineering/notice-board/advanced-training-course-bioengineer-and-the-new-technologies-in-the-electrophysiology-room)
- 4. Albarracín AL, Farfán FD, Coletti MA, Teruya PY, Felice CJ (2016) Electrophysiology for biomedical engineering students: a practical and theoretical course in animal electrocorticography. Adv Physiol Educ 40(3):402–409. <https://doi.org/10.1152/advan.00073.2015>
- 5. Attokaren MK, Jeong N, Blanpain L, Paulson AL, Garza KM, Borron B et al (2023) BrainWAVE: a fexible method for noninvasive stimulation of brain rhythms across species. eNeuro 6:ENEURO.0257–22. Epub ahead of print. PMID: 36754625. [https://doi.org/10.1523/](https://doi.org/10.1523/ENEURO.0257-22.2022) [ENEURO.0257-22.2022](https://doi.org/10.1523/ENEURO.0257-22.2022)
- 6. Vial F, Merchant SHI, McGurrin P, Hallett M (2023) How to do an electrophysiological study of myoclonus. J Clin Neurophysiol 40(2):93–99. Epub 2022 Jun 30. PMID: 36735457; PMCID: PMC9898630. <https://doi.org/10.1097/WNP.0000000000000885>
- 7. Chou CY, Agin-Liebes J, Kuo SH (2023) Emerging therapies and recent advances for Tourette syndrome. Heliyon 9(1):e12874. PMID: 36691528; PMCID: PMC9860289. [https://doi.](https://doi.org/10.1016/j.heliyon.2023.e12874) [org/10.1016/j.heliyon.2023.e12874](https://doi.org/10.1016/j.heliyon.2023.e12874)
- 8. Kornej J, Börschel CS, Benjamin EJ, Schnabel RB (2020) Epidemiology of atrial fbrillation in the 21st century: novel methods and new insights. Circ Res 127(1):4–20. Epub 2020 Jun 18. PMID: 32716709; PMCID: PMC7577553. [https://doi.org/10.1161/](https://doi.org/10.1161/CIRCRESAHA.120.316340) [CIRCRESAHA.120.316340](https://doi.org/10.1161/CIRCRESAHA.120.316340)
- 9. Li H, Song X, Liang Y et al (2022) Global, regional, and national burden of disease study of atrial fbrillation/futter, 1990–2019: results from a global burden of disease study, 2019. BMC Public Health 22:2015.<https://doi.org/10.1186/s12889-022-14403-2>
- 10. Khan AA, Boriani G, Lip GYH (2020) Are atrial high rate episodes (AHREs) a precursor to atrial fbrillation? Clin Res Cardiol 109:409–416.<https://doi.org/10.1007/s00392-019-01545-4>
- 11. Benjamin EJ, Virani SS, Callaway CW, Chamberlain AM, Chang AR, Cheng S et al (2018) American Heart Association Council on Epidemiology and Prevention Statistics Committee and Stroke Statistics Subcommittee. Heart Disease and Stroke Statistics-2018 update: a report from the American Heart Association. Circulation 137(12):e67–e492. Epub 2018 Jan 31. Erratum in: Circulation. 2018 Mar 20;137(12):e493. PMID: 29386200. [https://doi.](https://doi.org/10.1161/CIR.0000000000000558) [org/10.1161/CIR.0000000000000558](https://doi.org/10.1161/CIR.0000000000000558)
- 12. Kwok CS, Darlington D, Mayer J, Panchal G, Walker V, Zachariah D et al (2022) A review of the wide range of indications and uses of implantable loop recorders: a review of the literature. Heart 3:45–53. <https://doi.org/10.3390/hearts3020007>
- 13. Gautham A, Venkitaraman KR (2016) Designing of a single arm single lead ECG system for wet and dry electrode: a comparison with traditional system. Biomed Eng Appl Basis Commun 28(03):1650021.<https://doi.org/10.4015/S1016237216500216>
- 14. Nikodem J, Hrymniak B, Kluwak K, Zyśko D, Klempous R, Rozenblit J et al (2022) EUROCAST, LNCS 2023. Springer, Berlin. Chapter 60; 13789, 978-3-031-25311-9
- 15. Camm A, Naccarelli G, Mittal S, Crijns H, Hohnloser S, Ma C et al (2022) The increasing role of rhythm control in patients with atrial fbrillation. J Am Coll Cardiol 79(19):1932–1948. <https://doi.org/10.1016/j.jacc.2022.03.337>
