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 Positron emission tomography (PET) has a key role in the management of patients with focal epilepsy as a well-established, functional imaging modality. Especially among various PET agents to evaluate brain function,  $^{18}F$ -fluorodeoxyglucose (FDG) has been widely used because it reflects neuronal activity and allows quantification of cerebral glucose metabolism using tracer kinetic modeling. In the management of patients with medically intractable epilepsy, FDG PET became a routine process to localize epileptogenic foci, particularly in cases of patients presenting with normal anatomic structures on magnetic resonance imaging (MRI). Recently, this pivotal role of FDG PET in presurgical evaluation had been challenged by high-quality MRI $[1]$ .

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 Despite this trend, the role of PET as a functional imaging modality in the management of patients with epilepsy seems secure in terms of both demonstrating the epileptogenic zones and better understanding of the neurobiology of epilepsy. FDG PET could provide useful information to localize the epileptogenic focus even in patients with medically intractable focal epilepsy who have unremarkable MRI scans  $[1]$ . To investigate neurochemistry, which is considered crucial in epileptogenesis and spread of epileptic activities, several PET tracers have been introduced and actively explored its feasibility in clinical practice [2]. Moreover, the introduction of an epochmaking experimental tool, a dedicated small animal PET scanner and animal model for epilepsy, has accelerated investigations to unveil secrets of epilepsy.

# **FDG PET**

 Surgical interventions would be an accepted treatment option to effectively alleviate seizures in approximately 20–30% of the patients with focal epilepsy who became resistant to antiepileptic drugs  $[3, 4]$ . Although the success rates of surgical interventions in patients with temporal lobe epilepsies reach almost  $85\%$  [5–8], those rates decrease 50% to 60% in patients with cortical origin epilepsies  $[9, 10]$ . In this regard, careful selection of eligible patients and precise localization of the epileptogenic zones are imperative to achieve

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	Pathology $(\%)$	Surgical outcome $(\%)$
<b>MRI</b>	72	77
$^{18}$ F-FDG PET	85	86
<b>Ictal SPECT</b>	73	78

Table 12.1 Correct localization of MRI, 18F-FDG PET, and ictal SPECT

(Modified from reference 12.15)

a seizure-free outcome and minimize side effects related with unsuccessful surgery, and thus meticulous presurgical evaluations including scalp electroencephalography (EEG) and various imaging studies are required.

 FDG PET, as a noninvasive evaluation tool, has been reported to have high sensitivities with 60–90% in lateralizing temporal lobe epilepsy  $(TLE)$  [11]. On interictal FDG PET, the epileptogenic focus is usually seen as a hypometabolic area, which is considered to be seizure-related changes in the brain. The pathophysiologic basis of the hypometabolism remains elusive, but it has been suggested that the hypometabolism in the hippocampus may reflect the hippocampal neuronal loss, a histopathologic hallmark of medial temporal sclerosis [12].

 In regard to the diagnostic performance of various imaging methods to localize the epileptogenic foci, sensitivities were varied between medial temporal lobe epilepsy and neocortical epilepsies  $[13]$ . The diagnostic performance for extratemporal neocortical epilepsy is not particularly high. Recently, the introduction of nuclear imaging analysis methods such as statistical parametric mapping (SPM) helped the localization of the epileptogenic foci with improved sensitivities  $[13]$ . In a previous study using SPM, we investigated the diagnostic performance of FDG PET in pediatric patients with TLE, and the introduction of SPM was found to be helpful for the localization of the epileptogenic zones  $[14]$ .

 The sensitivity of FDG PET was compared in a head-to-head fashion with MRI or ictal singlephoton emission computed tomography (SPECT) using <sup>99m</sup>Tc-hexamethylpropyleneamine oxime (HMPAO) or ethylene cysteinate dimer [15] (Table 12.1). Among 118 patients who were operated on for medial temporal and neocortical epilepsies and were followed up for more than one year, the sensitivity of FDG PET was 85 %.

