

Mechanisms of Calcification in Aortic Valve Disease: Role of Mechanokinetics and Mechanodynamics

W. David Merryman · Frederick J. Schoen

Published online: 24 March 2013
© Springer Science+Business Media New York 2013

Abstract The aortic valve is highly responsive to cyclical and continuous mechanical forces, at the macroscopic and cellular levels. In this report, we delineate *mechanokinetics* (effects of mechanical inputs on the cells) and *mechanodynamics* (effects of cells and pathologic processes on the mechanics) of the aortic valve, with a particular focus on how mechanical inputs synergize with the inflammatory cytokine and other biomolecular signaling to contribute to the process of aortic valve calcification.

Keywords Calcific aortic valve disease · Calcification · Mechanobiology · Mechanokinetics · Mechanodynamics

Introduction

Aortic valve (AV) disease is a leading cause of cardiovascular morbidity in the USA and the developed world [1], and will likely increase in prevalence as life expectancy continues to rise in coming decades [2]. Biomechanical forces imposed during each cardiac cycle play a role in both the progression and the consequences of AV disease. In this Report, we borrow terms from the pharmacology literature to delineate AV *mechanokinetics* (how mechanical forces affect the valve cells and tissue) from AV *mechanodynamics*

(how valve cells and resultant pathologic processes in the tissue affect the mechanics), to provide a snapshot of the key evolving concepts related to the biomechanical influences on the causes and consequences of calcific aortic valve stenosis and potential strategies to prevent the implicated mechanobiologic pathways. Although the emphasis will be on recently published science, technology and conceptual analysis, limited older work will be included when pertinent and necessary to provide context.

AV Structure-Function: Cells, Matrix, and Whole Valve Dynamics in Health

The AV, situated at the junction of the left ventricle and the aorta, provides the check valve for blood leaving the heart for the systemic circulation. Because of high peripheral resistance that causes a substantial diastolic back pressure on the valve in the closed position, the AV exists in high-demand mechanical environment that requires a specialized architecture. The AV is made up of 3 equal sized leaflets or cusps that are shaped like half moons, hence the name ‘semi-lunar’ valve. Each cusp is a few hundred microns thick and is made up of 3 layers: fibrosa (near the aortic side), spongiosa, and ventricularis (near the ventricular side). Valvular structural specializations and tissue dynamics have been described in detail in several recent reviews [3•, 4•]. Valve function is enabled by a complex, highly differentiated, and highly responsive (both mechanically and biologically), dynamic tissue macro- and micro-structure, consisting of a layered architectural pattern composed of cells (valvular endothelial cells [VECs] at the blood-contacting surfaces and deep valvular interstitial cells [VICs]) and extracellular matrix (ECM) (including collagen, elastin, and glycosaminoglycans [GAGs]). The fibrosa layer close to the outflow surface is the principal load-bearing layer and is enriched in type I collagen, which is highly aligned and

This article is part of the Topical Collection on *Valvular Heart Disease*

W. D. Merryman (✉)
Department of Biomedical Engineering, Vanderbilt University,
2213 Garland Ave, 9445 MRB IV,
Nashville, TN 37232-0493, USA
e-mail: david.merryman@vanderbilt.edu

F. J. Schoen (✉)
Department of Pathology, Brigham and Women’s Hospital
Harvard Medical School, 75 Francis Street,
Boston, MA 02115, USA
e-mail: fschoen@partners.org

imparts specific and anisotropic (ie, different in the radial and circumferential directions) biomechanical responses [4•, 5]. The central layer (the spongiosa) is made up primarily of loose connective tissue rich in GAGs; this layer has been hypothesized to provide cushioning and lubrication between the 2 outer layers [6]. The layer facing the ventricular chamber (the ventricularis) is rich in elastin, which is believed to provide some recoil that assists cuspal closure [7].

The single layer of VECs lining the cuspal surfaces are distinct from endothelial cells that populate the inner surfaces of the aorta [8–11], and those covering the fibrosa have a different gene expression profile from those covering the ventricularis [12]. VECs may contribute to the regulation of valve calcification. Indeed, VECs covering the fibrosa have upregulated proteins expected to promote calcification, while VECs subjected to the ventricular hemodynamic waveform (ie, experienced in vivo by the VEC lining the ventricularis) have increased expression of the “atheroprotective” transcription factor Kruppel-like factor2 (KLF2) [13], expected to downregulate calcification.

