

# Chapter 3 Coronal and Axial Alignment: The Effects of Malalignment

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#### Introduction

The normal knee joint can support a lifetime of repetitive load, generally, without the development of degenerative changes. Excessive stress, which exceeds the tolerance of articular cartilage, disrupts articular homeostasis leading to deterioration of the articular cartilage. In physiological condition, the load applied to the knee joint is distributed across the compartments. Any deviation of the knee alignment, referred to as malalignment, negatively affects load distribution. Improper load distribution reduces the knee joint's ability to accommodate physiological forces which may cause damage to the articular cartilage.

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Cartilage lesions are one of the most challenging pathologies to manage successfully. When conservative treatment fails to relieve symptoms and recover functional limitations, surgery is usually recommended to treat both the cartilage defect and any underlying anatomic abnormalities. Despite these lesions being technically easily accessible, the analysis of concomitant pathologies is difficult; therefore, a rational approach to systematically evaluate and identify pathologic deviation of the knee alignment is required to plan specific treatment that addresses each pathologic component.

#### Imaging

Radiographic exams are the first step to evaluate knee alignment. A standard knee series includes a weight-bearing anteroposterior (AP) view in full extension, a posterioranterior view in flexion (PA Rosenberg), full-length hip-toankle alignment radiograph, true lateral view, and axial view with  $45^{\circ}$  or  $30^{\circ}$  of flexion.

Standard weight-bearing AP and Rosenberg views allow evaluation of femorotibial pathology. A standing hip-to-ankle alignment radiograph is the most accurate method to evaluate mechanical axis of the lower extremity. In a neutrally aligned knee, it is defined as a line from the center of the femoral head to the center of the ankle joint, passing across the center of the knee joint. By definition, if the line is offcenter at the knee toward the lateral compartment, it is valgus alignment, and if toward the medial compartment, it is varus alignment (Fig. [3.1\)](#page-2-0).

True lateral view with superposition of both femoral condyles is usually taken with an angle of flexion of 20°. This incidence allows evaluation of tibial slope, patellar height (Insall-Salvati; Caton-Deschamps; Blackburne-Peel), patellar tilt, and trochlear morphology (Dejour classification).

Low flexion axial radiograph allows assessment of trochlea and patella morphology and the position of the patella relative to the trochlea. The difficulty with this technique is that images are not taken near full extension where the troch<span id="page-2-0"></span>Figure 3.1 A long-length radiograph showing valgus alignment on the right and neutral alignment on the left



lea is most shallow. As the knee flexes, the trochlear groove deepens, and the patella slides medially, becoming more congruent with the femoral sulcus. Hence, trochlear dysplasia, patellar tilt, or subluxation are underestimated on the axial view due to the flexion required to obtain this incidence.

Computed tomography (CT) exam provides valuable information regarding the anatomy and kinematics of the knee joint, mainly the patellofemoral joint (PFJ). Allowing a true axial view of the PFJ, this exam can image in different degrees of flexion, letting one accurately define the anatomy

and relationship between the patella and the femoral trochlea. Another important contribution of CT is the ability to create overlapping images, allowing assessment of torsional deformities, such as femoral anteversion (FA) and external tibial torsion, as well as measurements of tibial tubercletrochlear groove (TT-TG) and/or tibial tubercle-posterior cruciate ligament (TT-PCL) distance.

Magnetic resonance imaging (MRI) is the most complete imaging technique. This exam allows for the simultaneous evaluation of all the structures that constitute the knee joint, distinguishing the different tissues. MRI exams can better evaluate articular morphology as well as meniscal and ligament tearing, chondral and osteochondral lesions, rotational deformities, and patellar alignment.

Table [3.1](#page-4-0) summarizes clinical exams and imaging studies used to evaluate patellofemoral joint disorders and underlying comorbidities.

#### Tibiofemoral Alignment and Cartilage Lesions

During a normal gait, knee reaction forces reach three times the body weight, increasing to six times the body weight during higher activity levels. In a normally aligned knee, approximately 60% of the weight-bearing force is transmitted through the medial compartment, the adduction moment being the primary contributing factor to an increased medial joint reaction force [\[1](#page-12-0)]. Biomechanical studies have demonstrated that varus and valgus alignment increase medial and lateral load, respectively [\[2](#page-12-1), [3](#page-12-2)]. Accordingly, malalignment has been recognized as an independent risk factor for development and progression of knee osteoarthritis (OA) [[4,](#page-12-3) [5](#page-12-4)]. After 18 months of follow-up, a valgus-aligned knee was five times more likely to present progression of lateral compartment OA compared with knees of neutral alignment; similarly, a varus-aligned knee increases risk of medial OA progression by a factor of 4.