## **Diagnostic Performance of FDG PET in Medial Temporal Lobe Epilepsy**

 Medial temporal lobe epilepsy is well known for its pathologic diagnostic criteria of hippocampal sclerosis and/or atrophy. These hippocampal changes are easily found by the recent generation MRI machines. Both the quantitative and the qualitative MRI interpretation give similar diagnostic effectiveness for TLE with the MRI machines. In cases of hipppocampal changes clearly identified on MRI, FDG PET reveals equally well the epileptogenic zones in medial temporal lobe epilepsy (Fig. 12.1a).

 The advanced equipment and acquisition methods such as 3-T MRI have increased the sensitivity of localization of epileptogenic zones. However, despite these advancements, MRI reveals no significant anatomic structures in the 20–25% of the patients with medically intractable epilepsy  $[16]$ . For those patients, FDG PET could provide useful data for lateralizing the lesion as well as the desirable location for an invasive scalp EEG recording. The use of FDG PET is reported to be cost effective, especially in patients with unremarkable MRI scans [11].

 In brief, FDG PET is helpful mainly for three types of medial TLE. The first type is represented by patients with ambiguous sclerosis (Fig. 12.1b). In a few patients with medial TLE, hippocampal sclerosis is not prominent even on MRI with the most recent techniques. The 3-T MRI with fluidattenuated inversion recovery (FLAIR) and multiple channel coils could identify relevant abnormalities only in 20% of patients with previously unremarkable MRI scans [1]. The second type is of bilateral sclerosis and/or atrophy  $(Fig. 12.1c)$  $(Fig. 12.1c)$  $(Fig. 12.1c)$ . Quite a few confusing cases have been filed among 600 fully investigated epilepsy patients at our institution. The third type is represented by those patients with inherently normal MRI findings (Fig. 12.1d). FDG PET and ictal SPECT were found to be similarly effective at localizing epileptogenic zones in nonlesional (MRI-negative) medial temporal lobe epilepsy [17].

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 **Fig. 12.1** Selected axial FDG PET images of lower brain for medial temporal lobe epilepsy. (a) A typical matching case with hippocampal atrophy and hypometabolism with decreased uptake of  ${}^{18}$ F-FDG (\*) in the left temporal lobe. (b) A case with ambiguous ictal EEG but with definite hypometabolism with decreased activity (\*) in the right

# **Diagnostic Performance of FDG PET in Neocortical Epilepsy**

 About one third to one half of medically intractable patients have neocortical epilepsy [18–20]. Neocortical epilepsy consists of lateral temporal, frontal, occipital, and parietal lobe epilepsy, in decreasing order of prevalence [19]. Neocortical epilepsy poses two types of problems in localization of epileptogenic zones. The first is that if MRI shows multiple candidate foci of the epileptogenic zones, it cannot be verified which is the culprit lesion for the seizure generation. The second is that if MRI does not show any structural lesion, that is to say, when the lesion is 'cryptogenic', it is difficult to determine where to apply

temporal lobe. (c) An example of bilateral hippocampal atrophy on MRI but unilateral hypometabolism (\*) in the right temporal lobe. (**d**) A nonlesional cryptogenic case on MRI but with mild hypometabolism (\*) in the right temporal lobe. All four patients underwent surgery with outcomes of Engel class 1

subdural grids and strips to find the seizure focus during subdural EEG studies. In such cases, FDG PET is helpful in providing useful information on the virtual location of subdural electrodes to find the epileptogenic zone. FDG PET can at least lateralize cryptogenic lesions, although it cannot localize a lesion.

According to our previous study  $[21]$ , positive predictive value of FDG PET in cryptogenic epilepsy is over 70%. Localization rates are different for various epileptogenic lobes. Lateral temporal lobe or frontal lobe epilepsies are relatively easy to diagnose among complex partial seizure patients. In frontal lobe epilepsy, the sensitivity of FDG PET was 36% in patients without structural lesions on MRI and 73% in patients with



**Fig. 12.2** A case with cryptogenic frontal lobe epilepsy. Selected axial T2-weighted, MR image of the brain was normal, and ictal EEG also was nonlocalizing. Selected axial FDG PET showed images of the head, definitive

hypometabolism with decreased uptake of <sup>18</sup>F-FDG (\*) in left frontal lobe. After successful frontal lobectomy, the patient became seizure-free

structural lesions in frontal lobe epilepsy [22]. In nonlesional cryptogenic cases, epileptogenic zones yield similar decreased metabolism to the lesions in explicit cases with subdural lesions (Fig. 12.2 ).