In contrast, VICs comprise a heterogeneous collection of cells with variable and dynamic features characteristics of fibroblasts, smooth muscle cells, and myofibroblasts [3•, 14]. In the normal AV, most VICs exhibit a fibroblast-like phenotype. However, when VICs are subjected to certain biomechanical or biochemical stimuli, they become activated, demonstrating a myofibroblast phenotype, with contractile features and increased protein synthesis [15, 16]. Furthermore, under certain stimuli, VICs assume a phenotype that resembles that of osteoblasts (see below). ECM architecture and VIC phenotype are dynamic not only in response to altered environmental conditions, but also throughout in-utero maturation, growth and adulthood, and disease [17]. Relevant to the present discussion, aged valves have markedly decreased VIC cell density. Indeed, VIC cell density of aged adult valves is only approximately 10 % that of fetal valves [17]. Additionally, collagen fibers become progressively more aligned with age (ie, more characteristic of a diastolic configuration) suggesting that there is an ongoing “creep” of aortic valve structure during adult life, consistent with the progressive stiffening of valve cusps with increasing age [18, 19].

AV Mechanokinetics Leading to Calcification: Role of Interstitial Cell Plasticity in AV Pathobiology

Most recent work in AV disease has focused on *mechanokinetics*, or how mechanical forces alter cellular function. The mechanical environment of the cusps can directly affect VIC differentiation [3•, 14, 20]; mechanical forces relevant to the valve function are shear stress from passing blood, buckling stresses during opening and closing, and planar stress when valve is closed [4•]. These

forces are effectively translated from the structural proteins of the valvular ECM to the cells as demonstrated by differences in VIC phenotype for the left-sided (aortic) and right-sided (pulmonary) semilunar valves [21]. Multiple studies have probed the effect of planar stress on VIC phenotype and function, primarily in the form of applied strain via in vitro bioreactors [22–24, 25•]. Studies have also examined the role of shear stress on VEC function and also studies of VEC-VIC communication [26, 27].

The hallmark of calcific aortic valve disease is the formation of nodules of calcific minerals (largely calcium phosphate, similar to the hydroxyapatite of bone) in the affected valvular tissue, and generally beginning in and most severely in the fibrosa [28], with frequent formation of bone within the calcific deposits (called osseous metaplasia) [29]. VICs associated with these calcific nodules exhibit an osteoblast-like phenotype and express extracellular bone matrix proteins. The cellular mechanisms involved in valvular calcific nodule morphogenesis are important and highly controversial; the current understanding is summarized in the recent publication from the NHLBI Aortic Stenosis Working Group on calcific aortic valve disease [30•].

Two hypotheses of calcific nodule morphogenesis from the resident VIC population dominate current thinking: the apoptotic/dystrophic calcification theory and the ossification theory (Fig. 1) [31, 32•]. Evidence suggests that these 2 approaches comprise a range of responses of VICs to biomechanical and biochemical stimulation and are not mutually exclusive. The apoptotic/dystrophic calcification theory describes a calcification mechanism in which cell injury is an important and early event. This mechanism is epitomized by the failure of bioprosthetic heart valves, in which calcification is initiated primarily within residual porcine aortic

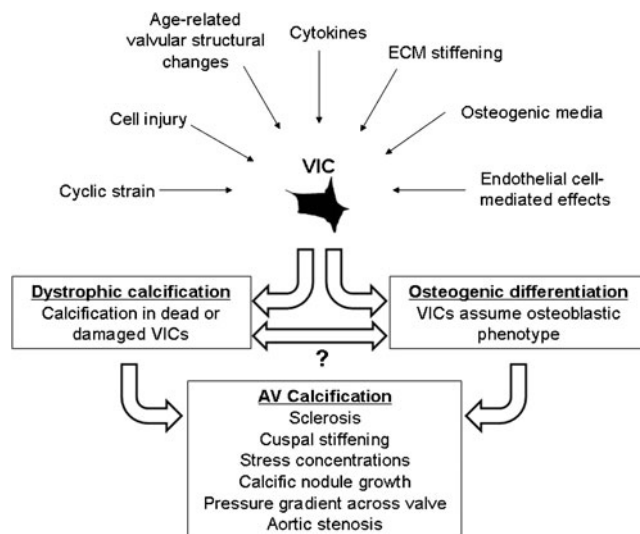


Fig. 1 Current hypotheses of aortic valve calcification mechanisms involving VICs. It is unclear if these pathways are mutually exclusive or if they are overlapping, and to what extent

