

13 Emerging Non-invasive Markers: Imaging, Blood, and Liver Clearance Tests

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Emerging Non-invasive Methods as a Surrogate for HVPG Measurement

Imaging Markers

Contrast-Enhanced Ultrasound

Contrast-enhanced ultrasound (CEUS) involves the intravenous administration of minute, gas-flled microbubbles that enhance the intravascular signal. The hepatic vein arrival time (HVAT) of the microbubble agent has been studied as a diagnostic tool for detecting advanced fbrosis and cirrhosis [\[1](#page-13-0)]. The peak enhancement time of the microbubble, which is defned as the interval time from the contrast onset in the splenic artery to the time to reach maximum intensity in the splenic vein, was shown to correlate with HVPG [[2\]](#page-13-1).

Several characteristics of the contrast agents have been studied in relation to PH. The subharmonic signal from the US contrast agents refected pressure changes in the ambient fuid. This was the basis of the subharmonic-aided pressure estimation technique (SHAPE) [\[3](#page-13-2)]. The SHAPE gradient between the portal vein and the hepatic vein was initially shown to correlate with HVPG in a pilot study of 45 patients [[4\]](#page-13-3) and validated in a prospective cohort of 125 patients [[5\]](#page-13-4). Assessment of the hepatic vascular network using computer-based analysis of the videos generated from CEUS yielded the 'hepatic vascular connectome' [[6\]](#page-13-5). Patients with cirrhosis

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had a lower clustering coefficient of the hepatic vascular connectome compared to healthy controls, and the clustering coefficient correlated with HVPG in 15 patients [\[6](#page-13-5)]. This method has been evaluated further in a multicentre study, but the results have not yet been published in detail. Although an excellent correlation with HVPG was reported in the initial results, the automated software was only able to provide portal pressure estimation in 56% of the patients studied [\[7](#page-13-6)]. The poor technical success rate may limit the generalisability of this technique.

Computed Tomography

The ratio of liver to spleen volume measured on contrast-enhanced computed tomography (CT) images was shown to correlate with HVPG [[8\]](#page-13-7). These CT scans were obtained preoperatively in patients being evaluated for hepatocellular carcinoma (HCC) resection, and the CT-based model was developed to stratify patients for resection surgery and liver transplantation. However, the correlation was poor in patients at extremes of the HVPG spectrum (i.e., normal, or very high) [[9,](#page-13-8) [10\]](#page-13-9).

Advances in the imaging-based 3D modelling with computational fuid analysis allow non-invasive assessment of intravascular blood fow and pressure, and these techniques are used in cardiology for the assessment of coronary arteries [[11\]](#page-13-10). Qi et al. recently used triple-phase CT angiography of the liver to develop a 'virtual HVPG' (vHVPG) [[12\]](#page-13-11). The vHVPG was calculated using a mathematical model that included the portal vein velocity measured using Doppler US. There was a moderate positive correlation between vHVPG and invasive HVPG $(R = 0.61)$, with an AUROC of 0.88 for diagnosing CSPH. Notably, interpretation of the vHVPG was time-consuming $(\sim 2.5 \text{ h/case})$ and the study included small numbers of patients without CSPH.

The development of a radiomics signature involves machine learning to extract high-dimensional quantitative features from radiological images. This was explored as a method to evaluate PH [[13\]](#page-13-12). Regions of interest were drawn on portal venous phase CT images of the liver and spleen, and 20,648 radiomics features were retrieved. This was reduced to seven features from the liver and four features from the spleen, which were included in a regression model to develop radiomics-based HVPG (rHVPG). The rHVPG had an AUROC of 0.85 for diagnosing CSPH and was validated in four external cohorts. The direct correlation between rHVPG and HVPG was not reported.

These CT-based methods involve ionising radiation, which limits utility especially for repeated measurements. The intravenous contrast for CT is also recognised to be nephrotoxic and can cause contrast-induced acute kidney injury [\[14](#page-13-13)].