- 16. Hindricks G, Potpara T, Dagres N, Arbelo E, Bax JJ, Blomström-Lundqvist C et al (2021) ESC Scientifc Document Group. 2020 ESC Guidelines for the diagnosis and management of atrial fbrillation developed in collaboration with the European Association for Cardio-Thoracic Surgery (EACTS): The Task Force for the diagnosis and management of atrial fbrillation of the European Society of Cardiology (ESC) Developed with the special contribution of the European Heart Rhythm Association (EHRA) of the ESC. Eur Heart J 42(5):373–498. Erratum in: Eur Heart J. 2021 Feb 1;42(5):507. Erratum in: Eur Heart J. 2021 Feb 1;42(5):546–547. Erratum in: Eur Heart J. 2021 Oct 21;42(40):4194. PMID: 32860505. [https://doi.org/10.1093/](https://doi.org/10.1093/eurheartj/ehaa612) [eurheartj/ehaa612](https://doi.org/10.1093/eurheartj/ehaa612)
- 17. Golubnitschaja O, Costigliola V (2012) EPMA: general report & recommendations in predictive, preventive and personalised medicine 2012: white paper of the European association for predictive preventive and personalised medicine. EPMA J 3(1):14. [https://doi.org/10.118](https://doi.org/10.1186/1878-5085-3-14) [6/1878-5085-3-14](https://doi.org/10.1186/1878-5085-3-14)
- 18. Vahanian A, Beyersdorf F, Praz F, Milojevic M, Baldus S, Bauersachs J et al (2022) 2021 ESC/ EACTS guidelines for the management of valvular heart disease. Eur Heart J 43(7):561–632. <https://doi.org/10.1093/eurheartj/ehab395>
- 19. Cribier A, Eltchaninoff H, Bash A, Borenstein N, Tron C, Bauer F et al (2002) Percutaneous transcatheter implantation of an aortic valve prosthesis for calcifc aortic stenosis: frst human case description. Circulation 106(24):3006–3008. [https://doi.org/10.1161/01.](https://doi.org/10.1161/01.CIR.0000047200.36165.B8) [CIR.0000047200.36165.B8](https://doi.org/10.1161/01.CIR.0000047200.36165.B8)
- 20. Sharma T, Krishnan AM, Lahoud R, Polomsky M, Dauerman HL (2022) National trends in TAVR and SAVR for patients with severe isolated aortic stenosis. J Am Coll Cardiol 80(21):2054–2056. <https://doi.org/10.1016/j.jacc.2022.08.787>
- 21. Mack MJ, Leon MB, Thourani VH et al (2019) Transcatheter aortic-valve replacement with a balloon-expandable valve in low-risk patients. N Engl J Med 380(18):1695–1705. [https://doi.](https://doi.org/10.1056/nejmoa1814052) [org/10.1056/nejmoa1814052](https://doi.org/10.1056/nejmoa1814052)
- 22. Nazif TM, Williams MR, Hahn RT, Kapadia S, Babaliaros V, Rodés-Cabau J et al (2014) Clinical implications of new-onset left bundle branch block after transcatheter aortic valve replacement: analysis of the PARTNER experience. Eur Heart J 35(24):1599–1607. [https://](https://doi.org/10.1093/eurheartj/eht376) doi.org/10.1093/eurheartj/eht376
- 23. Glikson M, Nielsen JC, Kronborg MB, Michowitz Y, Auricchio A, Barbash I et al (2021) 2021 ESC guidelines on cardiac pacing and cardiac resynchronization therapy. Eur Heart J 42(35):3427–3520. <https://doi.org/10.1093/eurheartj/ehab364>
- 24. Palmisano P, Guerra F, Aspromonte V, Dell'Era G, Pellegrino P, Laff M et al (2022) Management of older patients with unexplained, recurrent, traumatic syncope and bifascicular block: implantable loop recorder versus empiric pacemaker implantation—results of a propensity-matched analysis. Heart Rhythm 19(10):1696–1703. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.hrthm.2022.05.023) [hrthm.2022.05.023](https://doi.org/10.1016/j.hrthm.2022.05.023)