	<b>Clinical exam/imaging</b>	
<b>Consideration</b>	study	<b>Objective evaluation</b>
Coronal alignment	Valgus and varus alignment	Inspection on physical examination, mechanical axis view radiograph
Axial alignment	External tibial torsion increased femoral neck anteversion	Thigh-foot angle; CT or MRI version study hip/ knee/ankle
	Lateralized patellar force vector	Q angle; CT or MRI measurement of TT-TG and TT-PCL
		Patellar tilt
Sagittal alignment	Increased patellar height	True lateral with loading flexion radiographic, CT or MRI measurement of patella alta (Insall-Salvati, Caton-Deschamps, or Blackburne-Peel ratio)
	Tibial slope	True lateral view radiographic, CT or MRI
morphology	Patellofemoral Trochlear dysplasia	Radiographic crossing sign, trochlear boss, CT/ MRI findings (Dejour classification)

<span id="page-4-0"></span>Table 3.1 Preoperative considerations for cartilage restoration

#### Patellofemoral Alignment and Cartilage Lesions

Clinically, extensor mechanism alignment can be assessed measuring Q angle. Described as the direction of the quadriceps force and the patellar tendon reaction force, this angle determines the lateral vector of the extensor mechanism force. Despite the widely discussed potential for inaccuracy of the clinical measurement of the Q angle, a theoretical understanding of the influence of extensor mechanism alignment is crucial to comprehend the influence of anatomical abnormalities on patellofemoral contact forces.

Patellofemoral malalignment is a complex pathology with a wide spectrum of clinical presentation. Several features can influence the Q angle and, consequently, the PF reaction forces. No single factor may be the sole defining etiology, as patellofemoral malalignment is most frequently the result of an association of anatomic abnormalities. Therefore, a global understanding of the pathology is crucial to tailor the most suitable approach in each case.

# Coronal Alignment

Both valgus and varus alignment may contribute to modification of the contact stresses in the PFJ [\[6](#page-12-5), [7\]](#page-12-6). Valgus alignment increases the Q angle, which leads to an increment increase in the lateral vector of the quadriceps force, thereby overloading the lateral side of the PFJ. Conversely, varus alignment tends to reduce the Q angle, shifting the quadriceps force medially, therefore, increasing the contact stress on the medial side of the PFJ [[8\]](#page-12-7). Cahue et al. prospectively showed that valgus alignment was associated with lateral PF OA progression; likewise, varus alignment increased the risk for medial PF OA progression [[9\]](#page-12-8).

# Axial Alignment

Evaluation of the patellofemoral alignment in the axial plane can be challenging and should be evaluated carefully to understand the true source of abnormality. The tibial tubercletrochlear groove (TT-TG) distance is one of the most used parameters for the measurement of patellofemoral alignment, being largely correlated with O angle [[10,](#page-13-0) [11\]](#page-13-1). This measurement assesses the mediolateral distance between the center of the patellar tendon insertion at the tibial tubercle and the deepest point of the trochlear groove (Fig. [3.2](#page-6-0)). The TT-TG

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Figure 3.2 TT-TG measurement. Images from the trochlear groove and tibial tubercle are superimposed. Trochlear groove location is determined at the level where the posterior cortex of the femoral condyles is well defined. The trochlear line is drawn perpendicular to the posterior condylar axis, tangential to the posterior femoral condyles (dFCL), and passing through the deepest point of the trochlear groove (TG). Tibial tubercle image is selected at the level of the most anterior point of the tibial tuberosity. A line crossing through the center of the tibial tubercle (TT) is drawn perpendicular to the posterior femoral axis. The distance between these two parallel lines is the TT-TG distance. (Copyright © 2012 American Orthopaedic Society for Sports Medicine. Reprinted from Seitlinger et al. [\[15](#page-13-3)] with permission from SAGE publications)

distance can be measured with ease using both MRI and CT; however, the values resultant from these two techniques may not be interchangeable. Due to discrepancies in knee flexion during image acquisition, MRI exams tend to underestimate the TT-TG distance when compared with CT and should be taken into consideration during surgical planning [[12](#page-13-2)].