Magnetic Resonance Imaging

Haemodynamic Measures

Phase contrast (PC)-MRI is a non-invasive technique to measure fow in a blood vessel without the use of intravenous contrast. PC-MRI measures blood fow with high accuracy, confrmed by phantom models [\[15](#page-13-14), [16\]](#page-13-15) and by in vivo studies with direct measurement in deep canine arteries and veins [[17\]](#page-13-16).

		Correlation			
MRI parameters	Study	with HVPG	Notes		
Vessel flow (PC-MRI)					
Azygous vein flow	Gouva et al. 2016 [18]	$r^2 = 0.77$	$n = 69$; HVPG range 3 to 25 mmHg		
	Palaniyappan et al. 2016 [19]	$r = 0.66$	$n = 30$; mean HVPG 9.8 ± 6.1 mmHg		
Superior \bullet mesenteric artery velocity	Palaniyappan et al. 2016 [19]	$r = 0.53$			
Splenic artery velocity	Palaniyappan et al. 2016 [19]	$r = 0.58$			
Caval subtraction hepatic artery fraction	Chouhan et al. 2017 [20]	$r = 0.78$	$n = 12$; mean HVPG 12.3 ± 1.6 mmHg		
Tissue perfusion (arterial spin labelling (ASL)					
Liver tissue perfusion	Palaniyappan et al. 2016 [19]	$r = 0.38$	Correlation was absent in HVPG >10 mmHg		
Arrival time		$r = -0.47$			
Structural measures					
Liver _{T1} \bullet	Palaniyappan et al. 2016 [19]	$r = 0.84$			
Spleen T1 \bullet	Palaniyappan et al. 2016 [19]	$r = 0.40$	Correlation was absent in HVPG >10 mmHg		
	Levick et al. 2019 [25]	$r = 0.69$	$n = 19$, median HVPG 9.0 (IQR $4.0 - 14.0$		
Dynamic contrast-enhanced MRI (DCE-MRI)					
Liver distribution volume (DV)	Wagner et al. 2018 [31]	$r = 0.49$	$n = 34$; 12 patients <5 mmHg, 13 patients 5-10 mmHg, 9 patients \geq 10 mmHg		
Liver time to ٠ peak (TTP)		$r = 0.52$			
Liver upslope		$r = -0.57$			

Table 13.1 Summary of MRI parameters evaluated for the assessment of portal hypertension

PC-MRI measured azygous vein fow that has been shown to correlate with grade of oesophageal varices [[16\]](#page-13-15) and HVPG [\[18](#page-14-0), [19\]](#page-14-1) (Table [13.1](#page-2-0)). However, the correlation was absent in patients with CSPH [[19\]](#page-14-1). The relationship between hepatic infow and portal pressure is less well established. Portal venous fow does not correlate with HVPG [\[18](#page-14-0)[–20](#page-14-2)], but hepatic arterial fraction of the hepatic infow was shown to correlate with HVPG in 12 patients [\[20](#page-14-2)]. The hepatic artery fow in this study was obtained indirectly by subtracting the portal vein fow from the total hepatic blood flow (the difference between infra- and suprahepatic vena cava). PC-MRI measured fow in the splanchnic circulation (splenic artery and superior mesenteric artery) correlated significantly with HVPG [[19\]](#page-14-1).

Arterial spin labelling (ASL)-MRI is a non-invasive technique that quantifes tissue perfusion by using magnetically labelled arterial blood water protons as an endogenous tracer $[21]$ $[21]$. The liver perfusion and tissue arrival time measured using ASL-MRI have been shown to correlate with HVPG [\[19](#page-14-1)].

Structural and Architectural Changes

Native (non-contrast) longitudinal relaxation time (T1) can detect pathologically important processes in tissues [[22\]](#page-14-6) and is an established composite marker of liver infammation and fbrosis [[23,](#page-14-7) [24](#page-14-8)]. Furthermore, liver T1 correlated with HVPG, and this relationship was maintained in patients with CSPH [[19\]](#page-14-1). The T1 measurement was respiratory-triggered and multi-slice, and therefore a large volume of the liver could be sampled in a reasonable timeframe. Interestingly, the distribution of liver T1 values was shown to increase with worsening of PH, refecting the increasing heterogeneity of T1 values across the liver volume. This underscores the sampling variability associated with liver biopsy (and potentially transient elastography).