valve or bovine pericardial cells that have been devitalized by glutaraldehyde pretreatment [3•, 33]. The key event involves reaction of calcium-containing extracellular fluid with the phosphorus-containing membranes of the non-functional cells, which are incapable of excluding calcium ions. Calcification of dead or damaged cells is called dystrophic calcification, and is considered a passive phenomenon. Calcification is accelerated by young valve recipient age and increased mechanical stress. In calcific AV disease, the increased mechanical stress on resident VICs induced by aging-related valvular remodeling and other mechanical and biochemical processes could play an important role in cell injury [3•, 30•]. The cytokine transforming growth factor- β 1 (TGF- β 1) induces rapid dystrophic calcification in vitro through an apoptosis mediated process [34–37]. Conversely, bone morphogenetic proteins 2 and 4 (BMP-2 and BMP-4) are potent osteogenic morphogens that are associated with the ossification theory, which specifies regulated osteogenic differentiation of VICs rather than cell injury as the key event, and thus an active calcification process [32•, 38–41]. It is unclear if these calcification processes either can occur independent of one another yet concurrently, or if they are somehow linked or interdependent, or if they are mutually exclusive. Moreover, there is debate on whether VICs can attain osteoblastic function directly or only by progressing through a myofibroblast phenotype first [42]. Rodriguez et al. found that the core of nodules contain different types of mineralization as well as apoptotic cells [43]. Also, Chen et al. described ossifying nodules that did not contain apoptotic cells, noting that different types of nodules may be forming [44]. It is evident that a more detailed description and understanding of the mechanisms of calcific nodule morphogenesis are needed, and further investigation of the behavior of VICs and their interactions (such as cell-cell tension) in nodule formation is essential in clarifying the mechanisms involved.

This notion of cell-cell tension and cell-ECM interactions implicates a key role for mechanics in calcification, and there is synergism between the cytokines mentioned above and mechanical inputs, which complicates the debate of dystrophic calcification vs ossification even further. While the complex effects of cytokines on VIC proliferation, repair, and injury have been explored [45, 46•, 47, 48], mechanokinetic studies of calcific nodule formation are in their infancy. In vitro studies have found clear dependence of VIC phenotype and/or calcific nodule formation on substrate chemistry [50, 51], substrate stiffness [32•, 52], and applied strain [37, 53], similar to the seminal work that describes the mechano-dependent differentiation of stem cells [49]. The majority of these studies focus on dystrophic calcification as a result of substrate chemistry or strain; however, Yip et al. successfully generated calcific nodules without apoptosis by culturing VICs on substrates of low stiffness [32•]. The model developed in this study is the only in vitro model available for generating ossific nodules.

AV Mechanodynamics Following Calcification: What do we Know About Stenosis Mechanisms?

Calcification, regardless of the mechanism by which it arises, restricts the motion of the leaflets, causing sclerosis (defined as early calcification without significant pressure gradient across the valve) and ultimately stenosis (with a significant pressure gradient). In addition, early calcification is likely to lead to increased mechanical loading on the non-calcified portion of the leaflet, which could initiate calcification in these regions via the mechanisms described above. This theory is supported by clinical observations in patients who are diagnosed with AV sclerosis by echocardiography or computed tomographic imaging, estimated to be approximately 25 % of patients at age 65 [54]. Moreover, AV sclerosis is associated with an approximately 50 % increased risk of myocardial infarction and cardiac death over 5 years, probably primarily because AV sclerosis serves as a marker for coronary artery atherosclerosis. Once even mild valve obstruction is present, progression to AV stenosis is virtually inevitable, sometimes occurring in as little as 4–8 years after initial diagnosis [55], although progression is variable among patients. Once a nidus of sclerosis emerges within a leaflet, the stiffening of the leaflet follows, likely due to ‘strain magnification’ experienced by the surrounding, initially healthy, tissue (as described mathematically in [37]). Briefly, if the leaflets were a supple, highly compliant sheet (like latex), then a focal area that becomes stiff would in turn lead to greater than normal (ie, concentrated) strain in the region directly outside of the focal area. If strain leads to mechanobiologic changes to the VICs, then this strain magnification would proceed to change the VICs in a ripple effect emanating from the focal area. Over a few years, the ripple effect alters the leaflet properties and decreases compliance, likely leading to stenosis. An initial attempt at a computational model of the gross progression of disease has been published [56].

Congenital bicuspid aortic valve (BAV), the most frequent gross developmental cardiovascular malformation in humans, has an increased propensity to calcification and stenosis. BAV is usually uncomplicated in early life but frequently eventuates in calcific aortic stenosis or regurgitation in later life [57]. The vulnerability of BAV to calcification is so great that although the prevalence of BAV is (only) approximately 1 % in the overall population, congenital BAV is the anatomic substrate in approximately half of adults who have surgery for calcific aortic stenosis. In addition, calcification of a BAV occurs approximately a decade earlier in these patients than in those who have an anatomically normal valve. The mechanistic basis for the propensity for accelerated calcification of a BAV is uncertain. Nevertheless, in a finite element model, bicuspid valve geometry presented much higher stresses compared with the tricuspid model, particularly in the central basal region of the conjoint cusp (+800 %) [57]. However, another

computational model has suggested that the cellular deformations are not significantly different in the 2 geometries in the calcification-prone region [58]. Interestingly, not only have mutations in the transcriptional regulator NOTCH1 been linked to human developmental valve abnormalities but also NOTCH1 signaling represses osteoblast-like calcification pathways [59, 60].