Traditionally, a TT-TG distance of greater than 20 mm is considered pathologic, representing an excessive lateral position of the TT in relation to the trochlea, and has been accepted as the threshold for recommendation of distal realignment [[13\]](#page-13-4). However, a large TT-TG must be interpreted carefully. Other conditions such as trochlear dysplasia, distal femoral internal rotation, or tibial external rotation may lead to increased TT-TG distance; each should be evaluated to determine the site of potential treatment [\[14](#page-13-5), [15\]](#page-13-3). Tensho et al., compared the influence of trochlea medialization, tibial tubercle lateralization, and knee rotation, and found that knee rotation is the most important factor influencing TT-TG distance [[16\]](#page-13-6).

Tibial tubercle-posterior cruciate ligament (TT-PCL) distance was introduced as an adjunct measurement to evaluate the TT position [[15](#page-13-3)]. This parameter is assessed by measuring the distance between the medial margin of the PCL and the midpoint of the TT at the level of the patellar tendon attachment (Fig. [3.3\)](#page-8-0), normal values being less than 24 mm. As it is referenced to the tibia, this parameter is independent of trochlear morphology and femoral rotation. Therefore, femoral rotation abnormalities should be investigated in patients with a TT-TG distance more than 20 mm and normal TT-PCL distance.

The Q angle is also influenced by the rotational interaction between the femur and tibia. Lateral rotation of the tibia in relation to the femur moves the tibial tubercle (TT) laterally, resulting in an increase in the Q angle [\[17,](#page-13-7) [18\]](#page-13-8). Similarly, increased femoral anteversion leads to internal rotation of the distal femur, moving the patella medially, thereby, increasing the Q angle [\[19](#page-13-9), [20\]](#page-14-0).

During normal gait, the knee joint axis rotates externally, in relation to the pelvis, during the swing phase, and moves internally during the stance phase. The increment of the femoral anteversion leads to an abnormal internally rotated gait. While the body is moving forward, the knee joint axis is pointing medially. This leads to an increased internal rotation of the knee joint axis during stance phase, causing excessive lateral forces on the patella. This excessive lateralization increases tension on the MPFL and pressure on the lateral side of the patellofemoral joint while unloading the medial side. Hence, increased FA

<span id="page-8-0"></span>

Figure 3.3 TT-PCL measurement. Proximal tibia (below the joint and above the head of the fibula) and patellar tendon insertion (most inferior slice in which the ligament could still be clearly identified) images are superimposed. The TT-PCL distance is the mediolateral distance between the medial border of the posterior cruciate ligament (PCL) and the center of the insertion of the patellar tendon. Both lines are drawn perpendicular to a posterior tibial condyles reference line (dTCL), tangential to the proximal tibia below the joint and above the head of the fibula. (Copyright © 2012 American Orthopaedic Society for Sports Medicine. Reprinted from Seitlinger et al. [\[15](#page-13-3)] with permission from SAGE publications)

results in abnormal lateral patellofemoral pressure and the tendency for lateral subluxation.

Several techniques have been described to assess rotational alignment of the inferior limb. Femoral, tibial, and knee torsion can be assessed by overlapping axial cuts from the femoral head, base of the femoral neck or lesser trochanter, the knee joint (either tangent to the posterior condyles or between the medial and lateral epicondyles), the proximal tibia at the joint, and the ankle joint. Either CT or MRI studies can provide similar measurements. Femoral anteversion can be measured by drawing a line from the center of the

femoral neck to the femoral head and distally either along the transepicondylar axis (mean value 7.4°) or the tangent of the posterior femoral condyles (mean value 13.1°). These values differ by about 6°, with a range of 11° of retroversion to 22° of anteversion (Fig. [3.4\)](#page-9-0) [\[21](#page-14-1)].