A subsequent study reported an association between splenic T1 and HVPG but failed to show a correlation with liver T1 [\[25](#page-14-3)]. The methodology used to measure T1 could potentially explain this difference. In this study, a modifed look-locker inversion recovery (MOLLI) T1 mapping method was used which requires breathholding for every image slice acquired. The T1 measurements were obtained from regions of interest drawn on the liver and spleen and therefore could be susceptible to sampling variability due to the heterogeneity of T1 values across the organ. In addition, it has been shown that the hepatic fat content can be large enough to cause substantial MOLLI T1 alterations [\[26](#page-14-9)].

An MRI-based scoring system of the features of PH was studied as a surrogate measure of HVPG [\[27](#page-14-10)]. The PH score included the number of variceal sites, volume of ascites and maximum splenic diameter, with scores between 0 and 3 in each domain yielding a total score of 0 to 9 for each patient. The PH score correlated with HVPG and the AUROC for detection of PH and CSPH was 0.78 and 0.83, respectively.

Dynamic Contrast-Enhanced MRI (DCE-MRI)

Perfusion-weighted MRI can be performed by measuring the signal intensity in the tissue of interest after injection of contrast against time. Initial assumption of a linear relationship between the signal intensity and the concentration of gadolinium in the liver using a single-input single-compartment model is simplistic and inaccurate, as it does not take into account the separate portal venous and hepatic arterial contributions [\[28](#page-14-11)]. However, subsequent analysis of signal intensity over the portal vein, aorta and liver parenchyma against time can be ftted to a dual-input singlecompartment model [[29\]](#page-14-12).

Decreased portal fraction, total liver perfusion, increased arterial fraction as well as increased mean transit time (MTT) were related to severity of PH [\[30](#page-14-13)]. Signifcant correlation of DCE-MRI parameters including contrast time-to-peak, liver distribution volume and liver upslope correlated with HVPG [\[31](#page-14-4)].

4D fow MRI mapping with gadolinium-based contrast allows 3D vascular coverage and is a promising technique for comprehensive haemodynamic analyses.

Increased 4D fow parameters in the splanchnic circulation (splenic artery peak velocity, superior mesenteric vein, and splenic vein fow) were related to severity of PH. However, HVPG was not measured in this study and the composite PH score [\[27](#page-14-10)] was used as a surrogate measure of portal pressure.

The potential adverse events associated with the use of contrast agents limit the use of DCE-MRI in patients with chronic liver disease. Gadolinium-based contrast agents are reported to cause nephrogenic systemic fbrosis in patients with renal failure [[32\]](#page-14-14).

Combination MRI Markers

The combination of liver T1 and splenic artery velocity correlated with HVPG [[19\]](#page-14-1). These MR markers refect the underlying pathophysiological changes (structural and haemodynamic) in the development and progression of PH. Moreover, the linear model provided good prediction of HVPG across the spectrum of HVPG values from normal to CSPH and performed better than liver T1 or splenic artery velocity alone.

Magnetic Resonance Elastography (MRE)

Magnetic resonance elastography (MRE) is an alternative to the ultrasonographybased method to evaluate liver and spleen stiffness. Recent studies have validated the use of MRE for evaluating liver fbrosis [[33](#page-14-15)]. MRE has the theoretical advantage over ultrasonography-based elastography methods of evaluating stiffness over a larger area of liver, hence reducing sampling variability. Using MRE, the shear modulus can be assessed using either a 2D or 3D technique. MRE requires special hardware and software which could limit its widespread use.

In a recent meta-analysis, the diagnostic accuracy of spleen stiffness was higher than liver stiffness using MRE. The AUROC for detection of CSPH was 0.88 and 0.92 for liver and spleen stiffness, respectively [[34\]](#page-14-16). The correlation of MRE-measured liver and spleen stiffness with HVPG is summarised in Table [13.2](#page-4-0).