Quadricuspid aortic valves also occur, and calcific stenosis is unusual, although data are limited. Clinical and pathologic studies suggest that 1 %–2 % of surgically removed aortic valves are quadricuspid and that regurgitation is the predominant pathology [61, 62]. Whether there is a biomechanical reason accounting for the specific pathologic profile of quadricuspid valves is unknown.

Novel Mechanobiological Strategies to Prevent Calcification

While the specific mechanisms of calcification remain unclear, the clinical investigation of drugs and heart valve disease in the past 15 years has been both hopeful and cautionary. The hopeful story has been that lipid-lowering drugs (ie, statins) would prevent valve disease [63, 64], in a similar fashion to their effectiveness against atherosclerosis. In 2001, 2 retrospective observational clinical studies suggested that statins may inhibit progression of AV stenosis [65, 66]. However, prospective, randomized clinical studies appeared much less promising. A small double-blind, placebo controlled study showed no benefit of statins to reduce valve disease and a larger clinical study demonstrated, rather conclusively, that statins do not reduce major cardiovascular outcomes, including AV replacement, in patients with existing AV stenosis [67]. A more recent meta-analysis of 2,344 patients from previous trials shows that statins do not prevent the progression of AV stenosis [68]. In light of these findings, the enthusiasm for statin therapy as a potential preventive treatment for valve disease has been severely dampened. It is possible, however, that statins initiated earlier in the natural history of valve calcification might slow or prevent disease, but this is a very difficult hypothesis to test. Recent *in vitro* data demonstrated that C-type natriuretic peptide prevents myofibroblast differentiation of VICs and was also found to be upregulated by Simvastatin [69], suggesting a mechanism by which benefit could accrue from statins. A very recent report found that single nucleotide polymorphisms in the lipoprotein(a) locus was highly correlated with AV calcification and was across all patient populations examined [70]. Therefore, statin therapy may be more effective in patients with these polymorphisms.

One of the present authors (WDM) recently found 2 distinct pathways that may be selectively targeted to prevent calcification of VICs. First, the serotonin 2B receptor, which was implicated in the drug-induced valve disease [71] that

occurred with Fen-Phen, pergolide, and cabergoline, can be antagonized to prevent non-canonical TGF- β 1 signaling and calcification *in vitro* [72]. Targeting of the serotonin 2B receptor is similar to the much more focused on angiotensin receptors for treatment of valve disease [73]. Jaffre et al. [74] demonstrated that the serotonin 2B receptor works in concert with the angiotensin II type 1 receptor, to mediate hypertrophic signaling in cardiac fibroblasts. Angiotensin II demonstrates a mechano-dependent signaling activation during ventricular pressure overload similar to that noted above for serotonin 2B, and increased angiotensin II signaling at the type 1 receptor results in an increase in TGF- β 1 secretion and the subsequent downstream initiation of fibrosis. In the aforementioned study, Jaffre et al. conclusively demonstrated a necessary interdependence between serotonin 2B and angiotensin II type 1 receptors in regulating TGF- β 1 secretion. Many of the cardiac-related studies into the molecular signaling pathways of the 2 receptors have focused on their role in ventricular fibroblasts. This strategy needs to be further examined in small animal models of valve disease, but selective targeting strategy combined with the clear arrest of TGF- β 1 effects appears promising.

Second, the homophilic cadherin, cadherin-11, was found to be required for TGF- β 1-induced calcific nodule formation *in vitro* [75]. Because cadherin-11 is involved in bone formation, this provides a plausible common pathway between the ossific and dystrophic calcification pathways, and targeting cadherin-11 with functional blocking antibodies may be an additional strategy in preventing calcification. As the mechanism(s) becomes clear, there may be additional novel mechanobiologic targets that may prevent pathologic differentiation of VICs that leads to calcification.

Conclusions

There is still much to be examined in the mechanokinetics and mechanodynamics of heart valve calcification; however, in the past few years, there has been success in elucidating the early inflammatory mechanisms and potential intervention strategies to prevent these processes. A major challenge is relating *in vitro* findings to clinical directives through early detection of calcification. We believe that as mechanisms are better understood in the coming years, a molecular signature of early, pre-calcification that can be imaged *in vivo* may be possible. Further, if inflammatory processes in the VICs can be targeted and halted it may be possible to develop a non-surgical intervention strategy against calcific heart valve disease.