- 25. Udo EO, Zuithoff NPA, van Hemel NM, de Cock C, Hendriks T, Doevendans P et al (2012) Incidence and predictors of short- and long-term complications in pacemaker therapy: the FOLLOWPACE study. Heart Rhythm 9(5):728–735. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.hrthm.2011.12.014) [hrthm.2011.12.014](https://doi.org/10.1016/j.hrthm.2011.12.014)
- 26. Kypta A, Blessberger H, Lichtenauer M, Steinwender C (2016) Complete encapsulation of a leadless cardiac pacemaker. Clin Res Cardiol 105:94. [https://doi.org/10.1007/](https://doi.org/10.1007/s00392-015-0929-x) [s00392-015-0929-x](https://doi.org/10.1007/s00392-015-0929-x)
- 27. Mangieri A, Montalto C, Pagnesi M, Lanzillo G, Demir O, Testa L et al (2018) TAVI and post procedural cardiac conduction abnormalities. Front Cardiovasc Med 1:85. [https://doi.](https://doi.org/10.3389/fcvm.2018.00085) [org/10.3389/fcvm.2018.00085](https://doi.org/10.3389/fcvm.2018.00085)
- 28. El-Chami MF, Al-Samadi F, Clementy N, Garweg C, Martinez-Sande J, Piccini J et al (2018) Updated performance of the Micra transcatheter pacemaker in the real-world setting: a comparison to the investigational study and a transvenous historical control. Heart Rhythm 15(12):1800–1807. <https://doi.org/10.1016/j.hrthm.2018.08.005>
- 29. Roberts PR, Clementy N, al Samadi F, Garweg CH, Martinez-Sande J, Iacopino S et al (2017) A leadless pacemaker in the real-world setting: the Micra Transcatheter pacing system post-approval registry. Heart Rhythm 14(9):1375–1379. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.hrthm.2017.05.017) [hrthm.2017.05.017](https://doi.org/10.1016/j.hrthm.2017.05.017)
- 30. Mechulan A, Prevot S, Peret A, Nait-Saidi L, Miliani I, Leong-Feng L et al (2022) Micra AV leadless pacemaker implantation after transcatheter aortic valve implantation. PACE 45(11):1310–1315. <https://doi.org/10.1111/pace.14545>
- 31. Kusumoto FM, Schoenfeld MH, Barrett C, Edgerton JR, Ellenbogen KA, Gold MR et al (2019) 2018 ACC/AHA/HRS guideline on the evaluation and management of patients with bradycardia and cardiac conduction delay: executive summary: a report of the American College of Cardiology/American Heart Association task force on clinical practice guidelines, and the Heart Rhythm Society. Heart Rhythm 16(9):e227–e279. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.hrthm.2018.10.036) [hrthm.2018.10.036](https://doi.org/10.1016/j.hrthm.2018.10.036)
- 32. Chung MK, Fagerlin A, Wang PJ, Ajayi TB, Allen LA, Baykaner T et al (2021) Shared decision making in cardiac electrophysiology procedures and arrhythmia management. Circ Arrhythm Electrophysiol 14(12):e007958. <https://doi.org/10.1161/CIRCEP.121.007958>
- 33. Zanon F, Ellenbogen KA, Dandamudi G, Sharma PS, Huang W, Lustgarten DL et al (2018) Permanent his-bundle pacing: a systematic literature review and meta-analysis. Europace 20(11):1819–1826. <https://doi.org/10.1093/europace/euy058>
- 34. Ponnusamy SS, Arora V, Namboodiri N, Kumar V, Kapoor A, Vijayaraman P (2020) Left bundle branch pacing: a comprehensive review. J Cardiovasc Electrophysiol 31(9):2462–2473. Epub 2020 Jul 30.<https://doi.org/10.1111/jce.14681>
- 35. Pachon JC, Pachon EI, Pachon JC, Lobo TJ, Pachon MZ, Vargas RN et al (2005) "Cardioneuroablation"—new treatment for neurocardiogenic syncope, functional AV block

and sinus dysfunction using catheter RF-ablation. Europace 7:1–13. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.eupc.2004.10.003) [eupc.2004.10.003](https://doi.org/10.1016/j.eupc.2004.10.003)