			Correlation with HVPG
Parameter	Sample size, n	Study	(Correlation coefficient, r)
Liver stiffness	34	Wagner et al. 2018 [31]	0.486
	36	Ronot et al. 2014 [35]	0.44
	15	Gharib et al. 2017 [36]	0.64
	52	Danielsen et al. 2021 [37]	0.96
Spleen stiffness	34	Wagner et al. 2018 [31]	0.099 (NS)
	36	Ronot et al. 2014 [35]	0.57
	52	Danielsen et al. 2021 [37]	0.97

Table 13.2 Summary of the relationship between MRE measured liver and spleen stiffness with portal hypertension

NS not signifcant

Serum Markers

Simple liver fbrosis scores were developed using combinations of routine blood tests as indirect markers of liver scarring. Although these markers only correlate moderately with HVPG, some (e.g., Lok score) can diagnose CSPH and the presence of varices (Table [13.3\)](#page-6-0). Thrombocytopenia is an important indication of PH and many of the simple marker panels contain platelet count. The Enhanced Liver Fibrosis (ELF) test is derived from direct markers related to hepatic extracellular matrix turnover and has been extensively validated for the non-invasive assessment of liver fbrosis [[38\]](#page-14-20). The direct and indirect markers of fbrosis perform well in identifying advanced liver fbrosis and early stages of PH when it is largely driven by increased intrahepatic vascular resistance due to structural changes. However, these markers are unlikely to refect the haemodynamic changes that occur with severe PH. The ALBI score was originally devised as a measure of liver function in patients with hepatocellular carcinoma (HCC) [[39\]](#page-14-21). There was a weak positive correlation between ALBI score and HVPG ($r = 0.307$, $P < 0.001$) [\[40](#page-14-22)]. The ALBI score has also been shown to predict patients at risk of decompensation [[41\]](#page-14-23).

sCD163, a scavenger receptor expressed on macrophages, is a specifc marker of macrophage activation and is related to the severity of cirrhosis and PH [[42\]](#page-14-24). Combination of ELF and sCD163 had a superior diagnostic accuracy in identifying CSPH compared to each component individually (AUROC of 0.82, 0.88 and 0.90 for sCD163, ELF and combination, respectively) [\[43](#page-15-0)]. Von Willebrand factor (vWF) is related to endothelial dysfunction and circulating levels of vWF correlated with HVPG [\[44](#page-15-1)]. vWF was also reported to be related to bacterial translocation and infammation and associated with clinical outcomes independent of HVPG [[45\]](#page-15-2). The VITRO score is calculated as the ratio of vWF to thrombocytes, and the diagnostic accuracy of the VITRO score for detecting cirrhosis [\[46](#page-15-3)] and CSPH [\[47](#page-15-4)] was superior to vWF alone.

Indocyanine green (ICG) is administered intravenously and nearly exclusively extracted by the hepatic parenchyma and rapidly excreted in bile. Therefore, ICG clearance, which is quantitatively assessed by spectrophotometry, refects both hepatic function and hepatic blood fow. The ICG 15-minute retention test (ICG-R15) is performed on peripheral blood samples following a bolus injection of ICG and has been shown to be linearly correlated with HVPG ($r = 0.57 - 0.78$) [[50,](#page-15-5) [74](#page-16-0), [75\]](#page-16-1). The ICG-R15 can also be assessed in vivo using pulse dye densitometry fnger probes, but this has not yet been correlated with HVPG.

The HepQuant SHUNT test quantifes hepatic function by simultaneously measuring flow-dependent clearance of cholate from both portal and systemic circulations. In a small study of 20 patients, the SHUNT test was shown to correlate with HVPG [[76\]](#page-16-2). The derived disease severity index (DSI) has been shown to predict decompensation independent of MELD [\[77](#page-16-3)]. The 13C-methacetin breath test is another potential method to assess hepatic function and, in a study of 155 patients with NASH-related cirrhosis, detected CSPH with an AUROC of 0.83 [\[78](#page-16-4)].

These promising results with different liver 'clearance' tests need further validation in large multicentre studies.