Acknowledgments W. David Merryman has received funding from NIH, AHA, NSF, and the Wallace H. Coulter Foundation.

Conflict of Interest W. David Merryman declares that he has no conflict of interest.

Frederick J. Schoen declares that he has no conflict of interest.

References

Papers of particular interest, published recently, have been highlighted as:

- Of importance
- Of major importance

1. Roger VL, Go AS, Lloyd-Jones DM, Benjamin EJ, Berry JD, Borden WB, et al. Heart disease and stroke statistics—2012 update: a report from the American Heart Association. *Circulation*. 2012;125:e2–e220.
2. Taking care: ethical caregiving in our aging society. The President's Council on Bioethics. 2005;309.
3. •• Schoen FJ. Mechanisms of function and disease of natural and replacement heart valves. *Annu Rev Pathol*. 2012;7:161–83. *An up-to-date review of valve function and mechanisms of disease in pathologic native and replacement tissue valves.*
4. •• Sacks MS, Merryman WD, Schmidt DE. On the biomechanics of heart valve function. *J Biomech*. 2009;42:1804–24. *Comprehensive review of heart valve biomechanics.*
5. Merryman WD. Mechano-potential etiologies of aortic valve disease. *J Biomech*. 2010;43:87–92.
6. Stephens EH, Chu CK, Grande-Allen KJ. Valve proteoglycan content and glycosaminoglycan fine structure are unique to microstructure, mechanical load, and age: Relevance to an age-specific tissue-engineered heart valve. *Acta Biomater*. 2008;4:1148–60.
7. Schoen F. Aortic valve structure-function correlations: role of elastic fibers no longer a stretch of the imagination. *J Heart Valve Dis*. 1997;6:1–6.
8. Butcher JT, Nerem RM. Porcine aortic valve interstitial cells in 3-dimensional culture: comparison of phenotype with aortic smooth muscle cells. *J Heart Valve Dis*. 2004;13:478–85.
9. Butcher JT, Nerem RM. Valvular endothelial cells and the mechanoregulation of valvular pathology. *Philos Trans R Soc Lond B Biol Sci*. 2007;362:1445–57.
10. Butcher JT, Penrod AM, Garcia AJ, Nerem RM. Unique morphology and focal adhesion development of valvular endothelial cells in static and fluid flow environments. *Arterioscler Thromb Vasc Biol*. 2004;24:1429–34.
11. Young EW, Wheeler AR, Simmons CA. Matrix-dependent adhesion of vascular and valvular endothelial cells in microfluidic channels. *Lab Chip*. 2007;7:1759–66.
12. Simmons CA, Grant GR, Manduchi E, Davies PF. Spatial heterogeneity of endothelial phenotypes correlates with side-specific vulnerability to calcification in normal porcine aortic valves. *Circ Res*. 2005;96:792–9.
13. Weinberg EJ, Mack PJ, Schoen FJ, Garcia-Cardena G, Kaazempur Mofrad MR. Hemodynamic environments from opposing sides of human aortic valve leaflets evoke distinct endothelial phenotypes in vitro. *Cardiovasc Eng*. 2010;10:5–11.
14. Liu AC, Joag VR, Gotlieb AI. The emerging role of valve interstitial cell phenotypes in regulating heart valve pathobiology. *Am J Pathol*. 2007;171:1407–18.
15. Taylor PM, Batten P, Brand NJ, Thomas PS, Yacoub MH. The cardiac valve interstitial cell. *Int J Biochem Cell Biol*. 2003;35:113–8.
16. Hinz B. The myofibroblast: paradigm for a mechanically active cell. *J Biomech*. 2010;43:146–55.
17. Aikawa E, Whittaker P, Farber M, Mendelson K, Padera RF, Aikawa M, et al. Human semilunar cardiac valve remodeling by activated cells from fetus to adult: implications for postnatal adaptation, pathology, and tissue engineering. *Circulation*. 2006;113:1344–52.
18. Christie GW, Barratt-Boyes BG. Age-dependent changes in the radial stretch of human aortic valve leaflets determined by biaxial stretching. *Ann Thorac Surg*. 1995;60:S156–9.
19. Stephens EH, de Jonge N, McNeill MP, Durst CA, Grande-Allen KJ. Age-related changes in material behavior of porcine mitral and aortic valves and correlation to matrix composition. *Tissue Eng Part A*. 2010;16:867–78.
20. Wyss K, Yip CY, Mirzaei Z, Jin X, Chen JH, Simmons CA. The elastic properties of valve interstitial cells undergoing pathological differentiation. *J Biomech*. 2012;45:882–7.
21. Merryman WD, Youn I, Lukoff HD, Krueger PM, Guilak F, Hopkins RA, et al. Correlation between heart valve interstitial cell stiffness and transvalvular pressure: implications for collagen biosynthesis. *Am J Physiol Heart Circ Physiol*. 2006;290:H224–31.
22. Merryman WD, Lukoff HD, Long RA, Engelmayr Jr GC, Hopkins RA, Sacks MS. Synergistic effects of cyclic tension and transforming growth factor-beta1 on the aortic valve myofibroblast. *Cardiovasc Pathol*. 2007;16:268–76.
23. Balachandran K, Konduri S, Sucusky P, Jo H, Yoganathan AP. An ex vivo study of the biological properties of porcine aortic valves in response to circumferential cyclic stretch. *Ann Biomed Eng*. 2006;34:1655–65.
24. Balachandran K, Sucusky P, Jo H, Yoganathan AP. Elevated cyclic stretch alters matrix remodeling in aortic valve cusps: implications for degenerative aortic valve disease. *Am J Physiol Heart Circ Physiol*. 2009;296:H756–64.
25. •• Balachandran K, Sucusky P, Jo H, Yoganathan AP. Elevated cyclic stretch induces aortic valve calcification in a bone morphogenic protein-dependent manner. *Am J Pathol*. 2010;177:49–57. *Bioreactor (ex vivo) study utilizing porcine AVs where calcification required TGF-β1, added to osteogenic media but not due to osteogenic media.*
26. Butcher JT, Nerem RM. Valvular endothelial cells regulate the phenotype of interstitial cells in co-culture: effects of steady shear stress. *Tissue Eng*. 2006;12:905–15.
27. El-Hamamsy I, Balachandran K, Yacoub MH, Stevens LM, Sarathchandra P, Taylor PM, et al. Endothelium-dependent regulation of the mechanical properties of aortic valve cusps. *J Am Coll Cardiol*. 2009;53:1448–55.
28. Schoen FJ, Mitchell RN. The heart. In: Kumar V, Fausto N, Aster JC, Abbas A, editors. *Robbins/cotran pathologic basis of disease*. 8th ed. Philadelphia: W.B. Saunders; 2010. p. 529–87.
29. Mohler III ER, Chawla MK, Chang AW, Vyavahare N, Levy RJ, Graham L, et al. Identification and characterization of calcifying valve cells from human and canine aortic valves. *J Heart Valve Dis*. 1999;8:254–60.
30. •• Rajamannan NM, Evans FJ, Aikawa E, Grande-Allen KJ, Demer LL, Heistad DD, et al. Calcific aortic valve disease: not simply a degenerative process: a review and agenda for research from the National Heart and Lung and Blood Institute Aortic Stenosis Working Group. *Circulation*. 2011;124:1783–91. *An important assessment by a multi-disciplinary expert panel of the current understanding of AV disease mechanisms and future research needs.*
31. Gu X, Masters KS. Role of the Rho pathway in regulating valvular interstitial cell phenotype and nodule formation. *Am J Physiol Heart Circ Physiol*. 2011;300:H488–58.
32. •• Yip CY, Chen JH, Zhao R, Simmons CA. Calcification by valve interstitial cells is regulated by the stiffness of the extracellular matrix. *Arterioscler Thromb Vasc Biol*. 2009;29:936–42. *Describes the only model currently available to generate ossific nodules in vitro.*