 On the contrary, it is not easy to localize epileptogenic zones in occipital lobe epilepsy  $[23]$ . Areas showing the most severe hypometabolism are limited to the occipital lobes in some patients (Fig. [12.3 \)](#page-4-0), however, they are not limited in others. In those other cases, the areas of highest perfusion were also not limited to occipital lobes on ictal SPECT. The hypometabolism was localized even to the ipsilateral temporal lobes in a few patients (Fig. [12.4](#page-4-0)). Epileptogenic zones could have been misdiagnosed for temporal lobes in those patients. As for the occipital lobe epilepsy, the localization rate was found to be 47% by MRI and  $60\%$  by PET  $[23]$ . In such confusing cases of occipital lobe epilepsy, the examination of visual symptoms and visual field is mandatory  $[23]$ .

## **Comparison of Interictal FDG PET with Interictal Perfusion SPECT**

 The diagnostic performance of interictal SPECT for localization of epileptogenic zones is somewhat

disappointingly low as compared with that of interictal PET. The sensitivity of interictal perfusion SPECT was 44% on average by a meta-analysis  $[5]$ , and 34% in our cohort study including both temporal and neocortical epilepsy cases. The sensitivities of interictal PET have been reported to be improved over those of interictal SPECT  $(73-97%)$  [24-[26](#page-11-0)].

 Considering the dogma of metabolism and perfusion coupling in the brain, it is important to figure out the significance of, or the reason for, this discrepancy in the sensitivities of the two functional imaging modalities representing metabolism and perfusion. The reason why interictal FDG PET is excellent but interictal SPECT is poor for the localization of epileptogenic zones could be explained as follows.

Among greater than 300 patients, we identified 14 patients with increased perfusion in the zones that was determined to be epileptogenic by surgical outcome or invasive studies  $[27]$ . Four of those were patients in whom interictal SPECT was performed on the second day after ictal episode. The other four patients, seemingly hyperperfused, were studied on the third to fifth day after ictus (Fig.  $12.5a$ , b). This means that the interictal SPECT was in fact not performed at the interictal phase. Subclinical seizure activity just

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 **Fig. 12.3** Cases of occipital lobe epilepsy. Selected T2-weighted axial MR image of the brain (a) was normal, but metabolism with <sup>18</sup>F-FDG was decreased in the right occipital lobe epilepsy (\*) on the axial image of the head (**b**).



 **Fig. 12.4** Regional prevalence if interictal hypometabolism on <sup>18</sup>F-FDG PET in occipital lobe epilepsy. Occipital lobe is the most common site of hypometabolism

In another case, the MR image (c) was normal, but perfusion with <sup>99m</sup>Tc HMPAO was increased in the left occipital lobe (\*) on ictal SPECT of the head (d). Both patients became seizure-free after neocortical resection

prior to or during interictal studies might have resulted in this increased perfusion at the epileptogenic zones.

 On the other hand, 'delayed postictal perfusion abnormalities', even long after the previous ictus, could have resulted in the increased perfusion  $[28]$ . During the delayed postictal period at 6 h after ictal SPECT, we found remnant hyperperfusion in one half of patients (Fig.  $12.5c-e$ ). In one patient, severe hypoperfusion was found on delayed postictal SPECT, but showed recovery on interictal SPECT. Based on these findings, we suggest that even with EEG monitoring to

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**Fig. 12.5** Hyperperfusion on interictal SPECT using 99mTc HMPAO and delayed postictal hyperperfusion after ictus. In a patient with surgically confirmed right temporal lobe epilepsy, on the fourth day after ictal study (a), axial images of the head taken on interictal SPECT (**b**) showed similar increased perfusion in the right temporal lobe (\*)

prove that there is no ictal discharge during interictal SPECT, it cannot be verified that the 'true' interictal SPECT has been obtained.