- 36. Pachon JC, Pachon EI, Cunha Pachon MZ, Lobo TJ, Pachon JC, Santillana TG (2011) Catheter ablation of severe neurally mediatated refex (neurocardiogenic or vasovagal) syncope: cardioneuroablation long-term results. Europace 13:1231–1242. [https://doi.org/10.1093/](https://doi.org/10.1093/europace/eur163) [europace/eur163](https://doi.org/10.1093/europace/eur163)
- 37. Piotrowski R, Baran J, Sikorska A, Krynski T, Kulakowski P (2022) Cardioneuroablation for refex syncope: effcacy and effects on autonomic cardiac regulation—a prospective randomized trial. JACC Clin Electrophysiol 28:85. <https://doi.org/10.1016/j.jacep.2022.08.011>
- 38. Stec S, Jankowska-Polańska JD, Wileczek A, Josiak K, Śledź J et al (2022) Rationale and design of SAN.OK randomized clinical trial and registry: comparison of the effects of evidence-based pacemaker therapy and cardioneuroablation in sinus node dysfunction. Cardiol J 29(6):1031–1036.<https://doi.org/10.5603/CJ.a2022.0103>
- 39. Reichert A, Wileczek A, Stec S (2022) Cardioneuroablation for the effective treatment of recurrent vasovagal syncope to restore driving abilities. Kardiol Pol 80(11):1158–1160. [https://doi.](https://doi.org/10.33963/KP.a2022.0189) [org/10.33963/KP.a2022.0189](https://doi.org/10.33963/KP.a2022.0189)
- 40. Rudbeck-Resdal J, Christiansen MK, Johansen JB, Nielsen JC, Bundgaard H, Jensen HK (2019) Aetiologies and temporal trends of atrioventricular block in young patients: a 20-year nationwide study. Europace 21(11):1710–1716.<https://doi.org/10.1093/europace/euz206>
- 41. Tułecki Ł, Polewczyk A, Jacheć W, Nowosielecka D, Tomków K, Stefańczyk P et al (2021) A study of major and minor complications of 1500 Transvenous Lead extraction procedures performed with optimal safety at two high-volume referral centers. Int J Environ Res Public Health 18(19):10416. <https://doi.org/10.3390/ijerph181910416>
- 42. Sidhu BS, Gould J, Bunce C, Elliott M, Mehta V, Kennergren C et al (2020) ELECTRa Investigators group. The effect of Centre volume and procedure location on major complications and mortality from transvenous lead extraction: an ESC EHRA EORP European Lead extraction ConTRolled ELECTRa registry subanalysis. Europace 22(11):1718–1728. [https://](https://doi.org/10.1093/europace/euaa131) doi.org/10.1093/europace/euaa131
- 43. Haissaguerre M, Jais P, Shah DC, Takahashi A, Hocini M, Quiniou G et al (1998) Spontaneous initiation of atrial fbrillation by ectopic beats originating in the pulmonary veins. N Engl J Med 339(10):659–666.<https://doi.org/10.1056/NEJM199809033391003>
- 44. Kuck KH, Brugada J, Furnkranz A, Metzner A, Ouyang F, Chun KR et al (2016) Cryoballoon or radiofrequency ablation for paroxysmal atrial fbrillation. N Engl J Med 374:2235–2245. <https://doi.org/10.1056/NEJMoa1602014>
- 45. Defaye P, Kane A, Jacon P, Mondesert B (2010) Cryoballoon for pulmonary vein isolation: is it better tolerated than radiofrequency? Retrospective study comparing the use of analgesia and sedation in both ablation techniques. Arch Cardiovasc Dis 103(6–7):388–393. [https://doi.](https://doi.org/10.1016/j.acvd.2010.06.004) [org/10.1016/j.acvd.2010.06.004](https://doi.org/10.1016/j.acvd.2010.06.004)
- 46. Kuck KH, Albenque JP, Chun KRJ, Fürnkranz A, Busch M, Elvanet A, al. (2019) Repeat ablation for atrial fbrillation recurrence post Cryoballoon or radiofrequency ablation in the FIRE and ICE trial. Circ Arrhythm Electrophysiol 12(6):1–9. [https://doi.org/10.1161/](https://doi.org/10.1161/CIRCEP.119.007247) [CIRCEP.119.007247](https://doi.org/10.1161/CIRCEP.119.007247)