33. Schoen FJ, Levy RJ. Calcification of tissue heart valve substitutes: progress toward understanding and prevention. *Ann Thorac Surg.* 2005;79:1072–80.
34. Clark-Greuel JN, Connolly JM, Sorichillo E, Narula NR, Rapoport HS, Mohler III ER, et al. Transforming growth factor-beta1 mechanisms in aortic valve calcification: increased alkaline phosphatase and related events. *Ann Thorac Surg.* 2007;83:946–53.
35. Jian B, Narula N, Li QY, Mohler III ER, Levy RJ. Progression of aortic valve stenosis: TGF-beta1 is present in calcified aortic valve cusps and promotes aortic valve interstitial cell calcification via apoptosis. *Ann Thorac Surg.* 2003;75:457–65. discussion 65–6.
36. Proudfoot D, Skepper JN, Hegyi L, Bennett MR, Shanahan CM, Weissberg PL. Apoptosis regulates human vascular calcification in vitro: evidence for initiation of vascular calcification by apoptotic bodies. *Circ Res.* 2000;87:1055–62.
37. Fisher CI, Chen J, Merryman WD. Calcific nodule morphogenesis by heart valve interstitial cells is strain dependent. *Biomech Model Mechanobiol.* 2013;12:5–17.
38. David V, Martin A, Lafage-Proust MH, Malaval L, Peyroche S, Jones DB, et al. Mechanical loading down-regulates peroxisome proliferator-activated receptor gamma in bone marrow stromal cells and favors osteoblastogenesis at the expense of adipogenesis. *Endocrinology.* 2007;148:2553–62.
39. de Gorter DJ, van Dinther M, Korchynski O, Ten Dijke P. Biphasic effects of transforming growth factor-beta on bone morphogenetic protein-induced osteoblast differentiation. *J Bone Miner Res.* 2011;26:1178–87.
40. Hanson AD, Marvel SW, Bernacki SH, Banes AJ, van Aalst J, Loba EG. Osteogenic effects of rest inserted and continuous cyclic tensile strain on hASC lines with disparate osteodifferentiation capabilities. *Ann Biomed Eng.* 2009;37:955–65.
41. Lomashvili KA, Cobbs S, Hennigar RA, Hardcastle KI, O'Neill WC. Phosphate-induced vascular calcification: role of pyrophosphate and osteopontin. *J Am Soc Nephrol.* 2004;15:1392–401.
42. Monzack EL, Masters KS. Can valvular interstitial cells become true osteoblasts? A side-by-side comparison. *J Heart Valve Dis.* 2011;20:449–63.
43. Rodriguez KJ, Masters KS. Regulation of valvular interstitial cell calcification by components of the extracellular matrix. *J Biomed Mater Res A.* 2009;90:1043–53.
44. Chen JH, Yip CY, Sone ED, Simmons CA. Identification and characterization of aortic valve mesenchymal progenitor cells with robust osteogenic calcification potential. *Am J Pathol.* 2009;174:1109–19.
45. Xu S, Gotlieb AI. Wnt3a/beta-catenin increases proliferation in heart valve interstitial cells. *Cardiovasc Pathol.* 2013 (in press).
46. • Li C, Xu S, Gotlieb AI. The progression of calcific aortic valve disease through injury, cell dysfunction, and disruptive biologic and physical force feedback loops. *Cardiovasc Pathol.* 2013;22:1–8. *Excellent contemporary conceptual review of valvular interstitial cell biology in health and disease.*
47. Han L, Gotlieb AI. Fibroblast growth factor-2 promotes in vitro heart valve interstitial cell repair through the Akt1 pathway. *Cardiovasc Pathol.* 2012;21:382–9.
48. Xu S, Liu AC, Kim H, Gotlieb AI. Cell density regulates in vitro activation of heart valve interstitial cells. *Cardiovasc Pathol.* 2012;21:65–73.
49. Engler AJ, Sen S, Sweeney HL, Discher DE. Matrix elasticity directs stem cell lineage specification. *Cell.* 2006;126:677–89.
50. Benton JA, Kern HB, Anseth KS. Substrate properties influence calcification in valvular interstitial cell culture. *J Heart Valve Dis.* 2008;17:689–99.
51. Gu X, Masters KS. Regulation of valvular interstitial cell calcification by adhesive peptide sequences. *J Biomed Mater Res A.* 2010;93:1620–30.
52. Wang H, Haeger SM, Kloxin AM, Leinwand LA, Anseth KS. Redirecting valvular myofibroblasts into dormant fibroblasts through light-mediated reduction in substrate modulus. *PLoS One.* 2012;7:e39969.