### **Voxel-Based Analysis of FDG PET**

 SPM is a voxel-based approach for determining the significantly different area from normal controls (Fig. [12.6](#page-6-0) ). After spatially transforming and smoothing the individual PET data using the general linear model, the voxel count of the individual patient is compared with those of the normal controls. This analysis method is a very robust analytic tool to compare statistically abnormal cerebral perfusion with normal controls  $[22, 29, 30]$ .

Interestingly, SPM analysis of <sup>15</sup>O-water PET, FDG PET, and <sup>99m</sup>Tc-HMPAO interictal SPECT revealed that in the same patients the areas of hypoperfusion were mostly concordant with but smaller

and crossed cerebellar hyperperfusion (+). In the other patient with right temporal lobe epilepsy, perfusion was increased in the right temporal lobe (\*) on ictal SPECT ( **c** ) and also on 6-h delayed SPECT (d). On interictal SPECT (e), perfusion was relatively decreased in this temporal lobe (\*)

than the areas of hypometabolism (Fig.  $12.7$ ) [31]. This apparent uncoupling of perfusion and metabolism in epileptogenic zones is another reason why interictal perfusion SPECT is inferior to interictal FDG PET in localizing epileptogenic zones.

 On SPM analysis in frontal lobe epilepsy, using an uncorrected probability value of 0.005 as the threshold, the sensitivity of SPM analysis reached that of visual assessment. Sensitivity is decreasing as stricter thresholds are chosen to find abnormal area of decreased perfusion (Fig. [12.8](#page-7-0) ).

# **Quantification Using Automatic Volume of Interest on Population-Based Atlas**

 This method is structured on population-based standard anatomy, which was developed by the Montreal Neurological Institute and named SPAM (Fig. 12.9). SPAM, an acronym for "statistical

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**Fig. 12.6** SPM analysis results of <sup>18</sup>F-FDG PET and <sup>15</sup>O-water PET superimposed on MRI. Activities are the voxels that differ from the normal controls. In a coupled case, the left temporal lobe (\*) was found to have hypometabolic voxels on axial FDG PET images (**a**) and hypoperfused voxels

on water PET (**b**). In an uncoupled case, the right temporal lobe (\*) was found to have hypometabolic voxels on FDG PET axial images (c), however, there was no area of hypoperfusion on water PET (**d**)



Fig. 12.7 Number of hypoperfused voxels and hypometabolic voxels on <sup>15</sup>O-water PET and <sup>18</sup>F-FDG PET in the epileptogenic temporal lobes. Each data point represents voxel number per epileptogenic whole temporal lobe per patient. Numbers of hypometabolic voxels tended to be much greater than those of hypoperfused voxels

probabilistic anatomic map," differs from SPM. SPM is a voxel-based approach, whereas SPAM is an area-based approach. SPAM is an objective and operator-independent method of volume of interest (VOI) drawing. We have a populationaveraged anatomic definition of gyri and lobes in MRI template format. To construct SPAM, the Montreal group collected, parceled, and segmented normal MR images from 152 young subjects. Original PET images are transformed to an MRI template and the voxel counts are multiplied by the probabilities obtained from the SPAM template. For example, if the right hippocampus is chosen, the resulting image shows the probabilities of each voxel belonging to the right hippocampus. This method was first used to objectively quantify the asymmetric index, and these asymmetric indices could be used to localize epileptogenic zones on FDG PET [31].

 The methods to use SPAM for evaluation of extent and severity of hypometabolism on FDG

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*p* = corrected 0.1

 **Fig. 12.8** Example of SPM analysis with varying threshold. According to cutoff value of voxel height, SPM analysis became less sensitive when stricter criterion was

 **Fig. 12.9** SPAM)as an objective VOI) in PET image processing. Frontal and parietal (*left*) as well as temporal and occipital (*right*) lobes were displayed on the MRI template. These SPAM masks can be used as a VOI on the MRI template

applied. Sensitivity decreases according to the decrease in probability value



PET in the epileptogenic zones are depicted in Fig. [12.10 .](#page-8-0) The relation of hypometabolism and surgical prognosis of medial temporal lobe epilepsy could be evaluated. By successful application of SPAM to six gyri of temporal lobes, this analysis revealed that focal severity and extent were not related to the surgical outcome in medial temporal lobe epilepsy [32].