- 47. Ikenouchi T, Inaba O, Takamiya T, Inamura Y, Sato A, Matsumura Y et al (2021) The impact of left atrium size on selection of the pulmonary vein isolation method for atrial fbrillation: Cryoballoon or radiofrequency catheter ablation. In: Impact of LA size on selecting the PVI method, vol 231. Elsevier, Amsterdam, p 82.<https://doi.org/10.1016/j.ahj.2020.10.061>
- 48. Di Biase L, Conti S, Mohanty P, Bai R, Sanchez J, Walton D et al (2011) General anesthesia reduces the prevalence of pulmonary vein reconnection during repeat ablation when compared with conscious sedation: results from a randomized study. Heart Rhythm 8(3):368–372. <https://doi.org/10.1016/j.hrthm.2010.10.043>
- 49. Inoue K, Murakawa Y, Nogami A, Shoda M, Naito S, Kumagai K et al (2014) Current status of catheter ablation for atrial fbrillation—updated summary of the Japanese Catheter Ablation Registry of Atrial Fibrillation (J-CARAF). Circ J 78(5):1112–1120. [https://doi.org/10.1253/](https://doi.org/10.1253/circj.cj-13-1179) [circj.cj-13-1179](https://doi.org/10.1253/circj.cj-13-1179)
- 50. Yamaguchi T, Shimakawa Y, Mitsumizo S, Fukui A, Kawano Y, Otsubo T et al (2018) Feasibility of total intravenous anesthesia by cardiologists with the support of anesthesiologists during catheter ablation of atrial fibrillation. J Cardiol 72(1):19-25. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.jjcc.2017.12.008) iicc.2017.12.008
- 51. Pachon MJ, Pachon ME, Santillana PT, Lobo T, Pachon C, Pachon MJ et al (2015) Simplifed method for vagal effect evaluation in cardiac ablation and electrophysiological procedures. JACC Clin Electrophysiol 1(5):451–460.<https://doi.org/10.1016/j.jacep.2015.06.008>
- 52. Khodaei M, Candelino N, Mehrvarz A, Jalili N (2020) Physiological closed-loop control (PCLC) systems: review of a modern frontier in automation. IEEE Access 8:23965–24005. <https://doi.org/10.1109/ACCESS.2020.2968440>
- 53. Ghita M, Neckebroek M, Muresan C, Copot D (2020) Closed-loop control of anesthesia: survey on actual trends, challenges and perspectives. IEEE Access 8:206264–206279. [https://doi.](https://doi.org/10.1109/ACCESS.2020.3037725) [org/10.1109/ACCESS.2020.3037725](https://doi.org/10.1109/ACCESS.2020.3037725)
- 54. Ionescu C, Neckebroek M, Ghita M, Copot D (2021) An open source patient simulator for design and evaluation of computer based multiple drug dosing control for anesthetic and hemodynamic variables. IEEE Access 9:8680–8694.<https://doi.org/10.1109/ACCESS.2021.3049880>
- 55. Soltesz K, Dumont G, van Heusden K, Hägglund T, Ansermino J (2012) Simulated mid-ranging control of propofol and remifentanil using EEG measured hypnotic depth of anesthesia. In: Proceedings of 51st IEEE Conference on Decision and Control. CDC, Maui, pp 356–361. <https://doi.org/10.1109/CDC.2012.6426858>
- 56. Merigo L, Padula F, Pawlowski A, Dormido S, Guzman J, Latronico N et al (2018) A modelbased control scheme for depth of hypnosis in anesthesia. Biomed Signal Process Control 42:216–229
- 57. Pawłowski A, Schiavo M, Latronico N, Paltenghi M, Visioli A (2023) Event-based MPC for propofol administration in anesthesia. Comput Methods Programs Biomed 229:107289. ISSN 0169-2607. <https://doi.org/10.1016/j.cmpb.2022.107289>
- 58. Pawlowski A, Schiavo M, Latronico N, Paltenghi M, Visioli A (2022) Model predictive control using MISO approach for drug co-administration in anesthesia. J Process Control 117:98–111. <https://doi.org/10.1016/j.jprocont.2022.07.007>