Numerous studies have highlighted the importance of tibial torsion on patellar tracking [[17](#page-13-7), [22\]](#page-14-2). There is no consensus concerning the measurement techniques to determine the tibial torsion. Thus, the lack of a standardized method to measure tibial torsion is a major stumbling block to determining a pathologic threshold for this abnormality. Both MRI and CT studies have been demonstrated as reliable reproducible methods to assess tibial torsion [\[23](#page-14-3), [24\]](#page-14-4). The measurement is taken from two superimposed axial images: one of the proximal tibial epiphysis right above the proximal end of the fibula and the other tangent to the talar dome. This is the angle between the line tangent to the posterior tibial plateau rim and the bimalleolar axis as drawn through the centers of the anteroposterior aspect of the lateral and medial malleoli [\[24](#page-14-4), [25](#page-14-5)].

<span id="page-9-0"></span>

Figure. 3.4 Femoral neck anteversion (FNA) measurement using transepicondylar axis. (**a**) Orange line demonstrates femoral neck axis, connecting the center of the femoral head and the center of the femoral neck. (**b**) Yellow line shows transepicondylar axis, connecting the medial and lateral epicondyles

Biomechanical studies have shown the influence of both tibial and femoral rotation on patellofemoral contact pressure. Lee et al. demonstrated that increased external tibial rotation resulted in a lateral shift of the patella, thus increasing the pressure on the lateral facet  $[17]$ . A comparison of patients with chronic patellofemoral symptoms and asymptomatic controls showed that symptomatic patients presented significant increased external tibial torsion compared to controls [\[22](#page-14-2)]. Moreover, a biomechanical study analyzing PF contact pressures demonstrated that if a torsional and an angular deformity coexist, the rotatory component causes greater PF changes [\[26](#page-14-6)]. Takai et al. have evaluated femoral and tibial torsion in patients with unicompartmental PF arthrosis and demonstrated the high correlation between PF arthrosis and increased femoral anteversion (23° of femoral anteversion in the PF OA group versus 9° of anteversion in the control group) [[27\]](#page-14-7). Similarly, Lerat has found an increased risk for patellar chondropathy in patients with increased internal femoral torsion [[28\]](#page-14-8).

Patellar tilt and subluxation are additional factors that indicate PF malalignment and have been associated with deterioration of PF cartilage laterally. Patellar position can be easily assessed using axial radiographs or axial images from MRI or CT; however, the source of this incongruence is multifactorial and requires a deeper evaluation. In addition to the rotational deviation described earlier, a laxity or weakness of medial soft tissue restraints, such as the MPFL and vastus medialis, and/or a lateral tethering lead to an overload of the lateral facet. In this case, physical evaluation demonstrates a decrease in medial-lateral patellar translation.

#### Sagittal Alignment

The position of the patella in the sagittal axis is an additional factor influencing patellofemoral tracking. Essentially, patella alta or infera must be evaluated using an identified index. The main indexes currently used in the literature are Insall-Salvati, Caton-Deschamps, and Blackburne-Peel. All imaging techniques (lateral view radiographs, MRI, and CT) have demonstrated reliable and reproducible methods for measurement and can be interchangeable when assessing patellar height [\[29\]](#page-14-9). Mehl et al., in a case control study comparing patients with cartilage defects and normal controls, found that 67% of patients with a chondral lesion showed a pathologic Insall-Salvati index of >1.2, while this ratio was only 25.6% of the control group [\[30\]](#page-14-10). Additionally, an observational study of patients with osteoarthritis showed a significant association between patellar alignment and cartilage loss in both lateral and medial sides [[31](#page-15-0)].

# Patellofemoral Geometry

In addition to patellofemoral alignment, but no less significant, the contour of the trochlea and the patella is an important contributor to the patellofemoral contact force and consequently a risk factor for patellofemoral cartilage lesions. The geometry of the trochlea has been recognized as a risk factor for the development of cartilage lesions of the PF joint. Several studies have correlated patellofemoral cartilage loss with flat or shallow trochlea [\[31](#page-15-0)[–33](#page-15-1)]. Historically, trochlea morphology was mainly assessed using axial radiography or CT using bone landmarks. However, bone reference may not reproduce the articular cartilage surface, and investigation with MRI is advisable [[34\]](#page-15-2).

# Summary

In conclusion, identification and correction of underlying abnormal patellofemoral alignment is crucial for successful cartilage repair in the patellofemoral joint. Patients with fullthickness cartilage defects of the patella frequently demonstrate a high number of co-pathologies in association. Therefore, these pathologies must be identified accurately and considered carefully when planning surgical treatment of patellofemoral cartilage defects.

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