## **Prognostic Values of FDG PET in Surgical Interventions**

 The prognostic values of FDG PET in presurgical evaluations have been investigated both in TLE and neocortical epilepsies. The focal hypometabolism on presurgical FDG PET are known to have a significant correlation with postoperative

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**Fig. 12.10** Assessment of severity and extent of hypometabolism. Asymmetric indexes were calculated on six pairs of VOIs to represent the temporal lobe significant regional hypometabolism was estimated by comparing the

seizure-free outcomes  $[33, 34]$ . By a meta-analysis dealing with predictive diagnostic values of FDG PET in TLE patients, unilateral temporal lobe hypometabolism could predict a good surgical outcome in 86% of patients, and in 80% of patients with normal MRI [35]. Although MRI itself is strongly predictive of surgical outcome in TLE [33], FDG PET seems to have a comparably high predictive value and even to achieve clinical benefit in the patients with suspected TLE and normal MRI. In addition, presurgical FDG PET is sure to be cost effective for localization of epileptogenic zones, especially if its use is restricted to the evaluation of patients in whom MRI and scalp EEG do not provide a definitive answer  $[11]$ .

 In neocortical epilepsies, surgical outcomes as well as localization rates of epileptogenic zones were lower than those of TLE. However, according to our previous study, the localizing values of FDG PET and interictal EEG were well correlated with a seizure-free outcome, and the positive predictive value of FDG PET was 63% in patients with cryptogenic neocortical epilepsy [36].

PET images with those of controls by using SPM. The extent of hypometabolic area for each VOI was determined by counting the number of voxels with significantly decreased hypometabolism in each VOI segmented

## **Beyond FDG PET in Epilepsy**

 In vivo neurochemistry, considered to be responsible for neuronal modulation, has had much attention in the past decades with the hope of revealing the pathophysiology of epilepsy. In particular, γ-aminobutyric acid (GABA), a major inhibitory neurotransmitter that plays a major role in regulating neuronal excitability throughout the central nervous system, is supposed to play the key role in epilepsy  $[37]$ . Besides the GABAergic system, other neurotransmitters such as serotoninergic, dopaminergic systems have also been suggested to have a significant pathophysiologic role in the epileptic brain. In this regard, PET agents for GABAergic, serotoninergic, dopaminergic systems, etc. have been actively investigated to evaluate the involvement of theses neurotransmitters in vivo.

PET with  ${}^{11}$ C-flumazenil (FMZ), which binds to  $GABA<sub>A</sub>$  receptor, has been widely used to investigate the status of GABAergic system in TLE patients. On FMZ PET, epileptogenic zones  **Fig. 12.11** PET scans using radiotracers other than FDG in patients with focal epilepcies. Epileptogenic focus in the right temporal lobe showed relatively decreased glucose metabolism and reduced FMZ uptake (a: Modified from Ref. [38]). Epileptogenic focus, proved to be cortical dysplasia later on histology, showed no abnormal glucose metabolism, but increased AMT uptake in the right frontal cortex (**b**: Modified from Ref.  $[45]$ 



**FDG PET** 

**AMT PET** 

show decreased FMZ uptake as compared with the contralateral homotopic reference region and the remaining neocortex  $(Fig. 12.11a)$   $[38]$ . However, careful interpretation is needed for the abnormalities on FMZ PET because decreased FMZ uptake could be seen not only in the epileptogenic zone but also in the remote area. Several hypostheses including a secondary epileptogenesis model, multifocal cortical dysplasia, and underlying pathology associated with increased susceptibility to seizures have been suggested to explain the presence of the multiple decreased FMZ sites remote from the epileptogenic zones [39]. Recently, a novel <sup>18</sup>F-labeled PET agent  $(^{18}F$ -flurorflumazenil) binding to GABA  $_{\wedge}$  receptor was reported and expected to facilitate the use of FMZ PET in clinical practice  $[40]$ .