- 59. Pawlowski A, Merigo L, Guzmán J, Dormido S, Visioli A (2018) Two-degree-of-freedom control scheme for depth of hypnosis in anesthesia. IFAC Pap Online 51(4):72–77. [https://doi.](https://doi.org/10.1016/j.ifacol.2018.06.034) [org/10.1016/j.ifacol.2018.06.034](https://doi.org/10.1016/j.ifacol.2018.06.034)
- 60. Pawlowski A, Schiavo M, Latronico N, Paltenghi M, Visioli A (2022) Linear MPC for anesthesia process with external predictor. Comput Chem Eng 161:1–13. [https://doi.org/10.1016/j.](https://doi.org/10.1016/j.compchemeng.2022.107747) [compchemeng.2022.107747](https://doi.org/10.1016/j.compchemeng.2022.107747)
- 61. Vanluchene AL, Vereecke H, Thas O, Mortier EP, Shafer SL, Struys MM (2004) Spectral entropy as an electroencephalographic measure of anesthetic drug effect: a comparison with bispectral index and processed midlatency auditory evoked response. Anesthesiology 101(1):34–42. <https://doi.org/10.1097/00000542-200407000-00008>
- 62. Absalom A, Kenny G (2003) Closed-loop control of propofol anaesthesia using bispectral index: performance assessment in patients receiving computer controlled propofol and manually controlled remifentanil infusions for minor surgery. Br J Anaesth 90(6):737–741. [https://](https://doi.org/10.1093/bja/aeg137) doi.org/10.1093/bja/aeg137
- 63. Absalom A, Sutcliffe N, Kenny G (2002) Closed-loop control of anesthesia using bispectral index. Anesthesiology 96(1):67–73.<https://doi.org/10.1097/00000542-200201000-00017>
- 64. Liu N, Chazot T, Genty A, Landais A, Restoux A, McGee K et al (2006) Titration of propofol for anesthetic induction and maintenance guided by the bispectral index: closed-loop versus manual control. Anesthesiology 104(4):686–695. [https://doi.](https://doi.org/10.1097/00000542-200604000-00012) [org/10.1097/00000542-200604000-00012](https://doi.org/10.1097/00000542-200604000-00012)
- 65. Puri G, Kumar B, Aveek J (2007) Closed-loop anaesthesia delievery system (CLADS) using bispectral index; a performance assessment study. Anaesth Intensive Care 35(3):357–362. <https://doi.org/10.1177/0310057X0703500306>
- 66. van Heusden K, Dumont G, Soltesz K, Petersen C, Umedaly A, West N et al (2014) Design and clinical evaluation of robust PID control of propofol anesthesia in children. IEEE Trans Control Syst Technol 22(29):491–501. <https://doi.org/10.1109/TCST.2013.2260543>
- 67. Liu N, Chazot T, Hamada S, Landais A, Boichut N, Dussaussoy C et al (2011) Closed-loop coadministration of propofol and remifentanil guided by bispectral index: a randomized multicenter study. Anesth Analg 112:546–557.<https://doi.org/10.1213/ANE.0b013e318205680b>
- 68. Morley A, Derrick J, Mainland P, Lee B, Short T (2000) Closed loop control of anaesthesia: an assessment of the bispectral index as the target of control. Anesthesia 55:953–959. [https://doi.](https://doi.org/10.1046/j.1365-2044.2000.01527.x) [org/10.1046/j.1365-2044.2000.01527.x](https://doi.org/10.1046/j.1365-2044.2000.01527.x)
- 69. Struys M, Smet T, Versichelen L, Velde S, Broecke R, Mortier E (2001) Comparison of closed-loop controlled administration of propofol using bispectral index as the controlled variable versus standard practice controlled administration. Anesthesiology 95:6–1. [https://doi.](https://doi.org/10.1097/00000542-200107000-00007) [org/10.1097/00000542-200107000-00007](https://doi.org/10.1097/00000542-200107000-00007)