53. Hutcheson JD, Venkataraman R, Baudenbacher FJ, Merryman WD. Intracellular Ca(2+) accumulation is strain-dependent and correlates with apoptosis in aortic valve fibroblasts. *J Biomech.* 2012;45:888–94.
54. • Otto CM. Calcific aortic valve disease: new concepts. *Sem Thorac Cardiovasc Surg.* 2010;22:276–84. *Excellent contemporary review of clinical issues in calcific aortic valve disease.*
55. Faggiano P, Antonini-Canterin F, Erlicher A, Romeo C, Cervesato E, Pavan D, et al. Progression of aortic valve sclerosis to aortic stenosis. *Am J Cardiol.* 2003;91:99–101.
56. Weinberg EJ, Schoen FJ, Mofrad MR. A computational model of aging and calcification in the aortic heart valve. *PLoS One.* 2009;4:e5960.
57. Conti CA, Della Corte A, Votta E, Del Viscovo L, Bancone C, De Santo LS, et al. Biomechanical implications of the congenital bicuspid aortic valve: a finite element study of aortic root function from in vivo data. *J Thorac Cardiovasc Surg.* 2010;140:890–6.
58. Weinberg EJ, Kaazempur Mofrad MR. A multiscale computational comparison of the bicuspid and tricuspid aortic valves in relation to calcific aortic stenosis. *J Biomech.* 2008;41:3482–7.
59. Garg V, Muth AN, Ransom JF, Schluterman MK, Barnes R, King IN, et al. Mutations in NOTCH1 cause aortic valve disease. *Nature.* 2005;437:270–4.
60. Nigam V, Srivastava D. Notch1 represses osteogenic pathways in aortic valve cells. *J Mol Cell Cardiol.* 2009;47:828–34.
61. Yotsumato G, Iguro Y, Kinjo T, Matsumoto H, Masuda H, Sakata R. Congenital quadricuspid aortic valve: report of 9 surgical cases. *Ann Thorac Cardiovasc Surg.* 2003;9:134–7.
62. Tang Y-F, Xu J-B, Han L, Lu F-L, Lang X-L, Song Z-G, et al. Congenital quadricuspid aortic valve: analysis of 11 surgical cases. *Ch Med J.* 2011;124:2779–81.
63. Rajamannan NM, Edwards WD, Spelsberg TC. Hypercholesterolemia aortic-valve disease. *N Engl J Med.* 2003;349:717–8.
64. Rajamannan NM, Subramaniam M, Springett M, Sebo TC, Niekrasz M, McConnell JP, et al. Atorvastatin inhibits hypercholesterolemia-induced cellular proliferation and bone matrix production in the rabbit aortic valve. *Circulation.* 2002;105:2660–5.
65. Aronow WS, Ahn C, Kronzon I, Goldman ME. Association of coronary risk factors and use of statins with progression of mild valvular aortic stenosis in older persons. *Am J Cardiol.* 2001;88:693–5.
66. Novaro GM, Tiong IY, Pearce GL, Lauer MS, Sprecher DL, Griffin BP. Effect of hydroxymethylglutaryl coenzyme a reductase inhibitors on the progression of calcific aortic stenosis. *Circulation.* 2001;104:2205–9.
67. Rossebø AB, Pedersen TR, Boman K, Brudi P, Chambers JB, Egstrup K, et al. Intensive lipid lowering with simvastatin and ezetimibe in aortic stenosis. *N Engl J Med.* 2008;359:1343–56.
68. • Teo KK, Corsi DJ, Tam JW, Dumesnil JG, Chan KL. Lipid lowering on progression of mild to moderate aortic stenosis: meta-analysis of the randomized placebo-controlled clinical trials on 2344 patients. *Can J Cardiol.* 2011;27:800–8. *Meta-analysis of primary studies summarizing the data that do not support the hypothesis that statin therapy reduces AS progression.*
69. Yip CY, Blaser MC, Mirzaei Z, Zhong X, Simmons CA. Inhibition of pathological differentiation of valvular interstitial cells by C-type natriuretic peptide. *Arterioscler Thromb Vasc Biol.* 2011;31:1881–9.
70. • Thanassoulis G, Campbell CY, Owens DS, Smith JG, Smith AV, Peloso GM, et al. Genetic associations with valvular calcification and aortic stenosis. *N Engl J Med.* 2013;368:503–12. *A genome-wide association study that identifies a single nucleotide polymorphism in the LPA locus is associated with aortic-valve calcification across multiple ethnic groups, raising the possibility that lowering Lp(a) levels might reduce the incidence or progression of aortic valve disease.*