Table 13.3 Summary of Serum Marker Tests in Evaluating Portal Hypertension; Correlation with Hepatic Venous Pressure Gradient (HVPG), Diagnostic Accuracy in Estimating Clinically Signifcant Portal Hypertension (CSPH), and High-Risk Varices (HRV)/Varices Needing Treatment (VNT) Liver Clearance Tests

(continued)

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Non-invasive Methods for Assessment of HVPG Response

The non-invasive assessment of haemodynamic response following treatment for PH has been considered an unmet need in hepatology. Historically, a reduction in heart rate (HR) was assessed as a proxy for therapeutic response to non-selective betablockers (NSBB). However, changes in heart rate do not correlate with the changes in HVPG [\[79](#page-16-15), [80\]](#page-16-16). Nevertheless, the absolute beneft of identifying HVPG 'responders' is not fully established. Indeed, in the PREDESCI study, NSBB treatment without using portal pressure response in the follow-up to guide therapy improved decompensation-free survival. There are two important attributes for a non-invasive test to reliably monitor HVPG response. Firstly, the test should correlate with HVPG across a broad spectrum of HVPG values. As discussed previously, most non-invasive methodologies have been developed and validated as a binary predictor of CSPH and/or presence of varices, but the data on correlation with HVPG as a continuous variable are limited. Secondly, the inherent variability of the measurement should be small enough to detect the relatively modest changes in HVPG that may occur with pharmacological treatments. The haemodynamic response is defned by 10%–20% changes in HVPG from baseline which could correspond to absolute pressure changes as small as 2–4 mmHg. It follows that any non-invasive test with signifcant variability will lack suffcient sensitivity to detect the minor differences in HVPG. Notwithstanding, in the context of clinical trials, the within-individual variance of HVPG itself is a potential confounder in evaluating the haemodynamic response to interventions, especially in decompensated patients [\[81](#page-16-17)].

Doppler US-based assessment of blood flow showed some promise in detecting HVPG response following treatment with terlipressin [\[82](#page-16-18)] and propranolol [\[83\]](#page-16-19). However, the initial results have not been reproduced [\[84\]](#page-16-20). This is likely due to the technical variation associated with Doppler US which limits the ability to reliably detect changes in HVPG. PC-MRI is another potential method to non-invasively evaluate blood fow alterations. In a small feasibility study, a reduction in cardiac output as measured by PC-MRI fow in the abdominal aorta was reported following NSBB, but there were no statistically signifcant changes in fow in the other vessels analysed [\[85\]](#page-16-21). In this study, there were also no contemporaneous HVPG measurements.

Spleen stiffness measured using MRE signifcantly decreased following the administration of intravenous NSBB, but no change was observed in liver stiffness [\[37](#page-14-19)]. However, the changes in spleen stiffness were not related to HVPG response.

In addition, non-imaging-based markers of HVPG response have been evaluated. The expression of specifc vasoactive proteins of Ras homolog family member A (RhoA) and Rho-kinase (ROCK) pathway in the gastric mucosa correlated with acute haemodynamic response following intravenous propranolol [[86\]](#page-16-22). The haemodynamic responders showed lower expression of beta-arrestin2 (βArr2) in antral biopsies. This is not strictly a non-invasive test as the tissue samples are obtained by upper gastrointestinal endoscopy. Alternatively, using a serum metabolomic profling approach, the combination of two metabolites (phosphatidylcholine and eicosadienoic acid) also identifed acute HVPG responders to intravenous propranolol with an AUROC of 0.801 [\[87](#page-16-23)].

Conclusion

Although HVPG is an invasive and highly specialised method for the diagnosis of PH and assessment of treatment response, it has an important role in specifc clinical circumstances and in interventional trials. A number of non-invasive tests (other than ultrasound elastography) have been shown to correlate with HVPG and perform well for the diagnosis of CSPH [\[59](#page-15-16)], but further validation in larger cohorts of patients with diverse etiologies is generally required. Variability and reproducibility will remain a challenge for development of suitable PH monitoring biomarkers.

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