 To evaluate the serotonergic system, PET agents for serotonin metabolism or serotonin receptor have been developed. <sup>11</sup>C-alpha-methyl tryptophan (AMT), an analog of tryptophan, reflects serotonin synthesis in vivo or induction of the kynurenine pathway  $[41, 42]$ . AMT PET has been suggested to be useful to localize epileptogenic zones in cortical malformations (Fig.  $12.11b$ ) [43-45]. Increased cortical AMT uptake was most sensitive in children with tuberous sclerosis  $[43]$ . For the evaluation of the serotonin receptor status,  $^{18}$ F-MPPF, an antagonist of the  $5HT_{14}$  receptor, has been investigated in patients with focal epilepsies. A recent study reported that MPPF PET could lateralize an epileptogenic lobe with a sensitivity of 90%, and proved its usefulness in the presurgical evaluation of TLE patients  $[46]$ .

 The pathophysiologic role of the dopaminergic system in the epileptic brain is not yet clearly understood. Recently, the striatal dopaminergic system became an important target for both basic and clinical research because it was reported to play a key role in modulation of seizure activity in animal studies  $[47]$ . To characterize the striatal dopaminergic system in vivo, <sup>18</sup>F-fallypride, a high-affinity dopamine  $D_2/D_3$ -receptor antagonist, has been actively used in animal studies as well as in the clinical setting. With the introduction <span id="page-10-0"></span>of dedicated PET scanner for small animals, new PET agents for in vivo neurochemistry are expected to make advances in the understanding of the pathophysiology of epilepsy.

## **Conclusion**

 FDG PET is helpful in localizing epileptogenic zones, especially in patients with nonlesional epilepsy on MRI. Quantitative methods such as SPM and SPAM are believed to have the ability to enhance the objectivity of the analysis to find epileptogenic zones by revealing hypometabolic areas. In the near future, various PET agents other than FDG could be utilized to unveil the nature of the epilepsy.