71. Hutcheson JD, Setola V, Roth BL, Merryman WD. Serotonin receptors and heart valve disease—it was meant 2B. *Pharmacol Ther.* 2011;132:146–57.
72. • Hutcheson JD, Ryzhova LM, Setola V, Merryman WD. 5-HT (2B) antagonism arrests non-canonical TGF-beta1-induced valvular myofibroblast differentiation. *J Mol Cell Cardiol.* 2012;53:707–14. *Demonstrated that the serotonin 2B receptor could be antagonized to prevent calcification by VICs.*
73. Ngo DT, Sverdlov AL, Horowitz JD. Prevention of aortic valve stenosis: a realistic therapeutic target? *Pharmacol Ther.* 2012;135:78–93.
74. Jaffe F, Bonnin P, Callebert J, Debbabi H, Setola V, Doly S, et al. Serotonin and angiotensin receptors in cardiac fibroblasts coregulate adrenergic-dependent cardiac hypertrophy. *Circ Res.* 2009;104:113–23.
75. •• Hutcheson JD, Chen J, Sewell-Loftin MK, Ryzhova LM, Fisher CI, Su YR, et al. Cadherin-11 regulates cell-cell tension necessary for calcific nodule formation by valvular myofibroblasts. *Arterioscler Thromb Vasc Biol.* 2013;33:114–20. *Demonstrated that cadherin-11 is required for dystrophic calcification by VICs in vitro.*