## **References**

- 1. Duncan J. The current status of neuroimaging for epilepsy. Curr Opin Neurol. 2009;22(2):179–84.
- 2. la Fougère C, Rominger A, Förster S, Geisler J, Bartenstein P. PET and SPECT in epilepsy: a critical review. Epilepsy Behav. 2009;15:50–5.
- 3. Kwan P, Brodie MJ. Early identification of refractory epilepsy. N Engl J Med. 2000;342(5):314–9.
- 4. Engel Jr J, Wiebe S, French J. The quality standards subcommittee of the American Academy of Neurology; American Epilepsy Society; American Association of Neurological Surgeons. Practice parameter: temporal lobe and localized neocortical resections for epilepsy: report of the quality standards subcommittee of the American Academy of Neurology, in association with the American Epilepsy Society and the American Association of Neurological Surgeons. Neurology. 2003;60(4):538–47.
- 5. Devous Sr MD, Thisted RA, Morgan GF, Leroy RF, Rowe CC. SPECT brain imaging in epilepsy: a metaanalysis. J Nucl Med. 1998;39(2):285–93.
- 6. Wiebe S, Blume WT, Girvin JP, et al. A randomized, controlled trial of surgery for temporal-lobe epilepsy. N Engl J Med. 2001;345:311–8.
- 7. Schramm J, Kral T, Grunwald T, et al. Surgical treatment for neocortical temporal lobe epilepsy: clinical and surgical aspects and seizure outcome. J Neurosurg. 2001;94:33–42.
- 8. Foldvary N, Nashold B, Mascha E, et al. Seizure outcome after temporal lobectomy for temporal lobe epilepsy: a Kaplan-Meier survival analysis. Neurology. 2000;54:630–4.
- 9. Engel Jr J. Surgery for seizures. N Engl J Med. 1996;334(10):647–52.
- 10. Duchowny M, Jayakar P, Resnick T, et al. Epilepsy surgery in the first three years of life. Epilepsia. 1998;39(7):737–43.
- 11. O'Brien TJ, Miles K, Ware R, Cook MJ, Binns DS, Hicks RJ. The cost-effective use of <sup>18</sup>F-FDG PET in the presurgical evaluation of medically refractory focal epilepsy. J Nucl Med. 2008;49(6):931–7.
- 12. O'Brien TJ, Jupp B. In-vivo imaging with small animal FDG-PET: a tool to unlock the secrets of epileptogenesis? Exp Neurol. 2009;220(1):1–4.
- 13. Spencer SS, Theodore WH, Berkovic SF. Clinical applications: MRI, SPECT, and PET. Magn Reson Imaging. 1995;13(8):1119–24.
- 14. Lee JJ, Kang WJ, Lee DS, et al. Diagnostic performance of <sup>18</sup>F-FDG PET and ictal <sup>99m</sup>Tc-HMPAO SPET in pediatric temporal lobe epilepsy: uantitative analysis by statistical parametric mapping, statistical probabilistic anatomical map, and subtraction ictal SPET. Seizure. 2005;14(3):213–20.
- 15. Won HJ, Chang KH, Cheon JE, et al. Comparison of MR imaging with PET and ictal SPECT in 118 patients with intractable epilepsy. AJNR Am J Neuroradiol. 1999;20(4):593–9.
- 16. Lehéricy S, Semah F, Hasboun D, et al. Temporal lobe epilepsy with varying severity: MRI study of 222 patients. Neuroradiology. 1997;39(11):788–96.
- 17. Son YJ, Chung CK, Lee SK, et al. Comparison of localizing values of various diagnostic tests in nonlesional medial temporal lobe epilepsy. Seizure. 1999;8:465–70.
- 18. Nam H, Lee SK, Chung CK, et al. Incidence and clinical profile of extra-medial-temporal epilepsy with hippocampal atrophy. J Korean Med Sci. 2001;16:95–102.
- 19. Kutsy RL. Focal extratemporal epilepsy: clinical features, EEG patterns, and surgical approach. J Neurol Sci. 1999;166:1–15.
- 20. Zentner J, Hufnagel A, Ostertun B, et al. Surgical treatment of extratemporal epilepsy: clinical, radiologic, and histopathologic findings in 60 patients. Epilepsia. 1996;37:1072–80.
- 21. Lee DS, Lee SK, Chung J-K, et al. Predictive values of F-18 FDG-PET and ictal SPECT to find epileptogenic zones in cryptogenic neocortical epilepsies (Abstract). J Nucl Med. 1997;38:272.
- 22. Kim YK, Lee DS, Lee SK, et al. F-18 FDG-PET in localization of frontal lobe epilepsy: comparison of visual and SPM analysis. J Nucl Med. 2002;43:1167–74.
- 23. Kim SK, Lee DS, Lee SK, et al. Diagnostic performance of  $[^{18}F]$ -FDG-PET and ictal  $[^{99m}Tc]$ -HMPAO SPECT in occipital lobe epilepsy. Epilepsia. 2001;42:1531–40.
- 24. Spanaki MV, Spencer SS, Corsi M, et al. Sensitivity and specificity of quantitative difference SPECT analysis in seizure localization. J Nucl Med. 1999;40(5):730–6.
- 25. Weil S, Noachtar S, Arnold S, Yousry TA, Winkler PA, Tatsch K. Ictal ECD-SPECT differentiates

<span id="page-11-0"></span>between temporal and extratemporal epilepsy: confirmation by excellent postoperative seizure control. Nucl Med Commun. 2001;22(2):233–7.

- 26. Zaknun JJ, Bal C, Maes A, et al. Comparative analysis of MR imaging, ictal SPECT and EEG in temporal lobe epilepsy: a prospective IAEA multi-center study. Eur J Nucl Med Mol Imaging. 2008;35(1):107–15.
- 27. Lee DS, Kim SK, Lee SK, et al. Frequencies and implications of discordant findings of interictal SPECT and ictal SPECT in patients with intractable epilepsy (Abstract). Eur J Nucl Med. 1997;24:983.
- 28. Lee DS, Lee SK, Kim SK, et al. Late postictal residual perfusion abnormality in epileptogenic zone found on 6-hour postictal SPECT. Neurology. 2000;55:835–41.
- 29. Signorini M, Paulesu E, Friston K, et al. Rapid assessment of regional cerebral metabolic abnormalities in single subjects with quantitative and nonquantitative F-18 FDG-PET: a clinical validation of statistical parametric mapping. Neuroimage. 1999;9:63–80.
- 30. Van Bogaert P, Massager N, Tugendhaft P, et al. Statistical parametric mapping of regional glucose metabolism in mesial temporal lobe epilepsy. Neuroimage. 2000;12:129–38.
- 31. Kang KW, Lee DS, Cho JH, et al. Quantification of F-18 FDG-PET images in temporal lobe epilepsy patients using probabilistic brain atlas. Neuroimage. 2001;14:1–6.
- 32. Lee SK, Lee DS, Yeo JS, et al. FDG-PET images quantified by probabilistic atlas of brain and surgical prognosis of temporal lobe epilepsy. Epilepsia. 2002;43:1032–8.
- 33. Vinton AB, Carne R, Hicks RJ, et al. The extent of resection of FDG-PET hypometabolism relates to outcome of temporal lobectomy. Brain. 2007;130: 548–60.
- 34. O'Brien TJ, Hicks RJ, Ware R, Binns DS, Murphy M, Cook MJ. The utility of a 3-dimensional, large-fieldof-view, sodium iodide crystal-based PET scanner in the presurgical evaluation of partial epilepsy. J Nucl Med. 2001;42(8):1158–65.
- 35. Willmann O, Wennberg R, May T, Woermann FG, Pohlmann-Eden B. The contribution of <sup>18</sup>F-FDG PET in preoperative epilepsy surgery evaluation for patients with temporal lobe epilepsy a meta-analysis. Seizure. 2007;16(6):509–20.
- 36. Lee SK, Lee SY, Kim KK, Hong KS, Lee DS, Chung CK. Surgical outcome and prognostic factors of cryptogenic neocortical epilepsy. Ann Neurol. 2005;58(4): 525–32.
- 37. Treiman DM. GABAergic mechanisms in epilepsy. Epilepsia. 2001;42(Suppl 3):8–12.
- 38. Ryvlin P, Bouvard S, Le Bars D, et al. Clinical utility of flumazenil-PET versus [<sup>18</sup>F] fluorodeoxyglucose-PET and MRI in refractory partial epilepsy: a prospective study in 100 patients. Brain. 1998;121:2067–81.
- 39. Juhász C, Asano E, Shah A, et al. Focal decreases of cortical GABA, recpetor binding remote from the primary seizure focus:what do they indicate? Epilepsia. 2009;50(2):240–50.
- 40. Chang YS, Jeong JM, Yoon YH, et al. Biological properties of 2'-[<sup>18</sup>F]fluoroflumazenil for central benzodiazepine receptor imaging. Nucl Med Biol. 2005;32(3):263–8.
- 41. Diksic M, Nagahiro S, Sourkes TL, Yamamoto YL. A new method to measure brain serotonin synthesis in vivo. I. Theory and basic data for a biological model. J Cereb Blood Flow Metab. 1990;10(1):1–12.
- 42. Chugani DC, Muzik O. Alpha[C-11]methyl-L-tryptophan PET maps brain serotonin synthesis and kynurenine pathway metabolism. J Cereb Blood Flow Metab. 2000;20(1):2–9.
- 43. Chugani DC, Chugani HT, Muzik O, et al. Imaging epileptogenic tubers in children with tuberous sclerosis complex using alpha-[<sup>11</sup>C]methyl-L-tryptophan positron emission tomography. Ann Neurol. 1998;44(6):858–66.
- 44. Fedi M, Reutens D, Okazawa H, et al. Localizing value of alpha-methyl-L-tryptophan PET in intractable epilepsy of neocortical origin. Neurology. 2001;57(9):1629–36.
- 45. Juhász C, Chugani DC, Muzik O, et al. Alpha-methyl-L-tryptophan PET detects epileptogenic cortex in children with intractable epilepsy. Neurology. 2003;60:960–8.
- 46. Didelot A, Ryvlin P, Lothe A, Merlet I, Hammers A, Mauguière F. PET imaging of brain  $5-HT<sub>IA</sub>$  receptors in the preoperative evaluation of temporal lobe epilepsy. Brain. 2008;131:2751–64.
- 47. Starr MS. The role of dopamine in epilepsy. Synapse. 1996;22(2):159–94.